

THE EFFECTS OF REFRACTIVE INDEX MISMATCH ON  
MULTIPHOTON FLUORESCENCE EXCITATION  
MICROSCOPY OF BIOLOGICAL TISSUE

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Submitted to the faculty of the University Graduate School  
in partial fulfillment of the requirements  
for the degree  
Doctor of Philosophy  
in the Program of Biomolecular Imaging and Biophysics  
Indiana University

July 2010

Accepted by the Faculty of Indiana University, in partial fulfillment of the requirements for the degree of Doctor of Philosophy.

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## ACKNOWLEDGEMENTS

I would like to thank my mentor, Dr. Ken Dunn, for teaching me how to be a scientist.

I would also like to thank the other members of my research committee: Dr. Robert Bacallao, Dr. Ricardo Decca, and Dr. Michael Rubart. Dr. Decca, thank you for the hours at the whiteboard in your office, answering the millions of emails I sent you, and your incredible patience. Dr. Bacallao, thank you for excellent advice, the off the wall questions that were always exactly relevant enough to stretch my mind but never anything I would have thought of on my own, and your fantastic jokes. Dr. Rubart, thank you for your endless support, your thoughts and advice, and your incredibly prompt replies to my emails. I would not have been able to complete this dissertation project without you.

I would like to thank Dr. Simon Atkinson, my program director, for encouraging me to join the new graduate program in Biomolecular Imaging. I would like to thank Dr. Bruce Molitoris, the director of the Indiana Center for Biological Microscopy and chairman of the Nephrology Division of the Department of Medicine, for his support and encouragement.

Additionally, I would like to thank Jason Byars for his hours of programming in an attempt to minimize my masochism. I would like to thank Sherry Clendenon, my partner in crime. I would like to thank Cliff Babbey for always listening and lending advice. I would like to thank George Rhodes for training me in animal surgery and intravital microscopy. I would like to thank Ruben Sandoval for training me and helping

me over and over again. I would like to thank Jeff Clendenon for being an endless resource of information about microscopy and image processing. I would like to thank Bruce Henry for helping me with the microscopy. I would like to thank Exing Wang for designing the excitation path on the microscope where I conducted the majority of my experiments and for training me in alignment of the system. I would like to thank Heather Ward for teaching me how to fix and store tissue samples and trying to teach me Amira.

I would also like to thank all of my friends for supporting me through graduate school, especially Sarah Wean, Nicci Knipe, Henry Mang, David Southern, Stacy Bennett, Keri Jeter, Nikki Ray, and Tabitha Hardy.

Finally, I would like to thank my family for their endless support.

This work was supported by a George M. O'Brien award from the NIH (P30 DK 079312-01) and conducted at the Indiana Center for Biological Microscopy.

## ABSTRACT

Pamela Anne Young

### THE EFFECTS OF REFRACTIVE INDEX MISMATCH ON MULTIPHOTON FLUORESCENCE EXCITATION MICROSCOPY OF BIOLOGICAL TISSUE

**Introduction:** Multiphoton fluorescence excitation microscopy (MPM) is an invaluable tool for studying processes in tissue in live animals by enabling biologists to view tissues up to hundreds of microns in depth. Unfortunately, imaging depth in MPM is limited to less than a millimeter in tissue due to spherical aberration, light scattering, and light absorption. Spherical aberration is caused by refractive index mismatch between the objective immersion medium and sample. Refractive index heterogeneities within the sample cause light scattering. We investigate the effects of refractive index mismatch on imaging depth in MPM.

**Methods:** The effects of spherical aberration on signal attenuation and resolution degradation with depth are characterized with minimal light absorption and scattering using sub-resolution microspheres mounted in test sample of agarose with varied refractive index. The effects of light scattering on signal attenuation and resolution degradation with depth are characterized using sub-resolution microspheres in kidney tissue samples mounted in optical clearing media to alter the refractive index heterogeneities within the tissue.

**Results:** The studies demonstrate that signal levels and axial resolution both rapidly decline with depth into refractive index mismatched samples. Interestingly,

studies of optical clearing with a water immersion objective show that reducing scattering increases reach even when it increases refractive index mismatch degrading axial resolution. Scattering, in the absence of spherical aberration, does not degrade axial resolution. The largest improvements in imaging depth are obtained when both scattering and refractive index mismatch are reduced.

**Conclusions:** Spherical aberration, caused by refractive index mismatch between the immersion media and sample, and scattering, caused by refractive index heterogeneity within the sample, both cause signal to rapidly attenuate with depth in MPM. Scattering, however, seems to be the predominant cause of signal attenuation with depth in kidney tissue.

Kenneth W. Dunn, Ph.D., Chair

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## LIST OF ABBREVIATIONS

AFP	Actual focal position
AOM	Acousto-optic modulator
BABB	Benzyl alcohol/benzyl benzoate
CCD	Cooled charge-coupled device
CLSM	Confocal fluorescence laser scanning microscopy
EOM	Electro-optic modulator
DMSO	Dimethyl sulfoxide
FWHM	Full width at half maximum
GaAs	Gallium arsenide
GaAsP	Gallium arsenide phosphide
GFP	Green fluorescent protein
MPM	Multiphoton fluorescence excitation microscopy
NA	Numerical aperture
Nd:YVO <sub>4</sub>	Neodymium doped yttrium orthvanadate
NFP	Nominal focal position
PBS	Phosphate buffered saline
PEG	Polyethylene glycol
PMT	Photomultiplier tube
PSF	Point spread function
RFP	Red fluorescent protein
Ti:S	Titanium sapphire

## I. INTRODUCTION

### A. *Multiphoton fluorescence excitation microscopy in biomedical research*

*In vivo* imaging techniques have become widely utilized in biology. Techniques, such as positron emission tomography (PET), single photon emission computed tomography (SPECT), and magnetic resonance imaging (MRI), are excellent for studying whole organs and tissues but have spatial and temporal resolution that are too poor to characterize cellular processes at sub-second timescales [1]. Multiphoton fluorescence excitation microscopy (MPM) enables biologists to study processes hundreds of microns in depth in tissue in live animals with submicron resolution and timescales of seconds or less [2-13]. As a fluorescence technique, MPM can be used to localize multiple specific molecules simultaneously. MPM has also been shown to have low photon toxicity, allowing extended observation of highly sensitive processes without detectable damage [14]. MPM offers biologists the capability of characterizing cellular and subcellular processes deep into tissues in three dimensions in the context of tissues and organs in living animals.

In brain tissue, the first tissue to be studied using MPM, images were collected of neurons in invertebrate ganglia, mammalian brain slices, and intact mammalian brains [15, 16]. Since then MPM has been used to study blood flow [17-20], dendritic spine behavior [21-27], calcium dynamics in dendrites [28-33] and presynaptic boutons [34-36], and microglia cell dynamics [37, 38]. The effects of plaques on dendritic structure and dendritic spines have been examined in Alzheimer studies [39-42]. MPM has also been used for *in vivo* studies of stroke in mice [43, 44].



There have been numerous studies of the immune system to examine lymphocyte dynamics *in vivo* [45-56] and study model antigen systems to examine immune responses to infection *in vivo* [57-62]. Immune system studies using MPM have examined skin [63-65], spinal cord [66], gut [67], bone marrow [68, 69], and liver [70]. MPM has also been used to study intracellular signaling [71, 72], cell proliferation [55], chemotaxis [73-80], and T cell effector function [65, 81, 82].

MPM has also enabled biologists to study the cardiovascular system to examine calcium transients and study cellular transplantation in Langendorff-perfused mouse hearts [83-85]. Research has also been done using MPM to examine lymphocyte infiltration into atherosclerotic arteries [86].

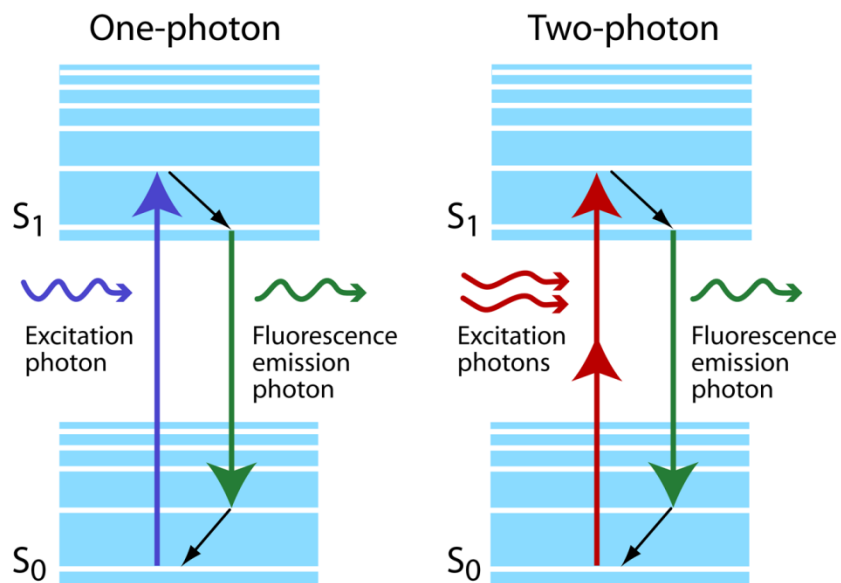
In live rats and mice, the kidney has been externalized and apposed to a coverslip on the stage of the microscope, and MPM images have been directly collected for measurement of basic renal physiological parameters [3, 87], including glomerular filtration and permeability, tubular fluid and blood flow, urinary concentration/dilution, and rennin content and release [88-92]. This method has also been used for studies of acute renal failure [93-95], microvascular leakage in a rat model of renal ischemia [96, 97], folic acid uptake and transport [98], organic anion transport [7], bacterial infections [57, 59-62], and nephrotoxicity of aminoglycoside antibiotics [99, 100]. Fixed embryonic kidneys from a mouse model of polycystic kidney disease have been studied to characterize renal development [101, 102].

## *B. Multiphoton fluorescence excitation microscopy*

### *1. Multiphoton fluorescence excitation*

Conventional fluorescence microscopy generates images by exciting fluorescent molecules, whether endogenous to the sample or added exogenously, allowing investigators to collect images of the distribution and behavior of these specific molecules. Short wavelengths of light excite the fluorescent molecule from the ground electronic state to an excited electronic state (Figure 1). Within each electronic state are vibrational states. The fluorescence molecule then loses a small amount of energy as heat as the molecule relaxes to a lower vibrational state. It then relaxes back to the ground state, emitting a photon with less energy and a longer wavelength than the excitation light. The difference between the excitation and emission wavelengths is known as the Stokes shift. A dichromatic mirror is used to separate the excitation wavelengths from the emission wavelengths, generating images with extremely high contrast. By specifically labeling multiple molecules in a tissue with spectrally distinct fluorophores, researchers can collect images of distributions of multiple molecules in the same sample to compare spatial relationships. Samples are excited sequentially with wavelengths specific for each probe, and fluorescence emissions are collected using barrier filters optimized for collection of each separate probe.

Unlike single-photon fluorescence excitation, multiphoton fluorescence excitation is based on a nonlinear process where two or more low energy photons are absorbed by a fluorescent molecule exciting the molecule to fluoresce (Figure 1). In the case of two-photon fluorescence excitation, this requires that the summed energy of the two photons be equal to the energy required to stimulate an electronic transition to a higher energy

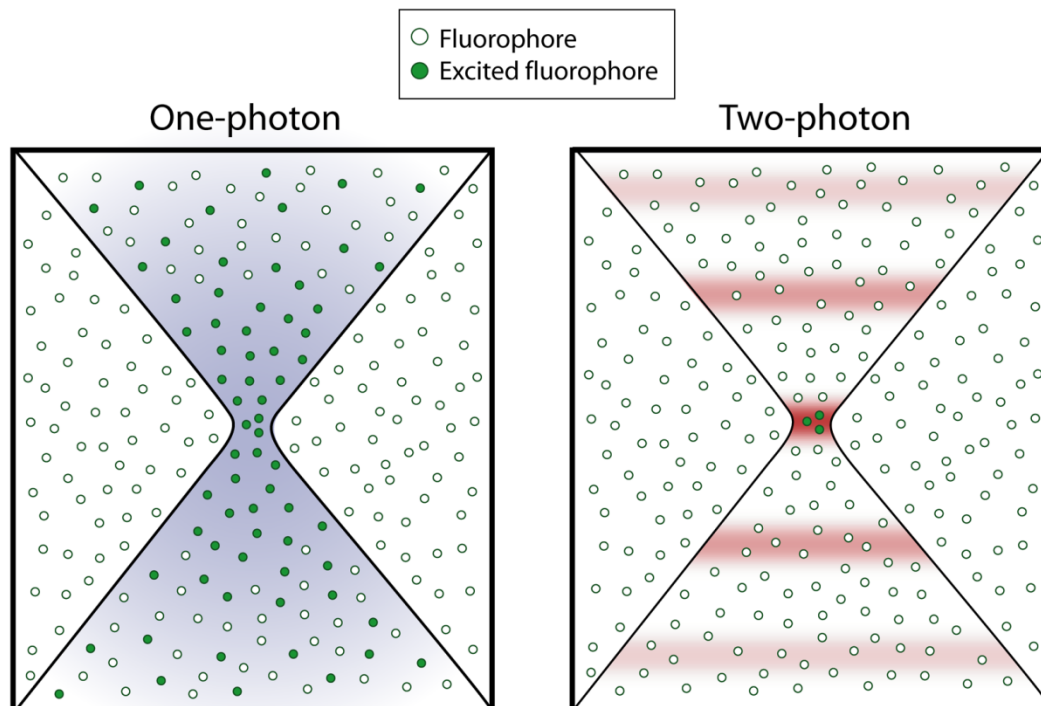


**Figure 1. Jablonski diagram**

Jablonski diagram demonstrating one- and two-photon fluorescence excitation. Two-photon excitation results from the simultaneous absorption of two low-energy photons by a fluorophore.

state. Because energy is inversely proportional to wavelength, the wavelength of the two-photon excitation spectra is generally approximately twice that of the single-photon excitation spectra, typically optimal between 700-1000 nm. In order for two photons to stimulate an electronic transition, they must arrive within the lifetime of the virtual excitation state, approximately  $10^{-16}$  seconds [5, 11, 103]. The probability that two-photon excitation will occur depends quadratically on the excitation power and is very low when typical energies are used for single-photon fluorescence microscopy [104]. The probability is improved to generate sufficient signal by pulsing near-infrared laser light temporally and focusing the light spatially with an objective lens [5] (Figure 2). Rapidly but briefly pulsing the laser generates a peak power sufficient to excite two-photon fluorescence but an average power low enough to avoid harming the sample. A typical MPM system generates a peak photon flux approximately one million times that at the surface of the sun [12]. However, it has been shown to be gentle enough not to harm developing hamster embryos [14].

Focusing the illuminating light spatially with an objective lens will create a conical geometry of the illuminating beam, causing the photon density to decrease with the square of axial distance from the focal plane. This, combined with the quadratic dependence of two-photon excitation, results in fluorescence decreasing with the fourth power of axial distance from the focus. Therefore, the photon density is only sufficient to cause two-photon excitation at the focus in a volume dependent upon the excitation wavelength, refractive index, and numerical aperture (NA) of the objective. High NA objectives make it possible to collect subfemtoliter focal volumes [11]. Because



**Figure 2. Fluorescence excitation for one- and two-photon microscopy**

In one-photon fluorescence microscopy, a continuous wave ultraviolet or visible light laser excites fluorophores throughout the volume. In two-photon microscopy, an infrared laser provides pulsed illumination such that the density of photons sufficient for simultaneous absorption of two photons by fluorophores only occurs at the focal point.

fluorescence excitation is localized to a single point in the sample, an image is formed by scanning the focus across the sample. A photomultiplier tube collects the emitted fluorescence to build up the image point by point. In order to acquire images in reasonable periods of time, each point in the sample is imaged very briefly, on the order of microseconds.

## 2. *Lasers*

MPM was first introduced in 1990 by Denk et al., who were able to generate the extremely high photon flux required for two-photon fluorescence excitation with appreciable probability [103]. They achieved this by combining the tight focusing of a laser scanning microscope with the temporal concentration from a 25 mW colliding-pulse, mode-locked dye laser (Clark Instruments, Pittsford, NY) ( $\lambda \sim 630$  nm) to produce a stream of pulses with 100 fs pulse duration at about 80 MHz repetition rate. Unfortunately, femtosecond dye lasers, like those they used, are impractical for the average biologist. Not only are they toxic, requiring regular dye changes leading to generation of a lot of toxic waste, but they also are difficult to tune, with changes of greater than 30 nm requiring an entire dye change [105].

However, in 1992, a “home-built” self-sustaining mode-locked titanium sapphire (Ti:S) crystal-based laser was applied to MPM [106]. Ti:S lasers have become the most common MPM excitation sources available. They consist of a pair of two separate lasers, a continuous-wave diode pump laser (typically Neodymium Doped Yttrium Orthvanadate (Nd:YVO<sub>4</sub>) crystal-based laser) and Ti:S laser, or may be in a single box containing both the pump laser and the Ti:S oscillator. Ti:S lasers use broadband optics so that the wavelength can be tuned within the range of 690-1020 nm, two-laser, or 720-920 nm,

single-box [11]. Many of these lasers are now computer-controlled, making them extremely user-friendly. The laser power available varies depending on the pump laser but ranges from 5-10 W pump, providing an average power of up to 1-2 W at the Ti:S peak wavelengths. However, a mode-locked Ti:S laser produces a pulsed laser beam with extremely high peak power.

A laser is “mode-locked” when only a certain set of frequencies are propagating in the laser cavity, with the phase between these frequencies creating destructive interference between all of the propagating frequencies except at one point in the cavity where the waves add constructively, resulting in a single short pulse of light. Typical mode-locked lasers have a pulse duration with full width at half maximum (FWHM) of 80-150 fs [11]. The distance between the two cavity end mirrors determines the repetition rate, typically ~80 MHz. Because femtosecond Ti:S lasers require many intracavity frequencies, the pulses have a large spectral bandwidth, typically with FWHM of ~10 nm, with a symmetrical Gaussian shape. The pulse duration and spectral bandwidth are related, therefore if the pulse passes through a dispersive media, because longer wavelengths travel faster than shorter wavelengths, the pulse becomes “positively chirped,” increasing the pulse duration but not changing the spectrum. Pulse broadening reduces the photon flux, decreasing two-photon fluorescence excitation. Lasers are available for MPM that correct for group velocity dispersion by adding negative dispersion to pre-chirp the laser.

### 3. *Beam intensity control*

The laser intensity can be controlled by neutral-density filters, a rotatable polarizer, an electro-optic modulator (EOM), or an acousto-optic modulator (AOM).

Neutral-density filters attenuate laser intensity independent of wavelength and come in two general types, absorptive gray glass filters or reflective metallic filters [107].

Because MPM utilizes high laser powers, absorptive gray glass filters may overheat.

Graded neutral density filters and filter wheels are good for general attenuation but are not fast enough to blank the beam during retrace with a linear galvanometer scanner.

Fast shuttering requires an EOM or AOM. An EOM uses a crystal, such as lithium niobate or gallium arsenide, that produces birefringence, induced by an electric field, to control laser intensity. Laser beam attenuation is controlled by varying the voltage applied to the Pockels cell. An EOM can also be used to modulate the phase, the frequency, or the direction of propagation of the laser beam [107]. EOMs have very high throughput, but incomplete extinction [108]. An AOM modulates the laser intensity using the optical effects of an acoustic field on a birefringent crystal [107]. A piezoelectric crystal is attached to the birefringent crystal and generates an acoustic field. The frequency of the acoustic wave affects the local density of crystal, and therefore the refractive index, creating a periodic diffractor. Light passing through the crystal is diffracted at an angle depending on the wavelength of light and frequency of the acoustic wave. The intensity of the deflected beam can be varied from 0-85% and switched on and off with a high extinction ratio. The dispersive materials used in EOMs and AOMs spread the laser pulse temporally, decreasing photon flux, and therefore the optical system would benefit from prechirping [108].

#### *4. Beam expander collimator*

A beam expander can be used to adjust the beam width of the laser at the back aperture of the objective. Underfilling the back aperture of the objective elongates and



enlarges the illumination profile at the focus of the objective and reduces the effective numerical aperture. Filling and overfilling the back aperture result in a diffraction-limited focus.

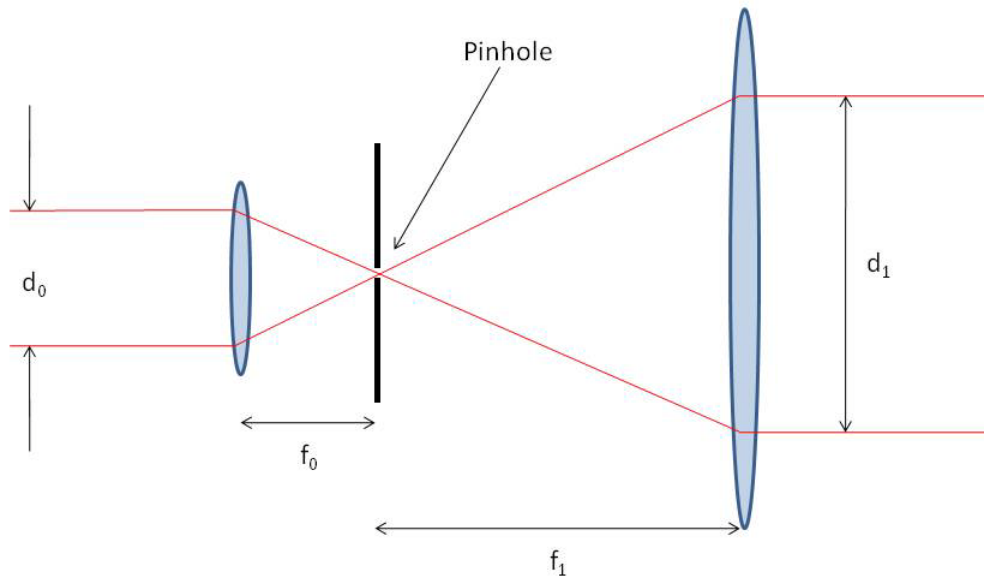
There are two main types of beam expanders. The Galilean type consists of a negative lens causing the beam to diverge followed by a positive lens that collimates the beam. The Keplerian type consists of two positive lenses with their focal points coincident (Figure 3). The Keplerian type beam expander can also be used in conjunction with a spatial filter to remove the scattered components of the beam. The spatial filter consists of a pinhole positioned at the focus of the converging beam.

#### 5. *Beam scanner*

MPM typically uses mirrors mounted on galvanometer motors to scan the focused laser beam across the sample. XY scanner designs include nonresonant linear galvanometers or resonant galvanometers [11]. Nonresonant linear galvanometers raster scan the beam, using a sawtooth pattern with a relatively slow linear recording time followed by a fast retrace [107]. The benefit of linear galvanometers is that they have adjustable scan speed, providing a digital zoom and the ability to rotate the scan axis [11]. Resonant galvanometers use a torsion spring to vibrate at a fixed frequency so recording time is during the trace and retrace [107]. They are able to achieve much faster scan rates but are not as capable of zooming, panning, or rotating [11].

#### 6. *Objectives*

For two-photon excitation to occur with appreciable probability, the laser must be condensed temporally, by pulsing, and spatially, using an objective lens to form a tight



**Figure 3. Schematic of Keplerian beam expander/collimator**

The schematic depicts  $D_0$  is the beam width of the incident light,  $f_0$  is the focal length of the first lens,  $f_1$  is the focal length of the second lens and  $d_1$  is the beam width of the expanded beam.

focus [5]. Because the objective lens in MPM acts as the condenser and objective, it needs to have excellent optics to form a tight focus and to provide good throughput to minimize light loss. Therefore ideal objective lenses use optics that have been optimized to transmit visible and near-infrared wavelengths. Although MPM can be achieved using low or high NA objectives, MPM benefits from the use of high NA objective not only because of the tight focus but also because of the large collection angle, enabling high NA objectives to collect more scattered emissions [109].

High NA objectives are available with water, glycerol, or oil immersion. Because oil has the highest refractive index, these objectives are capable of having the highest NA. However when focusing deep into an aqueous sample, refractive index mismatch causes spherical aberration which degrades image quality. Therefore water and glycerol immersion objectives are frequently the better choice for biological imaging. Water and glycerol objectives have been designed with a correction collar on the objective lens that moves optical elements inside the lens to correct for refractive index mismatch caused by coverslip thickness variation. This correction collar can also be used to correct for temperature-dependent index changes and the refractive index of the sample [110, 111].

A useful comparison of many objective lenses available from Leica Microsystems (Wetzlar, Germany), Carl Zeiss MicroImaging (GmbH, Germany), Nikon Instruments Inc. (Tokyo, Japan), and Olympus (Tokyo, Japan) can be found in reference [112].

## 7. *Detectors*

In MPM, three-dimensional localization is accomplished by excitation alone, making numerous detection options available. The most commonly used type of non-descanned detection is whole-area detection where fluorescence light passes through the

objective lens and is separated from the excitation light by a dichroic mirror and focused onto a detector using minimal optical surfaces [108]. This is highly efficient because the light path is short and direct reducing the loss of scattered emissions [108]. Another less common type of non-descanned detection is external detection, where the detector is placed adjacent to the sample such that fluorescence light bypasses the objective [108]. In theory, external detectors could be placed all around the sample to collect as much fluorescence light as possible; however, this method will obviously not work for large samples like in live animal imaging. Descanned detection is where the fluorescence light passes the objective lens and is reflected off the scanning mirrors. A confocal pinhole can be used to improve resolution, but because it rejects any scattered emissions, signal attenuates rapidly with depth into a scattering sample, defeating the purpose of using MPM [113-115]. Because optical sectioning is inherent in MPM, optimal detection is achieved by placing detectors in the most direct optical path to collect as many scattered emissions as possible [116].

Ideal MPM detectors have high quantum efficiency but low detector noise. Although cooled charge-coupled devices (CCDs) have high quantum efficiency, they have not found widespread use in MPM because of the high readout noise at the high frame rates necessary for MPM [11]. CCDs are two-dimensional arrays of photodetectors that exploit photoconductive or photovoltaic effects and operate by reading out a voltage proportional to the number of photons absorbed [117].

Imaging detectors are not necessary for point-scanning systems like MPM; however, scattered emissions may have a randomly divergent trajectory through the objective lens. Therefore a good choice of detector is a large-area photomultiplier tube

(PMT) [118, 119]. PMTs use a photocathode that absorbs signal photons, producing photoelectrons which are amplified by charge multiplication, producing a signal current [120]. The current is then digitized in intervals based on the timing of the scanning mirrors such that each pixel value in the image represents the signal intensity during the brief time period the appropriate area of the sample is being imaged [121]. PMTs have a rapid response and high gain, for a good dynamic range, but low quantum efficiency [11]. This is because most photons are either transmitted or reflected rather than absorbed and therefore do not contribute to the signal [120]. However, gallium arsenide (GaAs) and gallium arsenide phosphide (GaAsP) PMTs have markedly higher quantum efficiency than traditional multi-alkali PMTs [11, 120].

### *C. Single-photon versus two-photon microscopy*

Conventional fluorescence microscopy generates images with extremely high contrast by exciting fluorescent molecules in a sample, then collecting the fluorescence emissions while rejecting the excitation light. This works well for thin samples; however, thick samples generate fluorescence throughout the sample, causing out-of-focus fluorescence to appear in the image. Out-of-focus fluorescence reduces contrast [122] and the signal-to-noise ratio [123]. This problem was first addressed in 1957 with the development of the confocal fluorescence microscope [124]. Confocal fluorescence microscopy uses a set of conjugate apertures located in the illumination and detection path to ensure that the microscope illuminates and detects from the same focal volume. These pinholes function as spatial filters to eliminate stray light, rejecting out-of-focus fluorescence, effectively collecting an “optical section” within the thick sample.

Confocal fluorescence microscopy has advanced since 1957. Today, confocal fluorescence laser scanning microscopy (CLSM) is a technique that uses laser light to excite fluorescence in the sample and galvanometer scanning mirrors to raster scan the focus across the sample to build an image. By repeating this for multiple focal planes an image volume of the sample can be collected.

MPM and CLSM are very similar techniques. Both types of microscopy use point scanning to collect optical sections of the sample. Surprisingly, MPM and CLSM have similar resolution. Because CLSM uses ultraviolet and visible excitation wavelengths and MPM uses near-infrared, about twice the wavelength, the Rayleigh criterion predicts that under ideal conditions CLSM will have lateral resolution of approximately

$$r_{xy,confocal} \approx \frac{0.4\lambda_{em}}{NA}$$

and MPM will have lateral resolution of approximately

$$r_{xy,mpm} \approx \frac{0.7\lambda_{em}}{NA}$$

where  $\lambda_{em}$  is the emission wavelength and  $NA$  is the numerical aperture of the objective [125]. Similarly, axial resolution is predicted to be

$$r_{z,confocal} \approx \frac{1.4\lambda_{em}n}{NA^2}$$

$$r_{z,mpm} \approx \frac{2.3\lambda_{em}n}{NA^2}$$

where  $n$  is the refractive index of the objective lens immersion fluid [125]. However, “ideal imaging conditions” are rarely achieved. Frequently, when collecting images with CLSM, samples are dim causing a low signal-to-noise ratio which reduces resolution [125]. By opening up the pinhole, more signal can be collected, improving signal-to-

noise ratio, but this is also at the expense of resolution [125]. Typical pinhole adjustments result in CLSM resolution similar to MPM [11].

Though both CLSM and MPM can be used to collect image volumes, MPM is inherently better for deep tissue imaging. MPM utilizes near-infrared wavelengths of light (700-1000 nm) for excitation. These wavelengths are within an “optical window” in the absorption spectrum of biological tissue, making them ideal for imaging biological samples [6]. Also, because Rayleigh scattering has a wavelength dependence of  $\sim\lambda^{-4}$ , these longer excitation wavelengths scatter less than shorter wavelengths, improving imaging depth compared to CLSM [116].

MPM also has that advantage that no pinhole is required to collect an optical section. This means that all of the fluorescent emissions come from the focus and can be collected to form the image. Therefore, large-area detectors can be placed in the light path close to the objective lens, eliminating light loss from optical elements in the descanning path and scattering. Calculations have shown that nearly all of the fluorescence stimulated 100 microns deep in tissue are scattered before exiting the tissue [5, 119]. Centonze and White [116] have shown that using descanned detectors, MPM improves imaging depth 2-fold over CLSM. They have also shown that using non-descanned detectors, imaging depth improves three-fold over that of MPM with descanned detectors.

Another important advantage of MPM over CLSM is that photobleaching and photodamage are minimized [126]. CLSM excites fluorescence throughout the entire

	Confocal microscopy	Multiphoton microscopy
Excitation source	Ultraviolet or visible laser Limited number of wavelengths Low cost	Pulsed infrared laser Continuously variable wavelength High cost
Effective imaging depth	Typically <20 $\mu\text{m}$	Up to 500–600 $\mu\text{m}$ <sup>a</sup>
Spatial resolution (full width at half-maximum)	Theoretically up to 0.14 $\mu\text{m}$ laterally 0.57 $\mu\text{m}$ axially <sup>b</sup>	Theoretically up to 0.23 $\mu\text{m}$ laterally 0.93 $\mu\text{m}$ axially <sup>b</sup>
Sensitivity to scattering	High	Low
Photobleaching and phototoxicity	High – occurs throughout tissue volume	Low – restricted to focal plane
Image capture rate	Typically low, higher speeds possible via array scanning	Low, array scanning limited to thin samples

<sup>a</sup> See Kleinfeld et al. [1998] and Helmchen et al. [1999].

<sup>b</sup> Assuming 488 nm excitation for confocal and 900 nm excitation for multiphoton [Jonkman and Stelzer, 2002]. Note that the resolution of confocal and multiphoton systems are more similar in practice [e.g. Centonze and White, 1998].

**Table 1. Comparison of confocal and multiphoton microscopy**



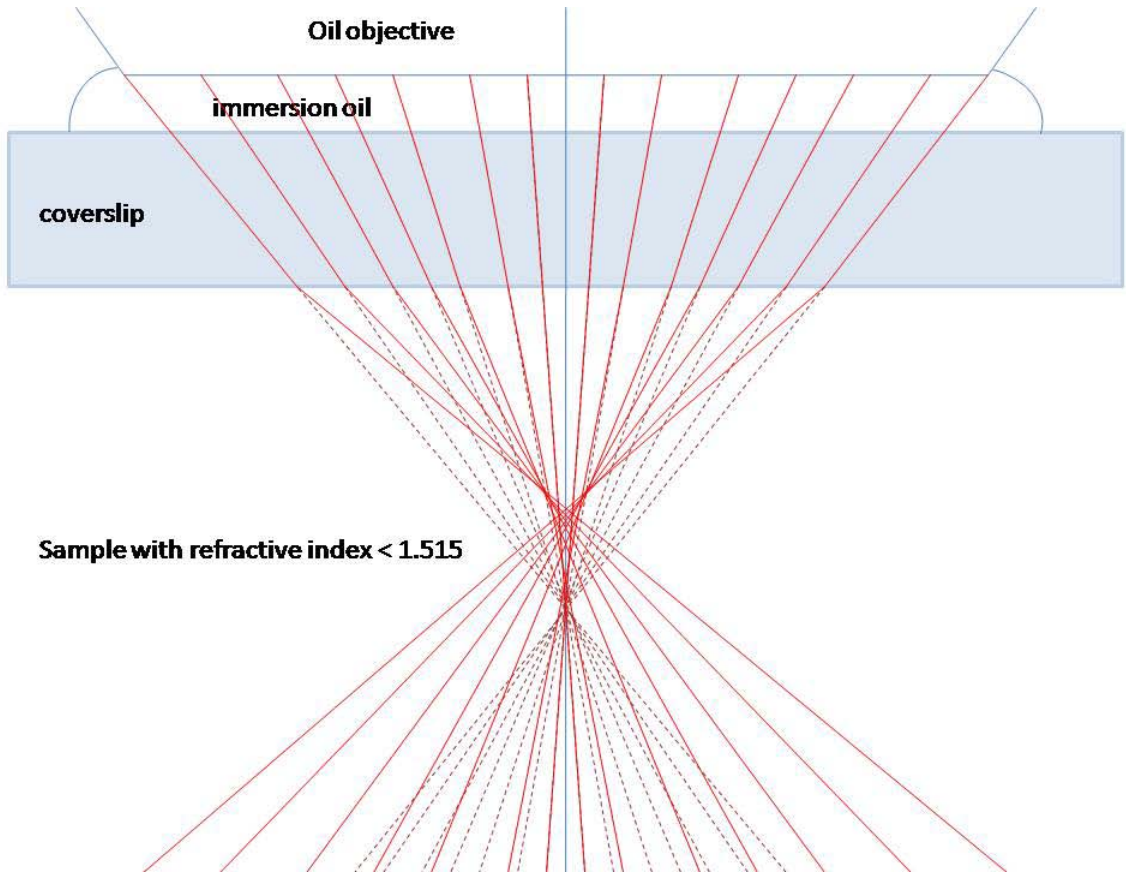
double-inverted cone of light leading to photobleaching and photodamage anywhere that cone intersects the sample [126]. MPM uses near-infrared excitation light and only excites the sample at the focus, a much smaller area exposed to photobleaching and photodamage [11]. However, it is important to note that MPM can still lead to considerable photodamage and photobleaching in the focal volume. In fact, photobleaching, expected to occur in proportion to the square of excitation power, has actually been shown to occur at higher-order [127].

#### *D. Imaging depth limitations of MPM*

Although MPM improves fluorescence signal with depth over other fluorescence techniques, imaging depth is still limited. Fluorescence signals can be expected to attenuate with depth in tissues due to reduced stimulation of fluorescence or reduced detection of fluorescence. This is caused by spherical aberration, light scattering, and absorption of light [5, 11, 110, 111, 115, 116, 119, 128-132]. Both excitation and detection of fluorescence at depth are sensitive to scattering and absorption of light. Spherical aberration is caused by refractive index mismatch between the objective immersion fluid and sample and will also limit signal at depth.

##### *1. Spherical aberration*

Although MPM has many advantages over CLSM with respect to imaging deep into biological tissue, MPM is still depth-limited. Deep tissue imaging typically involves imaging into a medium whose refractive index does not match that of the objective immersion fluid. Refractive index mismatch between the immersion fluid, coverslip, and



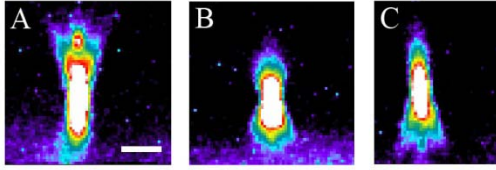
**Figure 4. Refractive index mismatch broadens the focal point**

Schematic (not to scale) of excitation light path. Dashed line indicates ideal case where sample refractive index is 1.515, matching immersion oil. Red line indicates excitation light path into sample with refractive index less than 1.515. The ideal case comes to a sharp focus, but when the sample has a different refractive index than the objective immersion fluid, the light bends upon encountering the sample, broadening the focal point.

sample causes spherical aberration [110, 111, 115, 128, 131, 132]. Spherical aberration is a condition where the focal point is broadened due to the peripheral rays of light coming to focus at a different place than the paraxial rays (Figure 4). Spherical aberration is an on-axis aberration. However, since MPM uses galvanometer scanning mirrors to raster scan the focal point of light to build the image, refractive index mismatch in MPM causes minor off-axis aberrations as well.

*a. Point spread function*

The effect of spherical aberration can be visualized by collecting images of the point spread function (PSF). The PSF describes the three-dimensional light intensity distribution at the focus and is a convolution of the illumination PSF, the light intensity distribution for the illumination process, and detection PSF, the probability that a fluorescent photon is able to propagate to the detector. The PSF can be visualized by collecting images of sub-resolution fluorescent microspheres. Figure 5 shows XZ cross-sectional images of 0.5 micron red fluorescent microspheres (F8812, Invitrogen, Eugene, OR, USA). Imaging was conducted using the Olympus FV1000 confocal microscope system that has been adapted for two-photon microscopy by the Indiana Center for Biological Microscopy. A Mai Tai Ti:S laser (Spectra-Physics, Mountain View, CA, USA) provided the excitation light at wavelength 800 nm. Image volumes were collected using a water immersion objective (Olympus, 60x Plan Apochromat, NA 1.2) designed for use with glass coverslips. Since correction for spherical aberration critically depends upon coverslip thickness, such objectives are equipped with correction collars. This collar moves the objective lens elements so that the paraxial and peripheral rays of light form a tight focus after traveling through a glass coverslip of defined thickness.



**Figure 5. Effect of correction collar adjustments on the point spread functions of fluorescent microspheres**

XZ cross-section of 0.5 micron fluorescent microspheres mounted immediately below the coverslip with collar settings (A) 0.13, (B) 0.17, and (C) 0.21 mm. Pseudocolor based on intensity. Scale bar = 2 microns. X=Z.

Conversely, the collar can be used to manipulate spherical aberration in a particular sample. In Figure 5, the images were collected with the objective collar adjusted for a nominal 0.13 mm thickness (A), 0.17 mm thickness (B), and 0.21 mm thickness (C). Since the coverslip was measured to be  $0.180 \pm 0.001$  mm thick, it is not surprising that the best results were obtained using the nominal 0.17 mm collar setting, which generated compact and vertically symmetrical PSFs (Figure 5B).

Adjusting the collar to 0.13 mm introduced negative spherical aberration into the imaging system (Figure 5A). Negative spherical aberration results from the refractive index of the sample being greater than the refractive index of the immersion fluid, resulting in displacement of peripheral rays to a deeper focus than axial rays. This causes diffraction rings that, when imaged using CLSM or MPM, extend toward the objective lens. In Figure 5A, this is reflected by the asymmetrical formation of rings projecting towards the objective lens.

Adjusting the collar to 0.21 mm resulted in positive spherical aberration (Figure 5C). Positive spherical aberration results from the refractive index of the sample being less than the refractive index of the immersion fluid, as in the case of imaging with an oil objective into water. Positive spherical aberration results in displacement of peripheral rays to a shallower focus than axial rays causing diffraction rings that, when imaged using CLSM or MPM, extend more intensely deeper into the sample. In Figure 5C, this is reflected by the formation of rings projecting away from the objective lens.

#### *b. Axial scaling*

Spherical aberration also results in axial scaling [132]. Axial scaling refers to the image volume being either compressed or stretched axially. Negative spherical

aberration results in an axially compressed image volume. Positive spherical aberration results in an image volume that is stretched axially. This is caused by the peripheral rays not focusing to the same place as the paraxial rays, resulting in a focal shift. The focal shift is the difference between the actual focal position (AFP) and the nominal focal position (NFP). The NFP is the distance between the coverslip and the focus in a system with refractive indices that are perfectly matched. Imaging depth is typically measured by the physical axial movement of the objective lens, which reflects the NFP. The AFP can be approximated from the NFP using the paraxial approximation, the ratio of the refractive index of the sample to the refractive index of the immersion medium [133]. The axial scaling factor is the ratio between the AFP and NFP. The axial scaling factor has been measured using CLSM and used to determine the correct thickness and refractive index of a sample [134, 135].

*c. Signal attenuation*

Since broadening of the image of the focal spot results in the rejection of fluorescence by the confocal pinhole, spherical aberration significantly reduces the collection of fluorescence at depth in confocal microscopy. The use of large area detectors makes the effects of spherical aberration on fluorescence collection much less pronounced in MPM [5]. Thus the fluorescence detection system of a multiphoton microscope makes it much less susceptible to the effects of both scattering and spherical aberration on signal collection.

However, the quality of the illumination focus, which is critically important to efficient multiphoton fluorescence stimulation, may be an issue that can be addressed to significantly improve MPM at depth. Because multiphoton fluorescence excitation is

critically dependent upon a tightly focused, diffraction limited spot, degradation of the focal spot will lead to decreased photon density and quadratically decreased fluorescence. It is well understood that spherical aberration degrades the tight focus of illumination light, and accordingly, studies in model systems have shown MPM will be highly sensitive to spherical aberration [115, 131, 136-138].

#### *d. Resolution*

Spherical aberration may also cause axial resolution degradation with depth. By broadening the focus, spherical aberration reduces resolution in widefield microscopy [139]. Because of the confocal pinhole, the effects of spherical aberration on resolution are not nearly as significant in CLSM [140]. The effects of spherical aberration on MPM are hard to predict. Focal broadening results in a decreased photon flux, but a high photon flux is crucial for achieving appreciable two-photon excitation. Therefore, resolution may decrease as the focus broadens, or it may not be affected because the photon density is insufficient to excite two-photon fluorescence. While some studies indicate that resolution of MPM decreases with depth into biological tissues [141, 142], other studies find no such effect [116, 130, 143]. However studies that have specifically looked at the effect of spherical aberration have found that resolution decreases with depth [131, 136, 143].

#### *2. Scattering*

Scattering is a predominant factor ultimately limiting the reach of MPM. Scattering results from refractive index heterogeneities in the tissue, for example from cell membranes or intracellular structures [144]. Biological samples are heterogeneous and do not have a uniform refractive index [145-147]. Kidney tissue, for example, is

made up of a rich vasculature, renal corpuscles, renal tubules, and covered in a fibrous capsule. This is unfortunate for biologists interested in using microscopy to study the kidney because the light path through kidney tissue has many interfaces where light is refracted and reflected, and even light in the “optical window” is strongly scattered [145]. Scattering arises due to refractive index mismatch at the boundaries between these inhomogeneities, such as at the extracellular fluid-cell membrane interface. Calculations have shown that nearly all of the fluorescence stimulated 100 microns deep in tissue are scattered before exiting the tissue [5, 119], making large-area detectors necessary for deep tissue imaging.

Because MPM can efficiently collect scattered light, scattering primarily impacts imaging depth by reducing power at the focus of illumination. Studies indicate that scattered photons do not contribute to two-photon excitation [5, 131, 143, 148]. Imaging depth ultimately is limited by the relative amount of excitation at the focus versus shallower depths. The decrease in fluorescence excitation caused by light scattering and absorption can be addressed by increasing laser power with depth into the sample or using a regenerative amplifier, at least up to the fundamental depth limit.

Scattering has been shown to fundamentally limit imaging depth [129]. In brain tissue, the fundamental imaging depth was found to be ~1 mm [9]. A regenerative amplifier was used as the excitation source to lower repetition rates while maintaining the average power, significantly increasing depth penetration. However, depth was limited by an increase in out-of-focus fluorescence from the surface of the sample. Near-surface fluorescence is caused by scattered excitation light, increasing the background signal such that fluorescence excited at the focus cannot be discerned from the background



levels. This was first reported by Ying et al. [142]. They described that with increasing scattering strength of the sample, the location of the maximum fluorescence intensity moves away from the focal region toward the surface of the sample where it is more evenly distributed, causing loss of the optical sectioning ability inherent in MPM.

By decreasing refractive index heterogeneity, the ultimate depth limit can be addressed. Reducing refractive index heterogeneity reduces scattering and out-of-focus fluorescence at the surface of the sample, thereby increasing the fundamental depth limit.

Using excitation powers below the level that causes out-of-focus fluorescence, it is difficult to predict how scattering will affect resolution. It seems unlikely that scattered light would contribute to the focus. This idea is supported by studies that show that imaging deep into scattering samples has no effect on resolution [116, 130, 143]. However, Schilders et al. showed that scattering does affect resolution [142]. In fact, they state that resolution degradation caused by refractive index mismatch is negligible compared to the degradation caused by scattering.

### 3. *Absorption*

Absorption is likely not a major limit to imaging depth, except in certain kinds of tissues. A few of the main compounds in biological tissue that absorb light are water, hemoglobin, lipids, cytochrome *c* oxidase, melanin, and myoglobin [144]. However, typical absorption coefficients for biological tissue in the visible and near-infrared wavelengths are more than an order of magnitude less than typical scattering coefficients [149-152]. In fact, scattering has been shown to typically be ten to one hundred times more significant than absorption [150, 153].

### *E. Optical clearing*

The application of optical clearing methods has been shown to decrease tissue scattering, increasing optical transmittance [146, 154-158]. The application of optical clearing agents reduces the mismatch between tissue components, reducing scattering and improving penetration depth of light. The refractive index of biological tissue can be defined as the sum of the background index and the mean index variation [146]. The background index is determined from the refractive indices of the interstitial fluid and the cytoplasm. The mean index variation is determined from the refractive indices of the major contributors to index variation, for example connective tissue fibers have refractive index 1.47, and organelles have refractive index 1.38-1.41. The ratio of the total refractive index of the tissue to the background index determines the reduced scattering coefficient. By immersing kidney tissue in media with refractive index greater than 1.33, the background index of the tissue is raised, reducing refractive index mismatch at interfaces within the tissue, and lowering the reduced scattering coefficient [146].

The immersion method for optical clearing is not new and was extremely popular from 1950-1970 for cell and microorganism phase-contrast microscopy studies [146]. There are numerous optical clearing agents. Glucose or glycerol solutions with various concentrations have been used in *in vitro* studies of bovine scleral tissue [146], human and rabbit dura mater [146], and skin [146, 159], porcine gastric tissue [154], tendon [157, 159, 160], cranial bone [160, 161], tooth [160], skeletal muscle [157] and mouse intestine [162]; in *in vivo* studies of scleral tissue by putting drops of 40% glucose in rabbit eye [146], of rabbit dura mater at the open cranium [146], and of skin [146]; and in *ex vivo* studies of porcine skin [163] and human skin [158]. FocusClear solution

(CelExplorer, Hsinchu, Taiwan) has been used in studies of collagen, chitosan, and cellulose [164]. Trazograph is an x-ray contrast agent, a derivative of 2,4,6-triiodobenzene acid (Trazograph-60, molecular weight ~500 and refractive index 1.437), and has been used for *in vitro* studies of human and bovine eye sclera and *in vivo* studies of skin using topical applications [146]. Polyethylene glycol (PEG) has been used in *in vitro* studies of bovine sclera [146]. Mannitol solutions have been used to study human and rabbit dura mater [146]. Dimethyl sulfoxide (DMSO) solutions have been used in *in vitro* studies of skin [146, 165] and porcine gastric tissue (in solution with glycerol and water) but are not good for *in vivo* studies because of potential toxicity [146]. Propylene glycol has been used in *in vitro*, *in vivo* and *ex vivo* studies of skin [146, 158], *in vitro* studies of human eye sclera [160] and cranial bone [161]. Oleic acid (a mono-unsaturated fatty acid) and cosmetic lotions and gels have been used in *in vitro* and *in vivo* studies of skin [146]. Gelatin gels containing clearing agents (Verografin, glycerol or glucose) have been designed to improve the efficiency of topical applications [146]. Methyl salicylate or benzyl alcohol/benzyl benzoate (BABB, in solution with ethanol) have been used in studies of brain, heart, kidney, tumor, red fluorescent protein (RFP) and green fluorescent protein (GFP) labeled cells [155] and mouse intestine [162]. Methyl salicylate was shown to be better at fluorescent preservation, though BABB solution achieved better optical clarity. Solutions of 2,2'-thiodiethanol in phosphate buffered saline (PBS) have been used to study mouse intestine [162, 166].

Clearing agents have different osmotic properties and dehydration abilities [146, 154, 159]. Dehydration can lead to structural changes in the sample including changes in collagen fibrils and interfibrillar spacings [167]. Change in tissue can be monitored by

measuring refractive index of agent in bath before and after clearing, and by measuring weight of tissue. Trazograph-60 has been shown to mostly replace the water in tissue during clearing, with the weight of the sample changing little before and after clearing [146]. However, the weight of samples decreases significantly after clearing with 40% glucose and PEG, indicating the water flux out of the tissue caused by 40% glucose and PEG is much stronger than the flux of solution into the tissue [146]. This is due to the osmotic gradient created by the solute, glucose or PEG. These optical clearing agents act upon tissues differently optically as well. It has been shown that DMSO decreases absorption and reduced scattering coefficients. However, glycerol increased wavelength dependent absorption coefficient but did not significantly decrease the reduced scattering coefficient in squamous epithelial tissue. This supports DMSO as the more effective optical clearing agent [156].

#### *F. Hypothesis*

Our hypothesis is that reducing refractive index mismatch and refractive index heterogeneity will improve imaging depth and resolution at depth in MPM.

We expect to find spherical aberration from refractive index mismatch between the immersion fluid, coverslip, and sample plays a significant role in signal attenuation. Here we quantify the effects of refractive index mismatch on signal levels, fluorescence excitation, and resolution as a function of depth in both test samples and biological samples.

We also quantify the effects of scattering on signal attenuation and resolution in MPM of fixed kidney tissue. We expect to find that optical clearing provides a simple method for significantly extending the reach of MPM.

We expect these studies will demonstrate the significance of the spherical aberration component and the scattering component to signal attenuation at depth in MPM of biological tissues.

## II. MATERIALS AND METHODS

### A. *Sample preparation*

#### 1. *Agarose sample preparation*

Samples of agarose were prepared with refractive indices  $1.342 \pm 0.002$ ,  $1.371 \pm 0.001$ ,  $1.404 \pm 0.001$ ,  $1.442 \pm 0.003$  (22° C) using varying concentrations of sucrose in NANOpure® water. Fluorescent microspheres with 0.2 micron diameter (FS02F, Bangs Laboratories, Inc., Fishers, IN, USA) were suspended in agarose while heated to a liquid state. The agarose then cooled at room temperature to solidify. A vibratome was used to section the agarose to 100 microns. The refractive index of the sample was measured with an Abbe refractometer.

Samples were mounted with #1.5 coverslips (Corning, Lowell, MA, USA) measured with a micrometer so that coverslip thickness was  $174 \pm 3$  microns. Before mounting, fluorescent microspheres were dried to the surface of the coverslip and surface of the slide to delineate the top and bottom of the sample in the image volumes.

#### 2. *Microsphere labeling*

Animal studies were conducted within the National Institutes of Health Guide for the Care and Use of Laboratory Animals standards. A 250 g Munich-Wistar rat was anesthetized with pentobarbital (60 mg/kg IP). The femoral vein was then catheterized and suncoast yellow fluorescent microspheres with 0.2 micron diameter (FS02F, Bangs Laboratories, Inc., Fishers, IN, USA) were injected. The animal was then euthanized, and the kidneys were excised. The kidney tissue was fixed by immersion in 4% paraformaldehyde in PBS, pH 7.4, overnight at 4° C. The tissue was sectioned to 100

microns and stored in 0.25 % paraformaldehyde in PBS, pH 7.4, at 4° C. Before image collection, the tissue was washed overnight in PBS at 4° C.

Samples were mounted with #1.5 coverslips (Corning, Lowell, MA, USA). Only coverslips with uniform thickness ( $181 \pm 2$  microns as measured at several locations) were used. The water immersion objective correction collar was set to the average coverslip thickness. Before mounting, suncoast yellow fluorescent microspheres with 0.2 micron diameter (FS02F, Bangs Laboratories, Inc., Fishers, IN, USA) were dried to the surface of the coverslip and surface of the slide to delineate the top and bottom of the sample in the image volumes.

### 3. *Immunofluorescence*

Rat kidney tissue was labeled and cleared as described [168]. Rat kidneys were perfusion fixed using 4% paraformaldehyde in PBS, pH 7.4. The tissue was then sectioned to 200-300 microns using a vibratome (Technical Products International, Inc., S. Louis, MO, USA). Samples were blocked and permeabilized in 0.5% Triton-X 100, 1% Bovine Serum Albumin (BSA), 5% Fetal Bovine Serum (FBS), 1x PBS pH 7.4. Tissue was labeled using Lens Culinaris Agglutinin-Fluorescein (Vector Labs, Burlingame, CA) at a dilution of 1:200, Hoechst 33342 (10mg/mL) (Invitrogen, Carlsbad, CA), and Phalloidin-Rhodamine at a dilution of 1:100 (Invitrogen, Carlsbad, CA).

Before image collection, samples were washed overnight in PBS at 4° C. Before mounting, the tissue was incubated in a graded series of glycerol in PBS solutions, 17.5%, 35%, and 70%, for at least 30 minutes at room temperature until samples settled to the bottom of the solution. Samples were incubated in mounting solutions for at least

30 minutes at room temperature until samples settled to the bottom of the solution and then transferred to a fresh aliquot at least once for at least 30 minutes or overnight. Samples were mounted in fresh solution with #1.5 coverslips (Corning, Lowell, MA, USA) measured with a micrometer, and water immersion objective correction collar was set accordingly using the ring value.

#### 4. *Mounting media*

Mounting media were prepared as described in Table 2. Media were prepared by weight. Refractive index was measured at room temperature ten times using an Abbe refractometer (Sino Science & Technology Co., Ltd., ZhangZhou, FuJian, China).

#### B. *Two-photon microscopy*

Samples were imaged using a FV1000 confocal microscope system (Olympus, Center Valley, PA, USA) that has been adapted for two-photon microscopy. The system is equipped with a Mai-Tai titanium-sapphire laser pumped by a 10 W Argon laser (Spectra-Physics, Santa Clara, CA, USA), a Pockels cell beam attenuator (Conoptics Inc., Danbury, CT, USA), and a Keplerian-style collimator/beam expander fabricated and aligned to fill the back aperture of the objective (Figure 6). The illumination path was aligned using a fluorescent slide to center the beam and the PSFs of suncoast yellow fluorescent microspheres with 0.2 micron diameter (FS02F, Bangs Laboratories, Inc., Fishers, IN, USA) mounted on a coverslip. We also used a leveling apparatus mounted on the translation stage to ensure the coverslip was perpendicular to the light path [169].

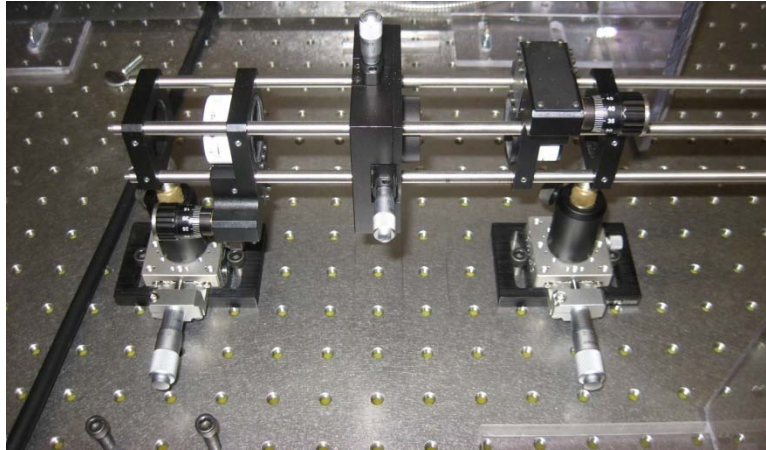
Images were collected using either a 60x NA 1.4 oil immersion objective (PLAPO60XO3, Olympus, Center Valley, PA, USA) using immersion oil with refractive



	Mounting Medium	Refractive Index (22°C)	Standard Deviation
A	98% PBS, 2% DABCO	1.3386	0.0002
B	49% PBS, 49% glycerol, 2% DABCO	1.4031	0.0005
C	19.6% PBS, 78.4% glycerol, 2% DABCO	1.4744	0.0002
D	13% benzyl alcohol, 85% glycerol, 2% DABCO	1.4836	0.0006
E	53% benzyl alcohol, 45% glycerol, 2% DABCO	1.511	0.001
F	83% benzyl alcohol, 15% glycerol, 2% DABCO	1.5297	0.0004

**Table 2. Mounting media**

Mounting media refractive indices measured with an Abbe refractometer.



**Figure 6. Beam expander/collimator**  
The beam expander/collimator on our system.

index 1.515 (UPLAPO60XW3/IR, Olympus, Center Valley, PA, USA) or a 60x NA 1.2 water immersion objective (Olympus, Center Valley, PA, USA) using water with refractive index 1.33. Images were collected either using descanned detectors with the confocal pinhole maximally open or using non-descanned detectors mounted on the right side port of an Olympus IX-81 microscope. The blue channel was collected using a bialkali PMT (Hamamatsu R1924AHA) and a 380-480 nm bandpass filter (Chroma HQ430/100M-2P). The green channel was collected using a multialkali PMT (Hamamatsu R6357HA) and a 500-550 nm bandpass filter (Chroma HQ525/50M). And the red channel was collected using a multialkali PMT (Hamamatsu R6357HA) with a 560-650 nm bandpass filter (Chroma HQ605/90M-2P). The PMT gain was constant and below PMT saturation, and PMT black level was constant for all images collected.

### *C. Signal attenuation and resolution degradation*

#### *1. Excitation and emission spectra*

Fluorescent microspheres with 0.2 micron diameter labeled with suncoast yellow (FS02F, Bangs Laboratories, Inc., Fishers, IN, USA) were dried on a #1.5 coverslip (Corning, Lowell, MA, USA) in 50% PBS / 50% glycerol with 1% DABCO. A spectral scan was collected every 25 nm from 500-700 nm emission wavelength with a bandwidth of 25 nm. This was repeated for excitation wavelengths 710, 740, 770, 800, 830, 860, 890, 920, and 950 nm. Laser power was measured immediately following the Pockels cell to ensure that all images were collected with the same laser power. Images were collected using a 60x NA 1.4 oil immersion objective (Olympus, Center Valley, PA,

USA) using immersion oil with refractive index 1.515. The images were 512x512 pixels with XY pixel dimension of 0.139 microns.

To analyze the spectral data, a 20x20 pixel square region was placed around each of thirteen microspheres from each image. A fourteenth 20x20 pixel square region was used to collect background data. The integrated intensity in each region was recorded. To find the fluorescence intensity of the microsphere, the integrated intensity in the background region was subtracted from the integrated intensity of the 20x20 pixel square region surrounding the microsphere. The data from the thirteen microspheres were then averaged and plotted on the excitation spectrum and emission spectrum curves.

## 2. *Fluorescence saturation*

Fluorescence saturation was measured after each realignment of the excitation path because laser power was being measured at the Pockels cell, not the stage, therefore realignment could cause a difference in excitation power at the stage. Fluorescence saturation was measured by collecting three images of microspheres dried on the coverslip in agarose samples with refractive index 1.342 using a 60x NA 1.4 oil immersion objective (Olympus, Center Valley, PA, USA) using immersion oil with refractive index 1.515. This was repeated for increasing laser power from 12.5-60 mW.

To analyze the spectral data, a 20x20 pixel square region was placed around each of 3-20 microspheres from each image. A 20x20 pixel square region was used to collect background data. The integrated intensity in each region was recorded. To find the fluorescence intensity of the microsphere, the integrated intensity in the background region was subtracted from the integrated intensity of the 20x20 pixel square region

surrounding the microsphere. The data from the microspheres in each image were then averaged and plotted versus laser power.

### 3. *Image collection*

The images were 512x512 pixels with XY pixel dimension of 0.101 microns. The axial step size was 0.10 microns. The pixel dwell time was 2.0 microseconds, and lines were Kalman averaged x2. The excitation wavelength was 800 nm. Fluorescence saturation was measured as described, and laser power was maintained constant for all images and below saturating levels. Images were collected using descanned detectors with the confocal pinhole maximally open. The PMT gain was constant and below PMT saturation, and PMT black level was constant for all images collected. A leveling apparatus mounted on the stage was used to ensure the coverslip was perpendicular to the light path [169]. Seven to ten image volumes were collected of each sample. The experiment was repeated three times for each sample.

### 4. *Signal attenuation analysis*

Data were analyzed using ImageJ [170] and a custom plugin written at the Indiana Center for Biological Microscopy which returns the fluorescence intensity of each microsphere, the image plane number of each microsphere, and the background intensity of the image volume. Fluorescence intensity of a microsphere was quantified as the average value of the 3x3x3 voxel region within the image of the microsphere with maximal integrated fluorescence intensity. The image plane number of the microsphere was determined from the center of this 3x3x3 voxel region. Background signal in each image volume was determined from the average intensity of the last ten image planes collected, below the microspheres mounted on the slide at the bottom of the image, and

was subtracted from the fluorescence intensity of each microsphere. The depth of each microsphere was measured in microns from the coverslip-sample interface, based on the physical movement of the objective, referred to as the nominal focal position (*NFP*). The *NFP* is calculated

$$NFP = z_{step} * (n_{plane} - n_{offset})$$

where  $z_{step}$  is the axial step size (0.10 microns/plane),  $n_{plane}$  is the image plane number of the microsphere, and  $n_{offset}$  is calculated by averaging the image plane numbers of all microspheres located at the coverslip. Microspheres were assumed to be located at the coverslip if they were within six image planes of the shallowest microsphere. Axial scaling from refractive index mismatch was not measured.

The data from three trials were combined and averaged in intervals such that there were 25 microspheres per bin. The intervals began at 0.5 microns deep to exclude microspheres that were dried on the coverslip and only include microspheres mounted within agarose. Bin widths ranged from 0.61 to 8.00 microns wide. Because we attempted to distribute the microspheres homogeneously within the agarose, the bin width was not related to depth in the sample.

The average intensity of the microspheres located at the coverslip was calculated and used to normalize the data. The error for the normalization of the data at the coverslip was calculated

$$|\delta_{normalization,n}| = \left( \frac{\sqrt{2}}{\langle x \rangle_{coverslip,n}} \right) * \delta_{coverslip,n}$$

where  $\langle x \rangle_{coverslip,n}$  is the average intensity of the microspheres located at the coverslip for three trials of samples with refractive index  $n$  and  $\delta_{coverslip,n}$  is the standard error for

the intensity of the microspheres located at the coverslip for three trials of samples with refractive index  $n$ .

5. *Resolution degradation analysis*

Axial resolution was measured using the image volumes collected of 0.2 micron fluorescent microsphere mounted in agarose samples. Although 0.2 microns is close to the lateral resolution of the microscope, measured to be 0.3 microns using the Olympus 60x NA 1.4 oil immersion objective, it is much less than the axial resolution, measured to be 0.9 microns using 800 nm two-photon excitation and collected using a 560-660 nm emission filter, and is therefore a reasonable size for axial resolution analysis.

Data were analyzed using ImageJ [170] and a custom plugin written at the Indiana Center for Biological Microscopy which returns pixel values from the line of pixels running axially through the center of the microsphere and the image plane number of the center of the microsphere. The center of the image of the microsphere was determined from the 3x3x3 voxel region within the image of the microsphere with maximal integrated fluorescence intensity. The *NFP* was calculated as described in *Signal attenuation analysis*. The FWHM for the fluorescence intensity distribution from each microsphere was then calculated by curve fitting the data using SigmaPlot (Systat Software, Inc., San Jose, CA, USA). The data were fit to a four parameter Gaussian curve

$$y = y_0 + ae^{-0.5\left(\frac{x-x_0}{b}\right)^2}.$$

The FWHM was then calculated

$$FWHM = 2b\sqrt{2\ln(2)} * z_{step}$$

where  $b$  is a fitting parameter from the four parameter Gaussian curve and  $z_{step}$  is the axial step size (0.10 microns/plane).

The data from three trials were combined and averaged in intervals such that there were 30 microspheres per bin. The intervals began at 0.5 microns deep to exclude microspheres that were dried on the coverslip and only include microspheres mounted within agarose. Bin widths ranged from 0.65 to 8.11 microns wide.

#### *D. Excitation attenuation*

##### *1. Image collection*

Agarose samples were mounted as described in *Agarose sample preparation*. Photobleaching data were collected by first focusing on a microsphere using very low excitation power (as determined by causing undetectable photobleaching after five minutes of continuous scanning). Once the microsphere was in focus, 300 images were collected at approximately 1 frame per second of this single image plane using an Olympus 60x NA 1.4 oil immersion objective. Laser power was measured and maintained constant just below the level that causes fluorescence saturation at the surface of the sample.

The nominal focal position (*NFP*) of each microsphere was measured from the coverslip based on the physical movement of the objective. Images were collected for microspheres located in 3-10 depths in each sample. The experiment was repeated three times for samples with each refractive index.

Fluorescence saturation was assessed by measuring laser power immediately following attenuation of the Pockels cell and then collecting an image of fluorescent



microspheres mounted on a #1.5 coverslip. This was repeated for a range of laser powers to determine at what laser power fluorescence intensity stopped depending quadratically on excitation power, indicating saturation of the fluorophore. Five images were collected at each laser power.

To minimize effects from variable levels of reactive oxygen species from sample to sample, the described agarose samples were mounted in sucrose solutions with 2% 1,4-Diazabicyclo(2,2,2)octane (DABCO), a singlet oxygen quencher [171].

## 2. *Excitation attenuation analysis*

Photobleaching depends on excitation power and is independent of collection efficiency [172]. Hence, photobleaching was measured as a function of depth to determine the effect of spherical aberration on fluorescence excitation as a function of depth.

For each image plane, the integrated intensity of pixels in a 20x20 region around a microsphere was calculated using MetaMorph Image Processing software version 4.6r5 (Molecular Devices, Downingtown, PA). A 20x20 region was placed in each image that contained no microsphere to measure the integrated intensity of the background. The background was subtracted from the integrated intensity of each 20x20 region containing a microsphere.

The fluorescence intensity did not decay exponentially during photobleaching; therefore, an exponential fit could not be used to determine the photobleaching rate. We have confirmed by overlaying curves (data not shown), however, that over long intervals the intensity is a universal function of  $\frac{t}{\tau_d}$  where  $t$  is time, and  $\frac{1}{\tau_d}$  is the depth dependent photobleaching rate. Therefore the intensity at depth  $d$  can be written as

$$I_d = I_{0d} f\left(\frac{t}{\tau_d}\right)$$

where  $I_0$  is the intensity at  $t = 0$  seconds.

This was done by first averaging the background subtracted intensity versus time data from each microsphere within the field. Intensity versus time data were then averaged for each microsphere within a five micron interval in depth. Intensity versus time data were then normalized to the intensity at  $t = 0$  seconds.

The normalized intensity versus time curve from the image plane collected at the surface of the sample was then scaled in time by multiplying the time axis by an empirical constant  $c_d$  such as to make the normalized intensity curves for all depths coincide. This constant  $c_d$  was determined by

$$c_d = \frac{t_d}{t_0}$$

where  $t_d$  is 5 minutes of photobleaching at depth  $d$  and  $t_0$  is the time at which

$$f\left(\frac{t_0}{\tau_0}\right) = \frac{I_{t_0}}{I_{0_0}} = \frac{I_{t_d}}{I_{0_d}} = f\left(\frac{t_d}{\tau_d}\right)$$

where  $I_{t_0}$  is the intensity at the surface of the sample at time  $t_0$ ,  $I_{t_d}$  is the intensity at depth  $d$  after five minutes of photobleaching. Therefore,  $t_0$  is the time necessary to photobleach the surface of the sample such that the normalized intensity at the surface  $\frac{I_{t_0}}{I_{0_0}}$  is equal to  $\frac{I_{t_d}}{I_{0_d}}$ , the normalized intensity after 5 minutes of photobleaching at depth  $d$ .

Therefore we found that for each depth there exists a constant  $c_d$  such that the curves overlaid each other, and thus there exists a universal curve  $f\left(\frac{t}{\tau_d}\right)$  valid for all depths.

This was repeated for each depth in five micron intervals.

Because there exists a universal curve valid for all depths, we can determine the depth dependence of the photobleaching rate  $\frac{1}{\tau_d}$  in our sample. For each depth  $d$  the photobleaching rate was normalized to its surface value as

$$\frac{\tau_0}{\tau_d} = \frac{t_0}{t_d} = \frac{1}{c_d}$$

where  $t_d = 5$  minutes. Hence,  $\frac{\tau_0}{\tau_d}$  is equivalent to the ratio of scales in the time axis to make  $\frac{I_{t_d}}{I_{0d}}$  curves for all depths coincide. Normalized photobleaching rates were averaged from the three trials.

Because there exists a universal curve  $f\left(\frac{t}{\tau_d}\right)$  valid for all depths, we could have used the time derivative of the function at  $t = 0$  seconds to find  $\tau_d$ . For  $t_d^* \ll \tau_d$ ,

$$\left. \frac{\partial f_0}{\partial t'} \right|_{t_0^*} = \left. \frac{\partial f_d}{\partial t'} \right|_{t_d^*}$$

where  $t' = \frac{t}{\tau_d}$  and  $f_d = f\left(\frac{t}{\tau_d}\right)$ .

### 3. *Excitation attenuation calibration data collection*

Calibration data was measured using fluorescent microspheres dried on a #1.5 coverslip (Corning, Lowell, MA, USA). The laser power was measured immediately following attenuation by the Pockels cell. Photobleaching data were collected as described above for five different fields at each laser power over a range below fluorescence saturation. The experiment was repeated three times.

## *E. Emission attenuation*

### *1. Calculation based on signal and excitation data*

Signal attenuation with depth results from the combined effect of the depth-dependent decrease in excitation of fluorescence and the decrease in collection of fluorescence emissions. By measuring signal attenuation with depth and excitation attenuation with depth, emission attenuation with depth can be estimated from

$$I_s = I_e^2 * I_c$$

where  $I_s$  is signal intensity normalized to the surface of the sample,  $I_e$  is the excitation intensity calculated from the photobleaching rate and normalized to the surface of the sample, and  $I_c$  is the corresponding collection intensity normalized to the surface of the sample.

To calculate the excitation intensity  $I_e$  from the photobleaching rate, the excitation calibration data was plotted on a log-log scale, and a linear fit was used to determine the power relationship between the photobleaching rate and the excitation power

$$R = I_e^p$$

$$\log R = p \log I_e$$

where  $R$  is the photobleaching rate,  $I_e$  is the excitation intensity, and  $p$  is the power relationship. Excitation intensity versus depth could then be calculated from the photobleaching rate versus depth measurements. Because excitation is nonlinear based on a two-photon process, the excitation intensity is then squared for direct comparison to the measured signal attenuation with depth.

The fluorescence signal intensity was averaged for 20 microspheres centered every five microns deep into the sample and normalized to the average fluorescence intensity at the surface of sample. Bin widths varied from 2.53 to 5.44 microns wide.

The fraction of signal attenuation with depth that can be attributed to emission attenuation is thus calculated

$$I_c = \frac{I_s}{I_e^2}$$

for five micron intervals deep into the sample.

## 2. *Comparison of descanned and non-descanned detectors*

To compare signal attenuation using descanned detectors with the pinhole maximally open and non-descanned detectors, image volumes were collected of an agarose sample with refractive index 1.342 containing 0.2 micron fluorescent microspheres (as described). Images were collected using the descanned detector as described and then the same fields were collected using the non descanned detector. The non-descanned detector is a GaAsP PMT (Hamamatsu H7422P-40) mounted on the right side port of an Olympus IX-81 microscope, along with a focusing lens (CVI BFPL-25.4-50.0-C-425-675) and 560-650 nm bandpass filter (Chroma HQ605/90M-2P). To avoid effects from photobleaching, in some cases images were collected with the non-descanned detector before collection with the descanned detector.

## F. *Analysis of outliers*

Data were omitted from analysis if fluorescence from the microsphere saturated the detector, or if the fluorescence intensity was greater than double that of other

microspheres at the same depth, indicating the microsphere was an aggregation. The data were then tested statistically to eliminate questionable outliers [173].

*G. Immunofluorescence image collection*

Five to ten XZ cross-sectional images were collected for each immunofluorescent kidney tissue sample. The images were collected with lateral pixel dimension of 0.345 microns and axial step of 0.35 microns. The pixel dwell time was 4.0 microseconds. The excitation wavelength was 800 nm. Images were collected using descanned detectors with the confocal pinhole maximally open. The gain and black level of the PMT were kept constant for all images collected. Because fluorescence intensity varied widely between samples mounted in the different media, the laser power was adjusted such that the image at surface of the tissue was just below PMT saturation.

The image volume of the glomerulus was collected using non-descanned detectors mounted on the right side port of an Olympus IX-81 microscope. The blue channel was collected using a bialkali PMT (Hamamatsu R1924AHA) and a 380-480 nm bandpass filter (Chroma HQ430/100M-2P). The green channel was collected using a multialkali PMT (Hamamatsu R6357HA) and a 500-550 nm bandpass filter (Chroma HQ525/50M). And the red channel was collected using a multialkali PMT (Hamamatsu R6357HA) with a 560-650 nm bandpass filter (Chroma HQ605/90M-2P). The image volume was collected with lateral pixel dimension of 0.414 microns and axial step of 0.41 microns. The pixel dwell time was 4.0 microseconds and lines were Kalman averaged x3. The excitation wavelength was 800 nm.

### III. RESULTS

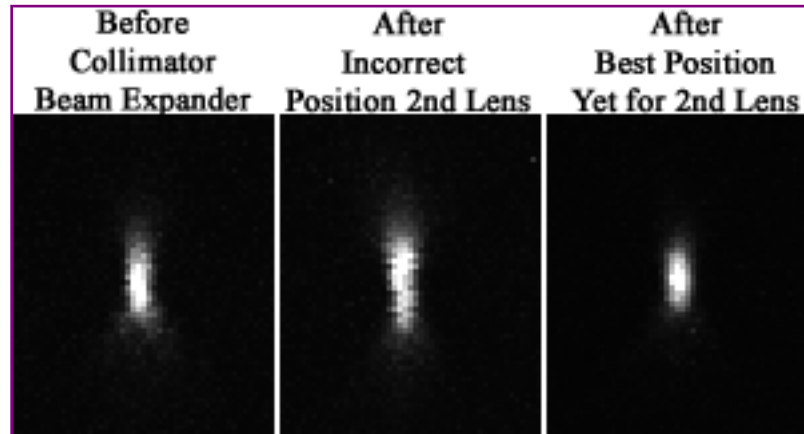
#### **Chapter 1. The Effect of Spherical Aberration on Multiphoton Microscopy**

##### *A. Alignment of the two-photon excitation light path*

The two-photon excitation light path was aligned such that 800 nm excitation light for a Mai Tai Ti:S laser was both centered in the objective lens and traveling perpendicular to the lens. Using a Keplerian beam expander/collimator, the laser beam was expanded 1.25x to fill the back aperture of an Olympus 60x oil immersion NA 1.4 objective with a back aperture of 8.4 mm. Figure 7 shows images of the axial PSF of the system. When the second lens of the collimator is misaligned, the laser beam diverges, and the PSF increases axially. When the collimator is aligned, the back aperture of the objective is filled and stray light is eliminated so the excitation beam forms a compact PSF.

##### *B. Characterization of suncoast yellow 0.2 micron microspheres*

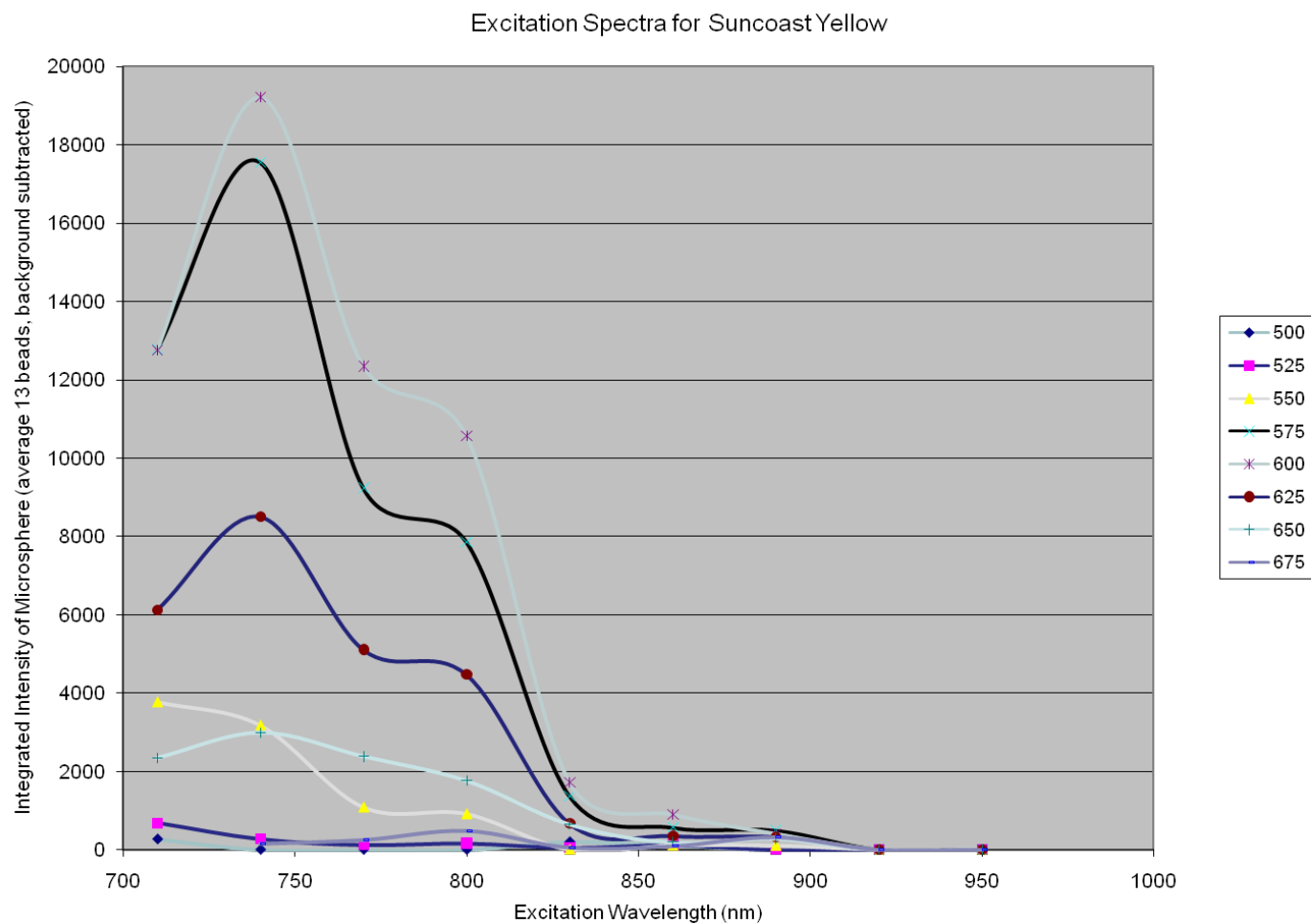
The excitation and emission spectra were measured for the 0.2 micron diameter microspheres labeled with suncoast yellow. A spectral scan was collected from 500-700 nm with 25 nm bandwidth and 25 nm step size. This was repeated for excitation wavelengths 710, 740, 770, 800, 830, 860, 890, 920, and 950 nm. The laser power was measured for each excitation wavelength and maintained constant. Figure 8 shows the excitation spectra for suncoast yellow with a peak excitation wavelength at 740 nm for all



**Figure 7. Beam expander/collimator alignment**

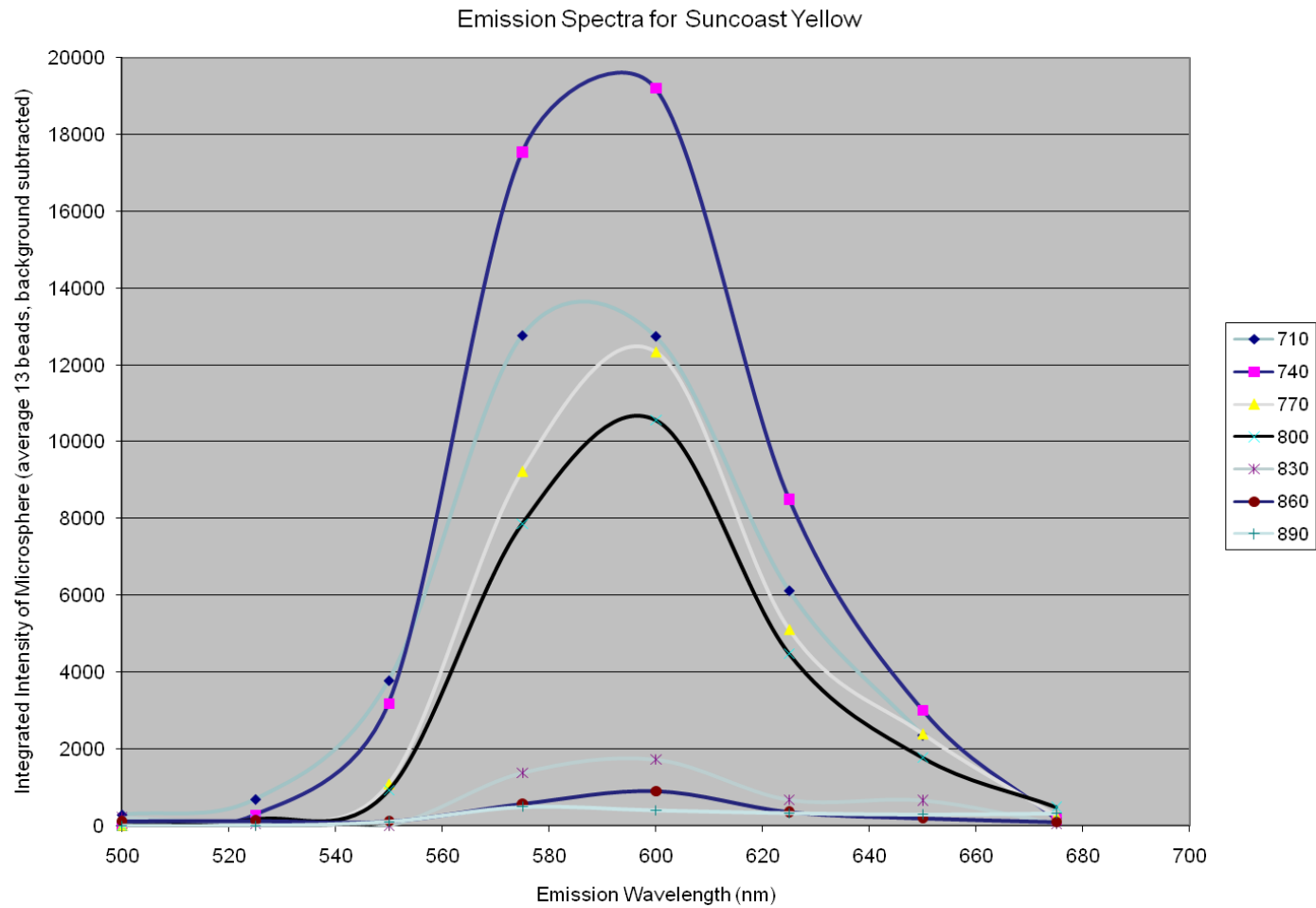
XZ projected images of sub-resolution microspheres mounted on #1.5 coverslip. Comparison of the PSF before the collimator was installed, after the collimator was installed but with incorrect alignment of the collimating lens, and after alignment such that the excitation beam is collimated and filling the back aperture of the objective.





**Figure 8. Excitation spectra for suncoast yellow 0.2 micron microspheres**

Suncoast yellow 0.2 micron microspheres mounted on #1.5 coverslip. Legend indicates emission wavelength (nm).



**Figure 9. Emission spectra for suncoast yellow 0.2 micron microspheres**

Suncoast yellow 0.2 micron microspheres mounted on #1.5 coverslip. Legend indicates excitation wavelength (nm).

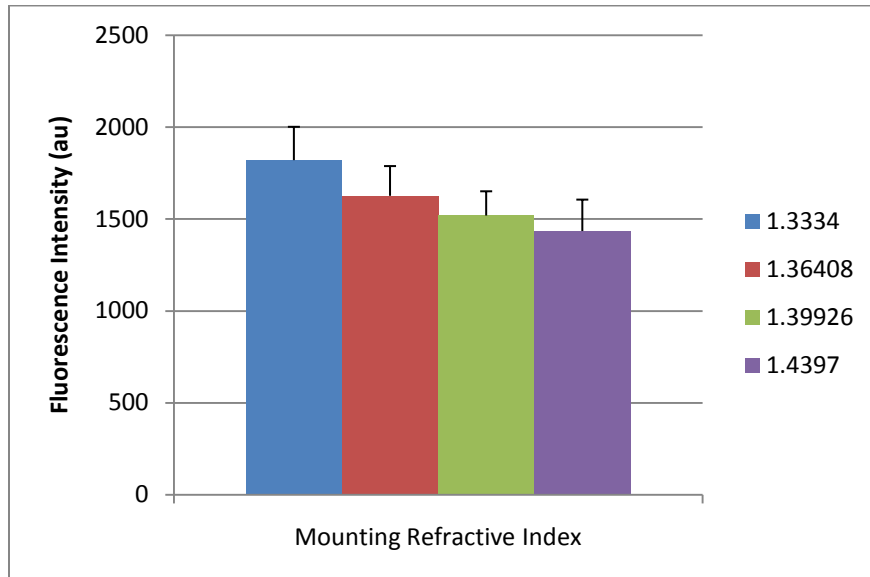
emission wavelengths measured. Figure 9 shows the emission spectra for suncoast yellow with peak emission wavelengths in the range of 575-600 nm for all excitation wavelengths. However for our studies, we used an excitation wavelength of 800 nm because 740 nm excitation caused extremely fast photobleaching (data not shown) and would have required such low laser power, it would have required additional optics to attenuate the laser enough to measure the fluorescence saturation curve.

*C. Effects from the media at the coverslip*

The fluorescence intensity of 0.2 microns microspheres at the coverslip-sample interface was compared for samples with different refractive index to investigate possible effects from the sucrose solutions on fluorescence intensity. Figure 10 shows that increasing sucrose concentration not only increased refractive index but also caused immediate decrease in fluorescence at the surface of the sample. Therefore to assess signal attenuation, fluorescence intensity data were normalized to the intensity at the surface of the sample.

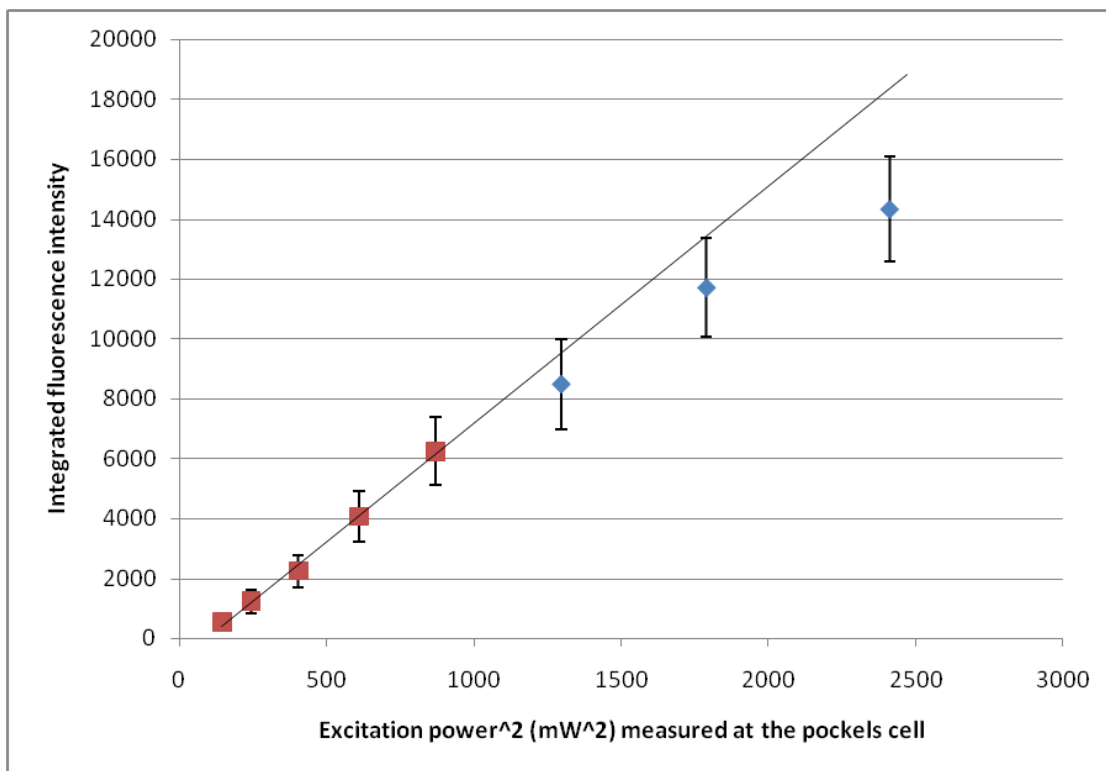
*D. Fluorescence saturation*

Fluorescence saturation was measured for suncoast yellow labeled 0.2 micron microspheres. The fluorescence intensity of microsphere dried on the coverslip and mounted with a 1.342 agarose sample was measured for laser powers ranging from 12.5-60 mW after each realignment of the excitation path (Figures 11-13). Fluorescence saturation was found to occur after 30 mW of excitation power, measured at the Pockels cell. Therefore, 30 mW was the excitation power used for our studies.



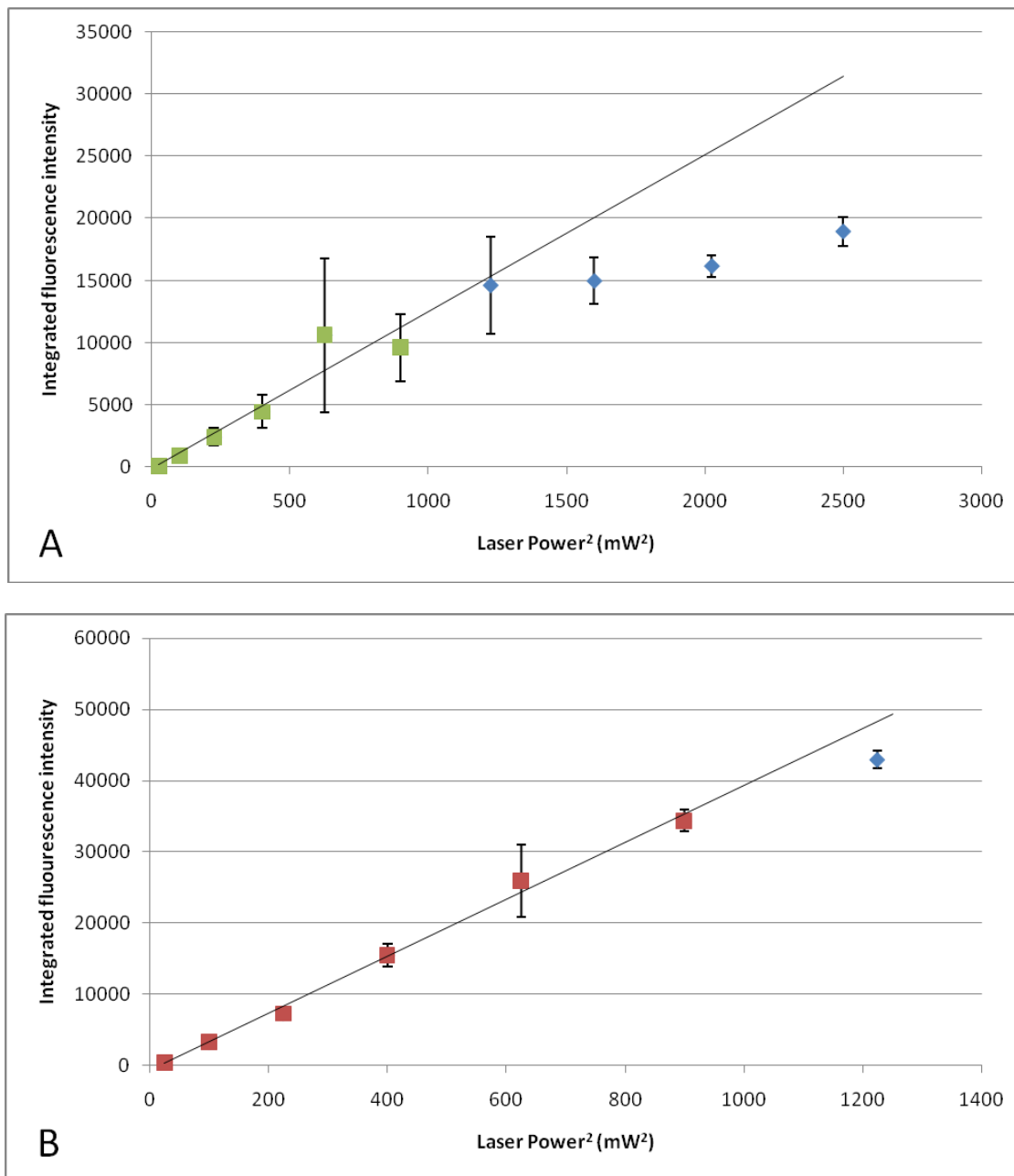
**Figure 10. Comparison of fluorescence intensity at the coverslip-sample interface for samples with different refractive index**

Fluorescence intensity was measured at the coverslip-sample interface for samples with different refractive index.



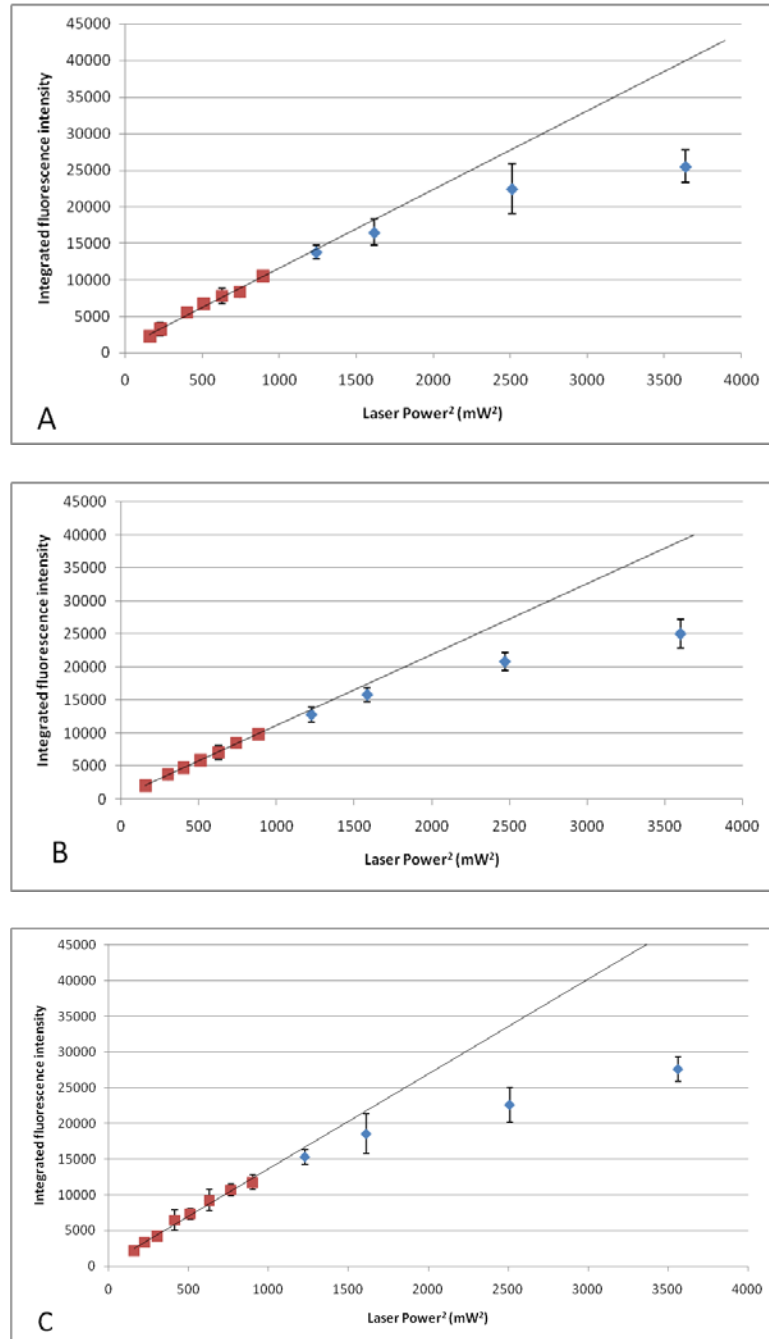
**Figure 11. Fluorescence saturation data**

Fluorescence saturation measured after excitation light path alignment before the signal attenuation study. Suncoast yellow 0.2 micron microspheres mounted on #1.5 coverslip. Each data point represents 50 microspheres collected in five images. Linear fit of data for the first 30 mW. Data collected with 800nm excitation wavelength, 600V detector gain, and XY pixel dimensions of 0.207um.



**Figure 12. Fluorescence saturation data**

Fluorescence saturation measured after excitation light path alignment before the excitation attenuation study without DABCO. Suncoast yellow 0.2 micron microspheres mounted on #1.5 coverslip. Laser power was measured at the Pockels cell. Data collected with 800nm excitation wavelength and 0.101 micron XY pixel dimensions. A) Each data point represents three images with 4-13 microspheres. Data collected with 540V detector gain. Linear fit of data for the first 30 mW. B) Each data point represents three images with 3-15 microspheres. Data collected with 640V detector gain. Linear fit of data for the first 30 mW.



**Figure 13. Fluorescence saturation data**

Fluorescence saturation measured after excitation light path alignment before the excitation attenuation study with DABCO. Suncoast yellow 0.2 micron microspheres mounted on #1.5 coverslip. Laser power was measured at the Pockels cell. Data collected with 800nm excitation wavelength, 535V detector gain, and 0.101 micron XY pixel dimensions. Linear fit of data for the first 30 mW. A) Each data point represents three images with 4-25 microspheres. B) Each data point represents three images with 4-14 microspheres. C) Each data point represents three images with 5-20 microspheres.

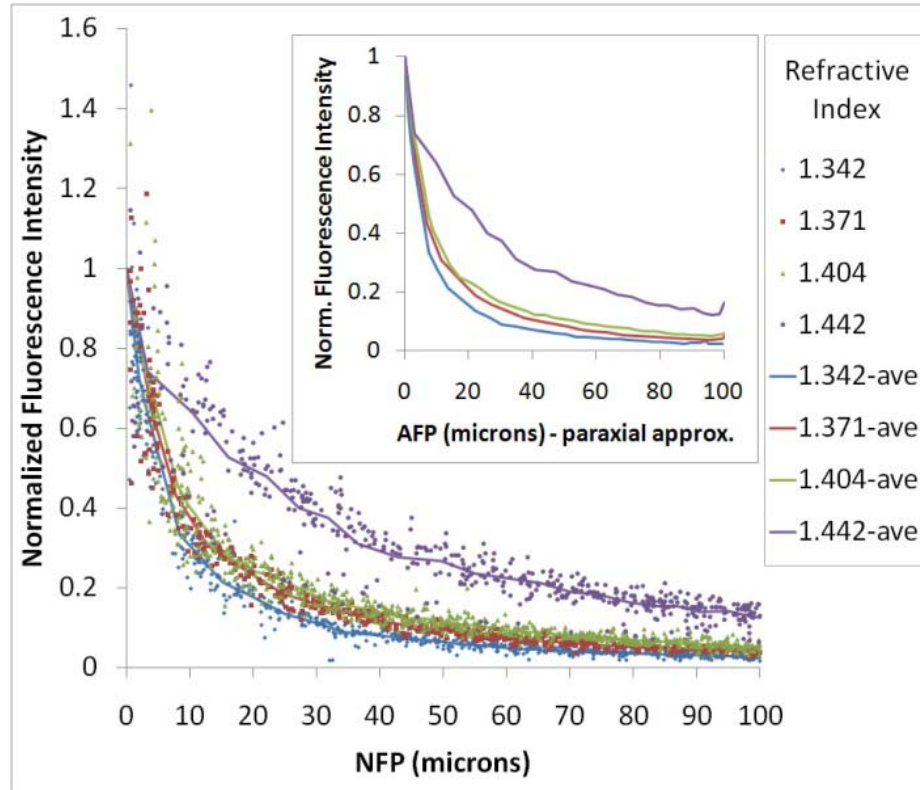
### *E. Signal attenuation*

Since two-photon fluorescence excitation is quadratically related to photon density, spherical aberration would be expected to diminish fluorescence excitation at depth into refractive index mismatched samples. In order to isolate the effects of spherical aberration on multiphoton fluorescence excitation, test samples were prepared with minimal light scattering and absorption to assess the effects of refractive index mismatch between the immersion medium, coverslip, and sample. Fluorescent microspheres were suspended in samples of agarose, prepared with different refractive indices using sucrose solutions. Images were collected with a 60X oil immersion objective NA 1.4. The average intensity of the microspheres located at the coverslip was calculated and used to normalize the data. Data from the individual microspheres at the coverslip are not plotted to improve visualization because among the 12 trials there are 597 individual microspheres at the surface of the samples (Figure 14). The error for the normalization of the data at the coverslip was calculated to be 2 % for each of the four samples.

In all cases fluorescence intensity decreased with depth. However, as expected, fluorescence intensity did not decrease as quickly in samples with refractive index closer to the refractive index of the immersion oil, 1.515. In fact, at 40 microns deep into the sample there is a 3.5-fold improvement in fluorescence signal in a sample with refractive index 1.442 compared to a sample with refractive index 1.342.

Refractive index mismatch not only broadens the focal point, but it also causes a focal shift [132]. In all samples, because the refractive index is less than that of the immersion oil, the focal point will be increasingly offset toward the coverslip with depth





**Figure 14. Fluorescence signal attenuation**

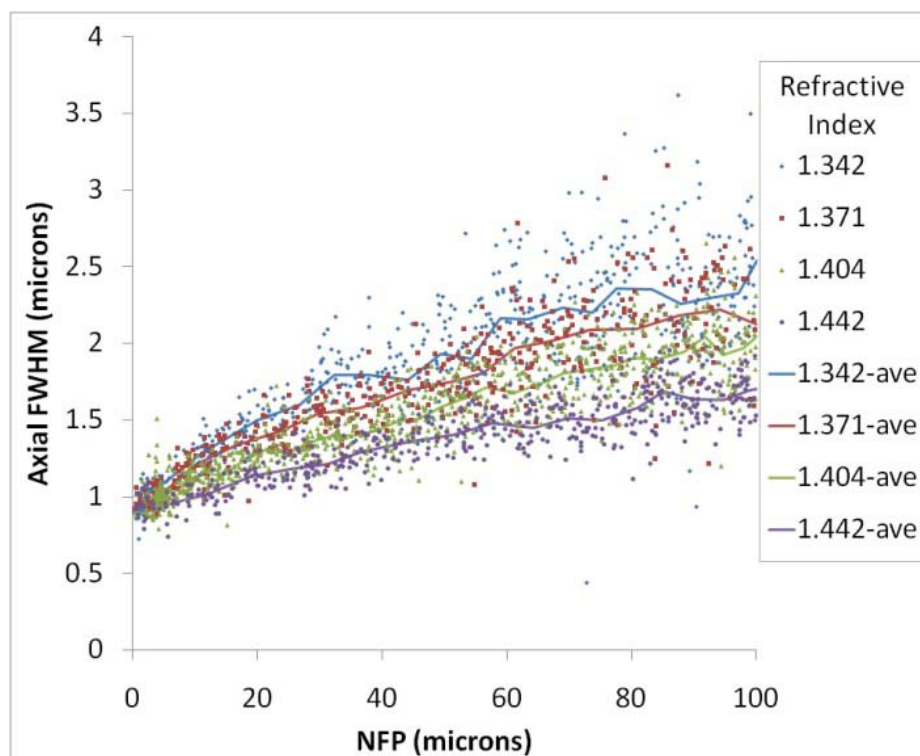
Fluorescence intensity of 0.2 micron microspheres mounted in agarose with varying refractive index, normalized to the average intensity at the surface, versus NFP. Images collected with 60x oil immersion objective NA 1.4 with immersion oil (refractive index 1.515). Lines represent the average of data from 25 microspheres per bin. Bin widths varied from 0.61 to 8.00 microns wide. Inset: Average normalized fluorescence intensity versus depth, where depth has been scaled using the paraxial approximation.

into the sample. In samples with refractive index 1.342, this offset is larger than in samples with refractive index 1.442. Therefore the NFP, the measurement of depth based on the physical movement of the stage, overestimates the AFP. By scaling depth using a paraxial approximation, the ratio of the refractive index of the sample to the refractive index of the immersion oil [133], the effect of refractive index mismatch on signal becomes even more pronounced (Figure 14-Inset). Using the paraxial approximation to scale imaging depth, at 40 microns deep into a sample with refractive index 1.442, there is a 3.9-fold improvement in fluorescence signal over a sample with refractive index 1.342.

#### *F. Resolution degradation*

The effects of spherical aberration on resolution are hard to predict knowing that decreased photon flux leads to decreased excitation. Axial resolution was measured as the FWHM of the intensity distributed axially through the centroid of point spread functions of sub-resolution microspheres mounted in agarose samples. At the surface of the samples the axial resolution was measured with standard error to be  $0.893 \pm 0.005$ ,  $0.908 \pm 0.006$ ,  $0.870 \pm 0.014$ , and  $0.928 \pm 0.005$  microns (mean  $\pm$  standard error) for the samples with refractive index 1.342, 1.371, 1.404, and 1.442 respectively. Data from individual microspheres at the coverslip are not plotted to improve visualization, only the average FWHM (Figure 15).

In all cases axial resolution degrades with imaging depth. However, the effect of depth on resolution is less pronounced in samples whose refractive index is closer to that of the immersion oil. Axial resolution degrades to 1.7 microns, nearly two-fold worse, at



**Figure 15. Axial resolution degradation**

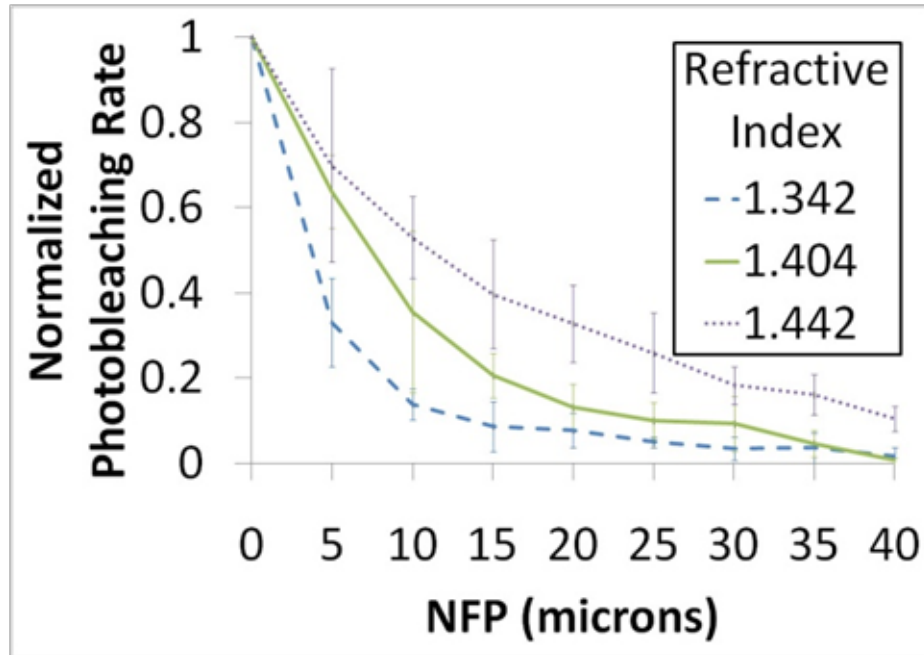
Axial intensity distribution FWHM of 0.2 micron fluorescent microspheres mounted in agarose with varying refractive index versus NFP. Images collected with 60x oil immersion objective NA 1.4 with immersion oil (refractive index 1.515). Lines represent the average of data from 30 microspheres per bin. Bin widths varied from 0.65 to 8.11 microns wide.

100 microns of depth into the sample with refractive index 1.442 but in less than 30 microns of depth into the sample with refractive index 1.342. At 100 microns deep into the sample with refractive index 1.342, axial resolution is 2.5 microns, nearly 3-fold worse than at the surface.

*G. Excitation attenuation*

*1. Photobleaching rate*

Because MPM relies on a multiphoton process, fluorescence excitation is highly dependent on photon density. Therefore, we expect the preponderance of the signal attenuation with depth in a refractive index mismatched sample to result from decreased fluorescence excitation with depth. Since it is not possible to directly measure the rate of fluorescence excitation, the effect of refractive index mismatch between the immersion medium, coverslip, and sample on two-photon excitation was assessed indirectly by measuring the effect of depth on photobleaching rates, which do not depend on fluorescence collection, only fluorescence excitation. Quantification of the rate of photobleaching of fluorescent microspheres mounted in agarose samples showed that photobleaching rates decreased with imaging depth (Figure 16). However, the rate of photobleaching at depth was higher in samples with refractive index closer to that of the immersion oil. At 30 microns, the sample with refractive index 1.442 had over 7-fold greater photobleaching than the sample with refractive index 1.342. The increase in photobleaching rate at depth indicates that refractive index mismatch markedly affects fluorescence excitation.



**Figure 16. Photobleaching rate attenuation**

Photobleaching rate normalized at the surface of the sample versus NFP. Images were collected with 60X oil immersion objective NA 1.4 with immersion oil (refractive index 1.515) for five minutes of 0.2 micron fluorescent microspheres mounted in agarose samples with varying refractive index. Photobleaching rate was calculated for the average of 10-15 microspheres in 5 micron intervals and normalized to the photobleaching rate at the surface. Error bars represent standard deviation of three trials.

## 2. *Excitation power versus photobleaching rate*

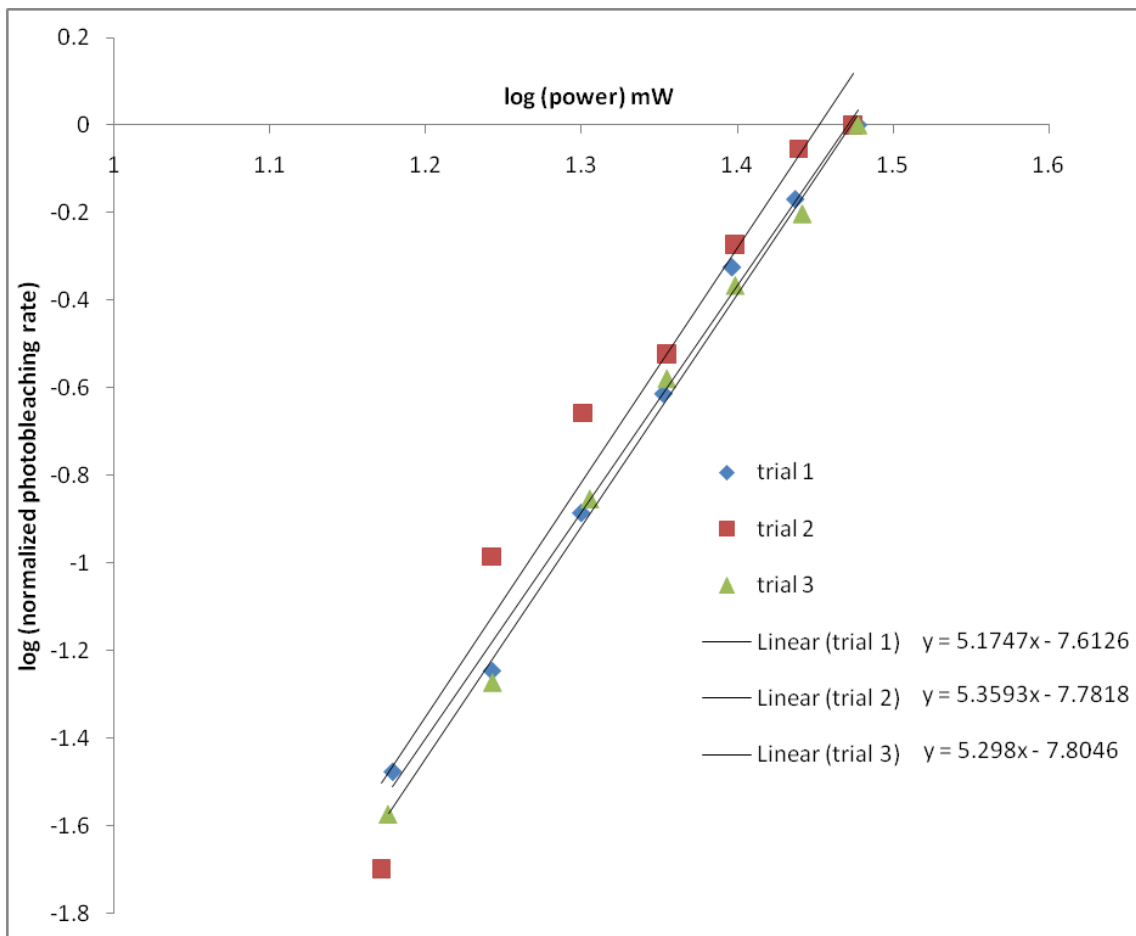
Photobleaching data were measured at the coverslip-sample interface for different laser powers to develop a calibration curve to convert photobleaching data to fluorescence excitation power (Figure 17). Excitation intensity data could then be compared directly to data calculated from a geometrical model of excitation intensity distribution. And by squaring the excitation intensity data to predict fluorescence excitation, we are able to compare these values with measured fluorescence signal to calculate fluorescence emission attenuation at depth.

We found that the photobleaching rate of suncoast yellow label microspheres is 5.2-power of excitation which is very different from the intensity-squared dependence of fluorescence excitation. Similarly, Patterson and Piston [127] measured photobleaching rates of different fluorophores and found them to depend on  $\geq 3$  power of the excitation intensity, with aminocoumarin dextran as high as  $5.1 \pm 0.2$ .

### *H. Emission attenuation*

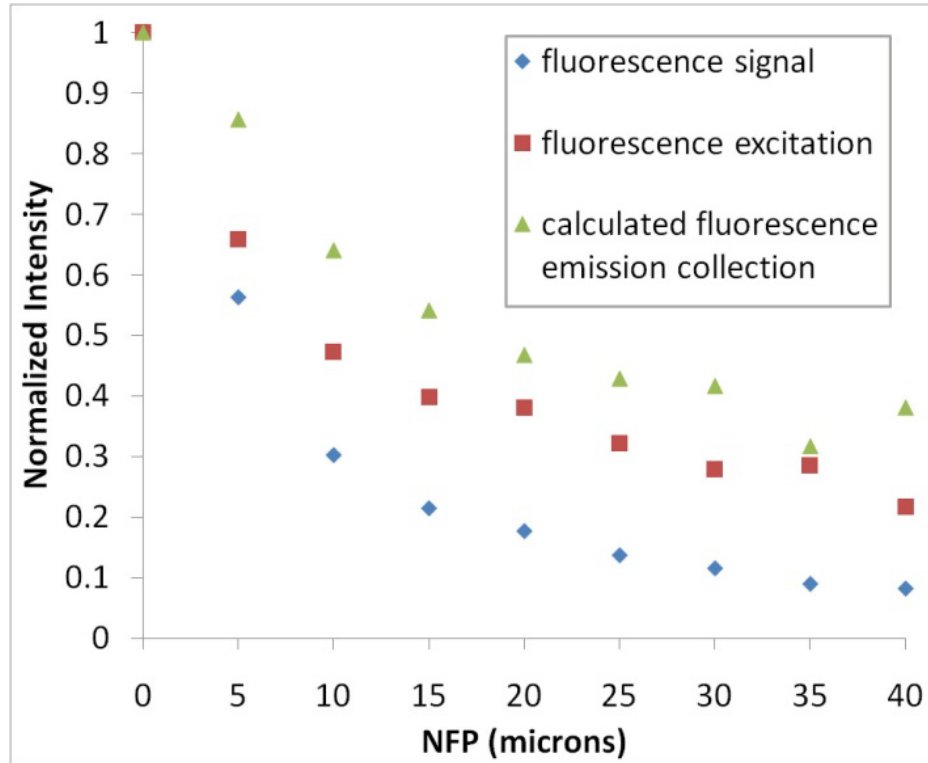
#### 1. *Fluorescence signal versus fluorescence excitation*

On first principles, signal attenuation with depth is caused by attenuation of fluorescence excitation and decreased collection efficiency of fluorescent emissions. Based on the measurements of signal attenuation and excitation attenuation with depth, the contribution of emission attenuation can be inferred. Excitation attenuation is shown to be the predominant contributor to signal attenuation (Figure 18). At 40 microns deep into the sample, only 20% of fluorescence is excited compared to fluorescence excitation



**Figure 17. Calibration data**

Photobleaching data were collected of 0.2 micron fluorescent microspheres dried on the coverslip mounted with agarose sample with 2% DABCO and refractive index 1.342. Data were collected for laser powers measured at the Pockels cell in the range of 12.5-30mW. Images were collected with an Olympus 60X oil immersion objective NA 1.4.



**Figure 18. Emission attenuation**

Signal attenuation and excitation attenuation versus NFP measured in agarose samples with refractive index 1.342 using a 60x oil immersion objective NA 1.4 with immersion oil (refractive index 1.515). Signal attenuation data are the average of data from 20 microspheres centered every five microns deep and normalized to the average fluorescence intensity at the surface. Excitation attenuation data are calculated from the photobleaching rates every five microns deep. Calculated fluorescence emission collection attenuation versus NFP calculated every five microns deep.



at the surface of the sample. Therefore, fluorescence excitation is attenuated by nearly 80%. However 40% of fluorescence emissions were collected at 40 microns deep into the sample compared to collection at the surface of the sample. Therefore, collection of emissions is attenuated by only about 60%.

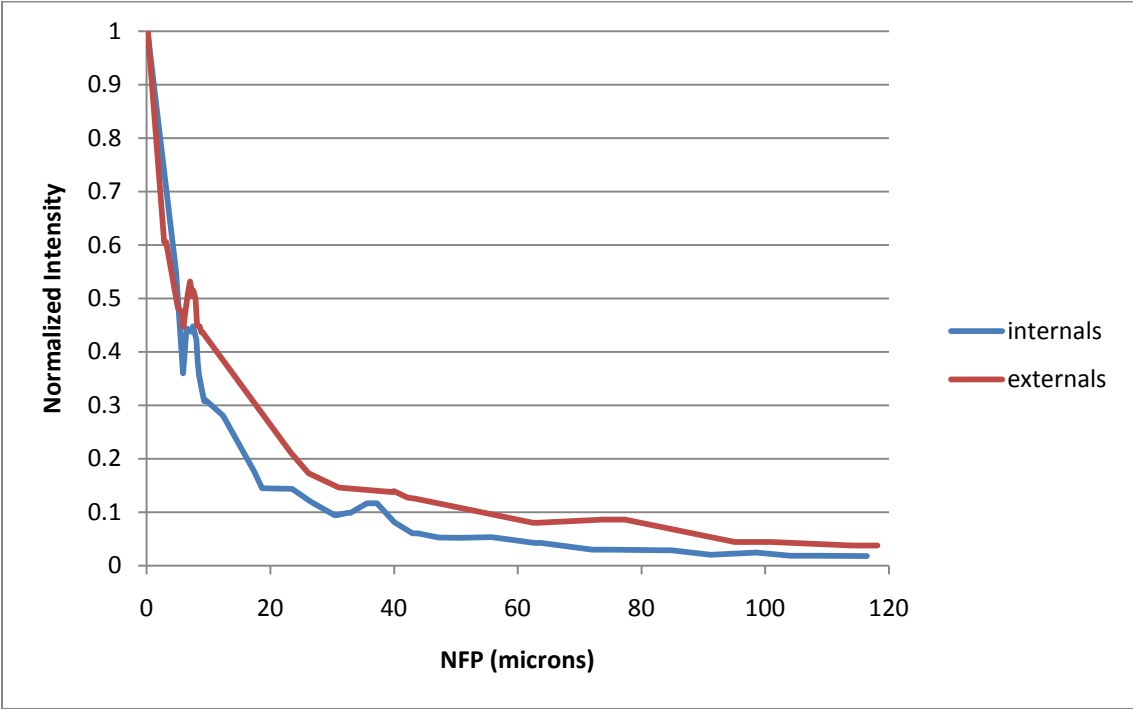
## 2. *Comparison of descanned and non-descanned detectors*

Non-descanned detectors have been shown to improve collection of scattered light, reducing the excitation power and detector gain necessary to generate bright images [116]. To assess how signal attenuation with depth compares between non-descanned and descanned detectors, image volumes were collected of agarose samples, refractive index 1.34 (Figure 19). At 50 microns in depth, signal attenuated by 92%, using non-descanned detectors, and by 95%, using the descanned detectors with the pinhole open fully. Therefore although non-descanned detectors collect over 60% more scattered light at 50 microns deep than descanned detectors, that only amounts to 3% more signal at 50 microns in depth.

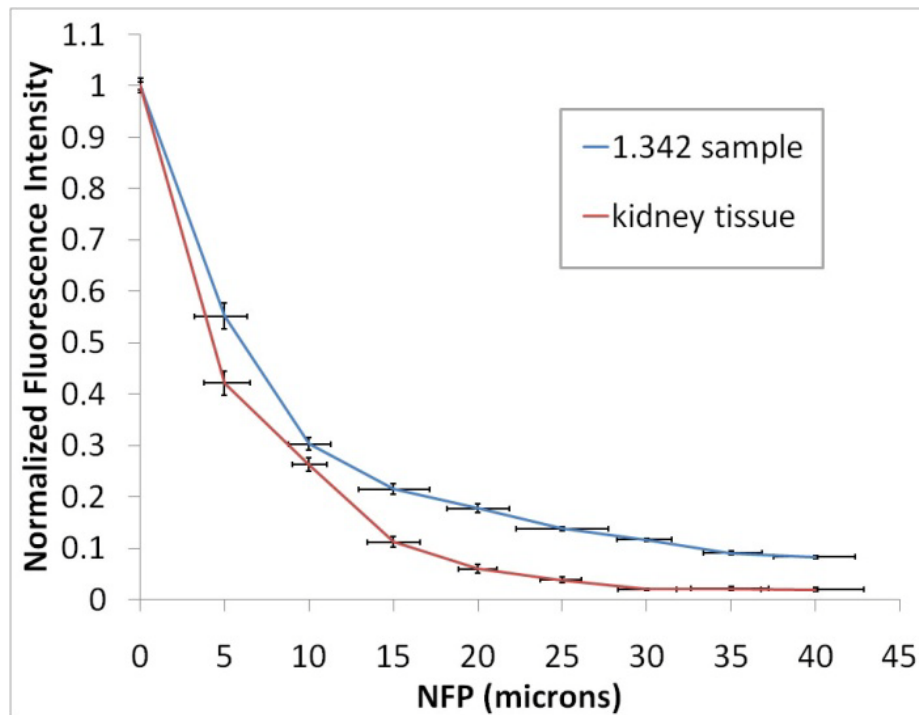
## I. *Signal attenuation in kidney tissue*

### 1. *Comparison of agarose and kidney tissue samples*

Images were collected of kidney tissue mounted in PBS, with refractive index 1.34, using an oil immersion objective. The rate of signal attenuation with depth into kidney tissue was compared to that found in an agarose sample with refractive index 1.342 (Figure 20). Spherical aberration was shown to cause 88% of signal to attenuate at 30 microns deep in a sample with refractive index 1.342. In fixed kidney tissue mounted



**Figure 19. Comparison of descanned and non-descanned detector**  
Signal attenuation data measured using suncoast yellow 0.2 micron microspheres mounted in an agarose sample with refractive index 1.342. Images were collected with an Olympus 60X oil immersion objective NA 1.4. These data represent signal attenuation of a single field.



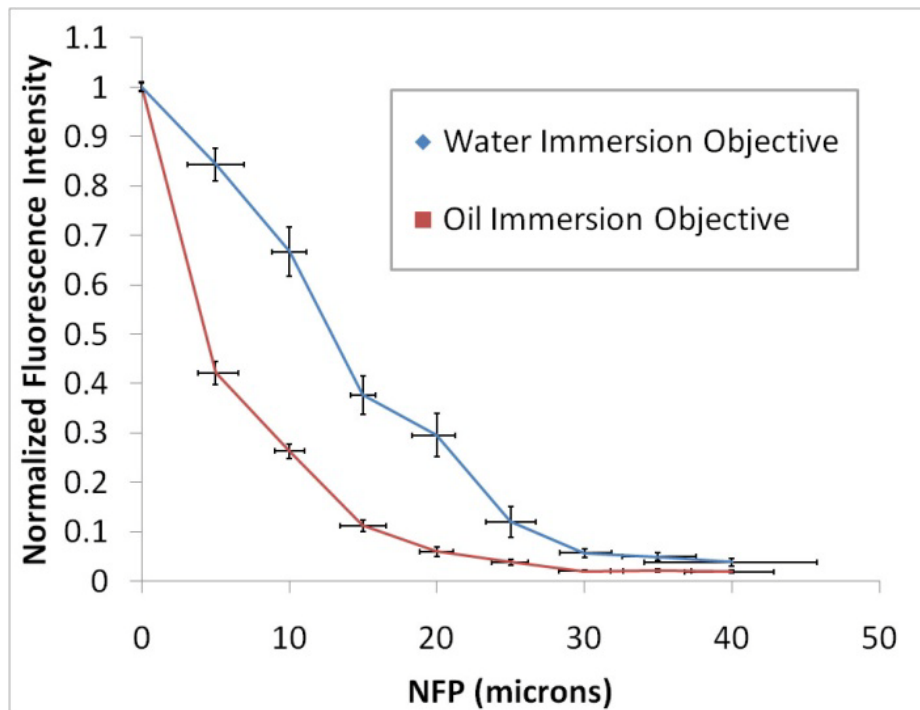
**Figure 20. Signal attenuation in kidney tissue**

Signal attenuation versus NFP of 0.2 micron fluorescent microspheres mounted in agarose with refractive index 1.404 or kidney tissue. Images were collected with a 60x oil immersion objective NA 1.4 with immersion oil (refractive index 1.515). The average of data from 20 microspheres are centered every five microns deep and normalized to the average fluorescence intensity at the surface. Error bars indicate the bin width and standard error.

in PBS, refractive index 1.34, signal attenuated by 98% at 30 microns deep, indicating 82% more signal attenuated that was not due to spherical aberration and was likely due to scattering.

## 2. *Comparison of water and oil immersion objectives*

By collecting images with a water immersion objective, refractive index mismatch between the immersion fluid, coverslip, and sample is reduced, decreasing the effect of spherical aberration (Figure 21). Signal is significantly improved in the first 25 microns of depth; however, by 40 microns deep the improvement is negligible.



**Figure 21. Water immersion objective versus oil immersion objective**

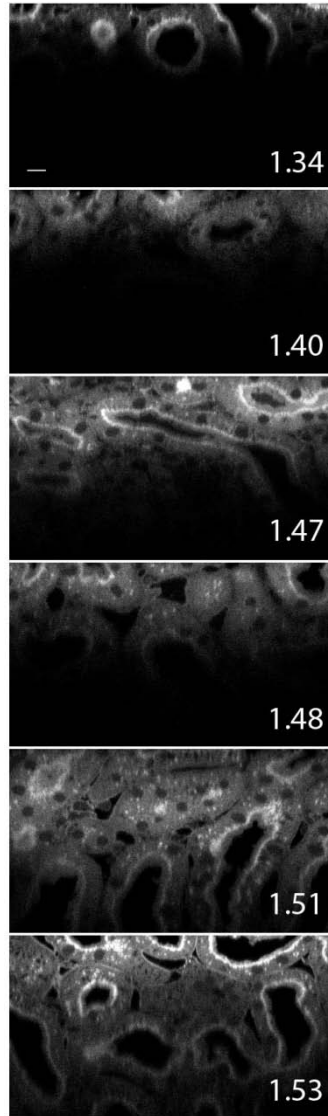
Signal attenuation of 0.2 micron fluorescent microspheres mounted in kidney tissue. Images were collected with a 60x oil immersion objective NA 1.4 with immersion oil (refractive index 1.515) or a 60x water immersion objective NA 1.2 with immersion water (refractive index 1.33). The average of data from 20 microspheres are centered every five microns deep and normalized to the average fluorescence intensity at the surface. Error bars indicate the bin width and standard error. Bin widths varied from 2.07 to 6.10 microns wide for data collected with the oil immersion objective and 1.71 to 11.68 microns wide for data collected with the water immersion objective.

## **Chapter 2. The effect of refractive index heterogeneity in multiphoton microscopy of kidney tissue**

### *A. The effect of mounting media refractive index on signal attenuation with depth in kidney tissue using a water immersion objective*

In order to evaluate the effect of the refractive index of mounting media on MPM of biological tissues, we collected image volumes of kidney tissue labeled with Lens Culinaris Agglutinin-Fluorescein and mounted in a set of clearing solutions with different refractive indices. Figure 22 shows a series of XZ cross-sectional images of kidney tissues mounted in different refractive index media collected with an Olympus 60x, NA 1.2 water immersion objective. Interestingly, the greatest depth was achieved in the samples mounted in the highest refractive index media, refractive index 1.51 and 1.53. This is surprising in that these samples should show the greatest amount of spherical aberration, resulting from the greatest refractive index mismatch between the immersion fluid and sample.

In order to quantify the effect of the refractive index of the mounting medium on the rate of signal attenuation with depth, we collected images of 0.2 micron fluorescent microspheres within kidney tissue mounted in media with refractive index 1.34, 1.40, or 1.51. Images were collected using an Olympus 60x NA 1.2 water immersion objective. The average intensity of the microspheres located at the coverslip was calculated and used to normalize the data. Data from the individual microspheres at the coverslip are not plotted to improve visualization because among the 9 trials there are 365 individual



**Figure 22. Qualitative study of signal attenuation caused by refractive index heterogeneity using water immersion objective**

Two-photon microscopy XZ cross-sectional images of kidney tissue mounted in media with refractive index 1.34, 1.40, 1.47, 1.48, 1.51, 1.53 and collected with an Olympus NA 1.2 water immersion objective. Pixel dimensions are 0.345x0.35 microns. Scale bar is 10 microns. Images collected by Sherry Clendenon.

microspheres at the surface of the samples. The standard error for the data at the coverslip was calculated to be 1-3% for each of the three samples.

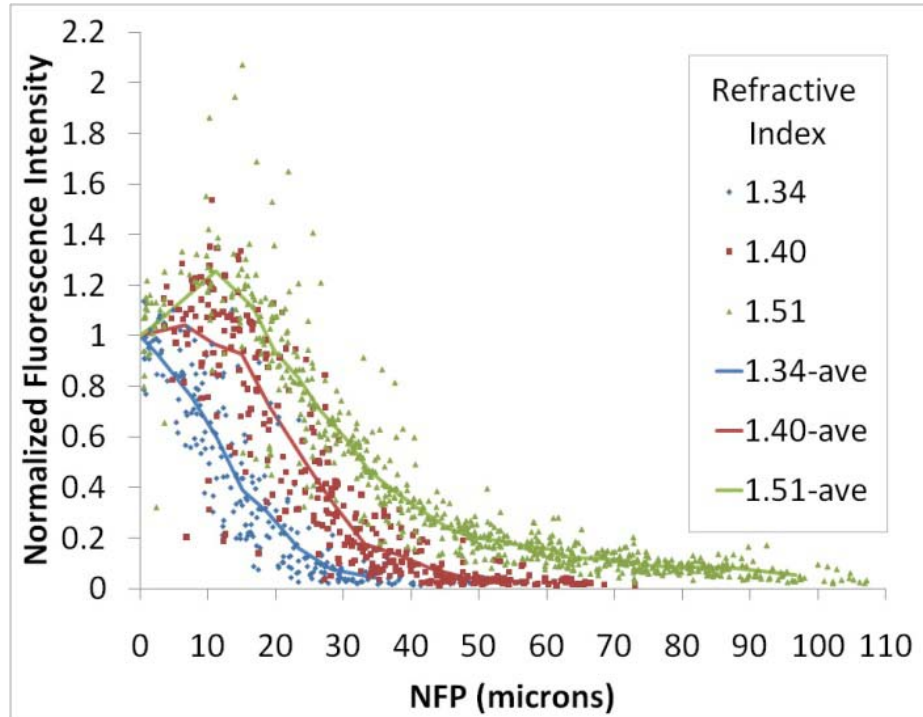
Quantization of microsphere fluorescence showed that, as in Figure 22, signal levels attenuated most rapidly in the sample mounted in a medium of low refractive index (Figure 23). For example, signal attenuated by 90% over an axial distance of 75 microns in kidney tissue with refractive index 1.51, but the same degree of attenuation was seen over only one third of this distance in a sample with refractive index 1.34. Thus, despite an increase in refractive index mismatch, signal improved with depth, in agreement with the images shown in Figure 22. This effect most likely resulted from a reduction in refractive index heterogeneity. Interestingly in Figure 23, maximum fluorescence intensity was not at the surface for all samples. Though this effect was outside the scope of our study, this may have resulted from the extra lens elements used in the correction collar of the water immersion objective.

Based upon refractive index mismatch, we expected that fluorescence intensity would attenuate most rapidly in samples mounted in media with higher refractive index. We previously found that refractive index mismatch compromised the achievable imaging depth. Interestingly, we get better depth penetration with high refractive index samples.

*B. The effect of mounting media refractive index on resolution degradation with depth in kidney tissue using a water immersion objective*

Although we get better depth penetration with high refractive index samples, the axial resolution is lower, as indicated by an increase in the axial FWHM of the intensity





**Figure 23. Quantitative study of signal attenuation caused by refractive index heterogeneity using water immersion objective**

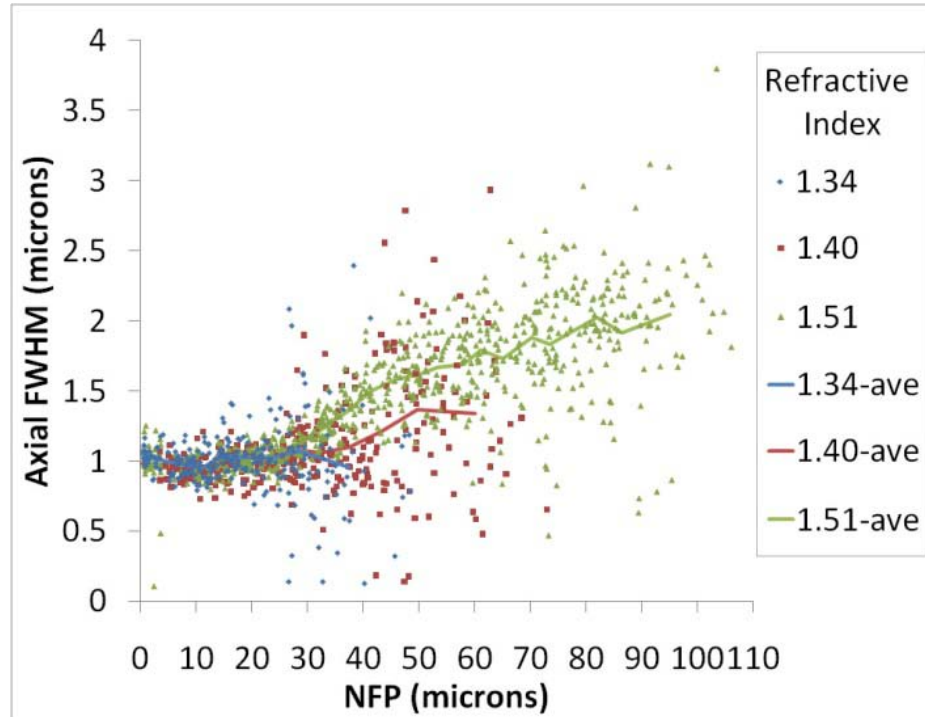
Two-photon microscopy of 0.2 micron fluorescent microspheres in kidney tissue mounted in media with refractive index 1.34, 1.40, or 1.51 and collected with an Olympus 60x NA 1.2 water immersion objective, refractive index 1.33. Line represents the average of data from 30 microspheres per bin. Bin widths varied from 2.34 to 13.42 microns wide.

profile on injected microspheres (Figure 24). Data from individual microspheres at the coverslip are again not plotted to improve visualization, only the average FWHM at the surface calculated for each sample with a standard error of 0.006-0.009 microns.

Samples mounted in media with refractive index 1.34 maintained axial resolution on the order of 1 micron up to 40 microns deep into tissue; whereas, the axial resolution of samples mounted in media with refractive index 1.51 was measured to be approximately 1.5 and 2.0 microns at depths of 40 and 80 microns, respectively. This is likely because scatter reduces illumination density but does not broaden it so much since scattered illumination photons are discarded from the illumination spot. So, unlike spherical aberration, scattering affects imaging depth by reducing the number of photons reaching the focus, but not really affecting the effective volume of excitation.

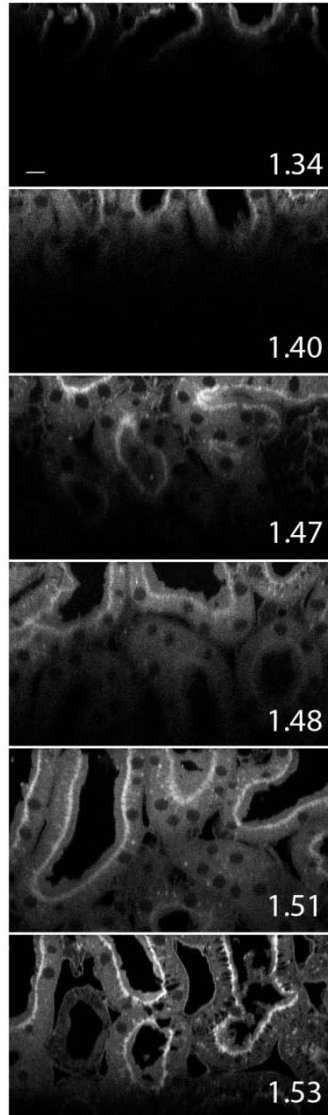
*C. The effect of reducing both refractive index heterogeneity and mismatch on signal attenuation with depth in kidney tissue*

Based upon previous results, ideally we would eliminate refractive index mismatch and scattering. In order to evaluate the effect of simultaneously reducing both, we collected images of kidney tissue labeled with Lens Culinaris Agglutinin-Fluorescein and mounted in various media, using an oil immersion objective. To minimize scattering and spherical aberration, the kidney tissue was mounted in different clearing solutions, and XZ cross-sectional images were collected using an Olympus 60x NA 1.4 oil immersion objective. The deepest imaging depth was achieved in the samples mounted in refractive index media 1.51, clearing the tissue and matching the refractive index of the immersion oil (Figure 25).



**Figure 24. Quantitative study of resolution degradation caused by refractive index heterogeneity using water immersion objective**

Two-photon microscopy of 0.2 micron fluorescent microspheres in kidney tissue mounted in media with refractive index 1.34, 1.40, or 1.51 and collected with an Olympus 60x NA 1.2 water immersion objective, refractive index 1.33. Line represents the average of data from 31 microspheres per bin. Bin widths varied from 2.50 to 19.86 microns wide (excluding the deepest bins for each sample the maximum bin width was 8.30 microns wide).



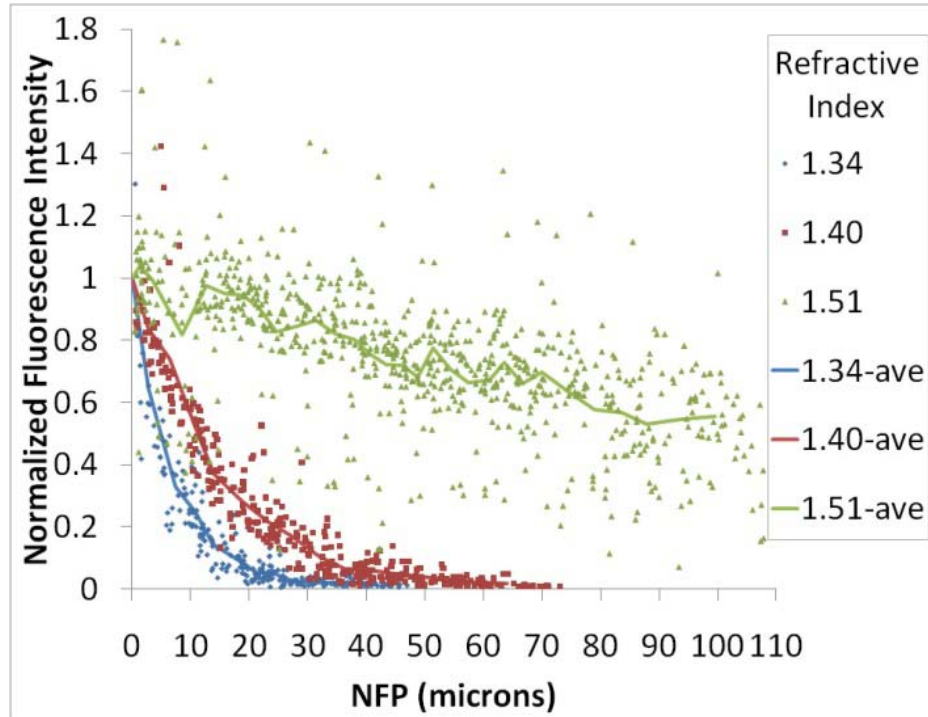
**Figure 25. Qualitative study of signal attenuation caused by refractive index heterogeneity using oil immersion objective**

Two-photon microscopy XZ cross-sectional images up to 100 microns into kidney tissue mounted in media with refractive index 1.34, 1.40, 1.47, 1.48, 1.51, 1.53 and collected with an Olympus 60x NA 1.4 oil immersion objective, refractive index 1.51. Pixel dimensions are 0.345x0.35 microns. Scale bar is 10 microns. Images collected by Sherry Clendenon.

These qualitative results were supported in quantitative analyses of fluorescent microspheres in kidney tissue. Samples were mounted in media with refractive indices of 1.34, 1.40, or 1.51 and imaged using an Olympus 60x NA 1.4 oil immersion objective (refractive index of the immersion oil, 1.515). The average intensity of the microspheres located at the coverslip was calculated and used to normalize the data. Data from the individual microspheres at the coverslip are not plotted to improve visualization because among the 9 trials there are 456 individual microspheres at the surface of the samples. The standard error for the data at the coverslip was calculated to be 1-2% for each of the three samples.

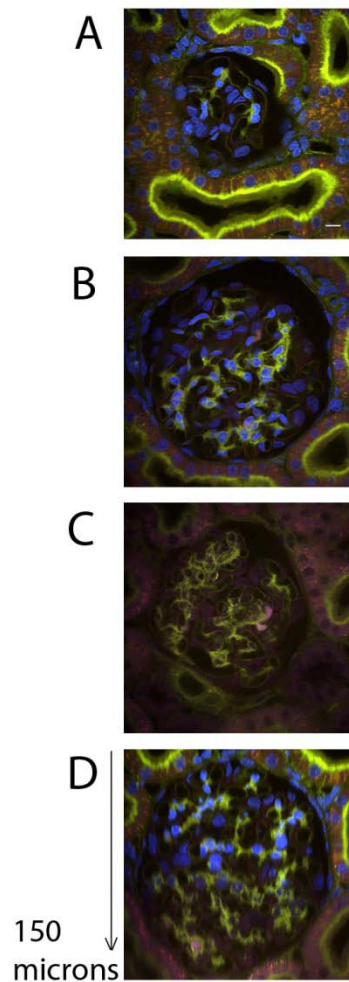
As shown in Figure 26, the rate of signal attenuation with depth was dramatically decreased in samples mounted in a high refractive index medium. Signal attenuated by 90% in less than 20 microns of depth into kidney tissue mounted in medium with refractive index 1.34, whereas in samples mounted in medium with refractive index 1.51 signal only attenuated by 45% in 100 microns of depth. These results support the notion that scattering of the excitation and fluorescent light, and not spherical aberration, is a major contributor to signal degradation under our experimental conditions.

Remarkable results were obtained in samples mounted in the highest refractive index media (Figure 27). High quality images were collected through the entire working distance of the objective, 150 microns. Interestingly, even though scattering has been significantly reduced, the shortest wavelength emissions still attenuate faster with depth than the longer wavelengths. This is evident from the Figure 27C, 125 microns deep into tissue, which has far more red signal (emission wavelengths 560-650 nm), than Figure 27A, 25 microns deep into tissue, which has far more blue signal (emission wavelengths



**Figure 26. Quantitative study of signal attenuation caused by refractive index heterogeneity using oil immersion objective**

Two-photon microscopy of 0.2 micron fluorescent microspheres in kidney tissue mounted in media with refractive index 1.34, 1.40, or 1.51 and collected with an Olympus 60X NA 1.4 oil immersion objective, refractive index 1.515. Line represents the average of data from 25 microspheres per bin. Bin widths varied from 1.30 to 11.29 microns wide.



**Figure 27. Optimization of refractive index heterogeneity and mismatch**

Two-photon microscopy of kidney tissue labeled with Hoechst, Lens Culinaris Agglutinin-Fluorescein, and Phalloidin-Rhodamine and mounted in media with refractive index 1.51. Image volume collected with Olympus 60x NA 1.4 oil immersion objective. Images were collected A) 25 microns deep, B) 75 microns deep, C) 125 microns deep, and D) XZ cross-section. Pixel dimensions are 0.414x0.414x0.41 microns. Scale bar is 10 microns. Contrast stretching and unsharp mask were the same for all images. Images collected by Sherry Clendenon.

380-480 nm). This is also evident in Figure 27D, XZ cross-section, with more blue signal near the surface and red signal at depth.

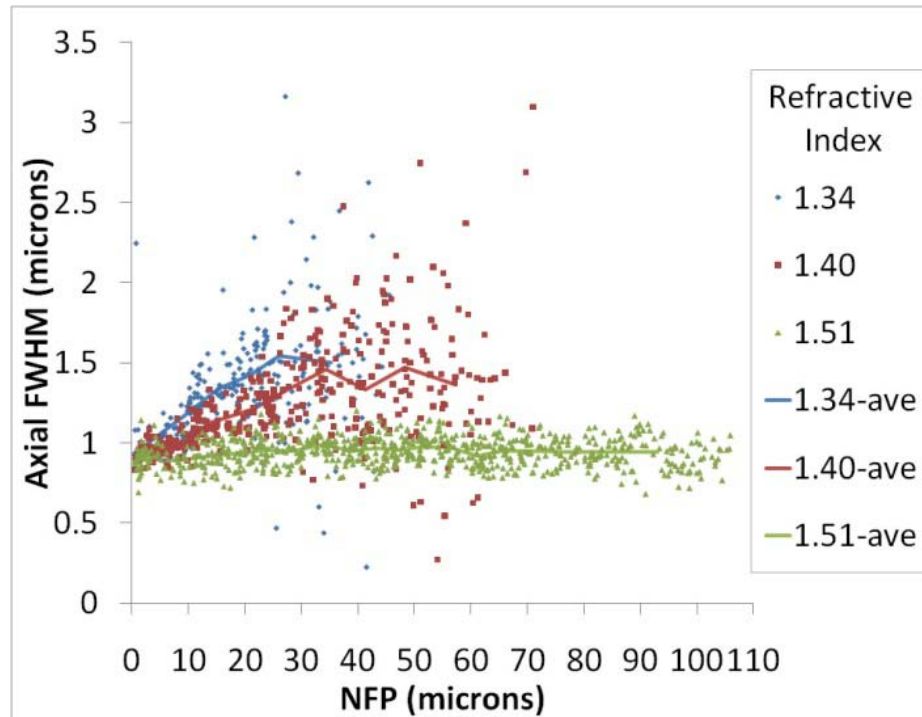
*D. The effect of reducing both refractive index heterogeneity and mismatch on resolution degradation with depth in kidney tissue*

Our previous studies demonstrate that refractive index mismatch compromises axial resolution in images collected at depth by MPM. Consistent with this observation, increasing the refractive index of the mounting medium to match that of the immersion medium profoundly improved the axial resolution of images of microspheres collected at depth in kidney tissue (Figure 28). Data from individual microspheres at the coverslip are again not plotted to improve visualization, only the average FWHM at the surface calculated for each sample with a standard error of 0.003-0.006 microns.

Quantitative analysis of microsphere point spread functions in these samples demonstrates that eliminating refractive index mismatch essentially eliminates depth-induced degradation in axial resolution. The axial resolution of samples mounted in media with refractive index 1.34 was measured to be approximately 1.5 microns 25 microns deep into tissue. Samples mounted in media with refractive index 1.51 maintained axial resolution on the order of 0.9 microns up to 100 microns deep into tissue.

The results of these studies demonstrate that additional profound improvement in reach and image quality can be achieved by minimizing spherical aberration and scattering.





**Figure 28. Quantitative study of resolution degradation caused by refractive index heterogeneity using oil immersion objective**

Two-photon microscopy of 0.2 micron fluorescent microspheres in kidney tissue mounted in media with refractive index 1.34, 1.40, or 1.51 and collected with an Olympus 60X NA 1.4 oil immersion objective, refractive index 1.515. Line represents the average of data from 40 microspheres per bin. Bin widths varied from 3.38 to 10.94 microns wide.

### Chapter 3. Mathematical model of refractive index mismatch in MPM using geometric optics

#### A. Theory

A mathematical model was developed using geometrical optics to predict the excitation light path from the objective lens to the focus through the immersion fluid, coverslip, and into a homogeneous sample. This geometrical model is used to calculate the first order approximation of the axial distribution of excitation and fluorescence intensity demonstrating the effect of refractive index mismatch in multiphoton fluorescence microscopy.

This geometrical model relies on Snell's law which states

$$n_1 \sin \alpha_1 = n_2 \sin \alpha_2$$

where  $n_1$  is the refractive index of the first medium,  $\alpha_1$  is the angle of incidence,  $n_2$  is the refractive index of the second medium, and  $\alpha_2$  is the angle of refraction. Using Snell's law and the objective lens parameters for an Olympus 60x NA 1.4 oil immersion objective lens (PLAPO60XO3) (Table 3), we calculate initial parameters (Figure 29).

By definition

$$NA = n_{obj} \sin \alpha_{NA}$$

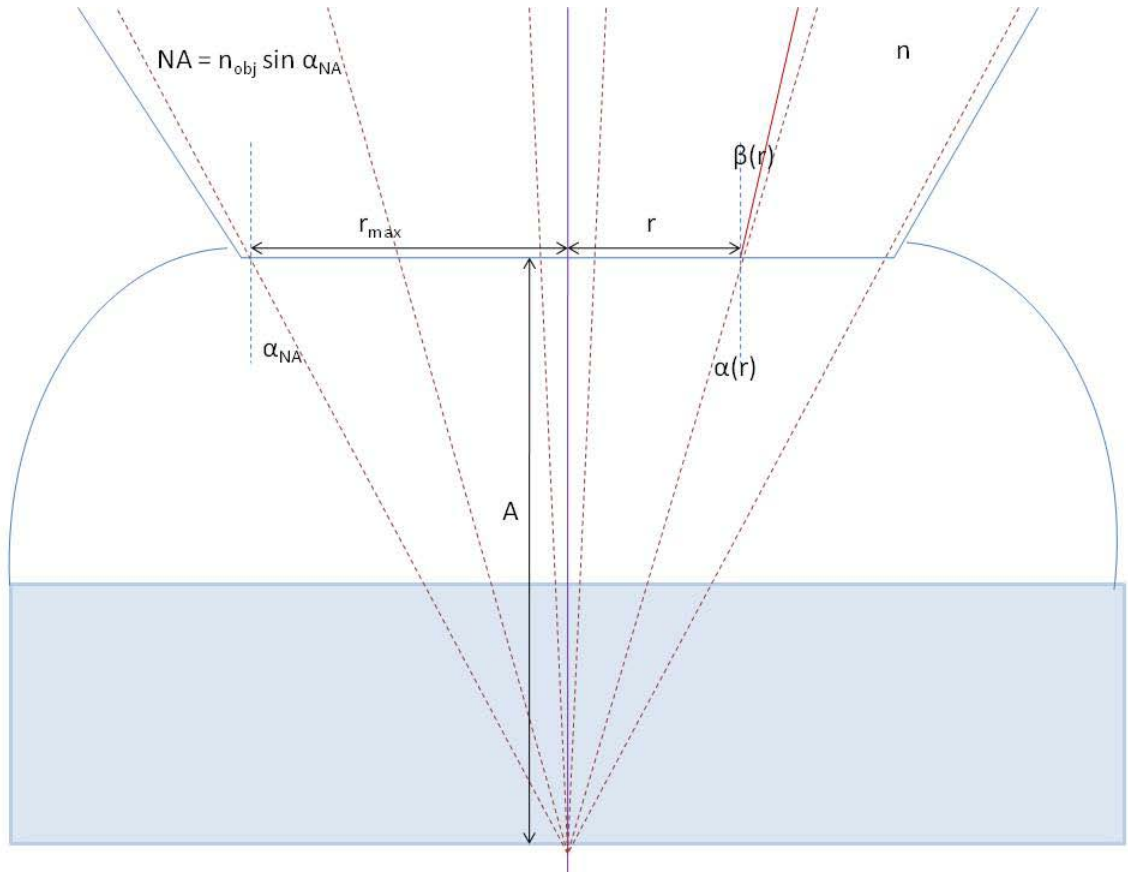
where  $NA$  is the numerical aperture of the objective lens,  $n_{obj}$  is the ideal refractive index as described by the objective manufacturer, and  $\alpha_{NA}$  is the aperture angle of the objective lens. By simple geometry

$$r_{max} = A \tan \alpha_{NA}$$

<b>Objective lens parameters</b>		
numerical aperture	$NA$	1.4
ideal refractive index	$n_{obj}$	1.515
working distance + ideal coverslip thickness (microns)	$A$	150 microns + 170 microns = 320
actual refractive index of objective lens	$n$	1.51633

**Table 3. Objective lens parameters**

Objective lens parameters for an Olympus 60x NA 1.4 oil immersion objective lens (PLAPO60XO3).



**Figure 29. Model schematic**

Using the objective parameters: numerical aperture,  $NA$ , ideal objective refractive index  $n_{obj}$ , working distance + ideal coverslip thickness,  $A$ , and actual objective lens refractive index,  $n$ , we calculate the maximum radius of incident light at the objective,  $r_{max}$ , the aperture angle,  $\alpha_{NA}$ , the angle of light from radius,  $r$ , assuming no refraction,  $\alpha(r)$ , and the actual angle of light from radius,  $r$ , incident on the objective lens,  $\beta(r)$ .

where  $r_{max}$  is the maximum radius of incident light at the objective,  $A$  is the sum of the working distance and the ideal coverslip thickness, and  $\alpha_{NA}$  is the aperture angle of the objective lens (Figure 29). And assuming no refraction, the angle of light from radius,  $r$ , can be defined as

$$\alpha(r) = \tan^{-1} \frac{r}{A}$$

where  $A$  is the sum of the working distance and the ideal coverslip thickness (Figure 29). However, because the actual refractive index of the objective lens is not the ideal refractive index indicated by the manufacturer for the immersion fluid of the system, we use Snell's law to define the actual angle of light incident on the objective lens

$$n \sin \beta(r) = n_{obj} \sin \alpha(r)$$

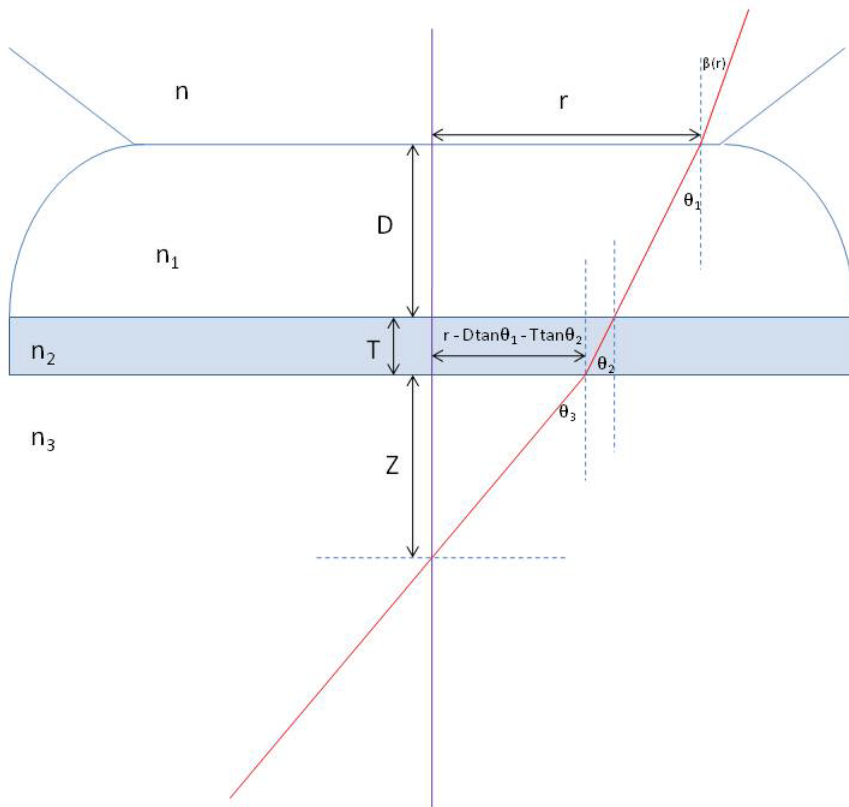
where  $n$  is the actual refractive index of the objective lens and  $n_{obj}$  is the ideal refractive index as described by the objective manufacturer (Figure 29). Using  $n$  and  $\beta(r)$ , we define refraction angles  $\theta_1$ ,  $\theta_2$ , and  $\theta_3$  for the objective lens-immersion fluid interface, immersion fluid-coverslip interface, and coverslip-sample interface respectively

$$n \sin \beta(r) = n_1 \sin \theta_1(r) = n_2 \sin \theta_2(r) = n_3 \sin \theta_3(r)$$

where  $n_1$  is the refractive index of the immersion fluid,  $n_2$  is the refractive index of the cover glass, and  $n_3$  is the refractive index of the sample (Figure 30). We calculate the depth into the sample,  $Z(r)$ , where light from a cone with radius,  $r$ , will focus

$$Z(r) = \frac{r - D \tan \theta_1(r) - T \tan \theta_2(r)}{\tan \theta_3(r)}$$

where  $D$  is the distance from the objective lens to the coverslip and  $T$  is the coverslip thickness. Using this calculation and radially stepping across the objective lens from



**Figure 30. Model schematic**

Using  $\beta(r)$  calculated from the objective parameters, for light from a specific radius,  $r$ , we calculate refraction angles,  $\theta_1(r)$ ,  $\theta_2(r)$ , and  $\theta_3(r)$ , for refractive indices,  $n_1$ ,  $n_2$ , and  $n_3$ , respectively, chosen based on values from actual experiments. Using the refraction angles,  $\theta_1(r)$ ,  $\theta_2(r)$ , and  $\theta_3(r)$ , we can calculate the depth into the sample from the coverslip-sample interface that light from a specific radius,  $r$ , focuses.

paraxial rays to peripheral rays, we are able to build a linear projection histogram representing the distribution of excitation intensity axially within the sample.

However, because we are modeling excitation intensity for a 0.2 micron diameter fluorescent microsphere, confining the focal spot to a single point is unreasonable. It is necessary to consider all rays that pass within the volume of the microsphere. Also, we know diffraction causes the focus to have an intensity distribution, PSF, with FWHM of 0.3 microns laterally and 0.9 microns axially at an excitation wavelength of 800 nm using a 60x oil immersion objective NA 1.4. Therefore, to determine the excitation intensity within the sample for a specific  $D$  and  $T$ , we sum the intensities from cones of light that focus within a range of a certain depth,  $Z_{fp}$ .

To determine the excitation intensity for a given  $Z_{fp}$ , we integrate the input laser beam intensity over  $r$  such that the excitation light passes within a range of  $Z_{fp}$  (Figure 31)

$$\int I(r)dr.$$

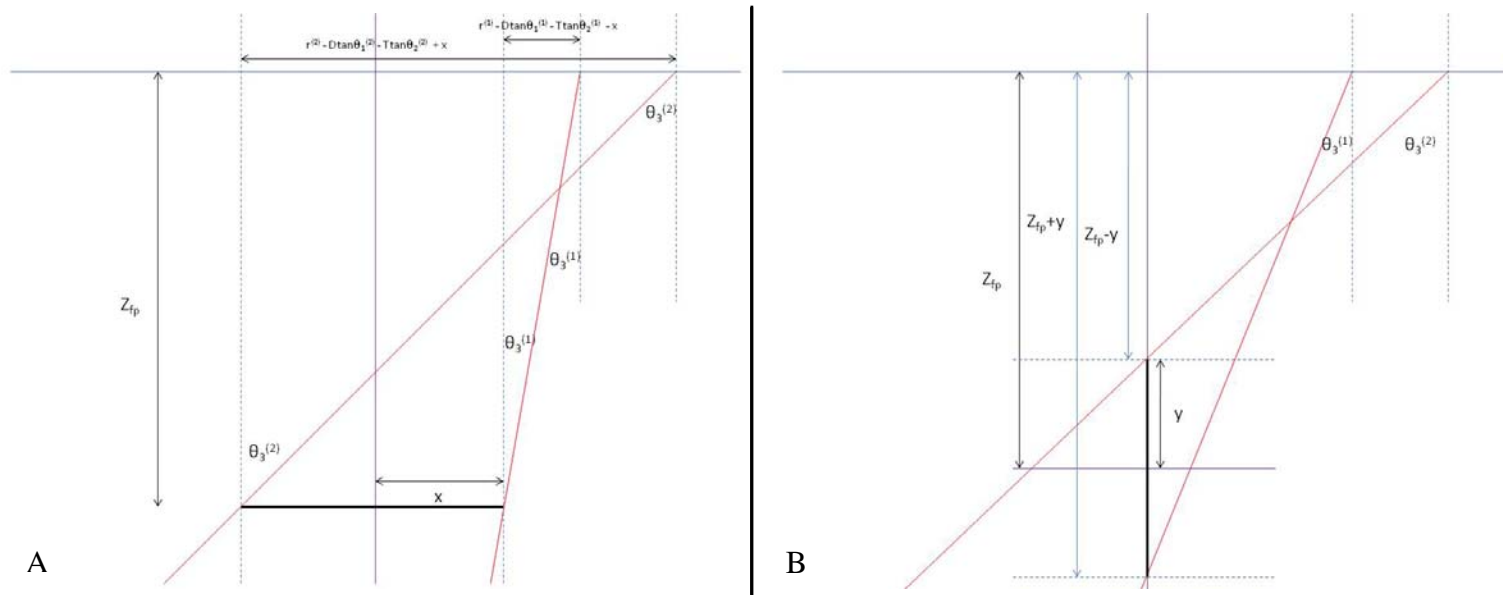
The axial range is defined such that  $Z(r)$  is bound by

$$Z_{fp} - y \leq Z(r) \leq Z_{fp} + y .$$

The lateral range is defined such that  $Z(r)$  and  $\tan \theta_3(r)$  are bound by

$$|Z(r) - Z_{fp}| \tan \theta_3(r) \leq x .$$

Although we are using geometrical optics to model our system, we model the input light as a Gaussian beam with a cylindrically symmetric wavefront using the beam radius and average power measured at the back aperture of the objective.



**Figure 31. Model Schematic**

The intensity for light rays focusing within an axial and lateral range of  $Z_{fp}$  is summed to determine the excitation intensity.



Using a Gaussian distribution for intensity yields

$$I(S) = \frac{2P_0}{\pi w^2} e^{-\frac{2S^2}{w^2}}$$

where  $P_0$  is the average power at the back aperture of the objective and  $w$  is the beam radius of the laser at the back aperture (Figure 32). The microscope objective is simplified to two lenses, the objective lens and a lens at the back aperture. The back aperture lens is idealized to take on all the properties of the lenses within the microscope objective such that light at the back aperture projects on to the objective lens with angle  $\beta(r)$ . The back aperture is assumed to be filled, which refers to the FWHM of the Gaussian beam equaling the diameter of the back aperture of the microscope objective. Therefore the beam radius,  $w$ , measured as half the FWHM of the Gaussian beam, equals the radius of the back aperture of the objective.

Assuming cylindrical symmetry, the excitation intensity integral becomes

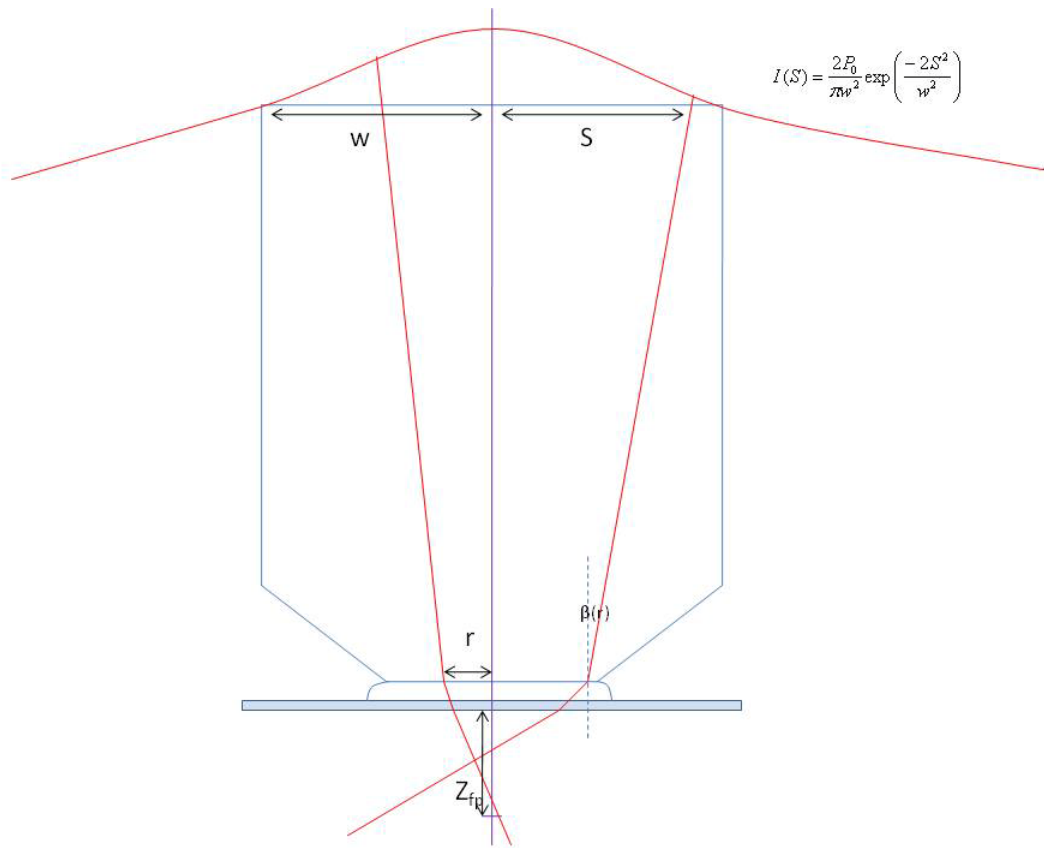
$$I = \int_{S_1}^{S_2} \frac{2P_0}{\pi w^2} e^{-\frac{2S^2}{w^2}} (2\pi S) dS$$

where  $S_1$  and  $S_2$  are determined using MATLAB (The MathWorks, Inc., Natick, MA, USA) to iterate over  $r$ , calculating  $S_1$  from  $r$  when it first encounter a ray within the axial or lateral range of  $Z_{fp}$ , and  $S_2$  when subsequently,  $r$  encounters a ray that is no longer in the axial or lateral range of  $Z_{fp}$  (Figure 31).  $S$  is calculated from  $r$  by

$$S(r) = \frac{w - r_{max}}{\tan(\sin^{-1} \frac{NA}{n})} \tan \beta(r) + r.$$

This is repeated though  $r_{max}$  summing intensities to get the total intensity at  $Z_{fp}$ .

To determine at what depth is the AFP for a particular  $D$  and  $T$ , this is repeated by iteratively stepping  $Z_{fp}$  from the coverslip-sample interface



**Figure 32. Model Schematic**

The excitation light input at the back aperture is assumed to have a Gaussian intensity distribution. The microscope objective is simplified to two lenses with the back aperture lens taking on all the properties of the lenses within the microscope objective such that light at the back aperture projects onto the objective lens with angle  $\beta(r)$ .

deep into the sample. The depth,  $Z_{fp}$ , where the maximum intensity is achieved is the AFP for  $D$  and  $T$  (Figure 33). To compare to experimental data, this is repeated for  $D$ , the distance from the coverslip to the objective lens, ranging through the full working distance of the objective to find the maximum intensity associate with each step of the objective,  $D$ . The NFP is

$$NFP = A - (D + T).$$

## B. *MATLAB*

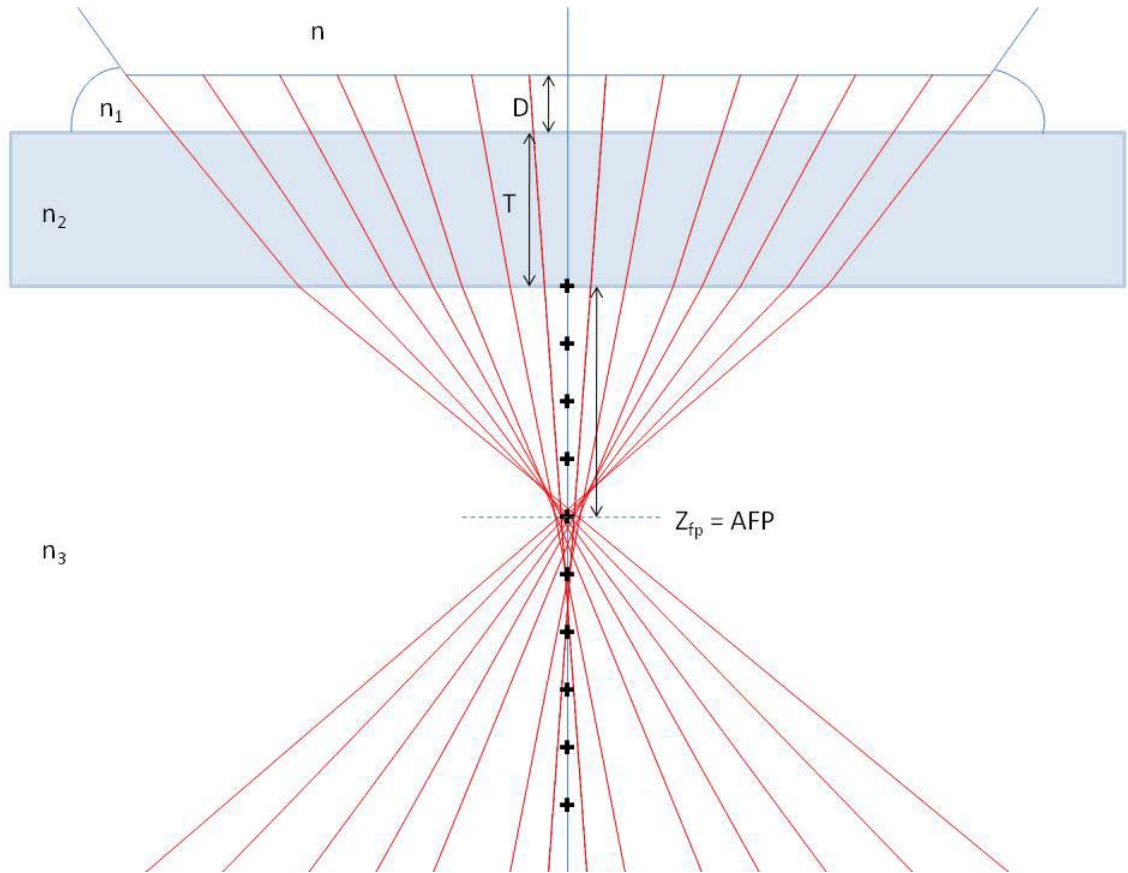
### 1. *Overview*

Because the mathematical model could not be solved analytically, MATLAB (The MathWorks, Inc., Natick, MA, USA) was used to calculate the excitation intensity versus focal depth numerically. The code can be found in Appendix 1.

The Intensity program was written to calculate the excitation intensity for a given AFP and distance between the objective and coverslip,  $D$ .

The Optimize D program was then written to find at what  $D$ , the distance between the objective and coverslip, the maximum intensity occurs for a given AFP and sample refractive index. The Optimize D program runs the Intensity program for all  $D$  through the full working distance of the objective.

The Optimize D Range program finds the optimized  $D$  value, the associated maximum intensity for a range of focal positions and a given sample refractive index. The Optimize D Range program was run for focal positions from 1 micron to 149 microns, with a 1 micron step.



**Figure 33. Model schematic**

The intensity for light rays focusing within a range of  $Z_{fp}$  is summed to determine the excitation intensity.  $Z_{fp}$  is iteratively stepped axially through the sample, to find the depth where the excitation intensity is maximal, the AFP.

The Overnight OD program produces saved files each containing a spreadsheet of the full range of focal positions from 1-149, each associated optimized D, and the associated maximum intensity. The Overnight OD program runs the Optimize D Range program for each sample refractive index input into an array.

## 2. *Intensity program*

The program `intensityford` was developed to calculate the excitation intensity at a specific focal plane. This program requires input values of `d`, the distance between the coverslip and the objective, `fp`, the focal plane, and `rstep`, the step size to iterate across the radius of the objective lens. This program steps across the radius of the objective lens and determines if the associated ray of excitation light propagates within a range of the focal plane, `fp`. This is determined using the function `thetans`, a convenience function that performs calculations that occur in several places described below. Using the values returned by `thetans`, the ray is tested to see if it propagates within the range of `fp` (Figure 31). If it is within either the lateral range, `lower <= tan(theta3)` and `tan(theta3) <= upper`, or the axial range, `fp-.1 <= z` and `z <= fp+.1`, then the variable `R1` is set equal to `r`. `R1` is the first `r` position where a ray of excitation light contributes to the excitation intensity at the focal plane, `fp`. `intensityford` continues stepping `r` across the objective lens until it finds an `r` that is not in bounds. It sets the previous `r` position equal to `R2`. `R2` is the last `r` position where a ray of excitation light contributes to the excitation intensity at the focal plane, `fp`. Because we are assuming the excitation light has a Gaussian wavefront filling the back aperture of the objective, the excitation intensity cannot be calculated directly from `R1`

and  $R_2$ . Using the function  $s$ , described below,  $R_1$  and  $R_2$  are converted to  $S_1$  and  $S_2$ , the associated radii at the back aperture of the objective.  $S_1$  and  $S_2$  are then used to calculate the integrated intensity from this ring of excitation as  $intensity = \pi * w^2 / 2 * \text{abs}(\text{sintensity}(S_2) - \text{sintensity}(S_1))$ . The function  $\text{sintensity}$  is described below. Because there may be more rays of excitation light that contribute to the excitation intensity farther along  $r$ , the function continues stepping  $r$  across the objective lens until it reaches  $r_{max}$ . If it encounters another  $r$  position in bounds, it repeats and adds the excitation intensity from this ring of light to the total intensity.

The function,  $\text{thetans}$ , performs calculations that occur in several places and requires input values for  $r$ , the radius at the objective lens to be tested, and  $d$  and  $f_p$ , which are the original values inputted into  $\text{intensityford}$ .  $\text{thetans}$  calculates  $\text{alphar}$ ,  $\text{beta}$ ,  $\text{theta1}$ ,  $\text{theta2}$ ,  $\text{theta3}$ ,  $z$ ,  $\text{lower}$ , and  $\text{upper}$ .  $\text{alphar}$  is the angle of light from radius,  $r$ , assuming no refraction.  $\text{beta}$  is the actual angle of light incident on the objective lens.  $\text{theta1}$  is the refraction angle from the objective lens-immersion fluid interface.  $\text{theta2}$  is the refraction angle for the immersion fluid-coverslip interface.  $\text{theta3}$  is the refraction angle for the coverslip-sample interface.  $z$  is the depth into the sample where light from a cone with radius,  $r$ , with focus.  $\text{lower}$  and  $\text{upper}$  are the bounds associated with the lateral range around  $f_p$  for a given radius  $r$ .  $\text{thetans}$  returns  $\text{beta}$ ,  $\text{theta3}$ ,  $z$ ,  $\text{lower}$ , and  $\text{upper}$ .

The function,  $s$ , calculates the radial position at the back aperture of the objective associate with a value  $r$ , the radial position at the objective lens, and  $\text{beta}$ , the actual angle of light incident on the objective lens calculated by the function  $\text{thetans}$ . This is calculated using the equation  $sposition = (w - r_{max}) / (\tan(\text{asin}(NA / N))) *$

$\tan(\beta) + r$ .  $w$ ,  $r_{\max}$ ,  $NA$ , and  $N$  are global variables defined in Table 4.  $w$  is the radius of the back aperture of the objective,  $r_{\max}$  is the radius of the objective lens,  $NA$  is the numerical aperture of the objective, and  $N$  is the actual refractive index of the objective lens glass.

The function, `sintensity`, calculates the excitation intensity for a given radial position along the back aperture of the objective,  $s$ , assuming a Gaussian wavefront. This is calculated using the equation  $sint = I * \exp(-2 * (s)^2 / (w^2))$ .  $I$  is the intensity at the peak of the Gaussian distribution, a global variable defined in Table 4.

### 3. *Optimize D program*

The program, `optimized`, was developed to use the data from the `intensityford` program to find the maximum intensity for the given focal plane and the associated distance between the objective and the coverslip. The program, `optimized`, requires input values  $f_p$ , the focal plane, and  $n_{ed}$ , the refractive index of the sample. The program runs `intensityford` for a range of  $d$ , the distance between the objective and coverslip, through the full working distance of the objective, stepping at micron intervals. The program, `intensityford`, returns the excitation intensity for a specific focal plane, given a specific distance between the objective and coverslip. To find the maximum intensity, `optimized` steps  $d$  through the working distance of the objective, running `intensityford` using  $d$ , the given  $f_p$ , and an  $rstep$  of 1. The variable `maxintensity` is set equal to the intensity value returned by `intensityford` if the new intensity is greater than the intensity for the previous  $d$ . This is repeated until the new intensity value is less than `maxintensity`. Once the maximum intensity is found, this is repeated for a smaller range of  $d$ ,  $d \pm 2$ , with a finer interval, where the step is reduced to a tenth of a micron.

Global variables		
NA	1.4	numerical aperture of the objective
NOBJ	1.515	refractive index of the objective
WOBJ	150	working distance of the objective in microns
T	170	coverslip thickness in microns
WDT	WOBJ+T	working distance + ideal coverslip thickness in microns
N	1.51633	actual refractive index of the objective lens glass
N1	1.515	refractive index of the immersion fluid
N2	1.515	refractive index of the cover glass
N3	ned	refractive index of the sample
ALPHA	asin(NA/NOBJ)	aperture angle
rmax	(WDT)*tan(ALPHA)	radius of the objective lens
w	4200	radius of the back aperture in microns and beam radius
P	2000	power in microWatts
I	$2*P/(3.14159*w^2)$	intensity at the peak of the Gaussian
delta	$10^{-58}$	fluorophore cross section in $m^4sec$
f	$82*10^6$	repetition rate of laser in Hz
tau	$100*10^{-15}$	temporal pulse width of laser in seconds
lambda	$800*10^{-9}$	wavelength in meters
X	0.1	lateral range to include at fp
ZRANGE	150	distance from coverslip into the sample in microns

**Table 4. Global variables**

Global variables used in geometrical model. Objective lens parameters based on an Olympus 60x NA 1.4 oil immersion objective lens (PLAPO60XO3).



This is again repeated with finer passes until the `dstep` is 0.0001 microns. Initially we attempted using built-in minimization functions, but we ran into problems with local minima and maxima. While a linear search is not ideal or efficient, it is reliable. `optimized` returns the distance between the objective and the coverslip where the excitation intensity is a maximum found during this final search.

#### 4. *Optimize D Range program*

The program, `optimizedrange`, was developed to find the maximum intensity and associated distance between the objective and coverslip for a range of focal positions and a given refractive index of the sample, `ned`. This program repeatedly runs `optimized` for the range of focal positions from 1 micron deep into the sample through `ZRANGE - 1`. Calculations are not defined at focal position 0 microns or when `ZRANGE = WOBJ`. `optimizedrange` returns an array with three values, the focal position, `fp`, the distance between the objective and the coverslip where the excitation intensity is a maximum, returned from `optimized`, and the maximum intensity returned from `intensityford`.

#### 5. *Overnight OD program*

The program, `overnightod`, was developed to run `optimizedrange` for multiple refractive indices of the sample input as an array, `ned`, and save the data in a separate spreadsheet for each refractive index. `overnightod` iterates over the input array, `ned`, and populates a spreadsheet with the focal position, `fp`, the distance between the objective and the coverslip where the excitation intensity is a maximum, returned from `optimized`, and the maximum intensity returned from `intensityford`.

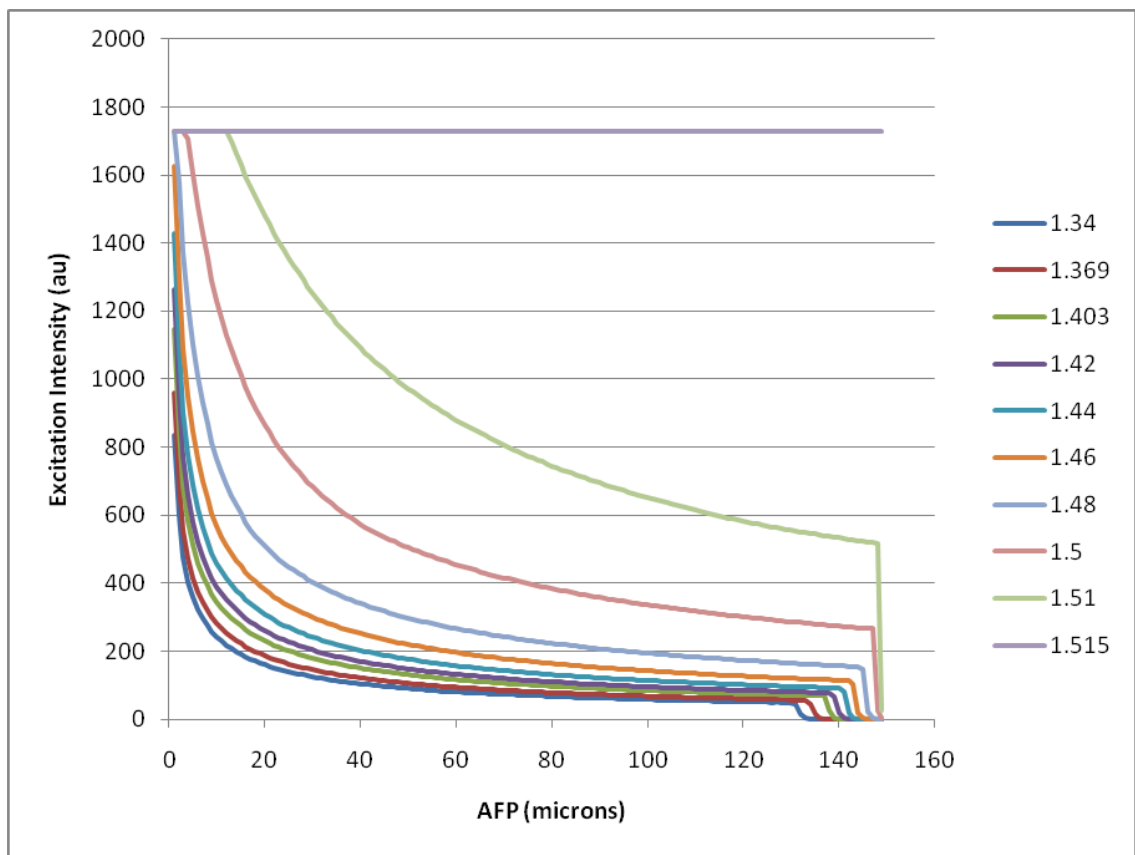
## 6. *Model calculations*

Calculations from the model are presented in Figure 34 and 35. Figure 34 is a plot of the maximum intensity returned from `intensityford` versus the AFP,  $f_p$ . In Figure 35 the maximum intensity data are normalized to the value at  $f_p = 1$  and are plotted versus the NFP, calculated as the difference between the working distance of the objective,  $w_{OBJ}$ , and the distance between the objective and the coverslip where the excitation intensity is a maximum, returned from `optimized`.

### C. *Comparison to empirical data*

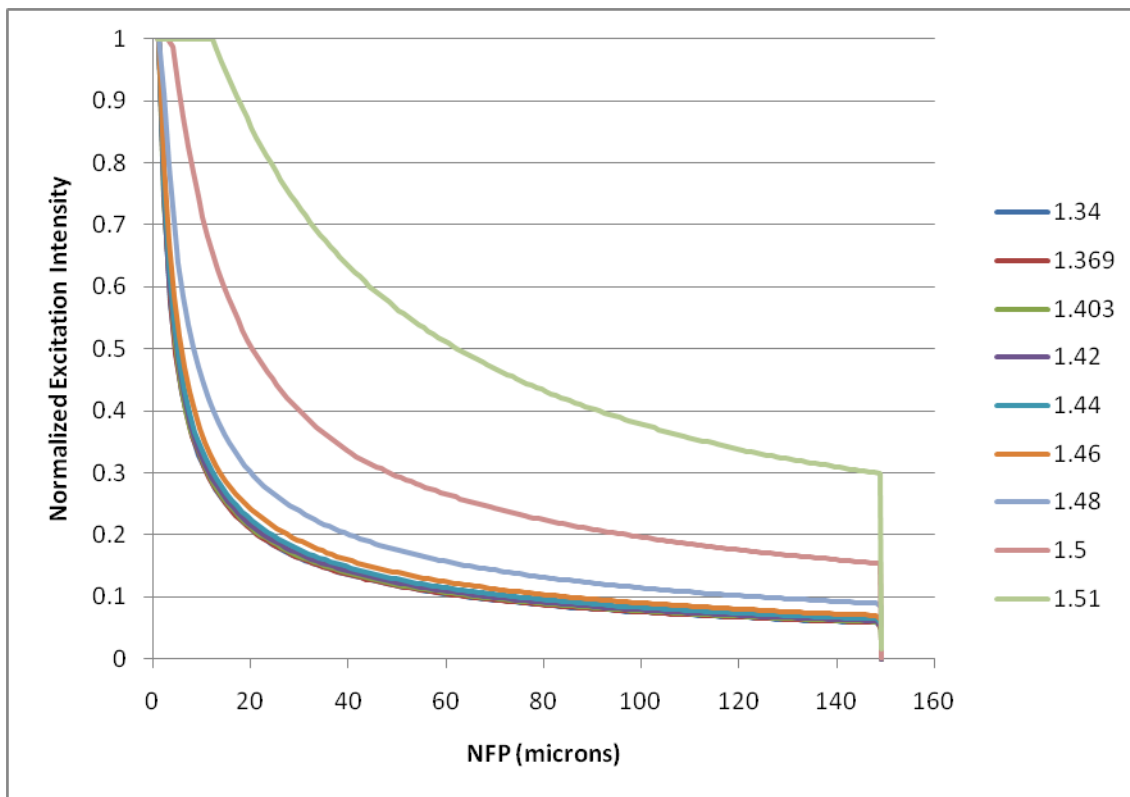
The geometrical model was developed to predict the excitation light path from the objective lens to the focus through the immersion fluid, coverslip, and into a homogeneous sample. This model is used to calculate the first order approximation of the axial distribution of excitation intensity. Calculations made based on the geometrical model were compared to the excitation attenuation data collected as described in *Excitation attenuation* (Figure 36). Briefly, photobleaching rates were measured over a range of depths in samples of agarose, a homogeneous sample, with refractive indices 1.34, 1.37, 1.40, 1.44 containing 0.2 micron fluorescent microspheres (Figure 16). Photobleaching rates were also collected at the coverslip-sample interface for a range of laser powers measured at the Pockels cell. A calibration curve was developed relating photobleaching rates and laser power (Figure 17). The calibration curve was then used to convert photobleaching rates versus depth to excitation power versus depth.

Model calculations and empirical data were normalized to the intensity five microns deep into the sample because the model was undefined at the coverslip-sample



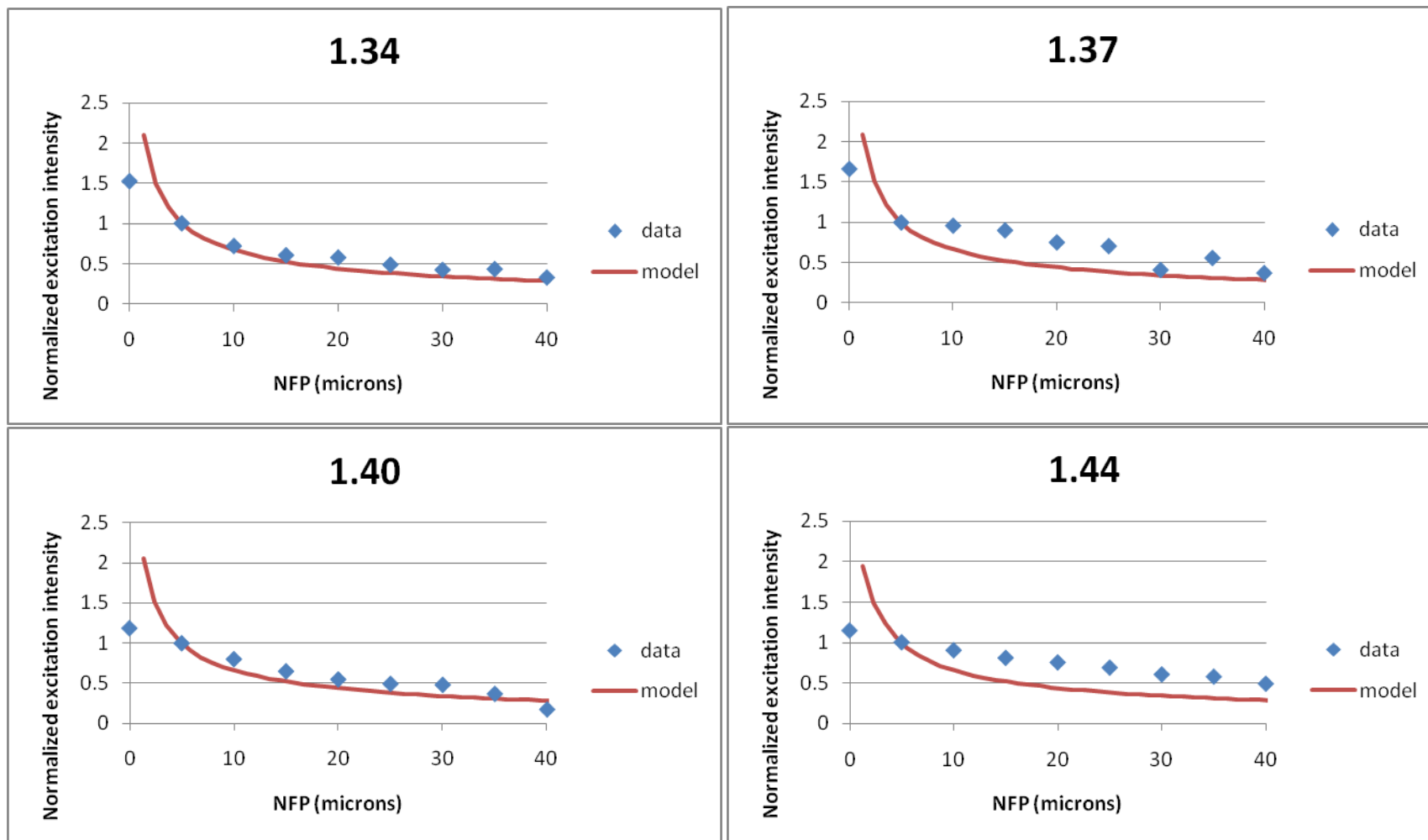
**Figure 34. Model calculations**

The intensity for light rays focusing within a range of  $Z_{fp}$  is summed to determine the excitation intensity.  $Z_{fp}$  is iteratively stepped axially through the sample, to find the depth where the excitation intensity is maximal, the AFP. This is repeated for  $D$ , the distance from the coverslip to the objective lens, ranging through the full working distance of the objective to find the maximum intensity associate with each step of the objective,  $D$ . The maximal intensity is plotted versus AFP.



**Figure 35. Model calculations**

The intensity for light rays focusing within a range of  $Z_{fp}$  is summed to determine the excitation intensity.  $Z_{fp}$  is iteratively stepped axially through the sample, to find the depth where the excitation intensity is maximal, the AFP. This is repeated for  $D$ , the distance from the coverslip to the objective lens, ranging through the full working distance of the objective to find the maximum intensity associate with each step of the objective,  $D$ . The NFP is calculated from  $D$ . The maximal intensity is normalized to the value at one micron below the coverslip-sample interface and is plotted versus NFP.



**Figure 36. Comparison of model and empirical data**

The photobleaching data were converted to excitation attenuation using the calibration curve. Because the model was undefined for  $Z_{fp} = 0$ , the model was calculated started at  $Z_{fp} = 1$  micron. Therefore both empirical data and model calculations were normalized to NFP = 5 microns.

interface. Because the model calculated a much faster attenuation rate than the experimental data, this also improved agreement between the model and empirical data. In fact, there is near agreement at depth for the 1.34 and 1.40 samples. However, overall the model was not a good predictor of the experimental data.

Although squaring the excitation intensity will model two-photon fluorescence excitation, signal attenuation data from Figure 14 were not compared to model predictions because attenuation of fluorescent emissions were not modeled.

## IV. DISCUSSION

### A. *Summary*

In Chapter 1, refractive index mismatch was shown to result in a rapid degradation of axial resolution, attenuation of signal and fluorescence excitation with depth, even in samples lacking significant scattering or absorption. This is likely due to spherical aberration-induced broadening of the focal point. In samples with reduced mismatch in refractive index, fluorescence excitation, signal, and resolution were improved.

In Chapter 2, we showed that refractive index heterogeneity in kidney tissue plays a significant role in signal attenuation with depth in MPM. Since refractive index heterogeneity causes scattering which has been shown to be a predominant cause of signal attenuation with depth, we investigated a simple way to minimize scatter, which profoundly improves image quality of deep tissue MPM images. Our clearing method utilizes a benzyl alcohol and glycerol solution to raise the background refractive index of kidney tissue, lowering the reduced scattering coefficient.

In Chapter 3, we modeled the effect of refractive index mismatch on fluorescence intensity with depth in multiphoton fluorescence microscopy. We took a geometrical optics approach, neglecting diffraction, to approximate to first order the axial distribution of light intensity typically used to trigger a two-photon event in multiphoton microscopy of biological tissue. However to improve the model, the excitation light was modeled as a Gaussian beam with a cylindrically symmetric wavefront using the beam radius and average power measured at the back aperture of the objective. Using this approach we

modeled how excitation intensity decreases due to refractive index mismatch between the immersion fluid and sample as one focuses deeper into a sample. These findings will be discussed in more detail below.

*B. The effect of refractive index mismatch on signal attenuation*

Refractive index mismatch between the immersion medium and sample causes spherical aberration which widens the focus of illumination light, reducing the photon density. Accordingly, studies in model systems have shown that spherical aberration causes fluorescence signal to attenuate with depth in MPM [115, 131, 136-138]. As expected, we found that fluorescence signal attenuated as a function of the magnitude of refractive index mismatch. This is likely due to spherical aberration-induced broadening of the focal point. In samples with reduced refractive index mismatch, fluorescence signal at depth was improved.

We and others have shown that further improvement in reach can be accomplished by manipulating spherical aberration via objective lens adjustment collars [110, 111]. More elaborate, but still easily implemented solutions for correcting spherical aberration in MPM include adaptive optics manipulations of the illumination beam, which has been shown to effectively address a variety of tissue-induced aberrations and thus improve the reach of MPM [138, 174, 175]. Unfortunately, adaptive optics requires collection of many images to derive the solution that will correct for the aberrations. This increases collection time, photobleaching, and photodamage. Time resolution is extremely important for collection of images of dynamic processes; therefore, current adaptive optics solutions are not well-suited for intravital imaging. Our



results suggest that, rather than using an exhaustive trial-and-error iterative approach, significant improvement in image quality may be more rapidly obtained with mirror solutions chosen from a much smaller subset of potential solutions directed at correcting spherical aberration.

*C. The effect of refractive index mismatch on excitation attenuation*

By measuring photobleaching rates, we were able to examine the effect of refractive index mismatch on excitation attenuation. The photobleaching rate depends on fluorescence excitation, but not on collection efficiency. Therefore, by comparing photobleaching rates at depth in samples with differing refractive indices, we showed that samples with greater refractive index mismatch had slower photobleaching rates at depth than those with less refractive index mismatch. These results indicate that greater refractive index mismatch causes more rapid attenuation of fluorescence excitation in MPM.

In principle, spherical aberration may reduce both excitation and collection of fluorescence. However, based upon the quadratic dependence of fluorescence excitation, and the use of non-descanned detectors, we anticipated that the preponderant effect of spherical aberration would be to reduce fluorescence excitation. As expected, excitation attenuation was shown to be the major contributor to signal attenuation with depth in MPM. Using an oil immersion objective, fluorescence excitation attenuated by nearly 80% at 40 micron-depth in agarose samples with refractive index 1.342. This is likely due to the quadratic dependence of fluorescence on excitation power when collecting

images with MPM. Therefore, optimizing fluorescence excitation as a function of depth is key to improving MPM images at depth.

*D. The effect of refractive index mismatch on emission attenuation*

Although spherical aberration was shown to predominantly affect excitation attenuation with depth in MPM, collection efficiency was also shown to depend on spherical aberration. Using the measured signal attenuation and excitation attenuation, we were able to calculate the fraction of fluorescence collected at depth compared to fluorescence collected at the surface of the sample. It was shown that collected emissions attenuated by 60% at 40 microns. Use of non-descanned detectors improves collection of scattered light, reducing the excitation power and detector gain necessary to generate bright images [116]. To assess how signal attenuation with depth compares between non-descanned and descanned detectors, image volumes were collected of agarose samples, refractive index 1.34. At 50 microns in depth, signal attenuated by 92%, using non-descanned detectors, and by 95%, using the descanned detectors with the pinhole open fully. Therefore although non-descanned detectors collect over 60% more scattered light at 50 microns deep than descanned detectors, that only amounts to 3% more signal at 50 microns in depth. Therefore regardless of detection method, attenuation of collection with depth is not nearly as important as attenuation of excitation.

*E. Signal attenuation in kidney tissue*

In order to assess the contribution of spherical aberration to signal attenuation in kidney tissue, signal attenuation was compared in kidney tissue and homogeneous test

samples of agarose with refractive index of 1.342, which matches the refractive index of the tissue mounting medium, PBS of 1.34. At 30 microns deep into the sample, signal attenuated by 98% in kidney and attenuated by 88% in a sample largely lacking in scattering and absorption, but similar in refractive index. Therefore, while a large fraction of signal attenuation in kidney tissue could be attributed to refractive index mismatch, an approximately equal further attenuation in signal (82%) was obtained in the kidney sample, likely due to light scatter and absorption induced by the tissue.

By collecting images with the water immersion objective, which closely matches the refractive index of kidney tissue mounted in PBS, fluorescent signal was greatly improved over the first 25 microns into the sample. However, at depths greater than 25 microns, the benefit of matching refractive index decreased. Therefore although, by comparing kidney tissue to test samples, it seemed that spherical aberration and scattering contributed equally to signal attenuation, these data indicate that spherical aberration is most significant at shallow depths while scattering is the predominant contributor further into biological tissue. Nonetheless, we have shown that spherical aberration can be a major contributor to depth-dependent signal attenuation in MPM, and that in fixed kidney tissue, signal attenuation can be improved by use of a water immersion objective.

Further studies in kidney tissue confirmed that scattering, caused by refractive index heterogeneity within the samples, plays a significant role in signal attenuation with depth in MPM. We investigated a simple method to minimize scatter, resulting in profound improvement of the quality of deep tissue MPM images. Our optical clearing method utilizes a benzyl alcohol and glycerol mixture to raise and homogenize the background refractive index of kidney tissue. By comparing different compilations of

optical clearing solutions to adjust the refractive indices of the media, we showed that reducing refractive index heterogeneity within fixed kidney tissue significantly improved imaging depth.

Although we have shown that refractive index mismatch between the immersion fluid and sample causes significant attenuation of signal and resolution with depth, studies with a water immersion objective show that reducing scattering increases reach despite an increase in spherical aberration. These data confirm that scattering is the predominant cause of signal attenuation at depth in fixed kidney tissue.

The largest improvements are obtained when both scattering and refractive index mismatch are reduced. Images collected using an oil immersion objective of kidney tissue mounted in media with refractive index 1.51 showed very minor signal attenuation with depth.

#### *F. Axial resolution degradation in kidney tissue*

The effect of refractive index mismatch on resolution is hard to predict knowing that decreased photon flux leads to decreased excitation. Refractive index mismatch between the immersion fluid and sample leads to spherical aberration which broadens the focus. In conventional, single-photon fluorescence excitation, the broadening of the focal spot by spherical aberration increases the volume of excitation. However, because of the quadratic dependence of two-photon fluorescence on excitation intensity, the effect on resolution depends upon the distribution of illumination in the distorted PSF, and spherical aberration may not necessarily increase the effective volume of excitation. Therefore, refractive index mismatch could reduce resolution except that focal

broadening also decreases the photon flux which reduces the probability of two-photon excitation occurring.

By collecting PSF data using fluorescent sub-resolution microspheres mounted in agarose samples with varied refractive indices, we found that refractive index mismatch caused axial resolution to degrade with imaging depth. We also found that in samples with less refractive index mismatch, axial resolution degradation was less pronounced at depth. This agrees with previous studies examining the effect of spherical aberration on axial resolution with depth [131, 136, 143].

Resolution might also be expected to be affected by the scattering that results from refractive index heterogeneity within kidney tissue. However, the effect of scattering on resolution depends upon the scattering anisotropy. Whereas highly anisotropic scattering may result in a broadened focal point, isotropic scattering may reduce the total number of photons at the focus without changing the size of the focus of effective fluorescence excitation.

Using sub-resolution fluorescent microspheres injected into kidney tissue and mounted with different optical clearing solutions to vary refractive index heterogeneity, we evaluated axial resolution at depth in kidney tissue. Axial resolution did not degrade in samples with heterogeneous refractive index when images were collected without refractive index mismatch between the immersion fluid and the sample mounting medium. Axial resolution was shown to depend only on spherical aberration but not on refractive index heterogeneity. In fact using the oil immersion objective, axial resolution degraded similarly in fixed kidney tissue mounted in PBS and agarose samples with refractive index 1.34 (Figures 15 and 28).

Our data are consistent with some studies that show that imaging deep into scattering samples has no effect on resolution [116, 130, 143] and contradicts those studies that show scattering degrades resolution with depth [141, 142]. However, both contradicting studies were conducted with refractive index mismatch between the objective immersion media (air) and the aqueous sample. Schilders et al. [142] point out that refractive index mismatch between the objective and sample leads to degradation of resolution; although, they state that resolution degradation caused by refractive index mismatch is negligible compared to the degradation caused by scattering. This may be the case for their samples with extremely short scattering-mean-free-path lengths; however, our data show that the degree of scattering in kidney tissue does not degrade axial resolution within 50 microns of depth (Figure 24). As for Ying et al. [141], their data support the work by Theer et al. on the fundamental imaging depth [129]. Both studies show that when imaging deep into tissue, scattering causes out-of-focus fluorescence at the surface of the sample, degrading image quality. We suggest that scattering on the order of that in biological tissue eliminates photons from the two-photon excitation PSF; therefore, within the fundamental imaging depth, axial resolution is not degraded. Whereas refractive index mismatch between the immersion medium and sample causes spherical aberration which broadens the focus and degrades axial resolution.

#### *G. Geometrical model of refractive index mismatch in MPM*

To model the effect of refractive index mismatch in MPM, we developed a geometrical model to approximate to first order the axial distribution of excitation

intensity as a function of focal depth. The model was not a good predictor of the excitation attenuation data collected. The model predicted a much steeper fall off in excitation than was actually measured. Because the model was undefined for a focal position at the coverslip, the data was normalized to 5 microns deep which did improve the fit at depth for the 1.34 sample and the 1.40 sample.

The model relies on many assumptions. We used geometrical optics instead of diffraction theory which has been shown to be an inaccurate predictor of axial scaling [135]. To improve the model, we modeled the excitation light as a Gaussian beam with a cylindrically symmetric wavefront using the beam radius and average power measured at the back aperture of the objective. To map the correct intensity from the back aperture to the focus, it was necessary to make assumptions about the oil immersion objective. We simplified the objective to two lenses and defined the back aperture lens based on the angles known about the front objective lens.

Therefore, even with improvements to the geometrical optics approach, our model does not accurately predict the effect of refractive index mismatch in MPM. Diffraction theory may generate an accurate model of fluorescence excitation in MPM. In confocal fluorescence microscopy, accurate models of axial scaling for increasing focusing depth from refractive index mismatch have been used to calculate the correct thickness of objects in tissues and the refractive index of tissues [134, 135]. This theoretical model was first suggested by Hell et al. and is based on vectorial diffraction theory using the Huygens-Fresnel principle and Fermat's principle [140]. Kuypers et al. refined it by taking into account the shape of the actual illumination profile for their system at the exit pupil of the objective lens when calculating the illumination PSF [135]. Török et al. have

also developed a rigorous theory of high aperture confocal PSFs when focusing through a dielectric interface, but they used the Debye approximation [176-178]. This was shown to produce the same results as the model derived by Hell et al. [179]. More recently, Nasse and Woehl developed a model of the illumination PSF in CLSM that takes into account imaging through up to three layers (immersion oil, glass coverslip, aqueous sample medium), and they account for objectives with collars to correct for certain coverslip thicknesses and refractive indices but are operated under non-design conditions [180].

However for MPM, models of the PSF have been limited to systems with low NA objective lenses [115, 181, 182]. Sheppard and Gu calculated the two-photon PSF was the same as the single-photon confocal PSF, but they did not examine the effects of refractive index mismatch [181]. Booth and Wilson defined the aberration function using Zernike polynomials like Török et al. and applied it to single-photon confocal fluorescence microscopy, two-photon conventional fluorescence microscopy, and two-photon confocal fluorescence microscopy [115]. Jacobsen et al. developed a model for refractive index mismatch-induced aberration in two-photon confocal fluorescence microscopy using high NA objectives based on the model by Hell et al. for single-photon confocal fluorescence microscopy; however, they note that a variety of photophysical and photochemical processes are not accounted for in the model that might also play a significant role in two-photon excitation image generation [137].



## V. CONCLUSIONS

We have examined the effects of refractive index mismatch on imaging depth in MPM. We investigated both refractive index mismatch between the microscope objective lens immersion fluid, the coverslip, and the sample as well as refractive index mismatch within the sample caused by refractive index heterogeneities. By reducing refractive index heterogeneity and scattering using optical clearing, we were able to improve imaging depth. However, it is important when using optical clearing media that the refractive index of the media matches that of the immersion fluid of the microscope objective. Although reducing refractive index heterogeneity, at the expense of refractive index mismatch, improves imaging depth, axial resolution degrades with depth. However, by reducing refractive index heterogeneities and matching the refractive index of the sample with the immersion fluid of the objective, we were able to improve imaging depth and axial resolution at depth over the entire working distance (150 microns) of an NA 1.4 oil immersion objective.

In conclusion, spherical aberration and scattering cause rapid signal attenuation in MPM of biological tissue. For quantitative studies using MPM, high quality images must be collected through the entire image volume. Therefore minimization of spherical aberration and scattering is crucial to collecting the highest quality and deepest fluorescent images necessary for quantitative analysis.

## VI. FUTURE STUDIES

The characterization of signal attenuation and resolution degradation with depth caused by refractive index mismatch and refractive index heterogeneity and their contribution to signal attenuation and resolution degradation with depth in kidney tissue are novel findings. There are however, a number of future studies that are needed to improve imaging depth in MPM. One of the studies would be to evaluate the effectiveness of underfilling the back aperture of the objective on the illumination path, which would effectively decrease the NA, improving signal attenuation with depth, but retaining the benefits of the large acceptance angle of a high NA objective for collecting emissions [130]. Although this does not affect fluorescence excitation [5], the effect on axial resolution would need to be evaluated. We expect that axial resolution will decrease at the surface; however, at depth, it is not intuitive how the axial resolution will compare to overfilling the back aperture of the objective. Because lower NA objectives are less sensitive to spherical aberration [183], axial resolution may actually be better at depth when imaging with an underfilled objective than an overfilled objective.

We and others have shown that further improvement in reach can be accomplished by manipulating spherical aberration via objective lens adjustment collars [110, 111]. Another study would be to develop and evaluate a lens system that can be placed in the excitation path to correct for spherical aberration at depth in samples of a known refractive index. Intelligent Imaging Innovations has developed a Spherical Aberration Correction System for confocal microscopy that is placed in the collection path to compensate for spherical aberration so more signal passes through the pinhole

reaching the detector. For MPM this lens system could be adjusted empirically for samples of unknown refractive index. By mounting fluorescent beads in a sample, the system could be empirically adjusted to minimize axial resolution at depth by examining the PSF. A better approach would be a lens system that could be adjusted with depth such that it automatically corrected for spherical aberration.

More elaborate, but still easily implemented solutions for improving imaging depth in MPM include adaptive optics manipulations of the illuminations beam, which has been shown to effectively address a variety of tissue-induced aberrations and thus improve the reach of MPM [138, 174, 175]. This system would compensate for both refractive index mismatch and refractive index heterogeneity. Or a more simplified approach would be to use adaptive optics to correct for spherical aberration, and not refractive index heterogeneity, which would greatly increase the speed necessary for adequate correction. Combining these approaches with an optical parametric oscillator as an infrared multiphoton light source and near-infrared fluorophores would help reduce effects from Rayleigh scattering and absorption of light by hemoglobin.

## VII. APPENDICES

### A. Geometrical model

This MATLAB program was written in collaboration with Jason Byars.

#### 1. Overnight OD program

```
function overnightod(ned)
% Iterate over the array ned and find the D value associated with the
% maximum intensity
% where ned is an array of possible refractive indices for a sample. It
% returns the focal plane,
% D position, and associated intensity. The results are saved in a file
% for
% later analysis.
for i=1:length(ned)
    range = optimizedrange(ned(i));
    name = sprintf('optimized%f.dat', ned(i));
    save(name, 'range');
end
```

#### 2. Optimize D Range program

```
function result = optimizedrange(ned)
% Find optimized D value and max intensity for fp = 1 to 149
%
%
global ZRANGE
ZRANGE=150
result = zeros(ZRANGE-1,3); % populate array with zeros
for fp=1:1:ZRANGE-1
    result(fp,1) = fp;
    result(fp,2) = optimized(fp, ned);
    result(fp,3) = intensityford(result(fp,2),fp,.01);
end % end for

end
```

#### 3. Optimize D program

```
function result = optimized(fp,ned)
% This function returns the distance between the objective and the
% coverslip
% for the maximum intensity.
% fp is the position of the focal plane in microns from the cover slip
% ned is the array of possible sample refractive indices

global D NA NOBJ WDT T N N1 N2 N3 ALPHA ZRANGE I w rmax X
NA = 1.4; % numerical aperture of the objective
NOBJ = 1.515; % refractive index of the objective
```

```

WOBJ = 150; % working distance of the objective in um
T = 170; % cover slip thickness in microns
WDT = WOBJ + T; % working distance + ideal coverslip
thickness in um
N = 1.51633; % actual refractive index of objective lens
glass
N1 = 1.515; % refractive index of the immersion fluid
N2 = 1.515; % actual refractive index of cover glass
N3 = ned; % hypothetical refractive index of the
sample
ALPHA = asin (NA/NOBJ); % aperture angle
rmax = (WDT)*tan (ALPHA); % radius of the objective lens
%step = 0.5;
w = 4200; % radius of the back aperture in microns and
pulse width
% assume filled objective
P = 2000; % power in uW
I = 2*P/(3.14159*w^2); % initial intensity
delta = 10^-58; % fluorophore cross section in m^4sec
f = 82*10^6; % repetition rate of laser in Hz
tau = 100*10^-15; % temporal pulse width of laser in seconds

lambda = 800*10^-9; % wavelength in meters

X=0.1; % lateral range to include at fp

%excitprob = delta*(P*10^-6)^2/(f^2*tau)*(NA^2/(2*1.0546*10^-
34*3*10^8*lambda))^2;
% rintensity is in microwatts! so plug it in here?

%zrange 5-150 step 5 where zrange always <= WOBJ
ZRANGE = 150; % distance from coverslip into the sample
in um

dmax = WOBJ-fp; % maximum depth into the sample in microns
d= dmax;
dstep = -1;
maxintensity = 0.0; % integrated intensity
disp(sprintf('doing fp %d', fp));
% loop over D range rough pass assuming after reaching a peak we can
stop
% searching
for d = dmax:dstep:1
    intensity = intensityford(d,fp,1);
    if maxintensity > intensity
        break;
    else
        maxintensity = intensity;
    end
end % end d loop

dmax = d+2; % search d-2 to d+2 for actual peak intensity location and
value
disp(sprintf('optimal d between %f and %f for dstep of %f intensity
%f',dmax-2, dmax, dstep, maxintensity));

```

```

dstep = dstep / 10; % reduce step size on each pass to refine search
% search cutoff of .0001 step size from emprical results
while ( abs(dstep) >= .0001 )
    maxintensity = 0;
    %disp(sprintf('%f:%f:%f',dmax,dstep,(dmax-20*abs(dstep)) ));
    for d = dmax:dstep:(dmax-20*abs(dstep))
        intensity = intensityford(d,fp,1);
        if maxintensity > intensity
            break;
        else
            maxintensity = intensity;
        end
    end % end d loop    d = d+1;
    dmax = d + 2*abs(dstep);
    %disp(sprintf('optimal d between %f and %f for dstep of %f
intensity %f',dmax+2*dstep,dmax, dstep, maxintensity));
    dstep = dstep / 10;
end
result = d + 10*abs(dstep); % move back to the d value that was the
peak
end %end function

```

#### 4. *Intensity program*

```

function intensity = intensityford(d,fp,rstep)
% For a given distance between coverslip and objective, focal plane,
and
% step to integrate over the objective radius, return the intensity
global rmax w
arr = floor(rmax); % integrating over integer steps for practical
time constraints
intensity = 0;
start = 1;
R1 = 1;
%search for doughnuts
while (R1 < arr && R1 ~= 0)
    S1 = 0; % the S value (radius at the back aperture)
associated with R1
    S2 = 0; % the S value (radius at the back aperture)
associated with R2
    R1 = 0; % the first r position that contributes to the
intensity
    R2 = 0; % the last r position that contributes to the
intensity

    % find R1
    for r = start:rstep:arr
        [beta,theta3, z, lower, upper] = thetans(r,d,fp);
        %disp(sprintf('fp %d d %d r %d %f <= %f <=
%f',fp,d,r,lower, tan(theta3), upper));
        if z < 0
            continue;
        end
        % if within bounds the intensity contributes
        if (lower <= tan(theta3) && tan(theta3) <= upper) || ( fp-
.1 <= z && z <= fp+.1 )

```

```

        R1 = r;
        if R1 == 1
            S1 = 0;
        else
            S1 = S(R1, beta);
        end
        break;
    end
end %end for
if (R1 == 0 || R1 == arr) %check for out of bound
    %disp(sprintf('fp %d d %d No R1', fp, d));
    break;
end
% find R2
for r = R1+rstep:rstep:arr
    [beta,theta3, z, lower, upper] = thetans(r,d,fp);
    if z < 0
        continue;
    end
    % if within bounds the intensity contributes
    if ((lower > tan(theta3) || tan(theta3) > upper) && ( fp-.1
> z || z > fp+.1 ) )
        R2 = r-rstep;
        [beta,theta3, z, lower, upper] = thetans(R2,d,fp);
        S2 = S(R2, beta);
        break;
    end
    if (r == arr)
        R2 = rmax;
        S2 = S(R2, beta);
    end
end %end for
if (R2 == 0)
    %disp(sprintf('fp %d d %d R1 %d No R2',fp, d, R1));
    break;
end
start = R2+rstep; % continue searching for contributing R
values after R2
intensity = intensity + pi*w^2/2*abs(sintensity(S2)-
sintensity(S1));
    end %end while
end

function [beta,theta3,z,lower,upper] =thetans(r,d,fp)
% This is a convenience function to perform calculations that occur in
% several places.
    global WDT NOBJ N N1 N2 N3 T X
    alphas = atan (r/(WDT)); % assuming no refraction, the
angle of light from radius
    beta = asin((NOBJ/N)*sin(alphas)); % the actual angle of light
incident on the objective lens
    theta1 = asin (N/N1*sin (beta)); % refraction angles for the
objective lens-immersion fluid interface
    theta2 = asin (N/N2*sin (beta)); % refraction angles for the
immersion fluid-coverslip interface

```

```

theta3 = asin (N/N3*sin (beta));          % refraction angles for the
coverslip-sample interface
z = (r-d*tan(theta1)-T*tan(theta2))/tan(theta3); % depth into the
sample where light from a cone with radius r will focus
lower = (r-d*tan(theta1)-T*tan(theta2)-X)/fp; % lateral range around
fp
upper = (r-d*tan(theta1)-T*tan(theta2)+X)/fp; % lateral range around
fp
end

function sposition = S(r, beta)
% radial distance at the back aperture associated with r for a given
beta
    global w NA N rmax
    sposition = (w-rmax)/(tan(asin(NA/N))*tan(beta)+r);
    %disp(sprintf('%f-
%f)/(tan(asin(%f/%f))*tan(%f)+%f',w,rmax,NA,N,beta,r));
end

function sint = sintensity(s)
% intensity calculation for a given S position
    global I w
    sint = I*exp(-2*(s)^2/(w^2));
    %disp(sprintf('r %.10f rmax %.10f beta %.10f S %.10f rintensity
%.10f', r, rmax, beta,S(r,rmax,beta), arr));
end

% warn about out of bounds later
function zoff = zindex(z, r)
% not used in final version
    global ZRANGE
    zoff = round(z);
    if (zoff <= 0 || zoff == NaN || zoff > ZRANGE)
        disp(sprintf('z is bad %f for r %f', z, r));
        zoff = -1;
    end
end

function s = finds(r, start)
% not used in final version
    global N NA w WDT NOBJ ALPHA
    alphas = atan (r/(WDT));
    beta = asin((NOBJ/N)*sin(alphas));
    rmax = (WDT)*tan (ALPHA);
    s = ((w-rmax)/(tan(asin(NA/N))*tan(beta) + r) - start;
    s = abs(s);
end

function arr = findr(s)
% not used in final version
    global WDT ALPHA
    rmax = (WDT)*tan (ALPHA);
    [arr, val] = fminbnd(@(x)finds(x, s), 0, rmax);
    %disp(sprintf('S %f R %f val %f', s, arr, val));
end

```



## B. *ImageJ plugins*

### 1. *Getting\_Loaded\_Olympus.java*

```
import ij.*;
import ij.io.*;
import ij.plugin.*;
import ij.process.*;
import java.io.*;
import java.util.Arrays;
import java.util.Comparator;

/** This filter just matches oif files. There is nothing exciting here.
 */
class OIFFilter implements FilenameFilter {
    public boolean accept(File dir, String name) {
        File foo = new File(dir.getPath() + File.separator + name);
        if (!foo.isFile()) return false;
        if (!foo.canRead()) return false;
        return (name.toLowerCase().endsWith(".oif"));
    }
}

/** This filter just matches tif files. There is nothing exciting here.
 */
class TiffFilter implements FilenameFilter {
    public boolean accept(File dir, String name) {
        File foo = new File(dir.getPath() + File.separator + name);
        if (!foo.isFile()) return false;
        if (!foo.canRead()) return false;
        return (name.toLowerCase().endsWith(".tif"));
    }
}

/** This comparator is used to determine the appropriate order of tiff files
 * based on channel and slice.
 */
class TIFFComparator implements Comparator<String> {
    public int compare(final String o1, final String o2) {
        int index = o1.lastIndexOf("_C0");
        index = o1.indexOf("Z", index)+1;
        int end = index;
        while (Character.isDigit(o1.charAt(end))) end++;
    }
}
```

```

        int z1 = Integer.valueOf(o1.substring(index,end)).intValue();
        index = o2.lastIndexOf("_C0");
        index = o2.indexOf("Z", index)+1;
        end = index;
        while (Character.isDigit(o2.charAt(end))) end++;
        int z2 = Integer.valueOf(o2.substring(index,end)).intValue();
        return z1-z2;
    }
}

/** This plugin quickly loads Olympus OIF files into ImageJ correctly dealing with stack
with
* greather than 1000 slices.
* @author Jason Byars <jbyars@iupui.edu>
* @version 0.001
*/
public class Getting_Loaded_Olympus implements PlugIn {
    String[][] slices;
    String src;
    int channels;

    /** This is the main method of the plugin. It prompts the user for the path to the
directory of tiffs
    * when not provided one as an argument.
    * @see ij.plugin.PlugIn#run(java.lang.String)
    * @param arg used to provide a single paramter, src when run from macros
    *
    */
    public void run(String arg) {
        channels = 0;
        slices = null;
        src = null;

        if (IJ.versionLessThan("1.40")) {
            IJ.showMessage("ImageJ 1.40 or greater required.");
            return;
        }

        try {
            if (Macro.getOptions() == null) {
                if (!showDialog())
                    return;
            } else {
                src = Macro.getValue(Macro.getOptions(), "src", "");
                if (src.trim() == "") {
                    IJ.showStatus("Error: no folder specified");
                }
            }
        }
    }
}

```

```

        return;
    }
}
if (!divineList())
    return;
load();
} catch (Exception e) {
    CharArrayWriter caw = new CharArrayWriter();
    PrintWriter pw = new PrintWriter(caw);
    e.printStackTrace(pw);
    IJ.write(caw.toString());
    IJ.showStatus("");
}

IJ.register(Getting_Loaded_Olympus.class);
}

/** Get a list of all the tiffs in the folder. Sort the list appropriately by channel
and
* z section.
*
*/
private boolean divineList() {
    try {
        File folder = new File(src);
        FilenameFilter filter = new TiffFilter();
        String[] tlist = folder.list(filter);
        if (tlist == null) {
            IJ.showStatus("Error: could not find any tiffs");
            return false;
        }
        if (tlist.length == 0) return false;

        StringBuffer pattern = new StringBuffer();
        for(int i=0; tlist != null && i < tlist.length; i++) {
            int index = tlist[i].lastIndexOf("_C0");
            String tmp = tlist[i].substring(index, index+5);
            if (pattern.indexOf(tmp) == -1) {
                pattern.append(tmp);
                channels++;
            }
        }
        //sort into channels in case there is an act of stupidity
        slices = new String[channels][];
        int index=0;
        String chtmp = "";

```

```

        for (int c=0; c<channels; c++) {
            slices[c] = new String[tlist.length/channels];
            int count=0;
            //get the pattern
            for(int i=0; tlist != null && i < tlist.length; i++) {
                if (tlist[i] == null) continue;
                index = tlist[i].lastIndexOf("_C0");
                String tmp = tlist[i].substring(index, index+5);
                if (chtmp.indexOf(tmp) == -1) {
                    chtmp = tmp;
                    break;
                }
            }
            for(int i=0; tlist != null && i < tlist.length; i++) {
                if (tlist[i] == null) continue;
                if (tlist[i].indexOf(chtmp) != -1) {
                    slices[c][count++] = tlist[i];
                    tlist[i] = null;
                }
            }
            //sort along z for dumb numbering
            Arrays.sort(slices[c], new TIFFComparator());
        }

    } catch (Exception e) {
        CharArrayWriter caw = new CharArrayWriter();
        PrintWriter pw = new PrintWriter(caw);
        e.printStackTrace(pw);
        IJ.write(caw.toString());
        IJ.showStatus("");
    }
    return true;
}

/** This method iterates over the list of tiffs and build large single channels
stacks.
*
*/
public void load() {
    Opener opener = new Opener();
    opener.setSilentMode(true);
    ImagePlus imp = null;
    ImageStack stack = null;
    for(int c=0; c<channels; c++) {
        imp = opener.openImage(src, slices[c][0]);
    }
}

```

```

        stack = imp.getStack();
        for (int i=1; i<lices[c].length; i++) {
            imp = opener.openImage(src, slices[c][i]);
            ImageProcessor ip = imp.getProcessor();
            File nfo = new File(slices[c][i]);
            stack.addSlice(nfo.getName(), ip);
            imp = null;
            IJ.showStatus((i+1)+"/"+slices[c].length);
            IJ.showProgress(i+1, slices[c].length);
        }
        int end = slices[0][0].lastIndexOf("_C0");
        String title = slices[0][0].substring(0,end);
        ImagePlus imp2 = new ImagePlus(title, stack);
        imp2.show();
    }
}

/** Prompt the user for the location of the folder of tiffs.
 *
 */
public boolean showDialog() {
    DirectoryChooser dc = new DirectoryChooser("Select the folder of tiffs");
    src = dc.getDirectory();
    if (src == null) return false;

    return true;
}

void showAbout() {
    String title = "About " + getClass().getName() + "...";
    IJ.showMessage(title, "This plugin open Olympus stacks with over 1000
slices correctly");
}

void error() {
    String title = "About " + getClass().getName() + "...";
    IJ.showMessage(title, "This plugin requires an Olympus folder of tiffs");
}
}

```

## 2. Pam\_Background.java

```
import ij.*;
import ij.measure.*;
import ij.plugin.*;

/** Find the mean of the last 10 slices of a stack.
 * @author Jason Byars <jbyars@iupui.edu>
 * @version 0.001
 */
public class Pam_Background implements PlugIn {

    ImagePlus imp;
    ResultsTable rt;

    /**
    *****
    public Pam_Background() {
        makeResultTable();
        IJ.register(Pam_Bead_Stats.class);
    }

    /**
    *****
    /** Find the mean of the last 10 slices of a stack.
    */
    private double last10Mean() {
        int orig = imp.getSlice();
        int first = imp.getNSlices()-9; //-9 does 10 slices
        first = (first < 1) ? 1 : first;
        long total = 0;
        for (int i=first; i<=imp.getNSlices(); i++) {
            imp.setSlice(i);
            for (int y=0; y<imp.getHeight(); y++) {
                for (int x=0; x<imp.getWidth(); x++) {
                    total += imp.getPixel(x,y)[0];
                }
            }
        }
        imp.setSlice(orig);
        double mean = total / (10.0*imp.getWidth()*imp.getHeight());
        return mean;
    }
}
```

```

//*****
*****
/** Create a results table.
 */
private void makeResultTable() {
    rt = new ResultsTable();
    rt.reset();
    rt.getFreeColumn("Mean");
    //fields for array of data points
}

//*****
*****
/** Find the mean of the last 10 slices of a stack and show the results in the results
table.
 * @see ij.plugin.PlugIn#run(java.lang.String)
 * @param arg used to provide a single paramter, src when run from macros
 */
public void run(String arg) {
    if (IJ.versionLessThan("1.40")) {
        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    imp = WindowManager.getCurrentImage();

    if (imp==null) {
        IJ.showMessage("You must have images open for this plugin!");
        return;
    }
    if (imp.getNSlices() < 10) {
        IJ.error("The stack has less than 10 slices. Try again hoser.");
        return;
    }

    double mean = last10Mean();
    rt.incrementCounter();
    rt.addLabel("Stack", imp.getTitle());
    rt.addValue(0, mean);

    rt.show("Mean of last 10 slices");
}

//*****
*****
void showAbout() {

```

```

        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This plugin finds the mean for the last 10 slices in
a stack.");
    }

    /*******
    *****
    void error() {
        IJ.showMessage(getClass().getName(), "Something went wrong.");
    }

}

```

### 3. *Pam\_Bead\_Stats.java*

```

import ij.*;
import ij.plugin.frame.*;
import ij.measure.*;
import ij.gui.*;
import java.awt.*;
import java.awt.event.*;

/** Given a region of interest it, it finds the brightest point and averages with the
specified
* number of surrounding points.
* @author Jason Byars <jbyars@iupui.edu>
* @version 0.005
*/
public class Pam_Bead_Stats extends PlugInFrame implements ActionListener {

    private static final long serialVersionUID = -8626748743748121467L;
    Panel panel;
    static Frame instance;
    GridBagConstraints gbc = new GridBagConstraints();
    ImagePlus imp;
    Roi currentRoi;
    ResultsTable rt;
    TextField txtPlanes;
    TextField txtRadius;
    int planes;
    int radius;

    public Pam_Bead_Stats() {
        super("Pam_Bead_Stats v0.005");
        if (IJ.versionLessThan("1.40")) {

```



```

        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    if (instance!=null) {
        instance.toFront();
        return;
    }
    instance = this;
    addKeyListener(IJ.getInstance());
    makeResultTable();
    showDialog();

    IJ.register(Pam_Bead_Stats.class);
}

public void actionPerformed(ActionEvent e) {
    imp = WindowManager.getCurrentImage();
    currentRoi = imp.getRoi();
    if (imp==null) {
        IJ.beep();
        IJ.showStatus("No image");
        return;
    }
    if (currentRoi == null) {
        IJ.beep();
        IJ.showStatus("No ROI");
        return;
    }
    if (currentRoi.getType() == Roi.LINE) {
        IJ.beep();
        IJ.showStatus("Rectangles or Ovals only!");
        return;
    }
    String label = e.getActionCommand();
    if (label==null) {
        IJ.showStatus("I have no idea what to do");
        return;
    }
    try {
        planes = Integer.parseInt(txtPlanes.getText());
        radius = Integer.parseInt(txtRadius.getText());
    } catch (NumberFormatException n) {
        IJ.showMessage("Give me real numbers!");
        return;
    }
}

```

```

    if (planes < 1) {
        IJ.showMessage("Invalid number of planes. Try again hoser.");
        return;
    }
    if (radius < 1) {
        IJ.showMessage("Invalid radius. Try again hoser.");
        return;
    }

    if (label == "Measure")
        measureit();
    else if (label == "Measure All")
        measureAll();
    else if (label == "Dump ROI")
        dumpROI();
    else
        imp.killRoi();
}

private void dumpROI() {
    int[] value = {0,0,0,0};
    int orig = imp.getSlice();
    Rectangle bounds = currentRoi.getBounds();
    ResultsTable tmp = new ResultsTable();
    tmp.reset();

    for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++)
        tmp.getFreeColumn("X"+x);

    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();

    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
            tmp.incrementCounter();
            for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
                if (currentRoi.contains(x,y))
                    value = imp.getPixel(x,y);
                else

```

```

        value[0] = 0;
        tmp.addValue((int) (x-bounds.getX()), value[0]);
    }
}
}
tmp.show("ROI x"+(int) bounds.getX()+" y"+ (int) bounds.getY()+"
z"+imp.getSlice());
imp.setSlice(orig);
}

private int[] findPeak() {
    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();
    int[] peak = {0,0,0,0,0};
    int[] value = {0,0,0,0};
    int multi = 1;

    Rectangle bounds = currentRoi.getBounds();
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
            for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
                if (!currentRoi.contains(x,y)) continue;
                value = imp.getPixel(x,y);

                if ( value[0] > peak[0] ) {
                    peak[0] = value[0];
                    peak[1] = x;
                    peak[2] = y;
                    peak[3] = z;
                    multi = 1;
                } else if (value[0] == peak[0]) {
                    multi++;
                }
            }
        }
    }

    peak[4] = multi;
    return peak;
}

```

```

private void measureAll() {
    RoiManager mgr = RoiManager.getInstance();
    if (mgr == null) {
        IJ.beep();
        IJ.showStatus("Roi Manager not open");
        return;
    }

    Roi[] rois = mgr.getRoisAsArray();

    int orig = imp.getSlice();
    for (int i=0; i < rois.length; i++) {
        currentRoi = rois[i];
        imp.setSlice(mgr.getSliceNumber(currentRoi.getName()));
        if (mgr.getSliceNumber(currentRoi.getName()) < 1) {
            IJ.error("I don't know what the slice is for ROI
"+currentRoi.getName());
        }
        measureit();
    }
    imp.setSlice(orig);
}

private void measureit() {
    int orig = imp.getSlice();

    int[] peak = findPeak();
    int[] value = {0,0,0,0};

    //ok do stats
    double intensity = 0;
    int voxels = 0;
    int xmin = peak[1]-radius;
    int xmax = peak[1]+radius;
    int ymin = peak[2]-radius;
    int ymax = peak[2]+radius;
    int zmin = peak[3]-radius;
    int zmax = peak[3]+radius;
    if ( xmin < 0 ) xmin = 0;
    if ( ymin < 0 ) ymin = 0;
    if ( zmin < 0 ) zmin = 0;
    if ( xmax > imp.getWidth()-1 ) xmax = imp.getWidth() - 1;
    if ( ymax > imp.getHeight()-1 ) ymax = imp.getHeight() - 1;
    if ( zmax > imp.getNSlices()-1 ) zmax = imp.getNSlices() - 1;
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
    }
}

```

```

        for (int y = ymin; y <= ymax; y++) {
            for (int x = xmin; x <= xmax; x++,voxels++) {
                value = imp.getPixel(x,y);
                intensity += value[0];
            }
        }
    }
    imp.setSlice(orig);

    if (rt.getCounter()==0) makeResultTable(); //results table closed
    rt.incrementCounter();
    rt.addLabel("Name",currentRoi.getName());
    rt.addValue(0,peak[1]);
    rt.addValue(1,peak[2]);
    rt.addValue(2,peak[3]);
    rt.addValue(3,peak[0]);
    rt.addValue(4,intensity);
    rt.addValue(5,intensity/voxels);
    rt.addValue(6,peak[4]);

    rt.show("Results for Peak Pixel");
    String s = "Peak "+peak[0]+" x: "+peak[1]+" y: "+peak[2]+" z: "+peak[3];
    IJ.showStatus(s);
}

private void makeResultTable() {
    rt = new ResultsTable();
    rt.reset();
    rt.getFreeColumn("X");
    rt.getFreeColumn("Y");
    rt.getFreeColumn("Z");
    rt.getFreeColumn("Peak");
    rt.getFreeColumn("Total Intensity");
    rt.getFreeColumn("Mean");
    rt.getFreeColumn("Multiple");
}

public void processWindowEvent(WindowEvent e) {
    super.processWindowEvent(e);
    if (e.getID()==WindowEvent.WINDOW_CLOSING) {
        instance = null;
    }
}

private void set_gbc(int row, int column, int width, int height, int fill) {
    set_gbc(row,column,width,height,fill,0,0);
}

```

```

    }

    private void set_gbc(int row, int column, int width, int height, int fill, int padx, int
pady) {
        gbc.gridy = row;
        gbc.gridx = column;
        gbc.gridwidth = width;
        gbc.gridheight = height;
        gbc.fill = fill; // GridBagConstraints.NONE .HORIZONTAL
.VERTICAL .BOTH
        gbc.ipadx = padx;
        gbc.ipady = pady;
        // leave other fields (eg, anchor) unchanged.
    }

    public void showDialog() {
        //because windows is stupid
        setLayout(new FlowLayout());
        panel = new Panel();
        GridBagLayout gridbag = new GridBagLayout();
        panel.setLayout(gridbag);
        String s = "Select a region around a bead.";
        Label l = new Label(s);
        set_gbc(0,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        s = "Specify how far above and below to look.";
        l = new Label(s);
        set_gbc(1,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        s = "Specify the radius to average.";
        l = new Label(s);
        set_gbc(2,0,4,1, GridBagConstraints.HORIZONTAL, 0, 10);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("Planes to check", Label.RIGHT);
        set_gbc(3,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        txtPlanes = new TextField("10", 20);
        set_gbc(3,2,2,1, GridBagConstraints.NONE);
        gridbag.setConstraints(txtPlanes,gbc);
        panel.add(txtPlanes, gbc);
        l = new Label("Radius", Label.RIGHT);
        set_gbc(4,0,2,1, GridBagConstraints.HORIZONTAL);
    }

```

```

        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        txtRadius = new TextField("1", 20);
        set_gbc(4,2,2,1, GridBagConstraints.NONE);
        gridbag.setConstraints(txtRadius,gbc);
        panel.add(txtRadius, gbc);
        Button b = new Button("Measure");
        b.addActionListener(this);
        b.addKeyListener(IJ.getInstance());
        set_gbc(5,0,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        b = new Button("Measure All");
        b.addActionListener(this);
        b.addKeyListener(IJ.getInstance());
        set_gbc(5,1,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        b = new Button("Dump ROI");
        b.addActionListener(this);
        b.addKeyListener(IJ.getInstance());
        set_gbc(5,2,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        b = new Button("Clear ROI");
        b.addActionListener(this);
        b.addKeyListener(IJ.getInstance());
        set_gbc(5,3,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        add(panel);

        pack();
        GUI.center(this);
        setVisible(true);
    }

    void showAbout() {
        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This app takes a region, finds the brightest point
and averages it with pixels in a radius of x.");
    }

    void error() {

```

```

        IJ.showMessage("Pam_Bead_Stats", "This plugin requires a defined
region to work");
    }

}

```

#### 4. *Pam\_Bead\_Stats2.java*

```

import ij.*;
import ij.plugin.frame.*;
import ij.measure.*;
import ij.gui.*;
import java.awt.*;
import java.awt.event.*;
import java.io.*;

/** Given a region of interest it, it finds the brightest point and averages with the
specified
* number of surrounding points.
* @author Jason Byars <jbyars@iupui.edu>
* @version 0.008
*/
public class Pam_Bead_Stats2 extends PlugInFrame implements ActionListener {

    private static final long serialVersionUID = 3102557507830434785L;

    /** A convenient class to track all the stats generated from each bright point.
    * @author Jason Byars <jbyars@iupui.edu>
    */
    class PamResults {
        public int hotPixel3x3; //hottest pixel in the selected integrated intensity
region
        public int hotPixelRoi; //hottest pixel in the whole region
        public int multiple; //number of regions w/
        public int x;
        public int y;
        public int z;
        public double mean;
        public double stdev;
        public double background;
        public double backgroundStdev;
        public double totalIntensity;
        public int voxels;
        String stackName;
        String roiName;
    }
}

```



```

/** Appends the stats for this point to a given results table.
 * @param rt the results table to append the stats to
 */
void reportRT(ResultsTable rt) {
    rt.incrementCounter();
    rt.addLabel("Name",roiName);
    rt.addValue(0, hotPixel3x3); // hottest pixel 3x3
    rt.addValue(1, hotPixelRoi); // hottest pixel roi
    rt.addValue(2, multiple); // number of regions w/ same total
intensity
    rt.addValue(3, x); // x
    rt.addValue(4, y); // y
    rt.addValue(5, z); // z
    rt.addValue(6, totalIntensity); // total intensity
    rt.addValue(7, mean); // mean
    rt.addValue(8, stdev); // standard deviation of the mean
    rt.addValue(9, background); // mean of last 10 planes in the stack
    rt.addValue(10, backgroundStdev); // standard deviation of the
background mean
}

/** Appends the stats for this point to a given csv file.
 * @param bf the BufferedWriter for the desired csv file
 */
void reportCSV(BufferedWriter bf) {
    String s =
String.format("%s,%s,%d,%d,%d,%d,%d,%d,%f,%f,%f,%f,%f",
                stackName,
                roiName,
                hotPixel3x3,
                hotPixelRoi,
                multiple,
                x,y,z,
                mean,
                stdev,
                background,
                backgroundStdev,
                mean-background);
    try {
        bf.write(s);
        bf.newLine();
    } catch (IOException e) {
        System.err.println(e);
    }
}

```

```

        }

};

Panel panel;
static Frame instance;
GridBagConstraints gbc = new GridBagConstraints();
ImagePlus imp;
Roi    currentRoi;
PamResults result;
ResultsTable rt;
TextField txtPlanes;
TextField txtRadius;
int planes;
int radius;
int peakIntensity;
int voxels;
double persistentbkg;
double persistentbkgstdev;
BufferedWriter csvout;

//*****
*****

public Pam_Bead_Stats2() {
    super("Pam_Bead_Stats2 v0.008");
    if (IJ.versionLessThan("1.40")) {
        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    if (instance!=null) {
        instance.toFront();
        return;
    }

    instance = this;
    addKeyListener(IJ.getInstance());

    IJ.register(Pam_Bead_Stats2.class);
}

//*****
*****

public void actionPerformed(ActionEvent e) {
    imp = WindowManager.getCurrentImage();
    currentRoi = imp.getRoi();
}

```

```

if (imp==null) {
    IJ.beep();
    IJ.showStatus("No image");
    return;
}
if (currentRoi == null) {
    IJ.beep();
    IJ.showStatus("No ROI");
    return;
}
if (currentRoi.getType() == Roi.LINE) {
    IJ.beep();
    IJ.showStatus("Rectangles or Ovals only!");
    return;
}
String label = e.getActionCommand();
if (label==null) {
    IJ.showStatus("I have no idea what to do");
    return;
}
try {
    planes = Integer.parseInt(txtPlanes.getText());
    radius = Integer.parseInt(txtRadius.getText());
} catch (NumberFormatException n) {
    IJ.showMessage("Give me real numbers!");
    return;
}

if (!validateArgs()) return;

if (label == "Measure")
    measureit();
else if (label == "Measure All")
    measureAll();
else if (label == "Dump ROI")
    dumpROI();
else
    imp.killRoi();
}

```

```

//*****

```

```

*****

```

```

private void dumpROI() {
    int[] value = {0,0,0,0};
    int orig = imp.getSlice();

```

```

Rectangle bounds = currentRoi.getBounds();
ResultsTable tmp = new ResultsTable();
tmp.reset();

for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++)
    tmp.getFreeColumn("X"+x);

int zmin = imp.getSlice() - planes;
int zmax = imp.getSlice() + planes;
if (zmin < 1) zmin = 1;
if (zmax > imp.getNSlices()) zmax = imp.getNSlices();

for (int z = zmin; z <= zmax; z++) {
    imp.setSlice(z);
    for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
        tmp.incrementCounter();
        for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
            if (currentRoi.contains(x,y))
                value = imp.getPixel(x,y);
            else
                value[0] = 0;
            tmp.addValue((int) (x-bounds.getX()), value[0]);
        }
    }
}
tmp.show("ROI x"+(int) bounds.getX()+" y"+ (int) bounds.getY()+"
z"+imp.getSlice());
imp.setSlice(orig);
}

//*****
*****

private void findPeak() {
    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();
    double value = 0;
    int multi = 1;
    Rectangle bounds = currentRoi.getBounds();
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);

```

```

        for (int y = (int) bounds.getY(); y <= (int) bounds.getY() + (int)
bounds.getHeight(); y++) {
            for (int x = (int) bounds.getX(); x <= (int) bounds.getX() +
(int) bounds.getWidth(); x++) {
                if (!currentRoi.contains(x,y)) continue;
                value = integratedIntensity(x,y,z);
                if ( peakIntensity > result.hotPixelRoi )
result.hotPixelRoi = peakIntensity;
                if ( (int) value > result.totalIntensity ) {
                    result.totalIntensity = (int) value;
                    result.x = x;
                    result.y = y;
                    result.z = z;
                    result.voxels = voxels;
                    result.hotPixel3x3 = peakIntensity;
                    multi = 1;
                } else if ((int) value == result.totalIntensity) {
                    multi++;
                }
            }
        }
    }
    result.mean = result.totalIntensity/result.voxels;
    result.stdev = integratedStdev(result.x,result.y,result.z, result.mean);

    result.multiple = multi;
    return;
}

```

```

//*****
*****

```

```

private double integratedIntensity(int x, int y, int z) {
    double intensity = 0;
    voxels = 0;
    peakIntensity = 0;
    int[] value = {0,0,0,0};
    int xmin = x-radius;
    int xmax = x+radius;
    int ymin = y-radius;
    int ymax = y+radius;
    int zmin = z-radius;
    int zmax = z+radius;
    if ( xmin < 0 ) xmin = 0;
    if ( ymin < 0 ) ymin = 0;
    if ( zmin < 1 ) zmin = 1;
    if ( xmax > imp.getWidth()-1 ) xmax = imp.getWidth() - 1;

```

```

if ( ymax > imp.getHeight()-1 ) ymax = imp.getHeight() - 1;
if ( zmax > imp.getNSlices() ) zmax = imp.getNSlices();
for (z = zmin; z <= zmax; z++) {
    imp.setSlice(z);
    for (y = ymin; y <= ymax; y++) {
        for (x = xmin; x <= xmax; x++,voxels++) {
            value = imp.getPixel(x,y);
            intensity += value[0];
            if (value[0] > peakIntensity)
                peakIntensity = value[0];
        }
    }
}
return intensity;
}

//*****
*****

private double integratedStdev(int x, int y, int z, double mean) {
    double total = 0;
    double voxels = 0;
    int xmin = x-radius;
    int xmax = x+radius;
    int ymin = y-radius;
    int ymax = y+radius;
    int zmin = z-radius;
    int zmax = z+radius;
    if ( xmin < 0 ) xmin = 0;
    if ( ymin < 0 ) ymin = 0;
    if ( zmin < 1 ) zmin = 1;
    if ( xmax > imp.getWidth()-1 ) xmax = imp.getWidth() - 1;
    if ( ymax > imp.getHeight()-1 ) ymax = imp.getHeight() - 1;
    if ( zmax > imp.getNSlices() ) zmax = imp.getNSlices();
    for (z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (y = ymin; y <= ymax; y++) {
            for (x = xmin; x <= xmax; x++,voxels++) {
                int value = imp.getPixel(x,y)[0];
                total += Math.pow(value - mean, 2);
            }
        }
    }
    double stdev = Math.sqrt(total/(voxels-1));
    return stdev;
}

```

```

//*****
*****
private double last10Mean() {
    int orig = imp.getSlice();
    int first = imp.getNSlices()-9; //-9 does 10 slices
    first = (first < 1) ? 1 : first;
    long total = 0;
    for (int i=first; i<=imp.getNSlices(); i++) {
        imp.setSlice(i);
        for (int y=0; y<imp.getHeight(); y++) {
            for (int x=0; x<imp.getWidth(); x++) {
                total += imp.getPixel(x,y)[0];
            }
        }
    }
    imp.setSlice(orig);
    double mean = total / (10.0*imp.getWidth()*imp.getHeight());
    return mean;
}

//*****
*****
private double last10Stdev(double mean) {
    int orig = imp.getSlice();
    int first = imp.getNSlices()-9; //-9 does 10 slices
    first = (first < 1) ? 1 : first;
    double total = 0;
    for (int i=first; i<=imp.getNSlices(); i++) {
        imp.setSlice(i);
        for (int y=0; y<imp.getHeight(); y++) {
            for (int x=0; x<imp.getWidth(); x++) {
                total += Math.pow(imp.getPixel(x,y)[0] - mean, 2);
            }
        }
    }
    imp.setSlice(orig);
    double stdev =
Math.sqrt(total/(imp.getWidth()*imp.getHeight()*(imp.getNSlices()-first+1)-1));
    return stdev;
}

//*****
*****
private void measureAll() {
    RoiManager mgr = RoiManager.getInstance();
    if (mgr == null) {

```

```

        IJ.beep();
        IJ.showStatus("Roi Manager not open");
        return;
    }

    Roi[] rois = mgr.getRoisAsArray();
    persistentbkg = last10Mean();
    persistentbkgstdev = last10Stdev(persistentbkg);

    int orig = imp.getSlice();
    for (int i=0; i < rois.length; i++) {
        currentRoi = rois[i];
        imp.setSlice(mgr.getSliceNumber(currentRoi.getName()));
        if (mgr.getSliceNumber(currentRoi.getName()) < 1) {
            IJ.error("I don't know what the slice is for ROI
"+currentRoi.getName());
        }
        measureit();
    }
    imp.setSlice(orig);
    persistentbkg = -1;
    persistentbkgstdev = -1;
}

//*****
*****

private void measureit() {
    int orig = imp.getSlice();
    result = new PamResults();
    result.stackName = imp.getTitle();
    result.roiName = currentRoi.getName();

    findPeak();
    //int[] value = {0,0,0,0};
    //peakIntensity = 0;

    //ok do stats
    imp.setSlice(orig);
    //these ops are constant for the stack, don't do them every time!
    if (persistentbkg >= 0 ) {
        result.background = persistentbkg;
        result.backgroundStdev = persistentbkgstdev;
    } else {
        result.background = last10Mean();
        result.backgroundStdev = last10Stdev(result.background);
    }
}

```



```

        if ( rt == null ) { // macro version!
            result.reportCSV(csvout);
        } else {
            if (rt.getCounter()==0) makeResultTable(); //results table closed
            result.reportRT(rt);
            rt.show("Results Integrated peak");
        }
        String s = "Peak "+result.totalIntensity+" x: "+result.x+" y: "+result.y+" z:
"+result.z;
        IJ.showStatus(s);
        result = null;
    }

    /**
    ****

    private void makeResultTable() {
        rt = new ResultsTable();
        rt.reset();
        rt.getFreeColumn("Hottest Pixel 3x3");
        rt.getFreeColumn("Hottest Pixel ROI");
        rt.getFreeColumn("Multiple");
        rt.getFreeColumn("X");
        rt.getFreeColumn("Y");
        rt.getFreeColumn("Z");
        rt.getFreeColumn("Total Intensity");
        rt.getFreeColumn("Mean");
        rt.getFreeColumn("Stdev");
        rt.getFreeColumn("Background");
        rt.getFreeColumn("Background Stdev");
    }

    /**
    ****

    public void processWindowEvent(WindowEvent e) {
        super.processWindowEvent(e);
        if (e.getID()==WindowEvent.WINDOW_CLOSING) {
            instance = null;
        }
    }

    /**
    ****

    public void run(String arg) {
        String options = "";
        String csvname = "";

```

```

if (IJ.versionLessThan("1.40")) {
    IJ.showMessage("ImageJ 1.40 or greater required.");
    return;
}
persistentbkg = -1;
persistentbkgstdev = -1;

if (Macro.getOptions() == null) {
    makeResultTable();
    showDialog();
} else { //validation
    options = Macro.getOptions();
    imp = WindowManager.getCurrentImage();
    if (imp == null) return;
    try {
        planes = Integer.parseInt(Macro.getValue(options,
"planes", "10"));
        radius = Integer.parseInt(Macro.getValue(options, "radius",
"1"));
        csvname = Macro.getValue(options, "csv", imp.getTitle());

    } catch (NumberFormatException e) {
        IJ.error("At least one of the arguments is not parseable! " +
options);
    }
    if (!validateArgs()) return;
    try {
        if (!csvname.toLowerCase().endsWith("csv")) csvname +=
".csv";

        File csv = new File(csvname);
        csvout = new BufferedWriter(new FileWriter(csv));
        csvout.write("planes," + planes + ",radius," + radius);
        csvout.newLine();
        csvout.write("image name,region name,hottest pixel
3x3,hottest pixel roi,multiple,x,y,z,mean,mean stdev,background,background
stdev,mean-background");
        csvout.newLine();
        measureAll();
        csvout.close();
    } catch (IOException e) {
        System.err.println(e);
    }
}
}

```

```

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill) {
    set_gbc(row,column,width,height,fill,0,0);
}

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill, int padx, int
pady) {
    gbc.gridy = row;
    gbc.gridx = column;
    gbc.gridwidth = width;
    gbc.gridheight = height;
    gbc.fill = fill; // GridBagConstraints.NONE .HORIZONTAL
.VERTICAL .BOTH
    gbc.ipadx = padx;
    gbc.ipady = pady;
    // leave other fields (eg, anchor) unchanged.
}

//*****
*****
private boolean validateArgs() {
    if (planes < 1) {
        IJ.showMessage("Invalid number of planes. Try again hoser.");
        return false;
    }
    if (radius < 1) {
        IJ.showMessage("Invalid radius. Try again hoser.");
        return false;
    }

    return true;
}

//*****
*****
public void showDialog() {
    //because windows is stupid
    setLayout(new FlowLayout());
    panel = new Panel();
    GridBagLayout gridbag = new GridBagLayout();
    panel.setLayout(gridbag);
    String s = "Select a region around a bead.";

```

```

Label l = new Label(s);
set_gbc(0,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
s = "Specify how far above and below to look.";
l = new Label(s);
set_gbc(1,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
s = "Specify the radius to average.";
l = new Label(s);
set_gbc(2,0,4,1, GridBagConstraints.HORIZONTAL, 0, 10);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("Planes to check", Label.RIGHT);
set_gbc(3,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtPlanes = new TextField("10", 20);
set_gbc(3,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtPlanes,gbc);
panel.add(txtPlanes, gbc);
l = new Label("Radius", Label.RIGHT);
set_gbc(4,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtRadius = new TextField("1", 20);
set_gbc(4,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtRadius,gbc);
panel.add(txtRadius, gbc);
Button b = new Button("Measure");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(5,0,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Measure All");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(5,1,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Dump ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(5,2,1,1, GridBagConstraints.NONE);

```

```

        gridbag.setConstraints(b,gbc);
        panel.add(b);
        b = new Button("Clear ROI");
        b.addActionListener(this);
        b.addKeyListener(IJ.getInstance());
        set_gbc(5,3,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        add(panel);

        pack();
        GUI.center(this);
        setVisible(true);
    }

    /*******
    *****/
    void showAbout() {
        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This app takes a region, finds the brightest point
and averages it with pixels in a radius of x.");
    }

    /*******
    *****/
    void error() {
        IJ.showMessage("Pam_Bead_Stats2", "This plugin requires a defined
region to work");
    }

}

```

### 5. *Pam\_Bead\_Stats3.java*

```

import ij.*;
import ij.plugin.frame.*;
import ij.plugin.filter.*;
import ij.measure.*;
import ij.process.*;
import ij.gui.*;
import java.awt.*;
import java.awt.event.*;

/** Given a region of interest it, it finds the brightest subregion. It then takes the central
pixel, return a range along
* Z, finds the max of the range, and does the FWHM.

```

```

* @author Jason Byars <jbyars@iupui.edu>
* @version 0.004
*/
public class Pam_Bead_Stats3 extends PlugInFrame implements ActionListener {

    private static final long serialVersionUID = 421671022521828779L;
    Panel panel;
    static Frame instance;
    GridBagConstraints gbc = new GridBagConstraints();
    ImagePlus imp;
    Roi    currentRoi;
    ResultsTable rt;
    TextField txtPlanes;
    TextField txtGaussianRadius;
    TextField txtMaxRadius;
    TextField txtIntegratedIntensity;
    TextField txtRange;
    GaussianBlur blur;
    double gaussianRadius;
    int maxRadius;
    int planes;
    int radius;
    int range;
    int peakIntensity;
    int voxels;
    int[] zrange;
    static final int window = 21; //size of substack for filtering

    //*****
    *****
    public Pam_Bead_Stats3() {
        super("Pam_Bead_Stats3 v0.004");
        if (IJ.versionLessThan("1.40")) {
            IJ.showMessage("ImageJ 1.40 or greater required.");
            return;
        }

        if (instance!=null) {
            instance.toFront();
            return;
        }
        instance = this;
        addKeyListener(IJ.getInstance());
        //makeResultTable();
        showDialog();
    }
}

```

```

IJ.register(Pam_Bead_Stats3.class);
}

//*****
*****

public void actionPerformed(ActionEvent e) {
    imp = WindowManager.getCurrentImage();
    currentRoi = imp.getRoi();
    if (imp==null) {
        IJ.beep();
        IJ.showStatus("No image");
        return;
    }
    if (currentRoi == null) {
        IJ.beep();
        IJ.showStatus("No ROI");
        return;
    }
    if (currentRoi.getType() == Roi.LINE) {
        IJ.beep();
        IJ.showStatus("Rectangles or Ovals only!");
        return;
    }
    String label = e.getActionCommand();
    if (label==null) {
        IJ.showStatus("I have no idea what to do");
        return;
    }
    try {
        planes = Integer.parseInt(txtPlanes.getText());
        range = Integer.parseInt(txtRange.getText());
        radius = Integer.parseInt(txtIntegratedIntensity.getText());
        maxRadius = Integer.parseInt(txtMaxRadius.getText());
        gaussianRadius =
Double.parseDouble(txtGaussianRadius.getText());
    } catch (NumberFormatException n) {
        IJ.showMessage("Give me real numbers!");
        return;
    }
    if (planes < 1) {
        IJ.showMessage("Invalid number of planes. Try again hoser.");
        return;
    }
    if (radius < 1) {
        IJ.showMessage("Invalid radius. Try again hoser.");
        return;
    }
}

```

```

    }

    //We're actually going to do something
    if (label == "Measure") {
        makeResultTable();
        measureit();
    } else if (label == "Measure All") {
        makeResultTable();
        measureAll();
    } else if (label == "Dump ROI")
        dumpROI();
    else
        imp.killRoi();
}

//*****
*****

void displayFWHM(int[] peak, int[] subpeak, double[] fwhm, double[] gfwhm,
ImagePlus tmp, ImagePlus gtmp, int zmin, int zmax, int zpad) {
    double [] x = new double[tmp.getNSlices()];
    double [] y = new double[tmp.getNSlices()];
    double [] result = new double[tmp.getNSlices()];

    for (int z=1; z<=tmp.getNSlices(); z++) {
        x[z-1] = z+zmin-1;
        tmp.setSlice(z);
        y[z-1] = tmp.getPixel(subpeak[0],subpeak[1])[0];
    }
    if (gaussianRadius > 0) {
        for (int z=1; z<=gtmp.getNSlices(); z++) {
            gtmp.setSlice(z);
            result[z-1] = gtmp.getPixel(subpeak[0],subpeak[1])[0];
        }
    }
    Plot p = new Plot("FWHM for "+currentRoi.getName(),"Z
plane","Intensity", (double[]) null,(double[]) null);
    p.setLimits(zmin, zmax, 0, fwhm[4]+100);
    p.setColor(Color.blue);
    p.addPoints(x,y,PlotWindow.CIRCLE);
    p.setColor(Color.red);

    if (gaussianRadius > 0) {
        p.setColor(Color.green);
        p.addPoints(x,result, PlotWindow.X);
        // add a fwhm curve
        double[] x2 = {gfwhm[1]+zpad,gfwhm[2]+zpad};

```



```

        double[] y2 = { gfwhm[4]/2.0, gfwhm[4]/2.0};
        double[] x3 = { gfwhm[3]+zpad, gfwhm[3]+zpad};
        double[] y3 = { gfwhm[4]/2.0, gfwhm[4]};
        p.setColor(Color.red);
        p.addPoints(x2,y2,PlotWindow.X);
        p.addPoints(x2,y2,PlotWindow.LINE);
        p.addPoints(x3,y3,PlotWindow.LINE);
    } else {
        double[] x2 = { gfwhm[1]+zpad,gfwhm[2]+zpad};
        double[] y2 = { gfwhm[4]/2.0, gfwhm[4]/2.0};
        double[] x3 = { gfwhm[3]+zpad, gfwhm[3]+zpad};
        double[] y3 = { gfwhm[4]/2.0, gfwhm[4]};
        p.setColor(Color.red);
        p.addPoints(x2,y2,PlotWindow.X);
        p.addPoints(x2,y2,PlotWindow.LINE);
        p.addPoints(x3,y3,PlotWindow.LINE);
    }

    // add label
    p.setColor(Color.black);
    //p.changeFont(new Font("Helvetica", Font.PLAIN, 24));
    p.addLabel(0.02, 0.1, String.format("Center:
%d,%d,%d",peak[0],peak[1],peak[2]));
    p.addLabel(0.02, 0.2, "Max pixel: "+fwhm[4]);
    if (fwhm[0] > 0)
        p.addLabel(0.02, 0.3, String.format("FWHM: %.2f",fwhm[0]));

    else
        p.addLabel(0.02, 0.3, String.format("FWHM: failed",fwhm[0]));

    if (gaussianRadius > 0) {
        p.addLabel(0.02, 0.4, "Gauss Max pixel: "+gfwhm[4]);
        if (gfwhm[0] > 0)
            p.addLabel(0.02, 0.5, String.format("Gauss FWHM:
%.2f",gfwhm[0]));
        else
            p.addLabel(0.02, 0.5, String.format("Gauss FWHM:
failed",gfwhm[0]));
    }

    //p.changeFont(new Font("Helvetica", Font.PLAIN, 16));
    p.setColor(Color.lightGray);
    p.show();
}

```

```

//*****
*****
private void dumpROI() {
    int[] value = {0,0,0,0};
    int orig = imp.getSlice();
    Rectangle bounds = currentRoi.getBounds();
    ResultsTable tmp = new ResultsTable();
    tmp.reset();

    for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++)
        tmp.getFreeColumn("X"+x);

    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();

    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
            tmp.incrementCounter();
            for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
                if (currentRoi.contains(x,y))
                    value = imp.getPixel(x,y);
                else
                    value[0] = 0;
                tmp.addValue((int) (x-bounds.getX()), value[0]);
            }
        }
    }
    tmp.show("ROI x"+(int) bounds.getX()+" y"+ (int) bounds.getY()+"
z"+imp.getSlice());
    imp.setSlice(orig);
}

//*****
*****
private double[] findFWHM(int[] peak, ImagePlus tmp) {
    double [] fwhm = {-1, 0,0,0,0};
    final int x = peak[0];
    final int y = peak[1];
    int z = peak[2];
    //int zmin = peak[2]-range;

```

```

//if ( zmin < 1 ) zmin = 1;
//int zmax = peak[2]+range;
//if ( zmax > tmp.getNSlices() ) zmax = tmp.getNSlices();

//find peak pixel, start w/ center and work out
tmp.setSlice(z);
double limit = tmp.getPixel(x,y)[0];
for(int zed = peak[2]-maxRadius; zed<= peak[2]+maxRadius; zed++) {
    tmp.setSlice(zed);
    int value = tmp.getPixel(x,y)[0];
    if (value > limit) {
        z = zed;
        limit = value;
    }
}

IJ.write(String.format("value %f z %d", limit, z));
fwhm[3] = z;
fwhm[4] = limit;
limit/=2.0;

int i=0;
double x1=0, x2=0, left=0, right=0, slope=0, offset=0;
for (i=z; i>=1; i--) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x1 = tmp.getPixel(x,y)[0];
        tmp.setSlice(i+1);
        x2 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
        left = i + (offset/slope);
        break;
    }
}
if (i<1) return fwhm; //out of bounds
for (i=z; i<=tmp.getNSlices(); i++) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x2 = tmp.getPixel(x,y)[0];
        tmp.setSlice(i-1);
        x1 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
    }
}

```

```

        right = i-1 + (offset/slope);
        break;
    }
}
if (i>tmp.getNSlices()) return fwhm; //out of bounds
fwhm[0] = right - left;
fwhm[1] = left;
fwhm[2] = right;
return fwhm;
}

//*****
*****

private int[] findPeak() {
    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();
    int[] peak = {0,0,0,0};
    int value = 0;

    Rectangle bounds = currentRoi.getBounds();
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) bounds.getY() + (int)
bounds.getHeight(); y++) {
            for (int x = (int) bounds.getX(); x <= (int) bounds.getX() +
(int) bounds.getWidth(); x++) {
                if (!currentRoi.contains(x,y)) continue;
                value = (int) integratedIntensity(x,y,z);
                if ( value > peak[3] ) {
                    peak[0] = x;
                    peak[1] = y;
                    peak[2] = z;
                    peak[3] = value;
                }
            }
        }
    }

    return peak;
}

//*****
*****

private void GaussIt(ImagePlus tmp, double rad) {

```

```

        ImageProcessor ip = tmp.getProcessor();
        if (blur == null)
            blur = new GaussianBlur();
        for (int i=1; i<tmp.getNSlices(); i++) {
            tmp.setSlice(i);
            blur.blur(ip,rad);
        }
        tmp.updateImage();
    }

//*****
*****

private double integratedIntensity(int x, int y, int z) {
    double intensity = 0;
    voxels = 0;
    int[] value = {0,0,0,0};
    int xmin = x-radius;
    int xmax = x+radius;
    int ymin = y-radius;
    int ymax = y+radius;
    int zmin = z-radius;
    int zmax = z+radius;
    if ( xmin < 0 ) xmin = 0;
    if ( ymin < 0 ) ymin = 0;
    if ( zmin < 1 ) zmin = 1;
    if ( xmax > imp.getWidth()-1 ) xmax = imp.getWidth() - 1;
    if ( ymax > imp.getHeight()-1 ) ymax = imp.getHeight() - 1;
    if ( zmax > imp.getNSlices() ) zmax = imp.getNSlices();
    for (z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (y = ymin; y <= ymax; y++) {
            for (x = xmin; x <= xmax; x++,voxels++) {
                value = imp.getPixel(x,y);
                intensity += value[0];
            }
        }
    }
    return intensity;
}

//*****
*****

//odd dimensions only, no funny business
private ImagePlus makeSubStack(String name, int x, int y, int zmin, int zmax, int
length, int width )
{

```

```

    final int xmin = x-(length/2);
    //final int xmax = x+(length/2);
    final int ymin = y-(width/2);
    //final int ymax = y+(width/2);
    /*
    int zmin = z-(depth/2);
    int zmax = z+(depth/2);
    if (zmin < 1) {
        depth-= ( 1-zmin);
        zmin = 1;
    }
    if (zmax > imp.getNSlices()) {
        depth-=(zmax-imp.getNSlices());
        zmax = imp.getNSlices();
    }
    */

    ImagePlus tmp = NewImage.createShortImage(name, length, width, zmax-
zmin+1, NewImage.FILL_BLACK);
    ImageProcessor ip = tmp.getProcessor();
    int[] data = new int[length*4];
    for (int i=zmin,w=1; i<=zmax; i++,w++) {
        imp.setSlice(i);
        tmp.setSlice(w);
        for (int j=0; j<width; j++) {
            imp.getProcessor().getRow(xmin, j + ymin, data, length);
            ip.putRow(0,j, data,length);
        }
    }
    tmp.updateImage();
    return tmp;
}

//*****
*****

private void measureAll() {
    RoiManager mgr = RoiManager.getInstance();
    if (mgr == null) {
        IJ.beep();
        IJ.showStatus("Roi Manager not open");
        return;
    }

    Roi[] rois = mgr.getRoisAsArray();

    int orig = imp.getSlice();

```

```

        for (int i=0; i < rois.length; i++) {
            currentRoi = rois[i];
            imp.setSlice(mgr.getSliceNumber(currentRoi.getName()));
            if (mgr.getSliceNumber(currentRoi.getName()) < 1) {
                IJ.error("I don't know what the slice is for ROI
"+currentRoi.getName());
            }
            measureit();
        }
        imp.setSlice(orig);
    }

    /*******
    *****/
    private void measureit() {
        final int orig = imp.getSlice();

        Duplicater d = new Duplicater();
        ImagePlus tmp, gtmp;

        try {
            int[] peak = findPeak();
            int[] subpeak = { 10,10,range+1 };
            int zmin=peak[2]-range;
            if (zmin<1) zmin = 1;
            int zmax=peak[2]+range;
            if (zmax>imp.getNSlices()) zmax = imp.getNSlices();

            int zpad=0;
            //if we are too close the front of the stack, we don't pad.
            if (peak[2]-range<1) {
                subpeak[2] = peak[2];
            } else {
                zpad = peak[2] - range - 1;
            }

            //ok we know 3x3 and center pixel
            tmp = makeSubStack("Before",peak[0],peak[1], zmin, zmax,
window>window);

            gtmp = d.duplicateStack(tmp, "After");
            GaussIt(gtmp, gaussianRadius);
            double[] fwhm = findFWHM(subpeak, tmp);
            double[] gfw hm = findFWHM(subpeak, gtmp);
            //ok do stats

```

```

        ImageStack c = new ImageStack(window*2,window,
tmp.getImageStack().getColorModel());
        ImageProcessor ip = tmp.getProcessor();
        ImageProcessor ip2;

        for (int zed=1; zed<=tmp.getNSlices(); zed++) {
            ip2 = ip.createProcessor(window*2,window);
            ip2.setValue(0);
            ip2.fill();
            ip2.insert(tmp.getStack().getProcessor(zed),0,0);
            ip2.insert(gttmp.getStack().getProcessor(zed),window,0);
            c.addSlice(null,ip2);
        }

        ImagePlus combined = new ImagePlus("Before/After Gauss " +
currentRoi.getName(), c);
        combined.setSlice(subpeak[2]);
        combined.resetDisplayRange();
        combined.show();

        if (rt.getCounter()==0) makeResultTable(); //results table closed
        rt.incrementCounter();
        rt.addLabel("Name",currentRoi.getName());
        rt.addValue(0,peak[0]); //center x
        rt.addValue(1,peak[1]); //center y
        rt.addValue(2,peak[2]); //center z
        rt.addValue(3,gfwhm[3]+zpad); //max z
        rt.addValue(4,gfwhm[4]); //max pixel value
        rt.addValue(5,fwhm[0]); //fwhm
        rt.addValue(6,fwhm[1]+zpad); //left position
        rt.addValue(7,fwhm[2]+zpad); //right position
        rt.addValue(8,gfwhm[0]); //gaussed fwhm
        rt.addValue(9,gfwhm[1]+zpad); //left position
        rt.addValue(10,gfwhm[2]+zpad); //right position
        //for (int z=peak[4]-range,i=6; z<=peak[4]+range; z++,i++) {
        //    imp.setSlice(z);
        //    rt.addValue(i,imp.getPixel(peak[0],peak[1])[0]);
        //}
        rt.show("Results Integrated FWHM");
        String s = "Peak "+peak[0]+" x: "+peak[1]+" y: "+peak[2]+" z:
"+peak[3];

        IJ.showStatus(s);
        displayFWHM(peak, subpeak, fwhm, gfwhm, tmp, gttmp, zmin,
zmax, zpad);

        tmp.flush();
        gttmp.flush();

```



```

        } catch (Exception e) {

        }
        imp.setSlice(orig);
    }

    /**
     *
     */
    private void makeResultTable() {
        rt = new ResultsTable();
        rt.reset();
        rt.getFreeColumn("Cen X");
        rt.getFreeColumn("Y");
        rt.getFreeColumn("Z");
        rt.getFreeColumn("Gauss Max Z");
        rt.getFreeColumn("Gauss Max pixel");
        rt.getFreeColumn("FWHM");
        rt.getFreeColumn("Left");
        rt.getFreeColumn("Right");
        rt.getFreeColumn("G FWHM");
        rt.getFreeColumn("G Left");
        rt.getFreeColumn("G Right");
        //fields for array of data points
    }

    /**
     *
     */
    public void processWindowEvent(WindowEvent e) {
        super.processWindowEvent(e);
        if (e.getID()==WindowEvent.WINDOW_CLOSING) {
            instance = null;
        }
    }

    /**
     *
     */
    private void set_gbc(int row, int column, int width, int height, int fill) {
        set_gbc(row,column,width,height,fill,0,0);
    }

    /**
     *
     */
    private void set_gbc(int row, int column, int width, int height, int fill, int padx, int
pady) {
        gbc.gridy = row;
        gbc.gridx = column;

```

```

        gbc.gridwidth = width;
        gbc.gridheight = height;
        gbc.fill = fill; // GridBagConstraints.NONE .HORIZONTAL
.VERTICAL .BOTH
        gbc.ipadx = padx;
        gbc.ipady = pady;
        // leave other fields (eg, anchor) unchanged.
    }

    //*****
*****

public void showDialog() {
    //because windows is stupid
    setLayout(new FlowLayout());
    panel = new Panel();
    GridBagLayout gridbag = new GridBagLayout();
    panel.setLayout(gridbag);
    String s = "Select a region around a bead.";
    Label l = new Label(s);
    set_gbc(0,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
    gridbag.setConstraints(l,gbc);
    panel.add(l, gbc);
    s = "Specify how far above and below to look.";
    l = new Label(s);
    set_gbc(1,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
    gridbag.setConstraints(l,gbc);
    panel.add(l, gbc);
    s = "Specify the radius to average.";
    l = new Label(s);
    set_gbc(2,0,4,1, GridBagConstraints.HORIZONTAL, 0, 10);
    gridbag.setConstraints(l,gbc);
    panel.add(l, gbc);
    l = new Label("Planes to check", Label.RIGHT);
    set_gbc(3,0,2,1, GridBagConstraints.HORIZONTAL);
    gridbag.setConstraints(l,gbc);
    panel.add(l, gbc);
    txtPlanes = new TextField("20", 20);
    set_gbc(3,2,2,1, GridBagConstraints.NONE);
    gridbag.setConstraints(txtPlanes,gbc);
    panel.add(txtPlanes, gbc);
    l = new Label("Range to Return", Label.RIGHT);
    set_gbc(4,0,2,1, GridBagConstraints.HORIZONTAL);
    gridbag.setConstraints(l,gbc);
    panel.add(l, gbc);
    txtRange = new TextField("50", 20);
    set_gbc(4,2,2,1, GridBagConstraints.NONE);
}

```

```

gridbag.setConstraints(txtRange,gbc);
panel.add(txtRange, gbc);
l = new Label("Integrated Intensity NxN", Label.RIGHT);
set_gbc(5,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtIntegratedIntensity = new TextField("3", 20);
set_gbc(5,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtIntegratedIntensity,gbc);
panel.add(txtIntegratedIntensity, gbc);
l = new Label("Max Radius", Label.RIGHT);
set_gbc(6,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtMaxRadius = new TextField("2", 20);
set_gbc(6,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtMaxRadius,gbc);
panel.add(txtMaxRadius, gbc);
l = new Label("Gaussian Radius", Label.RIGHT);
set_gbc(7,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtGaussianRadius = new TextField("1.0", 20);
set_gbc(7,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtGaussianRadius,gbc);
panel.add(txtGaussianRadius, gbc);
Button b = new Button("Measure");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(8,0,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Measure All");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(8,1,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Dump ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(8,2,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Clear ROI");
b.addActionListener(this);

```

```

        b.addKeyListener(IJ.getInstance());
        set_gbc(8,3,1,1, GridBagConstraints.NONE);
        gridbag.setConstraints(b,gbc);
        panel.add(b);
        add(panel);

        pack();
        GUI.center(this);
        setVisible(true);
    }

    /*******
    void showAbout() {
        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This app takes a region, finds the brightest point
and averages it with pixels in a radius of x.");
    }

    /*******
    void error() {
        IJ.showMessage("Pam_Bead_Stats3", "This plugin requires a defined region to
work");
    }
}

```

#### 6. *Pam\_Bead\_StatsMedian.java*

```

import ij.*;
import ij.plugin.frame.*;
import ij.plugin.filter.*;
import ij.measure.*;
import ij.process.*;
import ij.gui.*;
import java.awt.*;
import java.awt.event.*;
import java.awt.datatransfer.*;
import java.io.*;
import java.util.Arrays;

```

/\*\* Given a region of interest it, it finds the brightest subregion. It then takes the central pixel, return a range along

```

* Z, finds the max of the range, and does the FWHM. Decided the median filtered
smoothing was not a good enough fit. There were
* concerns it was underestimating.
* @author Jason Byars <jbyars@iupui.edu>
* @version 0.008
*/
public class Pam_Bead_StatsMedian extends PlugInFrame implements ActionListener,
ClipboardOwner {

```

```

    private static final long serialVersionUID = -4437255474438582193L;

```

```

/** Convenience class to track subregion location and peak intensity.
*/

```

```

class Vektor {
    public int x;
    public int y;
    public int z;
    public int peak;

    public Vektor() {
        x = y = z = peak = 0;
    }

    public String toString() {
        String s = "Peak "+peak+" x: "+x+" y: "+y+" z: "+z;
        return s;
    }
};

```

```

/** Convenience class to track subregion stats.
*/

```

```

class PamMedianResults {
    public double fwhm;
    public double dlh;
    public double left;
    public double right;
    public double peak;
    public int peakz;
    public double l1;
    public double l2;
    public double r1;
    public double r2;

    public PamMedianResults() {
        fwhm = -1;
        left = 0;

```

```

        right = 0;
        dlh = 0;
        peak = 0;
        peakz = 0;
        l1 = l2 = r1 = r2 = 0;
    }
};

```

```

Panel panel;
static Frame instance;
GridBagConstraints gbc = new GridBagConstraints();
ImagePlus imp;
ImagePlus origImg;
ImagePlus filteredImg;
PamMedianResults origResults;
PamMedianResults filteredResults;
Roi    currentRoi;
ResultsTable rt;
boolean median3d;
Checkbox chkMedian3d;
TextField txtPlanes;
TextField txtMedianRadius;
TextField txtIntegratedIntensity;
TextField txtRange;
TextField txtFlattop;
GaussianBlur blur;
double backgroundsubtract;
double medianRadius;
int planes;
int integratedRadius;
int range;
int peakIntensity;
int voxels;
int[] zrange;
double [] index;
double []    zValues;
double [] medianResults;
static final int window = 21; //size of substack for filtering
int flattop; //if 3 or more pixels are at max value, it is a flattop problem
BufferedWriter csvout;

```

```

//*****
*****
public Pam_Bead_StatsMedian() {
    super("Pam_Bead_StatsMedian v0.008");
    if (IJ.versionLessThan("1.40")) {

```

```

        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    if (instance!=null) {
        instance.toFront();
        return;
    }
    instance = this;
    addKeyListener(IJ.getInstance());

    IJ.register(Pam_Bead_StatsMedian.class);
}

//*****
*****

public void actionPerformed(ActionEvent e) {
    imp = WindowManager.getCurrentImage();
    currentRoi = imp.getRoi();
    if (imp==null) {
        IJ.beep();
        IJ.showStatus("No image");
        return;
    }
    if (currentRoi == null) {
        IJ.beep();
        IJ.showStatus("No ROI");
        return;
    }
    if (currentRoi.getType() == Roi.LINE) {
        IJ.beep();
        IJ.showStatus("Rectangles or Ovals only!");
        return;
    }
    String label = e.getActionCommand();
    if (label==null) {
        IJ.showStatus("I have no idea what to do");
        return;
    }
    try {
        planes = Integer.parseInt(txtPlanes.getText());
        range = Integer.parseInt(txtRange.getText());
        integratedRadius =
Integer.parseInt(txtIntegratedIntensity.getText());
        medianRadius = Double.parseDouble(txtMedianRadius.getText());
        flattop = Integer.parseInt(txtFlattop.getText());

```

```

        median3d = chkMedian3d.getState();
    } catch (NumberFormatException n) {
        IJ.showMessage("Give me real numbers!");
        return;
    }

    if (!validateArgs()) return;

    //We're actually going to do something
    if (label == "Measure") {
        makeResultTable();
        measureit();
    } else if (label == "Measure All") {
        makeResultTable();
        measureAll();
    } else if (label == "Dump ROI") {
        dumpROI();
    } else if (label == "Copy Values") {
        copyValues();
    } else if (label == "Copy Median") {
        copyMedian();
    } else if (label == "Check Outlier") {
        checkOutlier();
    } else
        imp.killRoi();
}

//*****
*****
void checkOutlier() {
    final int orig = imp.getSlice();
    ImagePlus tmp;

    Vektor peak = findPeak();
    Vektor subpeak = new Vektor();
    subpeak.x = window/2;
    subpeak.y = window/2;
    subpeak.z = range+1;
    int zmin=peak.z-range;
    if (zmin<1) zmin = 1;
    int zmax=peak.z+range;
    if (zmax>imp.getNSlices()) zmax = imp.getNSlices();

    //int zpad=0;
    //if we are too close the front of the stack, we don't pad.
    if (peak.z-range<1) {

```



```

        subpeak.z = peak.z;
    } else {
        //zpad = peak.z - range -1;
    }

    //ok we know 3x3 and center pixel
    tmp = makeSubStack("Before",peak.x,peak.y, zmin, zmax,
window>window);
    //PamMedianResults fwhm = findFWHM(subpeak, tmp);

    int cubed = (int)Math.pow(2*integratedRadius+1,3);
    double[][] index = new double[tmp.getNSlices()];
    double[] centerValues = new double[tmp.getNSlices()];
    double[] meanValues = new double[tmp.getNSlices()];
    double[][] zValues = new double[tmp.getNSlices()];

    int maxpixel = 0;
    double intensity = 0;
    int value = 0;
    int xminr = peak.x-integratedRadius;
    int xmaxr = peak.x+integratedRadius;
    int yminr = peak.y-integratedRadius;
    int ymaxr = peak.y+integratedRadius;
    if ( xminr < 0 ) xminr = 0;
    if ( yminr < 0 ) yminr = 0;
    if ( xmaxr > imp.getWidth()-1 ) xmaxr = imp.getWidth() - 1;
    if ( ymaxr > imp.getHeight()-1 ) ymaxr = imp.getHeight() - 1;
    for (int j=zmin; j<=zmax; j++) {
        intensity = 0;
        int zminr = j-integratedRadius;
        int zmaxr = j+integratedRadius;
        if ( zminr < 1 ) zminr = 1;
        if ( zmaxr > imp.getNSlices() ) zmaxr = imp.getNSlices();
        index[j-zmin] = new double[cubed];
        zValues[j-zmin] = new double[cubed];

        for (int z = zminr, n=0; z <= zmaxr; z++) {
            imp.setSlice(z);
            for (int y = yminr; y <= ymaxr; y++) {
                for (int x = xminr; x <= xmaxr; x++, n++) {
                    value = imp.getPixel(x,y)[0];
                    index[j-zmin][n] = j;
                    zValues[j-zmin][n] = value;
                    intensity+=value;
                    if (value > maxpixel) maxpixel = value;
                }
            }
        }
    }

```

```

        }
    }
    intensity = intensity / cubed;
    imp.setSlice(j);
    centerValues[j-zmin]= imp.getPixel(peak.x, peak.y)[0];
    meanValues[j-zmin] = intensity;
}

double[] zindex = new double[tmp.getNSlices()];
for (int i=zmin; i<=zmax; i++) zindex[i-zmin] = i;
Plot p = new Plot("Check Outliers for "+currentRoi.getName(),"Z
plane","Intensity", (double[]) null,(double[]) null);
p.setLimits(zmin, zmax, 0, maxpixel+100); //100
p.setColor(Color.blue);
for (int j=0; j<tmp.getNSlices(); j++) {
    p.addPoints(index[j],zValues[j],Plot.DOT);
}
p.addLabel(0.02, 0.2, "Integrated Values");
p.setColor(Color.orange);
p.addPoints(zindex, meanValues, PlotWindow.LINE);
p.addLabel(0.02, 0.3, "NxN Mean");
p.setColor(Color.green);
p.addPoints(zindex, centerValues, PlotWindow.X);
p.addLabel(0.02, 0.4, "Center Value");
p.setColor(Color.black);
p.addLabel(0.02, 0.1, String.format("Center:
%d,%d,%d",peak.x,peak.y,peak.z));
p.show();
imp.setSlice(orig);
}

//*****
*****

void copyValues() {
    Clipboard systemClipboard = null;
    try {systemClipboard = getToolkit().getSystemClipboard();}
    catch (Exception e) {systemClipboard = null; }
    if (systemClipboard==null)
    {IJ.error("Unable to copy to Clipboard."); return;}
    IJ.showStatus("Copying z values...");
    CharArrayWriter aw = new CharArrayWriter(index.length*4);
    PrintWriter pw = new PrintWriter(aw);
    for (int i=0; i<index.length; i++) {
        pw.print(IJ.d2s(index[i],0)+"\t"+IJ.d2s(zValues[i],0)+"\n");
    }
    String text = aw.toString();
}

```

```

        pw.close();
        StringSelection contents = new StringSelection(text);
        systemClipboard.setContents(contents, this);
        IJ.showStatus(text.length() + " characters copied to Clipboard");
    }

    /*******
    void copyMedian() {
        Clipboard systemClipboard = null;
        try {systemClipboard = getToolkit().getSystemClipboard();}
        catch (Exception e) {systemClipboard = null; }
        if (systemClipboard==null)
        {IJ.error("Unable to copy to Clipboard."); return;}
        IJ.showStatus("Copying median values...");
        CharArrayWriter aw = new CharArrayWriter(index.length*4);
        PrintWriter pw = new PrintWriter(aw);
        for (int i=0; i<index.length; i++) {
            pw.print(IJ.d2s(index[i],0)+"\t"+IJ.d2s(medianResults[i],0)+"\n");
        }
        String text = aw.toString();
        pw.close();
        StringSelection contents = new StringSelection(text);
        systemClipboard.setContents(contents, this);
        IJ.showStatus(text.length() + " characters copied to Clipboard");
    }

    /*******
    void displayFWHM(Vektor peak, Vektor subpeak, int zmin, int zmax, int zpad) {
        index = new double[origImg.getNSlices()];
        zValues = new double[origImg.getNSlices()];
        medianResults = new double[origImg.getNSlices()];

        for (int z=1; z<=origImg.getNSlices(); z++) {
            index[z-1] = z+zmin-1;
            origImg.setSlice(z);
            zValues[z-1] = origImg.getPixel(subpeak.x,subpeak.y)[0];
        }
        if (medianRadius > 0) {
            for (int z=1; z<=filteredImg.getNSlices(); z++) {
                filteredImg.setSlice(z);
                medianResults[z-1] =
filteredImg.getPixel(subpeak.x,subpeak.y)[0];
            }
        }
    }

```

```

        Plot p = new Plot("FWHM for "+currentRoi.getName(),"Z
plane","Intensity", (double[]) null,(double[]) null);
        p.setLimits(zmin, zmax, 0, origResults.peak+100); //100
        p.setColor(Color.blue);
        p.addPoints(index,zValues,PlotWindow.CIRCLE);

        // add label
        //compute double half max
        p.setColor(Color.black);
        p.addLabel(0.02, 0.1, String.format("Center:
%d,%d,%d",peak.x,peak.y,peak.z));
        p.addLabel(0.02, 0.2, String.format("Max pixel: %d z:
%d",(int)origResults.peak,(int)origResults.peakz));
        if (origResults.fwhm > 0) {
            p.addLabel(0.02, 0.3, String.format("FWHM:
%.2f",origResults.fwhm));
            p.addLabel(0.02, 0.4, String.format("DLH:
%.2f",origResults.dlh));
        } else
            p.addLabel(0.02, 0.3, String.format("FWHM:
failed",origResults.fwhm));
        if (medianRadius > 0) {
            p.addLabel(0.02, 0.5, String.format("Median Max pixel: %d z:
%d",(int)filteredResults.peak,(int)filteredResults.peakz));
            if (filteredResults.fwhm > 0) {
                p.addLabel(0.02, 0.6, String.format("Median FWHM:
%.2f",filteredResults.fwhm));
                p.addLabel(0.02, 0.7, String.format("DLH:
%.2f",filteredResults.dlh));
            } else
                p.addLabel(0.02, 0.6, String.format("Median FWHM:
failed",filteredResults.fwhm));
        }

        //debug show mean
        p.setColor(Color.orange);
        double[] meanValues = new double[origImg.getNSlices()];
        double size = Math.pow(2*integratedRadius+1, 3);

        for (int z=zmin,i=0; z<=zmax; z++,i++) {
            meanValues[i] = integratedIntensity(peak.x,peak.y,z)/size;
            //IJ.write(String.format("integrated intensity %f", meanValues[i]));
        }
        p.addPoints(index,meanValues,PlotWindow.LINE);

        if (medianRadius > 0) {

```

```

//fwhm cross
p.setColor(new Color(150,150,255));
double[] x2 = {origResults.left+zpad,origResults.right+zpad};
double[] y2 = {origResults.peak/2.0, origResults.peak/2.0};
double[] x3 = {origResults.peakz+zpad, origResults.peakz+zpad};
double[] y3 = {origResults.peak/2.0, origResults.peak};
p.addPoints(x2,y2,PlotWindow.X);
p.addPoints(x2,y2,PlotWindow.LINE);
p.addPoints(x3,y3,PlotWindow.LINE);

p.setColor(Color.green);
p.addPoints(index,medianResults, PlotWindow.X);
// add a fwhm curve
x2[0] = filteredResults.left+zpad;
x2[1] = filteredResults.right+zpad;
y2[0] = filteredResults.peak/2.0;
y2[1] = filteredResults.peak/2.0;
x3[0] = filteredResults.peakz+zpad;
x3[1] = filteredResults.peakz+zpad;
y3[0] = filteredResults.peak/2.0;
y3[1] = filteredResults.peak;
p.setColor(Color.red);
p.addPoints(x2,y2,PlotWindow.X);
p.addPoints(x2,y2,PlotWindow.LINE);
p.addPoints(x3,y3,PlotWindow.LINE);
} else {
double[] x2 =
{filteredResults.left+zpad,filteredResults.right+zpad};
double[] y2 = {filteredResults.peak/2.0, filteredResults.peak/2.0};
double[] x3 = {filteredResults.peakz+zpad,
filteredResults.peakz+zpad};
double[] y3 = {filteredResults.peak/2.0, filteredResults.peak};
p.setColor(Color.red);
p.addPoints(x2,y2,PlotWindow.X);
p.addPoints(x2,y2,PlotWindow.LINE);
p.addPoints(x3,y3,PlotWindow.LINE);
}

//p.changeFont(new Font("Helvetica", Font.PLAIN, 16));
p.setColor(Color.lightGray);
p.show();
}

//*****
*****

```

```

private void dumpROI() {
    int[] value = {0,0,0,0};
    int orig = imp.getSlice();
    Rectangle bounds = currentRoi.getBounds();
    ResultsTable tmp = new ResultsTable();
    tmp.reset();

    for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++)
        tmp.getFreeColumn("X"+x);

    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();

    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
            tmp.incrementCounter();
            for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
                if (currentRoi.contains(x,y))
                    value = imp.getPixel(x,y);
                else
                    value[0] = 0;
                tmp.addValue((int) (x-bounds.getX()), value[0]);
            }
        }
        tmp.show("ROI x"+(int) bounds.getX()+" y"+ (int) bounds.getY()+"
z"+imp.getSlice());
        imp.setSlice(orig);
    }

    //*****
    *****
    /* fwhm[0] = full width half max
    fwhm[1] = left limit
    fwhm[2] = right limit
    fwhm[3] = peak pixel z
    fwhm[4] = peak pixel
    fwhm[5] = dlh
    */
    private PamMedianResults findFWHM(Vektor peak, ImagePlus tmp) {

```

```

//double [] fwhm = {-1, 0,0,0,0,0};
PamMedianResults result = new PamMedianResults();
final int x = peak.x;
final int y = peak.y;
int z = 0;

//find peak pixel where ever it may be
//tmp.setSlice(z);
double limit = 0;
for(int zed = 1; zed<= tmp.getNSlices(); zed++) {
    tmp.setSlice(zed);
    int value = tmp.getPixel(x,y)[0];
    if (value > limit) {
        z = zed;
        limit = value;
    }
}

IJ.write(String.format("value %f z %d", limit, z));
result.peakz = z;
result.peak = limit;
limit/=2.0;

int i=0;
double x1=0, x2=0, left=0, right=0, slope=0, offset=0;
for (i=z; i>=1; i--) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x1 = tmp.getPixel(x,y)[0];
        tmp.setSlice(i+1);
        x2 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
        left = i + (offset/slope);
        result.l1 = i;
        result.l2 = i+1;
        break;
    }
}
if (i<1) return result; //out of bounds
for (i=z; i<=tmp.getNSlices(); i++) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x2 = tmp.getPixel(x,y)[0];

```

```

        tmp.setSlice(i-1);
        x1 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
        right = i-1 + (offset/slope);
        result.r1 = i-1;
        result.r2 = i;
        break;
    }
}
if (i>tmp.getNSlices()) return result; //out of bounds
result.fwhm = right - left;
result.left = left;
result.right = right;
double dlh = ( result.peakz-left > right-result.peakz) ? result.peakz-left :
right-result.peakz;
dlh*=2;
result.dlh = dlh;

return result;
}

//*****
*****
/* peak[0] = x coordinate of peak 0 based
peak[1] = y coordinate of peak 0 based
peak[2] = z coordinate of peak 1 based
peak[3] = peak value
*/
private Vektor findPeak() {
    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();
    //int[] peak = {0,0,0,0};
    Vektor peak = new Vektor();
    int value = 0;

    Rectangle bounds = currentRoi.getBounds();
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) bounds.getY() + (int)
bounds.getHeight(); y++) {
            for (int x = (int) bounds.getX(); x <= (int) bounds.getX() +
(int) bounds.getWidth(); x++) {
                if (!currentRoi.contains(x,y)) continue;

```



```

        value = (int) integratedIntensity(x,y,z);
        if ( value > peak.peak ) {
            peak.x = x;
            peak.y = y;
            peak.z = z;
            peak.peak = value;
        }
    }
}

return peak;
}

//*****
*****
private int[] fixBounds(ImagePlus tmp, int x, int y, int z) {
    int[] v = new int[6];
    v[0] = x-integratedRadius;
    v[1] = x+integratedRadius;
    v[2] = y-integratedRadius;
    v[3] = y+integratedRadius;
    v[4] = z-integratedRadius;
    v[5] = z+integratedRadius;
    if ( v[0] < 0 ) v[0] = 0;
    if ( v[2] < 0 ) v[2] = 0;
    if ( v[4] < 1 ) v[4] = 1;
    if ( v[1] > imp.getWidth()-1 ) v[1] = imp.getWidth() - 1;
    if ( v[3] > imp.getHeight()-1 ) v[3] = imp.getHeight() - 1;
    if ( v[5] > imp.getNSlices() ) v[5] = imp.getNSlices();
    return v;
}

//*****
*****
/*
private void GaussIt(ImagePlus tmp, double rad) {
    ImageProcessor ip = tmp.getProcessor();
    if (blur == null)
        blur = new GaussianBlur();
    for (int i=1; i<tmp.getNSlices(); i++) {
        tmp.setSlice(i);
        blur.blur(ip,rad);
    }
    tmp.updateImage();
}
}

```

```

*/

//*****
*****
private double integratedIntensity(int x, int y, int z) {
    double intensity = 0;
    voxels = 0;
    int[] value = {0,0,0,0};
    int[] v = fixBounds(imp,x,y,z);
    int xmin = v[0];
    int xmax = v[1];
    int ymin = v[2];
    int ymax = v[3];
    int zmin = v[4];
    int zmax = v[5];
    for (z = zmin; z <= zmax; z++) {
        //imp.setSlice(z);
        imp.setPosition(1,z,1);
        //imp.setPositionWithoutUpdate(1,z,1);
        for (y = ymin; y <= ymax; y++) {
            for (x = xmin; x <= xmax; x++,voxels++) {
                value = imp.getPixel(x,y);
                intensity += value[0];
            }
        }
    }
    return intensity;
}

//*****
*****
// just needed to avoid abstract class
public void lostOwnership(Clipboard clipboard, Transferable contents) {}

//*****
*****
//odd dimensions only, no funny business
private ImagePlus makeSubStack(String name, int x, int y, int zmin, int zmax, int
length, int width )
{
    final int xmin = x-(length/2);
    //final int xmax = x+(length/2);
    final int ymin = y-(width/2);
    //final int ymax = y+(width/2);
    /*

```

```

int zmin = z-(depth/2);
int zmax = z+(depth/2);
if (zmin < 1) {
depth-= ( 1-zmin);
zmin = 1;
}
if (zmax > imp.getNSlices()) {
depth-=(zmax-imp.getNSlices());
zmax = imp.getNSlices();
}
*/

ImagePlus tmp = NewImage.createShortImage(name, length, width,zmax-
zmin+1, NewImage.FILL_BLACK);
ImageProcessor ip = tmp.getProcessor();
int[] data = new int[length*4];
for (int i=zmin,w=1; i<=zmax; i++,w++) {
    imp.setSlice(i);
    tmp.setSlice(w);
    for (int j=0; j<width; j++) {
        imp.getProcessor().getRow(xmin, j + ymin, data, length);
        ip.putRow(0,j, data,length);
    }
}
tmp.updateImage();
return tmp;
}

//*****
*****

double mad(ImagePlus tmp, int x, int y, int z) {
double size = Math.pow(2*integratedRadius+1, 3);
double[] array = new double[(int) size];
int orig = tmp.getSlice();
int[] v = fixBounds(tmp,x,y,z);
int xmin = v[0];
int xmax = v[1];
int ymin = v[2];
int ymax = v[3];
int zmin = v[4];
int zmax = v[5];
int n = 0;
String s = "mad: " + z;

for(z = zmin; z<=zmax; z++) {
    tmp.setSlice(z);

```

```

        for(y = ymin; y<=ymax; y++) {
            for(x = xmin; x<=xmax; x++) {
                array[n++] = tmp.getPixel(x,y)[0];
                s += " "+array[n-1];
            }
        }
    }
    Arrays.sort(array);
    double median = array[array.length/2];
    int i;
    for (i=0; i<array.length; i++) {
        array[i] = Math.abs(array[i] - median);
    }

    Arrays.sort(array);
    s+= String.format("= %.0f point %d zmin %d zmax %d median %f",
array[array.length/2],(int) i/2, zmin, zmax,median);
    IJ.write(s);
    tmp.setSlice(orig);
    return array[array.length/2];
}

//*****
*****

double madmedian(ImagePlus tmp, int x, int y, int z) {
    double size = Math.pow(2*integratedRadius+1, 3);
    double[] array = new double[(int) size];
    int orig = tmp.getSlice();
    int[] v = fixBounds(tmp,x,y,z);
    int xmin = v[0];
    int xmax = v[1];
    int ymin = v[2];
    int ymax = v[3];
    int zmin = v[4];
    int zmax = v[5];
    int n = 0;

    for(z = zmin; z<=zmax; z++) {
        tmp.setSlice(z);

        for(y = ymin; y<=ymax; y++) {
            for(x = xmin; x<=xmax; x++) {
                array[n++] = tmp.getPixel(x,y)[0];
            }
        }
    }
}

```

```

    }
    Arrays.sort(array);
    tmp.setSlice(orig);
    double median = array[array.length/2];
    return median;
}

//*****
*****

private void measureAll() {
    RoiManager mgr = RoiManager.getInstance();
    if (mgr == null) {
        IJ.beep();
        IJ.showStatus("Roi Manager not open");
        return;
    }

    Roi[] rois = mgr.getRoisAsArray();

    int orig = imp.getSlice();
    for (int i=0; i < rois.length; i++) {
        currentRoi = rois[i];
        imp.setSlice(mgr.getSliceNumber(currentRoi.getName()));
        if (mgr.getSliceNumber(currentRoi.getName()) < 1) {
            IJ.error("I don't know what the slice is for ROI
"+currentRoi.getName());
        }
        measureit();
    }
    imp.setSlice(orig);
}

//*****
*****

private void medianFilter(ImagePlus before, ImagePlus after) {
    final int window = 2*((int)medianRadius)+1;
    int data[] = new int[window*window];
    final int xmin = before.getWidth() / 2 - ((int)medianRadius);
    final int xmax = before.getWidth() / 2 + ((int)medianRadius);
    final int ymin = before.getHeight() / 2 - ((int)medianRadius);
    final int ymax = before.getHeight() / 2 + ((int)medianRadius);
    //IJ.write(String.format("%d %d %d %d",xmin,xmax,ymin,ymax));
    for (int z=1; z<before.getNSlices(); z++) {
        int i=0;
        String s = "z: "+z;
        before.setSlice(z);

```

```

        after.setSlice(z);
        for (int y=ymin; y<=ymax;y++) {
            for (int x=xmin; x<=xmax; x++) {
                data[i++] = before.getPixel(x,y)[0];
                s += " "+data[i-1];
                //IJ.write(String.format("%d",data[i-1]));
            }
        }
        //sort
        Arrays.sort(data);
        s+= "= "+data[i/2]+" point "+i/2;
        IJ.write(s);
        //IJ.write(String.format("%d %d", data[i/2], window*window/2));
        ImageProcessor ip = after.getProcessor();
        ip.putPixel(after.getWidth()/2,after.getHeight()/2,data[i/2]);
    }
    after.updateImage();
}
//*****
*****
private void chkMedian3dFilter(ImagePlus before, ImagePlus after) {
    final int window = 2*((int)medianRadius)+1;
    int data[] = new int[window*window*window];
    final int xmin = before.getWidth() / 2 - ((int)medianRadius);
    final int xmax = before.getWidth() / 2 + ((int)medianRadius);
    final int ymin = before.getHeight() / 2 - ((int)medianRadius);
    final int ymax = before.getHeight() / 2 + ((int)medianRadius);

    //IJ.write(String.format("%d %d %d %d",xmin,xmax,ymin,ymax));
    for (int z=1; z<before.getNSlices(); z++) {
        int i=0;
        String s = "z: "+z;
        for (int ztmp=z-(int)medianRadius; ztmp<=z+(int)medianRadius;
ztmp++) {
            before.setSlice(ztmp);
            after.setSlice(ztmp);
            for (int y=ymin; y<=ymax;y++) {
                for (int x=xmin; x<=xmax; x++) {
                    data[i++] = before.getPixel(x,y)[0];
                    s += " "+data[i-1];
                    //IJ.write(String.format("%d",data[i-1]));
                }
            }
        }
        //sort
        Arrays.sort(data);

```

```

        s+= String.format("= %d point %d zmin %d zmax
%d",data[i/2],i/2,(int)(z-medianRadius),(int)(z+medianRadius));
        IJ.write(s);
        //IJ.write(String.format("%d %d", data[i/2],
window*window*window/2));
        ImageProcessor ip = after.getProcessor();
        after.setSlice(z);
        ip.putPixel(after.getWidth()/2,after.getHeight()/2,data[i/2]);
    }
    after.updateImage();
}

//*****
*****

private void measureit() {
    final int orig = imp.getSlice();

    Duplicater d = new Duplicater();

    try {
        Vektor peak = findPeak();
        Vektor subpeak = new Vektor();
        subpeak.x = window/2;
        subpeak.y = window/2;
        subpeak.z = range+1;
        int zmin=peak.z-range;
        if (zmin<1) zmin = 1;
        int zmax=peak.z+range;
        if (zmax>imp.getNSlices()) zmax = imp.getNSlices();

        int zpad=0;
        //if we are too close the front of the stack, we don't pad.
        if (peak.z-range<1) {
            subpeak.z = peak.z;
        } else {
            zpad = peak.z - range -1;
        }

        //ok we know 3x3 and center pixel
        origImg = makeSubStack("Before",peak.x,peak.y, zmin, zmax,
window,window);

        filteredImg = d.duplicateStack(origImg, "After");
        filteredImg.updateImage();

        //IJ.run("Median...", "radius=" +medianRadius);
        if (median3d)

```

```

        chkMedian3dFilter(origImg, filteredImg);
    else
        medianFilter(origImg, filteredImg);
    origResults = findFWHM(subpeak, origImg);
    filteredResults = findFWHM(subpeak, filteredImg);
    //ok do stats
    /*
        ImageStack c = new ImageStack(window*2,window,
tmp.getImageStack().getColorModel());
        ImageProcessor ip = tmp.getProcessor();
        ImageProcessor ip2;

        for (int zed=1; zed<=tmp.getNSlices(); zed++) {
ip2 = ip.createProcessor(window*2,window);
ip2.setValue(0);
ip2.fill();
ip2.insert(tmp.getStack().getProcessor(zed),0,0);
ip2.insert(filteredImg.getStack().getProcessor(zed),window,0);
c.addSlice(null,ip2);
        }
        */
    //no point show combined. Only 1 pixel changes
    //ImagePlus combined = new ImagePlus("Before/After Median " +
currentRoi.getName(), c);
    //combined.setSlice(subpeak[2]);
    //combined.resetDisplayRange();
    //combined.show();

    if ( rt == null ) {
        reportCSV(peak,subpeak,zpad);
    } else {
        if (rt.getCounter()==0) makeResultTable(); //results table

closed
        reportRT(peak,subpeak,zpad);
        rt.show("Results Integrated FWHM");
        IJ.showStatus(peak.toString());
        displayFWHM(peak, subpeak, zmin, zmax, zpad);
    }

    origImg.flush();
    filteredImg.flush();
} catch (Exception e) {

}
imp.setSlice(orig);
}

```



```

//*****
*****
private void makeResultTable() {
    rt = new ResultsTable();
    rt.reset();
    rt.getFreeColumn("Cen X");
    rt.getFreeColumn("Y");
    rt.getFreeColumn("Z");
    rt.getFreeColumn("Median Max Z");
    rt.getFreeColumn("Median Max pixel");
    rt.getFreeColumn("FWHM");
    rt.getFreeColumn("DLH");
    rt.getFreeColumn("Left");
    rt.getFreeColumn("Right");
    rt.getFreeColumn("Med FWHM");
    rt.getFreeColumn("Med DLH");
    rt.getFreeColumn("Med Left");
    rt.getFreeColumn("Med Right");
    rt.getFreeColumn("Status");
    rt.getFreeColumn("MAD Max");
    rt.getFreeColumn("MAD Max Med");
    rt.getFreeColumn("MAD L1");
    rt.getFreeColumn("MAD L1 Med");
    rt.getFreeColumn("MAD L2");
    rt.getFreeColumn("MAD L2 Med");
    rt.getFreeColumn("MAD R1");
    rt.getFreeColumn("MAD R1 Med");
    rt.getFreeColumn("MAD R2");
    rt.getFreeColumn("MAD R2 Med");
    //fields for array of data points
}

//*****
*****
private double validate(double max, Vektor subpeak) {
    int count=0;

    for (int z=1; z<=origImg.getNSlices(); z++) {
        origImg.setSlice(z);
        if (max == origImg.getPixel(subpeak.x,subpeak.y)[0]) count++;
        if (count >= flattop) {
            return 1.0;
        }
    }
}

```



```

        filteredResults.fwhm,
        filteredResults.dlh,
        filteredResults.left+zpad,
        filteredResults.right+zpad,
        validate(origResults.peak,subpeak),
        mad(origImg>window/2>window/2>filteredResults.peakz),
        madmedian(origImg>window/2>window/2>filteredResults.peakz),
        mad(origImg>window/2>window/2>(int) filteredResults.l1),
        madmedian(origImg>window/2>window/2>(int)
filteredResults.l1),
        mad(origImg>window/2>window/2>(int) filteredResults.l2),
        madmedian(origImg>window/2>window/2>(int)
filteredResults.l2),
        mad(origImg>window/2>window/2>(int) filteredResults.r1),
        madmedian(origImg>window/2>window/2>(int)
filteredResults.r1),
        mad(origImg>window/2>window/2>(int) filteredResults.r2),
        madmedian(origImg>window/2>window/2>(int)
filteredResults.r2));
        try {
            csvout.write(s);
            csvout.newLine();
        } catch (IOException e) {
            IJ.write(e.getMessage());
        }
    }

    //*****
*****

private void reportRT(Vektor peak, Vektor subpeak, int zpad) {
    rt.incrementCounter();
    rt.addLabel("Name",currentRoi.getName());
    rt.addValue(0,peak.x); //center x
    rt.addValue(1,peak.y); //center y
    rt.addValue(2,peak.z); //center z
    rt.addValue(3,filteredResults.peakz+zpad); //max z
    rt.addValue(4,filteredResults.peak); //max pixel value
    rt.addValue(5,origResults.fwhm); //fwhm
    rt.addValue(6,origResults.dlh); //dlh
    rt.addValue(7,origResults.left+zpad); //left position
    rt.addValue(8,origResults.right+zpad); //right position
    rt.addValue(9,filteredResults.fwhm); //median fwhm
    rt.addValue(10,filteredResults.dlh); //median dlh
    rt.addValue(11,filteredResults.left+zpad); //left position
    rt.addValue(12,filteredResults.right+zpad); //right position
}

```

```

        rt.addValue(13,validate(origResults.peak,subpeak));
        rt.addValue(14,mad(origImg>window/2>window/2,filteredResults.peakz));

        rt.addValue(15,madmedian(origImg>window/2>window/2,filteredResults.peakz));
        rt.addValue(16,mad(origImg>window/2>window/2,(int)
filteredResults.l1));
        rt.addValue(17,madmedian(origImg>window/2>window/2,(int)
filteredResults.l1));
        rt.addValue(18,mad(origImg>window/2>window/2,(int)
filteredResults.l2));
        rt.addValue(19,madmedian(origImg>window/2>window/2,(int)
filteredResults.l2));
        rt.addValue(20,mad(origImg>window/2>window/2,(int)
filteredResults.r1));
        rt.addValue(21,madmedian(origImg>window/2>window/2,(int)
filteredResults.r1));
        rt.addValue(22,mad(origImg>window/2>window/2,(int)
filteredResults.r2));
        rt.addValue(23,madmedian(origImg>window/2>window/2,(int)
filteredResults.r2));
        //for (int z=peak[4]-range,i=6; z<=peak[4]+range; z++,i++) {
        //    imp.setSlice(z);
        //    rt.addValue(i,imp.getPixel(peak[0],peak[1])[0]);
        //}
    }

    //*****
    *****

    public void run(String arg) {
        String options = "";
        String csvname = "";
        backgroundsubtract = 0;

        if (IJ.versionLessThan("1.40")) {
            IJ.showMessage("ImageJ 1.40 or greater required.");
            return;
        }

        if (Macro.getOptions() == null) {
            makeResultTable();
            showDialog();
        } else { //validation
            options = Macro.getOptions();
            imp = WindowManager.getCurrentImage();
            if (imp == null) return;
            try {

```

```

        planes = Integer.parseInt(Macro.getValue(options,
"planes", "20"));
        range = Integer.parseInt(Macro.getValue(options, "range",
"50"));
        integratedRadius =
Integer.parseInt(Macro.getValue(options, "integratedradius", "1"));
        medianRadius = Integer.parseInt(Macro.getValue(options,
"medianradius", "1"));
        flattop = Integer.parseInt(Macro.getValue(options,
"flattop", "3"));
        median3d = Macro.getValue(options, "3d", "false") !=
"false";
        backgroundsubtract =
Integer.parseInt(Macro.getValue(options, "subtract", "0"));
        csvname = Macro.getValue(options, "csv", imp.getTitle());

    } catch (NumberFormatException e) {
        IJ.error("At least one of the arguments is not parseable! " +
options);
    }
    if (!validateArgs()) return;
    try {
        if (!csvname.toLowerCase().endsWith("csv")) csvname +=
".csv";

        File csv = new File(csvname);
        csvout = new BufferedWriter(new FileWriter(csv));
        csvout.write("planes," + planes + ",range," + range +
",integrated radius," + integratedRadius +
",median radius," + medianRadius + ",flat
top," + flattop + ",3D," + median3d + ",background sub," + backgroundsubtract);
        csvout.newLine();
        csvout.write("image name,region name,x,y,z,median max
z,median max pixel,fwhm,dlh,left,right,median fwhm,med dlh,median left,median
right,status,mad max,mad max med,mad l1,mad l1 med,mad l2,mad l2 med,mad r1,mad
r1 med,mad r2,mad r2 med");
        csvout.newLine();
        if (backgroundsubtract>0) //in case pam wants to subtract
separately
            IJ.run("Subtract...",
"value="+backgroundsubtract+" stack");
        measureAll();
        csvout.close();
    } catch (Exception e) {
        CharArrayWriter caw = new CharArrayWriter();
        PrintWriter pw = new PrintWriter(caw);
        e.printStackTrace(pw);
    }

```

```

        IJ.write(caw.toString());
        IJ.showStatus("");
    }
}

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill) {
    set_gbc(row,column,width,height,fill,0,0);
}

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill, int padx, int
pady) {
    gbc.gridy = row;
    gbc.gridx = column;
    gbc.gridwidth = width;
    gbc.gridheight = height;
    gbc.fill = fill; // GridBagConstraints.NONE .HORIZONTAL
.VERTICAL .BOTH
    gbc.ipadx = padx;
    gbc.ipady = pady;
    // leave other fields (eg, anchor) unchanged.
}

//*****
*****
private boolean validateArgs() {
    if (planes < 1) {
        IJ.showMessage("Invalid number of planes. Try again hoser.");
        return false;
    }
    if (range < 10) {
        IJ.showMessage("Invalid range to display. Try again hoser.");
        return false;
    }
    if (integratedRadius < 1) {
        IJ.showMessage("Invalid integrated radius. Try again hoser.");
        return false;
    }
    if (medianRadius < 1) {
        IJ.showMessage("Invalid median radius. Try again hoser.");
        return false;
    }
}

```

```

        if (flattop < 2) {
            JJ.showMessage("Invalid flattop radius. Try again hoser.");
            return false;
        }

        return true;
    }

    //*****
    *****
    public void showDialog() {
        //because windows is stupid
        setLayout(new FlowLayout());
        panel = new Panel();
        GridBagLayout gridbag = new GridBagLayout();
        panel.setLayout(gridbag);
        String s = "Select a region around a bead.";
        Label l = new Label(s);
        set_gbc(0,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        s = "Specify how far above and below to look.";
        l = new Label(s);
        set_gbc(1,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        s = "Specify the radius to average.";
        l = new Label(s);
        set_gbc(2,0,4,1, GridBagConstraints.HORIZONTAL, 0, 10);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("Planes to check", Label.RIGHT);
        set_gbc(3,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        txtPlanes = new TextField("20", 20);
        set_gbc(3,2,2,1, GridBagConstraints.NONE);
        gridbag.setConstraints(txtPlanes,gbc);
        panel.add(txtPlanes, gbc);
        l = new Label("Range to Return", Label.RIGHT);
        set_gbc(4,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        txtRange = new TextField("50", 20);
        set_gbc(4,2,2,1, GridBagConstraints.NONE);
        gridbag.setConstraints(txtRange,gbc);
    }

```

```

panel.add(txtRange, gbc);
l = new Label("Integrated Intensity radius", Label.RIGHT);
set_gbc(5,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtIntegratedIntensity = new TextField("1", 20);
set_gbc(5,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtIntegratedIntensity,gbc);
panel.add(txtIntegratedIntensity, gbc);
//l = new Label("Max Radius", Label.RIGHT);
//set_gbc(6,0,2,1, GridBagConstraints.HORIZONTAL);
//gridbag.setConstraints(l,gbc);
//panel.add(l, gbc);
//txtMaxRadius = new TextField("2", 20);
//set_gbc(6,2,2,1, GridBagConstraints.NONE);
//gridbag.setConstraints(txtMaxRadius,gbc);
//panel.add(txtMaxRadius, gbc);
l = new Label("Median Radius", Label.RIGHT);
set_gbc(6,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtMedianRadius = new TextField("1", 20);
set_gbc(6,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtMedianRadius,gbc);
panel.add(txtMedianRadius, gbc);
l = new Label("Flat top pixels", Label.RIGHT);
set_gbc(7,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtFlattop = new TextField("3", 20);
set_gbc(7,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtFlattop,gbc);
panel.add(txtFlattop, gbc);
chkMedian3d = new Checkbox("3D Median");
set_gbc(8,2,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(chkMedian3d, gbc);
panel.add(chkMedian3d, gbc);
Button b = new Button("Measure");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(9,0,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Measure All");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());

```



```

set_gbc(9,1,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Dump ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(9,2,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Clear ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(9,3,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Copy Values");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(10,0,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Copy Median");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(10,1,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Check Outlier");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(10,2,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
l = new Label("Status:");
set_gbc(11,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("0 - valid");
set_gbc(12,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("Blue - original values");
set_gbc(12,2,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("1 - flat top");

```

```

        set_gbc(13,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("Green - median filtered values");
        set_gbc(13,2,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("2 - noisy left of peak");
        set_gbc(14,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("Orange - mean of integrated");
        set_gbc(14,2,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("3 - noisy right of peak");
        set_gbc(15,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);

        add(panel);

        pack();
        GUI.center(this);
        setVisible(true);
    }

    /**
     *
     */
    void showAbout() {
        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This app takes a region, finds the brightest point
and averages it with pixels in a radius of x.");
    }

    /**
     *
     */
    void error() {
        IJ.showMessage("Pam_Bead_StatsMedian", "This plugin requires a
defined region to work");
    }
}

```

## 7. Pam\_Bead\_StatsResolution.java

```
import ij.*;
import ij.plugin.frame.*;
import ij.plugin.filter.*;
import ij.measure.*;
import ij.process.*;
import ij.gui.*;
import java.awt.*;
import java.awt.event.*;
import java.awt.datatransfer.*;
import java.io.*;

/** Given a region of interest it, it finds the brightest subregion. It then takes the central
pixel, return a range along
 * Z, finds the max of the range, and does the FWHM. This is the final incarnation that
was used. Sigmaplot was used for the fittings.
 *
 * @author Jason Byars <jbyars@iupui.edu>
 * @version 0.001
 */
public class Pam_Bead_StatsResolution extends PlugInFrame implements
ActionListener, ClipboardOwner {

    private static final long serialVersionUID = 2145848743530492113L;

    /** Convenience class to track subregion location and peak intensity.
 */
    class Vektor {
        public int x;
        public int y;
        public int z;
        public int peak;

        public Vektor() {
            x = y = z = peak = 0;
        }

        public String toString() {
            String s = "Peak "+peak+" x: "+x+" y: "+y+" z: "+z;
            return s;
        }
    };

    /** Convenience class to track stats for a given subregion.
 */
}
```

```

class PamStatsResults {
    public double fwhm;
    public double dlh;
    public double left;
    public double right;
    public double peak;
    public int peakz;
    public double l1;
    public double l2;
    public double r1;
    public double r2;

    public PamStatsResults() {
        fwhm = -1;
        left = 0;
        right = 0;
        dlh = 0;
        peak = 0;
        peakz = 0;
        l1 = l2 = r1 = r2 = 0;
    }
};

Panel panel;
static Frame instance;
GridBagConstraints gbc = new GridBagConstraints();
ImagePlus imp;
ImagePlus origImg;
PamStatsResults origResults;
Roi    currentRoi;
ResultsTable rt;
TextField txtPlanes;
TextField txtIntegratedIntensity;
TextField txtRange;
TextField txtFlattop;
GaussianBlur blur;
double backgroundsubtract;
int planes;
int integratedRadius;
int range;
int peakIntensity;
int voxels;
int[] zrange;
double [] index;
double []    zValues;
static final int window = 21; //size of substack for filtering

```

```
int flattop; //if 3 or more pixels are at max value, it is a flattop problem
BufferedWriter csvout;
```

```
//*****
*****
```

```
public Pam_Bead_StatsResolution() {
    super("Pam_Bead_StatsResolution v0.001");
    if (IJ.versionLessThan("1.40")) {
        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    if (instance!=null) {
        instance.toFront();
        return;
    }
    instance = this;
    addKeyListener(IJ.getInstance());

    IJ.register(Pam_Bead_StatsResolution.class);
}
```

```
//*****
*****
```

```
public void actionPerformed(ActionEvent e) {
    imp = WindowManager.getCurrentImage();
    currentRoi = imp.getRoi();
    if (imp==null) {
        IJ.beep();
        IJ.showStatus("No image");
        return;
    }
    if (currentRoi == null) {
        IJ.beep();
        IJ.showStatus("No ROI");
        return;
    }
    if (currentRoi.getType() == Roi.LINE) {
        IJ.beep();
        IJ.showStatus("Rectangles or Ovals only!");
        return;
    }
    String label = e.getActionCommand();
    if (label==null) {
        IJ.showStatus("I have no idea what to do");
        return;
    }
}
```

```

    }
    try {
        planes = Integer.parseInt(txtPlanes.getText());
        range = Integer.parseInt(txtRange.getText());
        integratedRadius =
Integer.parseInt(txtIntegratedIntensity.getText());
        flattop = Integer.parseInt(txtFlattop.getText());
    } catch (NumberFormatException n) {
        IJ.showMessage("Give me real numbers!");
        return;
    }

    if (!validateArgs()) return;

    //We're actually going to do something
    if (label == "Measure") {
        makeResultTable();
        measureit();
    } else if (label == "Measure All") {
        makeResultTable();
        measureAll();
    } else if (label == "Dump ROI") {
        dumpROI();
    } else if (label == "Copy Values") {
        copyValues();
    } else if (label == "Check Outlier") {
        checkOutlier();
    } else
        imp.killRoi();
}

//*****
*****

void checkOutlier() {
    final int orig = imp.getSlice();
    ImagePlus tmp;

    Vektor peak = findPeak();
    Vektor subpeak = new Vektor();
    subpeak.x = window/2;
    subpeak.y = window/2;
    subpeak.z = range+1;
    int zmin=peak.z-range;
    if (zmin<1) zmin = 1;
    int zmax=peak.z+range;
    if (zmax>imp.getNSlices()) zmax = imp.getNSlices();
}

```

```

//int zpad=0;
//if we are too close the front of the stack, we don't pad.
if (peak.z-range<1) {
    subpeak.z = peak.z;
} else {
//    zpad = peak.z - range -1;
}

//ok we know 3x3 and center pixel
tmp = makeSubStack("Before",peak.x,peak.y, zmin, zmax,
window>window);
//PamStatsResults fwhm = findFWHM(subpeak, tmp);

int cubed = (int)Math.pow(2*integratedRadius+1,3);
double[][] index = new double[tmp.getNSlices()];
double[] centerValues = new double[tmp.getNSlices()];
double[] meanValues = new double[tmp.getNSlices()];
double[][] zValues = new double[tmp.getNSlices()];

int maxpixel = 0;
double intensity = 0;
int value = 0;
int xminr = peak.x-integratedRadius;
int xmaxr = peak.x+integratedRadius;
int yminr = peak.y-integratedRadius;
int ymaxr = peak.y+integratedRadius;
if ( xminr < 0 ) xminr = 0;
if ( yminr < 0 ) yminr = 0;
if ( xmaxr > imp.getWidth()-1 ) xmaxr = imp.getWidth() - 1;
if ( ymaxr > imp.getHeight()-1 ) ymaxr = imp.getHeight() - 1;
for (int j=zmin; j<=zmax; j++) {
    intensity = 0;
    int zminr = j-integratedRadius;
    int zmaxr = j+integratedRadius;
    if ( zminr < 1 ) zminr = 1;
    if ( zmaxr > imp.getNSlices() ) zmaxr = imp.getNSlices();
    index[j-zmin] = new double[cubed];
    zValues[j-zmin] = new double[cubed];

    for (int z = zminr, n=0; z <= zmaxr; z++) {
        imp.setSlice(z);
        for (int y = yminr; y <= ymaxr; y++) {
            for (int x = xminr; x <= xmaxr; x++, n++) {
                value = imp.getPixel(x,y)[0];
                index[j-zmin][n] = j;
            }
        }
    }
}

```

```

                zValues[j-zmin][n] = value;
                intensity+=value;
                if (value > maxpixel) maxpixel = value;
            }
        }
    }
    intensity = intensity / cubed;
    imp.setSlice(j);
    centerValues[j-zmin]= imp.getPixel(peak.x, peak.y)[0];
    meanValues[j-zmin] = intensity;
}

double[] zindex = new double[tmp.getNSlices()];
for (int i=zmin; i<=zmax; i++) zindex[i-zmin] = i;
Plot p = new Plot("Check Outliers for "+currentRoi.getName(),"Z
plane","Intensity", (double[]) null,(double[]) null);
p.setLimits(zmin, zmax, 0, maxpixel+100); //100
p.setColor(Color.blue);
for (int j=0; j<tmp.getNSlices(); j++) {
    p.addPoints(index[j],zValues[j],Plot.DOT);
}
p.addLabel(0.02, 0.2, "Integrated Values");
p.setColor(Color.orange);
p.addPoints(zindex, meanValues, PlotWindow.LINE);
p.addLabel(0.02, 0.3, "NxN Mean");
p.setColor(Color.green);
p.addPoints(zindex, centerValues, PlotWindow.X);
p.addLabel(0.02, 0.4, "Center Value");
p.setColor(Color.black);
p.addLabel(0.02, 0.1, String.format("Center:
%d,%d,%d",peak.x,peak.y,peak.z));
p.show();
imp.setSlice(orig);
}

//*****
*****

void copyValues() {
    Clipboard systemClipboard = null;
    try {systemClipboard = getToolkit().getSystemClipboard();}
    catch (Exception e) {systemClipboard = null; }
    if (systemClipboard==null)
        {IJ.error("Unable to copy to Clipboard."); return;}
    IJ.showStatus("Copying z values...");
    CharArrayWriter aw = new CharArrayWriter(index.length*4);
    PrintWriter pw = new PrintWriter(aw);

```



```

        for (int i=0; i<index.length; i++) {
            pw.print(IJ.d2s(index[i],0)+"\t"+IJ.d2s(zValues[i],0)+"\n");
        }
        String text = aw.toString();
        pw.close();
        StringSelection contents = new StringSelection(text);
        systemClipboard.setContents(contents, this);
        IJ.showStatus(text.length() + " characters copied to Clipboard");
    }

    //*****
    *****
    void displayFWHM(Vektor peak, Vektor subpeak, int zmin, int zmax, int zpad) {
        index = new double[origImg.getNSlices()];
        zValues = new double[origImg.getNSlices()];

        for (int z=1; z<=origImg.getNSlices(); z++) {
            index[z-1] = z+zmin-1;
            origImg.setSlice(z);
            zValues[z-1] = origImg.getPixel(subpeak.x,subpeak.y)[0];
        }
        Plot p = new Plot("FWHM for "+currentRoi.getName(),"Z
plane","Intensity", (double[]) null,(double[]) null);
        p.setLimits(zmin, zmax, 0, origResults.peak+100); //100
        p.setColor(Color.blue);
        p.addPoints(index,zValues,PlotWindow.CIRCLE);

        // add label
        //compute double half max
        p.setColor(Color.black);
        p.addLabel(0.02, 0.1, String.format("Center:
%d,%d,%d",peak.x,peak.y,peak.z));
        p.addLabel(0.02, 0.2, String.format("Max pixel: %d z:
%d",(int)origResults.peak,(int)origResults.peakz));
        if (origResults.fwhm > 0) {
            p.addLabel(0.02, 0.3, String.format("FWHM:
%.2f",origResults.fwhm));
            p.addLabel(0.02, 0.4, String.format("DLH:
%.2f",origResults.dlh));
        } else
            p.addLabel(0.02, 0.3, String.format("FWHM:
failed",origResults.fwhm));

        //debug show mean
        p.setColor(Color.orange);
        double[] meanValues = new double[origImg.getNSlices()];

```

```

double size = Math.pow(2*integratedRadius+1, 3);

for (int z=zmin,i=0; z<=zmax; z++,i++) {
    meanValues[i] = integratedIntensity(peak.x,peak.y,z)/size;
    //IJ.write(String.format("integrated intensity %f", meanValues[i]));
}
p.addPoints(index,meanValues,PlotWindow.LINE);

double[] x2 = {origResults.left+zpad,origResults.right+zpad};
double[] y2 = {origResults.peak/2.0, origResults.peak/2.0};
double[] x3 = {origResults.peakz+zpad, origResults.peakz+zpad};
double[] y3 = {origResults.peak/2.0, origResults.peak};
p.setColor(Color.red);
p.addPoints(x2,y2,PlotWindow.X);
p.addPoints(x2,y2,PlotWindow.LINE);
p.addPoints(x3,y3,PlotWindow.LINE);

//p.changeFont(new Font("Helvetica", Font.PLAIN, 16));
p.setColor(Color.lightGray);
p.show();
}

//*****
*****
private void dumpROI() {
    int[] value = {0,0,0,0};
    int orig = imp.getSlice();
    Rectangle bounds = currentRoi.getBounds();
    ResultsTable tmp = new ResultsTable();
    tmp.reset();

    for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++)
        tmp.getFreeColumn("X"+x);

    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();

    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) (bounds.getY() +
bounds.getHeight()); y++) {
            tmp.incrementCounter();

```

```

        for (int x = (int) bounds.getX(); x <= (int) (bounds.getX() +
bounds.getWidth()); x++) {
            if (currentRoi.contains(x,y))
                value = imp.getPixel(x,y);
            else
                value[0] = 0;
            tmp.addValue((int) (x-bounds.getX()), value[0]);
        }
    }
    tmp.show("ROI x"+(int) bounds.getX()+" y"+ (int) bounds.getY()+"
z"+imp.getSlice());
    imp.setSlice(orig);
}

//*****
*****

/* fwhm[0] = full width half max
fwhm[1] = left limit
fwhm[2] = right limit
fwhm[3] = peak pixel z
fwhm[4] = peak pixel
fwhm[5] = dlh
*/
private PamStatsResults findFWHM(Vektor peak, ImagePlus tmp) {
    //double [] fwhm = {-1, 0,0,0,0,0};
    PamStatsResults result = new PamStatsResults();
    final int x = peak.x;
    final int y = peak.y;
    int z = 0;

    //find peak pixel where ever it may be
    //tmp.setSlice(z);
    double limit = 0;
    for(int zed = 1; zed<= tmp.getNSlices(); zed++) {
        tmp.setSlice(zed);
        int value = tmp.getPixel(x,y)[0];
        if (value > limit) {
            z = zed;
            limit = value;
        }
    }

    IJ.write(String.format("value %f z %d", limit, z));
    result.peakz = z;
    result.peak = limit;
}

```

```

limit/=2.0;

int i=0;
double x1=0, x2=0, left=0, right=0, slope=0, offset=0;
for (i=z; i>=1; i--) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x1 = tmp.getPixel(x,y)[0];
        tmp.setSlice(i+1);
        x2 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
        left = i + (offset/slope);
        result.l1 = i;
        result.l2 = i+1;
        break;
    }
}
if (i<1) return result; //out of bounds
for (i=z; i<=tmp.getNSlices(); i++) {
    tmp.setSlice(i);
    if (tmp.getPixel(x,y)[0] <= limit) {
        //interpolate
        x2 = tmp.getPixel(x,y)[0];
        tmp.setSlice(i-1);
        x1 = tmp.getPixel(x,y)[0];
        offset = limit - x1;
        slope = x2 - x1;
        right = i-1 + (offset/slope);
        result.r1 = i-1;
        result.r2 = i;
        break;
    }
}
if (i>tmp.getNSlices()) return result; //out of bounds
result.fwhm = right - left;
result.left = left;
result.right = right;
double dlh = ( result.peakz-left > right-result.peakz) ? result.peakz-left :
right-result.peakz;
dlh*=2;
result.dlh = dlh;

return result;
}

```

```

//*****
*****
/* peak[0] = x coordinate of peak 0 based
peak[1] = y coordinate of peak 0 based
peak[2] = z coordinate of peak 1 based
peak[3] = peak value
*/
private Vektor findPeak() {
    int zmin = imp.getSlice() - planes;
    int zmax = imp.getSlice() + planes;
    if (zmin < 1) zmin = 1;
    if (zmax > imp.getNSlices()) zmax = imp.getNSlices();
    //int[] peak = {0,0,0,0};
    Vektor peak = new Vektor();
    int value = 0;

    Rectangle bounds = currentRoi.getBounds();
    for (int z = zmin; z <= zmax; z++) {
        imp.setSlice(z);
        for (int y = (int) bounds.getY(); y <= (int) bounds.getY() + (int)
bounds.getHeight(); y++) {
            for (int x = (int) bounds.getX(); x <= (int) bounds.getX() +
(int) bounds.getWidth(); x++) {
                if (!currentRoi.contains(x,y)) continue;
                value = (int) integratedIntensity(x,y,z);
                if ( value > peak.peak ) {
                    peak.x = x;
                    peak.y = y;
                    peak.z = z;
                    peak.peak = value;
                }
            }
        }
    }

    return peak;
}

//*****
*****
private int[] fixBounds(ImagePlus tmp, int x, int y, int z) {
    int[] v = new int[6];
    v[0] = x-integratedRadius;
    v[1] = x+integratedRadius;
    v[2] = y-integratedRadius;

```

```

        v[3] = y+integratedRadius;
        v[4] = z-integratedRadius;
        v[5] = z+integratedRadius;
        if ( v[0] < 0 ) v[0] = 0;
        if ( v[2] < 0 ) v[2] = 0;
        if ( v[4] < 1 ) v[4] = 1;
        if ( v[1] > imp.getWidth()-1 ) v[1] = imp.getWidth() - 1;
        if ( v[3] > imp.getHeight()-1 ) v[3] = imp.getHeight() - 1;
        if ( v[5] > imp.getNSlices() ) v[5] = imp.getNSlices();
        return v;
    }

    /**
    *****
    */
    private void GaussIt(ImagePlus tmp, double rad) {
        ImageProcessor ip = tmp.getProcessor();
        if (blur == null)
            blur = new GaussianBlur();
        for (int i=1; i<tmp.getNSlices(); i++) {
            tmp.setSlice(i);
            blur.blur(ip,rad);
        }
        tmp.updateImage();
    }
    */

    /**
    *****
    private double integratedIntensity(int x, int y, int z) {
        double intensity = 0;
        voxels = 0;
        int[] value = {0,0,0,0};
        int[] v = fixBounds(imp,x,y,z);
        int xmin = v[0];
        int xmax = v[1];
        int ymin = v[2];
        int ymax = v[3];
        int zmin = v[4];
        int zmax = v[5];
        for (z = zmin; z <= zmax; z++) {
            //imp.setSlice(z);
            imp.setPosition(1,z,1);
            //imp.setPositionWithoutUpdate(1,z,1);
            for (y = ymin; y <= ymax; y++) {
                for (x = xmin; x <= xmax; x++,voxels++) {

```

```

        value = imp.getPixel(x,y);
        intensity += value[0];
    }
}
}
return intensity;
}

/*****
*****/
// just needed to avoid abstract class
public void lostOwnership(Clipboard clipboard, Transferable contents) {}

/*****
*****/
//odd dimensions only, no funny business
private ImagePlus makeSubStack(String name, int x, int y, int zmin, int zmax, int
length, int width )
{
    final int xmin = x-(length/2);
    //final int xmax = x+(length/2);
    final int ymin = y-(width/2);
    //final int ymax = y+(width/2);
    /*
    int zmin = z-(depth/2);
    int zmax = z+(depth/2);
    if (zmin < 1) {
        depth-= ( 1-zmin);
        zmin = 1;
    }
    if (zmax > imp.getNSlices()) {
        depth-=(zmax-imp.getNSlices());
        zmax = imp.getNSlices();
    }
    */

    ImagePlus tmp = NewImage.createShortImage(name, length, width, zmax-
zmin+1, NewImage.FILL_BLACK);
    ImageProcessor ip = tmp.getProcessor();
    int[] data = new int[length*4];
    for (int i=zmin,w=1; i<=zmax; i++,w++) {
        imp.setSlice(i);
        tmp.setSlice(w);
        for (int j=0; j<width; j++) {
            imp.getProcessor().getRow(xmin, j + ymin, data, length);

```

```

        ip.putRow(0,j, data,length);
    }
}
tmp.updateImage();
return tmp;
}

//*****
*****
private void measureAll() {
    RoiManager mgr = RoiManager.getInstance();
    if (mgr == null) {
        IJ.beep();
        IJ.showStatus("Roi Manager not open");
        return;
    }

    Roi[] rois = mgr.getRoisAsArray();

    int orig = imp.getSlice();
    for (int i=0; i < rois.length; i++) {
        currentRoi = rois[i];
        imp.setSlice(mgr.getSliceNumber(currentRoi.getName()));
        if (mgr.getSliceNumber(currentRoi.getName()) < 1) {
            IJ.error("I don't know what the slice is for ROI
"+currentRoi.getName());
        }
        measureit();
    }
    imp.setSlice(orig);
}

//*****
*****
private void measureit() {
    final int orig = imp.getSlice();

    try {
        Vektor peak = findPeak();
        Vektor subpeak = new Vektor();
        subpeak.x = window/2;
        subpeak.y = window/2;
        subpeak.z = range+1;
        int zmin=peak.z-range;
        if (zmin<1) zmin = 1;
        int zmax=peak.z+range;

```



```

        if (zmax>imp.getNSlices()) zmax = imp.getNSlices();

        int zpad=0;
        //if we are too close the front of the stack, we don't pad.
        if (peak.z-range<1) {
            subpeak.z = peak.z;
        } else {
            zpad = peak.z - range -1;
        }

        //ok we know 3x3 and center pixel
        origImg = makeSubStack("Before",peak.x,peak.y, zmin, zmax,
window>window);

        origResults = findFWHM(subpeak, origImg);

        if ( rt == null ) {
            reportCSV(peak,subpeak,zpad);
        } else {
            if (rt.getCounter()==0) makeResultTable(); //results table

            reportRT(peak,subpeak,zpad);
            rt.show("Results Integrated FWHM");
            IJ.showStatus(peak.toString());
            displayFWHM(peak, subpeak, zmin, zmax, zpad);
        }

        origImg.flush();
    } catch (Exception e) {

    }
    imp.setSlice(orig);
}

//*****
*****

private void makeResultTable() {
    rt = new ResultsTable();
    rt.reset();
    rt.getFreeColumn("Cen X");
    rt.getFreeColumn("Y");
    rt.getFreeColumn("Z");
    rt.getFreeColumn("Max");
    rt.getFreeColumn("FWHM");
    rt.getFreeColumn("DLH");
    rt.getFreeColumn("Left");
}

```

```

        rt.getFreeColumn("Right");
        rt.getFreeColumn("Status");
        //fields for array of data points
    }

    /*******
    *****/
    private double validate(double max, Vektor subpeak) {
        int count=0;

        for (int z=1; z<=origImg.getNSlices(); z++) {
            origImg.setSlice(z);
            if (max == origImg.getPixel(subpeak.x,subpeak.y)[0]) count++;
            if (count >= flattop) {
                return 1.0;
            }
        }

        double hmax = origResults.peak/2.0;
        for (int z=(int) Math.ceil(origResults.left-1); z>0; z--) {
            origImg.setSlice(z);
            //IJ.write(String.format("hmax %f > %d at %d starting %f", hmax,
filteredImg.getPixel(subpeak[0],subpeak[1])[0], z, filteredResults[1]));
            if (origImg.getPixel(subpeak.x,subpeak.y)[0] > hmax) {
                return 2.0;
            }
        }
        for (int z=(int) Math.floor(origResults.right+1); z<origImg.getNSlices();
z++) {
            origImg.setSlice(z);
            if (origImg.getPixel(subpeak.x,subpeak.y)[0] > hmax) {
                return 3.0;
            }
        }

        return 0.0;
    }

    /*******
    *****/
    public void processWindowEvent(WindowEvent e) {
        super.processWindowEvent(e);
        if (e.getID()==WindowEvent.WINDOW_CLOSING) {
            instance = null;
        }
    }
}

```

```

//*****
*****
private void reportCSV(Vektor peak, Vektor subpeak, int zpad) {
    try {
        String s =
String.format("%s,%s,%d,%d,%f,%f,%f,%f,%f,%f,%f",

                imp.getTitle(),

                currentRoi.getName(),

                peak.x,

                peak.y,

                peak.z,

                origResults.peak,

                origResults.fwhm,

                origResults.dlh,

                origResults.left+zpad,

                origResults.right+zpad,

                validate(origResults.peak,subpeak));
        for (int z=1; z<=origImg.getNSlices(); z++) {
            origImg.setSlice(z);
            s +=
String.format(",%d",origImg.getPixel(subpeak.x,subpeak.y)[0]);
        }
        csvout.write(s);
        csvout.newLine();
    } catch (IOException e) {
        IJ.write(e.getMessage());
    } catch (Exception e) {
        IJ.write(e.getMessage());
    }
}

//*****
*****
private void reportRT(Vektor peak, Vektor subpeak, int zpad) {

```

```

rt.incrementCounter();
rt.addLabel("Name",currentRoi.getName());
rt.addValue(0,peak.x); //center x
rt.addValue(1,peak.y); //center y
rt.addValue(2,peak.z); //center z
rt.addValue(3,origResults.peak);
rt.addValue(4,origResults.fwhm); //fwhm
rt.addValue(5,origResults.dlh); //dlh
rt.addValue(6,origResults.left+zpad); //left position
rt.addValue(7,origResults.right+zpad); //right position
rt.addValue(8,validate(origResults.peak,subpeak));
}

//*****
*****
public void run(String arg) {
    String options = "";
    String csvname = "";
    backgroundsubtract = 0;

    if (IJ.versionLessThan("1.40")) {
        IJ.showMessage("ImageJ 1.40 or greater required.");
        return;
    }

    if (Macro.getOptions() == null) {
        makeResultTable();
        showDialog();
    } else { //validation
        options = Macro.getOptions();
        imp = WindowManager.getCurrentImage();
        if (imp == null) return;
        try {
            planes = Integer.parseInt(Macro.getValue(options,
"planes", "20"));
            range = Integer.parseInt(Macro.getValue(options, "range",
"50"));
            integratedRadius =
Integer.parseInt(Macro.getValue(options, "integratedradius", "1"));
            flattop = Integer.parseInt(Macro.getValue(options,
"flattop", "3"));
            backgroundsubtract =
Integer.parseInt(Macro.getValue(options, "subtract", "0"));
            csvname = Macro.getValue(options, "csv", imp.getTitle());

        } catch (NumberFormatException e) {

```

```

        IJ.error("At least one of the arguments is not parseable! " +
options);
    }
    if (!validateArgs()) return;
    try {
        if (!csvname.toLowerCase().endsWith("csv")) csvname +=
".csv";
        File csv = new File(csvname);
        csvout = new BufferedWriter(new FileWriter(csv));
        csvout.write("planes," + planes + ",range," + range +
",integrated radius," + integratedRadius +
",flat top," +
flattop + ",background sub," + backgroundsubtract);
        csvout.newLine();
        csvout.write("image name,region
name,x,y,z,max,fwhm,dlh,left,right,status");
        for (int i=0; i<(range*2+1); i++) csvout.write(", "+i);
        csvout.newLine();
        if (backgroundsubtract>0) //in case pam wants to subtract
separately
            IJ.run("Subtract...",
"value="+backgroundsubtract+" stack");
        measureAll();
        csvout.close();
    } catch (Exception e) {
        CharArrayWriter caw = new CharArrayWriter();
        PrintWriter pw = new PrintWriter(caw);
        e.printStackTrace(pw);
        IJ.write(caw.toString());
        IJ.showStatus("");
    }
}
}

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill) {
    set_gbc(row,column,width,height,fill,0,0);
}

//*****
*****
private void set_gbc(int row, int column, int width, int height, int fill, int padx, int
pady) {
    gbc.gridy = row;
    gbc.gridx = column;

```

```

        gbc.gridwidth = width;
        gbc.gridheight = height;
        gbc.fill = fill; // GridBagConstraints.NONE .HORIZONTAL
.VERTICAL .BOTH
        gbc.ipadx = padx;
        gbc.ipady = pady;
        // leave other fields (eg, anchor) unchanged.
    }

    /**
     *
     */
    private boolean validateArgs() {
        if (planes < 1) {
            IJ.showMessage("Invalid number of planes. Try again hoser.");
            return false;
        }
        if (range < 10) {
            IJ.showMessage("Invalid range to display. Try again hoser.");
            return false;
        }
        if (integratedRadius < 1) {
            IJ.showMessage("Invalid integrated radius. Try again hoser.");
            return false;
        }
        if (flattop < 2) {
            IJ.showMessage("Invalid flattop radius. Try again hoser.");
            return false;
        }

        return true;
    }

    /**
     *
     */
    public void showDialog() {
        //because windows is stupid
        setLayout(new FlowLayout());
        panel = new Panel();
        GridBagConstraints gridbag = new GridBagConstraints();
        panel.setLayout(gridbag);
        String s = "Select a region around a bead.";
        Label l = new Label(s);
        set_gbc(0,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
        gridbag.setConstraints(l, gbc);
        panel.add(l, gbc);
        s = "Specify how far above and below to look.";
    }

```

```

l = new Label(s);
set_gbc(1,0,4,1, GridBagConstraints.HORIZONTAL, 0, 0);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
s = "Specify the radius to average.";
l = new Label(s);
set_gbc(2,0,4,1, GridBagConstraints.HORIZONTAL, 0, 10);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("Planes to check", Label.RIGHT);
set_gbc(3,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtPlanes = new TextField("20", 20);
set_gbc(3,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtPlanes,gbc);
panel.add(txtPlanes, gbc);
l = new Label("Range to Return", Label.RIGHT);
set_gbc(4,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtRange = new TextField("50", 20);
set_gbc(4,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtRange,gbc);
panel.add(txtRange, gbc);
l = new Label("Integrated Intensity radius", Label.RIGHT);
set_gbc(5,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtIntegratedIntensity = new TextField("1", 20);
set_gbc(5,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtIntegratedIntensity,gbc);
panel.add(txtIntegratedIntensity, gbc);
l = new Label("Flat top pixels", Label.RIGHT);
set_gbc(6,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
txtFlattop = new TextField("3", 20);
set_gbc(6,2,2,1, GridBagConstraints.NONE);
gridbag.setConstraints(txtFlattop,gbc);
panel.add(txtFlattop, gbc);
Button b = new Button("Measure");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(7,0,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);

```

```

panel.add(b);
b = new Button("Measure All");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(7,1,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Dump ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(7,2,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Clear ROI");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(7,3,1,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Copy Values");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(8,0,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
b = new Button("Check Outlier");
b.addActionListener(this);
b.addKeyListener(IJ.getInstance());
set_gbc(8,1,1,1, GridBagConstraints.NONE);
gridbag.setConstraints(b,gbc);
panel.add(b);
l = new Label("Status:");
set_gbc(9,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("0 - valid");
set_gbc(10,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("Blue - original values");
set_gbc(10,2,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);
panel.add(l, gbc);
l = new Label("1 - flat top");
set_gbc(11,0,2,1, GridBagConstraints.HORIZONTAL);
gridbag.setConstraints(l,gbc);

```



```

        panel.add(l, gbc);
        l = new Label("Orange - mean of integrated");
        set_gbc(11,2,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("2 - noisy left of peak");
        set_gbc(12,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);
        l = new Label("3 - noisy right of peak");
        set_gbc(13,0,2,1, GridBagConstraints.HORIZONTAL);
        gridbag.setConstraints(l,gbc);
        panel.add(l, gbc);

        add(panel);

        pack();
        GUI.center(this);
        setVisible(true);
    }

    /*******
    *****
    void showAbout() {
        String title = "About " + getClass().getName() + "...";
        IJ.showMessage(title, "This app takes a region, finds the brightest point
and averages it with pixels in a radius of x.");
    }

    /*******
    *****
    void error() {
        IJ.showMessage(getClass().getName(), "This plugin requires a defined
region to work");
    }
}

```

## C. *Excel macros*

### 1. *Common\_Tools*

Option Explicit

```
Public WSColl As Collection
Public CHColl As Collection
```

```
Public Const c_badpoint As Integer = 6
Public Const c_saturated As Integer = 3
Public Const c_pamdecide As Integer = 7
Public Const c_dontgraph As Integer = 15
```

```
Const c_name As Integer = 1
Const c_roi As Integer = 2
Const c_z As Integer = 8
Const c_meanbkg As Integer = 13
```

```
Sub StopAllEvents()
    ''' There are problems with out of control event cascades
    Application.EnableEvents = False
    'Your code here.
    Application.EnableEvents = True
End Sub
```

```
Sub stop_excel(control As IRibbonControl)
    ''' Disable the GUI so an event cascade isn't triggered
    ''' control is not used
    Application.EnableEvents = False
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
End Sub
```

```
Sub start_excel(control As IRibbonControl)
    ''' Enables the GUI to process user events
    ''' control is not used
    Application.EnableEvents = True
    Application.ScreenUpdating = True
    Application.DisplayAlerts = True
End Sub
```

```
Private Sub BuildCustomMenu()
    ''' This adds the right click functionality of the plugin.
    ''' At the moment that is just the ability to remove and restore rows from the processed
    sheet.s
```

```

Dim ctrl As CommandBarControl
Dim btn As CommandBarControl
Dim i As Integer

'add a 'popup' control to the cell commandbar (menu)
Set ctrl = Application.CommandBars("Cell").Controls.Add(Type:=msoControlButton,
Before:=1, Temporary:=True)
ctrl.Caption = "Remove row"
ctrl.OnAction = "remove_row"
Set ctrl = Application.CommandBars("Cell").Controls.Add(Type:=msoControlButton,
Before:=2, Temporary:=True)
ctrl.Caption = "Restore row"
ctrl.OnAction = "restore_row"
Set ctrl = Application.CommandBars("Row").Controls.Add(Type:=msoControlButton,
Before:=1, Temporary:=True)
ctrl.Caption = "Remove row"
ctrl.OnAction = "remove_row"
Set ctrl = Application.CommandBars("Row").Controls.Add(Type:=msoControlButton,
Before:=2, Temporary:=True)
ctrl.Caption = "Restore row"
ctrl.OnAction = "restore_row"
End Sub

Private Sub DeleteCustomMenu()
''' This goes through and removes any additions to the right click menus.
''' It is used to prevent duplicate entries and cleanup.
Dim ctrl As CommandBarControl

'go thru all the cell commandbar controls and delete our menu item
For Each ctrl In Application.CommandBars("Cell").Controls
If ctrl.Caption = "Restore row" Or _
ctrl.Caption = "Remove row" Then
ctrl.Delete
End If
Next
For Each ctrl In Application.CommandBars("Row").Controls
If ctrl.Caption = "Restore row" Or _
ctrl.Caption = "Remove row" Then
ctrl.Delete
End If
Next
End Sub

Function GetRolling(arr As Range, low As Double, high As Double, zmicrons As
Integer, col As Integer)

```

```

Dim rw As Range
Dim count, i As Integer
Dim total As Double
Dim currentUpdating As Boolean

currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

total = 0
count = 0
' count points
For i = arr.Row To arr.Row + arr.Rows.count - 1
    If Cells(i, zmicrons).value >= low And Cells(i, zmicrons).value < high Then
        total = total + Cells(i, col).value
        count = count + 1
    End If
Next i

If count < 1 Then
    GetRolling = 0
Else
    GetRolling = total / count
End If
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

Function GetRollingStdev(arr As Range, low As Double, high As Double, zmicrons As
Integer, col As Integer, meancol As Range)
    Dim count, i As Integer
    Dim total As Double
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    total = 0
    count = 0
    ' count points
    For i = arr.Row To arr.Row + arr.Rows.count - 1
        If Cells(i, zmicrons).value >= low And Cells(i, zmicrons).value < high Then
            total = total + (Cells(i, col).value - meancol.value) ^ 2
            count = count + 1
        End If
    
```

```

Next i
If count < 2 Then
    GetRollingStdev = 0
Else
    GetRollingStdev = Sqr(total / (count - 1))
End If

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

Function GetTTest(arr As Range, fwhm As Range, rolling As Range, stdev As Range)
    Dim t As Double
    If stdev.value <> 0 Then
        ' t test
        t = Abs(fwhm.value - rolling.value) / stdev.value
        If count < 3 Then
            Cells(fwhm.Row, c_resttest).Interior.ColorIndex = c_dontgraph
        ElseIf count > 147 And t >= Sheets("ASTM").Cells(Application.Min(count, 147)
- 1, 3).value Then
            Cells(fwhm.Row, c_resttest).Interior.ColorIndex = c_pamdecide
        ElseIf t >= Sheets("ASTM").Cells(Application.Min(count, 147) - 1, 3).value Then
            Cells(fwhm.Row, c_resttest).Interior.ColorIndex = c_badpoint
        Else
            Cells(fwhm.Row, c_resttest).Interior.ColorIndex = 0
        End If
    Else
        Cells(fwhm.Row, c_resttest).Interior.ColorIndex = c_badpoint
    End If
    GetTTest = t
End Function

' Because excel screws this up a disturbing amount of the time!
Function GetStopRow(ByVal start_row As Integer)
    Dim i As Integer
    Dim s As String
    i = start_row
    s = Cells(i, 1).value
    Do
        i = i + 1
    Loop Until (s <> Cells(i, 1)) Or (i > ActiveSheet.UsedRange.Rows.count)
    GetStopRow = i - 1
End Function

' flag row in raw sheet
Function highlight_and_delete_row(arr As Range, color As Integer) As Boolean

```

```

Dim j As Integer
Dim name, roi As String
highlight_and_delete_row = False

name = arr.Cells(1, 1).value
roi = arr.Cells(1, 2).value
For j = 3 To Sheets("Raw").UsedRange.Rows.count
    If Sheets("Raw").Cells(j, 1).value = name And Sheets("Raw").Cells(j, 2).value = roi
Then
        Range(Sheets("Raw").Cells(j, 1), Sheets("Raw").Cells(j, 26)).Interior.ColorIndex
= color
        GoTo FOUND_IT
    End If
Next j
MsgBox arr.Address & " cannot be found in the raw sheet"
Exit Function
FOUND_IT:
arr.Rows(1).EntireRow.Delete
highlight_and_delete_row = True
End Function

```

```

Public Function MyDocsPath() As String

```

```

    MyDocsPath = Environ$("USERPROFILE") & "\\My Documents\"

```

```

End Function

```

```

Sub remove_row()

```

```

    If (ActiveSheet.name <> "Processed" And ActiveSheet.name <> "Binning") Or
Selection.Rows.count < 1 Then

```

```

        Exit Sub

```

```

    End If

```

```

    Dim currentUpdating As Boolean

```

```

    currentUpdating = Application.ScreenUpdating

```

```

    Application.ScreenUpdating = False

```

```

    Application.DisplayAlerts = False

```

```

    Dim color As Integer

```

```

    Dim cl As Range

```

```

    Dim i, first, last As Integer

```

```

    ' loop rows

```

```

    first = Selection.Row

```

```

    last = Selection.Row + Selection.Rows.count - 1

```

```

For i = first To last
' find color
  For Each cl In Cells(first, c_name).EntireRow.Cells
    If cl.Interior.ColorIndex > 0 Then
      color = cl.Interior.ColorIndex
      GoTo FOUND_COLOR
    End If
  Next cl
  color = c_badpoint
FOUND_COLOR:
  Call highlight_and_delete_row(Cells(first, c_name).EntireRow, color)
Next i

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = False
End Sub

```

```

Sub restore_row()
  If ActiveSheet.name <> "Raw" Or Selection.Rows.count < 1 Then
    Exit Sub
  End If
  ' find the sample in processed
  Dim j, first, last As Integer
  Dim name, roi As String
  Dim arr, src As Range
  Dim raw, processed As Worksheet
  Dim currentUpdating As Boolean

  currentUpdating = Application.ScreenUpdating
  Application.ScreenUpdating = False
  Application.DisplayAlerts = False

  Set raw = Sheets("Raw")
  Set processed = Sheets("Processed")

  Set src = Selection.Rows(1).EntireRow
  name = src.Cells(1, c_name).value
  roi = src.Cells(1, c_roi).value
  first = 0
  last = 0
  For j = 3 To processed.UsedRange.Rows.count
    If processed.Cells(j, c_name).value = name Then
      first = j
      GoTo FOUND_BEGINNING
    End If
  Next j

```

```

FOUND_BEGINNING:
  For j = first + 1 To processed.UsedRange.Rows.count
    If processed.Cells(j, c_name).value <> name Then
      last = j - 1
      GoTo FOUND_END
    End If
  Next j
FOUND_END:
  Set arr = Range(Cells(first, c_name), Cells(last, 26))
  ' insert row at end of sample in processed
  last = last + 1
  processed.Rows(last).EntireRow.Insert
  processed.Rows(last).EntireRow.value = src.value
  'processed.Range(processed.Cells(last, c_name), processed.Cells(last,
c_meanbkg)).Interior.ColorIndex = 40
  ' resort the sample
  Debug.Print "sorting " & first & " " & last
  With processed.Sort
    .SortFields.Clear
    .SortFields.Add Key:=Range(processed.Cells(first, c_z), processed.Cells(last, c_z)),
-
    SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
    .SetRange Range(processed.Cells(first, c_name), processed.Cells(last, c_meanbkg))
    .Header = xlNo
    .Orientation = xlTopToBottom
    .SortMethod = xlPinYin
    .Apply
  End With
  ' Plug in all the stats stuff
  Call Stat_Columns(first, last)
  Application.ScreenUpdating = currentUpdating
  Application.DisplayAlerts = True

  raw.Activate
End Sub

Sub Ribbon_Loaded(ribbon As IRibbonUI)
  ' put everything to do on startup here!
  Call DeleteCustomMenu
  Call BuildCustomMenu
End Sub

Sub Setup_Workbook()
  Dim currentUpdating As Boolean
  Dim i As Integer
  Dim s As Worksheet

```



```

Dim tmp As Workbook
Dim WSOBJ As CWorksheetObject

Set WSOBJ = New CWorksheetObject
Set WSColl = New Collection

currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

If Workbooks.count = 0 Then
    Set tmp = Workbooks.Add
    tmp.Title = "Analysis"
End If

Sheets.Add after:=Worksheets(Worksheets.count)
Sheets.Add after:=Worksheets(Worksheets.count)
Sheets.Add after:=Worksheets(Worksheets.count)
Sheets.Add after:=Worksheets(Worksheets.count)

For i = ActiveWorkbook.Worksheets.count - 4 To 1 Step -1
    Worksheets(i).Delete
Next i
Set s = Sheets(1)
s.name = "Raw"
Set s = Sheets(2)
s.name = "Processed"
Set WSOBJ.WS = s
WSColl.Add Item:=WSOBJ, Key:=s.name

Set s = Sheets(3)
s.name = "ASTM"
Set s = Sheets(4)
s.name = "Binning"

Application.DisplayAlerts = False
Application.ScreenUpdating = currentUpdating
End Sub

Sub UnSelectActiveCell()
    Dim Rng As Range
    Dim FullRange As Range

    If Selection.Cells.count > 1 Then
        For Each Rng In Selection.Cells
            If Rng.Address <> ActiveCell.Address Then

```

```

        If FullRange Is Nothing Then
            Set FullRange = Rng
        Else
            Set FullRange = Application.Union(FullRange, Rng)
        End If
    End If
Next Rng

If FullRange.Cells.count > 0 Then
    FullRange.Select
End If
End If

End Sub

```

## 2. *Pam\_Tools*

Option Explicit

```

Const c_name As Integer = 1
Const c_roi As Integer = 2
Const c_hot3x3 As Integer = 3
Const c_hotpixel As Integer = 4
Const c_multiple As Integer = 5
Const c_x As Integer = 6
Const c_y As Integer = 7
Const c_z As Integer = 8
Const c_mean As Integer = 9
Const c_meanstdev As Integer = 10
Const c_background As Integer = 11
Const c_backgroundstdev As Integer = 12
Const c_meanbkg As Integer = 13
Const c_intensityerror As Integer = 14
Const c_offset As Integer = 15
Const c_offsetstdev As Integer = 16
Const c_zmicrons As Integer = 17
Const c_zerror As Integer = 18
Const c_count As Integer = 19
Const c_rollingz As Integer = 20
Const c_rollingzstdev As Integer = 21
Const c_ttest As Integer = 22
Const c_smoothedz As Integer = 23
Const c_smoothedcount As Integer = 24
Const c_graph_zmicrons As Integer = 26
Const c_graph_meanbkg As Integer = 27

```

```

Const c_graph_rollingz As Integer = 28
Const c_avgz As Integer = 30
Const c_avgmeanbkg As Integer = 31
Const c_stdevz As Integer = 32
Const c_stdevmeanbkg As Integer = 33
Const c_minz As Integer = 34
Const c_maxz As Integer = 35

Public smite As Boolean

Sub smite_status(control As IRibbonControl, state As Boolean)
    smite = state
End Sub

Sub addToolBar(ByVal barName As String)
    Dim bar As CommandBar
    On Error Resume Next
    Set bar = Application.CommandBars(barName)
    If Not bar Is Nothing Then
        Application.CommandBars(barName).Delete
    End If

    Set bar = Application.CommandBars.Add(barName, Position:=msoBarFloating,
    Temporary:=True)
End Sub

Private Sub ThisAddIn_Shutdown(ByVal sender As Object, ByVal e As
System.EventArgs) Handles Me.Shutdown
    Application.CommandBars("Monte Carlo").Delete()

End Sub

' This is just a stub show I can pick icons easier
Sub Show_icons()
    Dim oToolbar As CommandBar
    Dim oButton As CommandBarButton
    Dim MyToolbar As String
    Dim i As Integer

    ' Give the toolbar a name
    MyToolbar = "Icon List"

    ' First, delete the toolbar if it already exists
    ' On Error Resume Next ' so that it doesn't stop on the next line if the toolbar's already
there

```

```

' Build the command bar
addToolBar (MyToolbar)
Set oToolbar = Application.CommandBars(MyToolbar)
'Set oToolbar = CommandBars.Add(Name:=MyToolbar, Position:=msoBarFloating,
Temporary:=True)
If Err.Number <> 0 Then ' Probably means the toolbar's already there, so we have
nothing to do
    Debug.Print Err.Number & " " & Err.Description
    Exit Sub
End If

On Error GoTo ErrorHandler

' loop adding buttons
For i = 1 To 255
    Set oButton = oToolbar.Controls.Add(Type:=msoControlButton)

    ' And set some of the button's properties
    With oButton
        .DescriptionText = "Merge a folder of CSVs into 1 sheet" 'Tooltip text when
mouse if placed over button
        .Caption = "" & i 'Text if Text in Icon is chosen
        .Style = msoButtonIcon ' Button displays as icon, not text or both
        .FaceId = i '52 is my favorite pig; chooses icon #52 from the available Office
icons
    End With

    Next i

oToolbar.Visible = True

NormalExit:
Exit Sub ' so it doesn't go on to run the errorhandler code

ErrorHandler:
'Just in case there is an error
Debug.Print Err.Number & vbCrLf & Err.Description
Resume NormalExit:

End Sub

' Merge csv and generate sheets for Pam
' from the Dark Lord of Information
'
'Sub Auto_Open()
' Dim oToolbar As CommandBar

```

```

' Dim oButton As CommandBarButton
' Dim MyToolbar As String

' Give the toolbar a name
' MyToolbar = "Pam Tools"

' First, delete the toolbar if it already exists
' On Error Resume Next ' so that it doesn't stop on the next line if the toolbar's already
there

' Build the command bar
' Build the command bar
' addToolBar (MyToolbar)
' Set oToolbar = Application.CommandBars(MyToolbar)
' If Err.Number <> 0 Then ' Probably means the toolbar's already there, so we have
nothing to do
'     Debug.Print Err.Number & " " & Err.Description
'     Exit Sub
' End If

' On Error GoTo ErrorHandler

' Now add a button to the new toolbar
' Set oButton = oToolbar.Controls.Add(Type:=msoControlButton)

' And set some of the button's properties
' With oButton
'     .DescriptionText = "Merge a folder of CSVs into 1 sheet" 'Tooltip text when
mouse is placed over button
'     .Caption = "Merge CSVs" 'Text if Text in Icon is chosen
'     .OnAction = "mergeCSVs" 'Runs the Sub Button1() code when clicked
'     .Style = msoButtonIcon ' Button displays as icon, not text or both
'     .FaceId = 23 '52 is my favorite pig; chooses icon #52 from the available Office
icons
' End With

' Now add a button to the new toolbar
' Set oButton = oToolbar.Controls.Add(Type:=msoControlButton)

' And set some of the button's properties
' With oButton
'     .DescriptionText = "Sort, remove maxxed, and compute common parameters"
'Tooltip text when mouse is placed over button
'     .Caption = "Prune" 'Text if Text in Icon is chosen
'     .OnAction = "prune" 'Runs the Sub Button1() code when clicked
'     .Style = msoButtonIcon ' Button displays as icon, not text or both

```

```

'     .FaceId = 108
' End With

' Now add a button to the new toolbar
' Set oButton = oToolbar.Controls.Add(Type:=msoControlButton)

' And set some of the button's properties
' With oButton
'     .DescriptionText = "Group beads according to depth" 'Tooltip text when mouse if
placed over button
'     .Caption = "Binning" 'Text if Text in Icon is chosen
'     .OnAction = "fruitcake" 'Runs the Sub Button1() code when clicked
'     .Style = msoButtonIcon ' Button displays as icon, not text or both
'     .FaceId = 107
' End With

' Set oButton = oToolbar.Controls.Add(Type:=msoControlButton)

' And set some of the button's properties
' With oButton
'     .DescriptionText = "Group beads according to depth" 'Tooltip text when mouse if
placed over button
'     .Caption = "Graphs" 'Text if Text in Icon is chosen
'     .OnAction = "graphs" 'Runs the Sub Button1() code when clicked
'     .Style = msoButtonIcon ' Button displays as icon, not text or both
'     .FaceId = 17
' End With

' You can set the toolbar position and visibility here if you like
' By default, it'll be visible when created
' oToolbar.Top = 150
' oToolbar.Left = 150
' oToolbar.Visible = True

NormalExit:
' Exit Sub ' so it doesn't go on to run the errorhandler code

ErrorHandler:
'Just in case there is an error
' MsgBox Err.Number & vbCrLf & Err.Description
' Resume NormalExit:
End Sub

Sub fruitcake(control As IRibbonControl)
    Dim free_col, i, j, k As Integer
    Dim processed As Worksheet

```

```
Set processed = Worksheets(2)
```

```
Dim currentUpdating As Boolean
```

```
currentUpdating = Application.ScreenUpdating
```

```
Application.ScreenUpdating = False
```

```
Application.DisplayAlerts = False
```

```
free_col = processed.UsedRange.Columns.count + 2
```

```
Cells(1, free_col).Select
```

```
ActiveCell.value = "binning"
```

```
Cells(2, free_col).Select
```

```
ActiveCell.value = "z (microns)"
```

```
Cells(2, free_col + 1).Select
```

```
ActiveCell.value = "z avg"
```

```
Cells(2, free_col + 2).Select
```

```
ActiveCell.value = "z stdev"
```

```
Cells(2, free_col + 3).Select
```

```
ActiveCell.value = "z error"
```

```
Cells(2, free_col + 4).Select
```

```
ActiveCell.value = "z error total"
```

```
Cells(2, free_col + 5).Select
```

```
ActiveCell.value = "intensity"
```

```
Cells(2, free_col + 6).Select
```

```
ActiveCell.value = "intensity stdev"
```

```
Cells(2, free_col + 7).Select
```

```
ActiveCell.value = "intensity error"
```

```
Cells(2, free_col + 8).Select
```

```
ActiveCell.value = "total intensity error"
```

```
Cells(2, free_col + 9).Select
```

```
ActiveCell.value = "count"
```

```
Dim start_row, stop_row, last_row As Integer
```

```
Dim low, high As Double
```

```
Dim arr As Range
```

```
start_row = 3
```

```
stop_row = processed.UsedRange.Rows.count
```

```
k = start_row
```

```
For j = 0 To 150 Step 5
```

```
    Cells(k, free_col).value = j
```

```
    If j = 0 Then
```

```
        low = -100
```

```
    Else
```

```
        low = j - 2.5
```

```
    End If
```

```

    If j = 150 Then
        high = 1000
    Else
        high = j + 2.5
    End If

    Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zmicrons))
    Cells(k, free_col + 1).Select
    ActiveCell.Formula = "=GetZAvg(" & arr.Address & "," & low & "," & high & ")"
    Cells(k, free_col + 2).Select
    ActiveCell.Formula = "=GetZStdev(" & arr.Address & "," & low & "," & high & ")"
    Cells(k, free_col + 3).Select
    Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zerror))
    ActiveCell.Formula = "=GetZError(" & arr.Address & "," & low & "," & high & ")"
    Cells(k, free_col + 4).Select
    ActiveCell.Formula = "=iferror(sqrt(V$" & k & "^2 + W$" & k & "^2)," & Chr(34)
& "undefinied" & Chr(34) & ")"
    Cells(k, free_col + 5).Select
    Set arr = ActiveSheet.Range(Cells(start_row, c_mean), Cells(stop_row,
c_zmicrons))
    ActiveCell.Formula = "=GetIntensity(" & arr.Address & "," & low & "," & high &
")"
    Cells(k, free_col + 6).Select
    ActiveCell.Formula = "=GetIntensityStdev(" & arr.Address & "," & low & "," &
high & ")"
    Cells(k, free_col + 7).Select
    Set arr = ActiveSheet.Range(Cells(start_row, c_intensityerror), Cells(stop_row,
c_zmicrons))
    ActiveCell.Formula = "=GetIntensityError(" & arr.Address & "," & low & "," &
high & ")"
    Cells(k, free_col + 8).Select
    ActiveCell.Formula = "=iferror(sqrt(Z$" & k & "^2 + AA$" & k & "^2)," & Chr(34)
& "undefinied" & Chr(34) & ")"
    Cells(k, free_col + 9).Select
    Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zmicrons))
    ActiveCell.Formula = "=GetCount(" & arr.Address & "," & low & "," & high & ")"
    k = k + 1
Next j

Application.ScreenUpdating = False
Application.DisplayAlerts = currentUpdating
End Sub

```



```

Sub graph(control As IRibbonControl)
    Dim arr As Range
    Dim dst, xaxis, meanbkg As Range
    Dim current, i, start_row, stop_row As Long
    Dim zlimit As Double
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    'Application.EnableEvents = False

    'copy
    current = 3
    stop_row = ActiveSheet.UsedRange.Rows.count
    For i = 3 To stop_row
        If (Cells(i, c_ttest).Interior.ColorIndex < 1 Or Cells(i, c_ttest).Interior.ColorIndex =
c_dontgraph) Then
            Cells(current, c_graph_zmicrons).value = Cells(i, c_zmicrons).value
            Cells(current, c_graph_meanbkg).value = Cells(i, c_meanbkg).value
            Cells(current, c_graph_rollingz).value = Cells(i, c_smoothedz).value
            current = current + 1
        End If
    Next i
    Set arr = Range(Cells(3, c_zmicrons), Cells(stop_row, c_zmicrons))
    Set dst = Range(Cells(3, c_graph_zmicrons), Cells(stop_row, c_graph_zmicrons))
    'dst.value = arr.value
    Set xaxis = dst
    Set arr = Range(Cells(3, c_meanbkg), Cells(stop_row, c_meanbkg))
    Set dst = Range(Cells(3, c_graph_meanbkg), Cells(stop_row, c_graph_meanbkg))
    'dst.value = arr.value
    Set meanbkg = dst
    Set arr = Range(Cells(3, c_smoothedz), Cells(stop_row, c_smoothedz))
    Set dst = Range(Cells(3, c_graph_rollingz), Cells(stop_row, c_graph_rollingz))
    'dst.value = arr.value
    stop_row = current

    'sort
    With ActiveSheet.Sort
        .SortFields.Clear
        .SortFields.Add Key:=Range(Cells(3, c_graph_zmicrons), Cells(stop_row,
c_graph_zmicrons)), _
        SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
        .SetRange Range(Cells(3, c_graph_zmicrons), Cells(stop_row, c_graph_rollingz))
        .Header = xlNo
        .Orientation = xlTopToBottom
    End With
End Sub

```

```

        .SortMethod = xlPinYin
        .Apply
    End With

    ' find start_row based on Z criteria!
    start_row = 3
    ' idiot check
    If Not IsNumeric(Cells(1, c_stdevmeanbkg).value) Or IsEmpty(Cells(1,
c_stdevmeanbkg).value) Then
        MsgBox "Error: Graph from Z must be a number!"
        Exit Sub
    End If
    zlimit = Cells(1, c_stdevmeanbkg).value
    For start_row = 3 To stop_row
        If Cells(start_row, c_graph_zmicrons).value >= zlimit Then
            Exit For
        End If
    Next start_row

    'generate extra averaged stuff
    Debug.Print "Start row " & start_row
    Set arr = Range(Cells(start_row, c_graph_rollingz), Cells(stop_row,
c_graph_rollingz))
    Call BinZ(arr)

    'graph

    Dim CHObj As MyChartObject

    Set CHObj = New MyChartObject
    Set CHColl = New Collection

    Range(Cells(start_row, c_graph_zmicrons), Cells(stop_row, 28)).Activate
    ActiveSheet.Shapes.AddChart(Excel.XlChartType.xlXYScatter).Select
    Set CHObj.CO = ActiveChart
    Debug.Print ActiveChart.name
    CHColl.Add Item:=CHObj, Key:=ActiveChart.name

    Set xaxis = Range(Cells(start_row, c_graph_zmicrons), Cells(stop_row,
c_graph_zmicrons))
    Set meanbkg = Range(Cells(start_row, c_graph_meanbkg), Cells(stop_row,
c_graph_meanbkg))
    Set dst = Range(Cells(start_row, c_graph_rollingz), Cells(stop_row,
c_graph_rollingz))

    'ActiveChart.SeriesCollection.NewSeries

```

```

ActiveChart.SeriesCollection(1).name = ""mean-background""
ActiveChart.SeriesCollection(1).XValues = xaxis
ActiveChart.SeriesCollection(1).Values = meanbkg
'ActiveChart.SeriesCollection.NewSeries
ActiveChart.SeriesCollection(2).name = ""smoothed Z""
ActiveChart.SeriesCollection(2).XValues = xaxis
ActiveChart.SeriesCollection(2).Values = dst

ActiveChart.SeriesCollection(1).Select
With Selection
    .MarkerStyle = xlMarkerStyleDiamond
    .MarkerSize = 2
End With
ActiveChart.SeriesCollection(2).Select
With Selection
    .MarkerStyle = 1
    .MarkerSize = 2
End With
ActiveChart.Axes(xlCategory).MinimumScale = 0
Dim offset As Integer
offset = ActiveChart.Parent.Top + ActiveChart.Parent.Height + 50

' chart 2.0
Set CHObj = New MyChartObject
Set CHColl = New Collection

Range(Cells(start_row, c_graph_zmicrons), Cells(stop_row,
c_graph_rollingz)).Activate
ActiveSheet.Shapes.AddChart(Excel.XlChartType.xlXYScatter).Select
Set CHObj.CO = ActiveChart
Debug.Print ActiveChart.name
CHColl.Add Item:=CHObj, Key:=ActiveChart.name

ActiveChart.SeriesCollection(1).name = ""mean-background""
ActiveChart.SeriesCollection(1).XValues = xaxis
ActiveChart.SeriesCollection(1).Values = meanbkg

Set xaxis = Range(Cells(3, c_avgz), Cells(Range(Cells(65536,
c_avgz).Address).End(xlUp).Row, c_avgz))
Set dst = Range(Cells(3, c_avgmeanbkg), Cells(Range(Cells(65536,
c_avgmeanbkg).Address).End(xlUp).Row, c_avgmeanbkg))
ActiveChart.SeriesCollection(2).name = ""Averaged Z""
ActiveChart.SeriesCollection(2).XValues = xaxis
ActiveChart.SeriesCollection(2).Values = dst

ActiveChart.SeriesCollection(1).Select

```

```

With Selection
    .MarkerStyle = xlMarkerStyleDiamond
    .MarkerSize = 2
End With
ActiveChart.SeriesCollection(2).Select
With Selection
    .MarkerStyle = 1
    .MarkerSize = 2
End With
ActiveChart.Axes(xlCategory).MinimumScale = 0
ActiveChart.Parent.Top = offset

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
Application.EnableEvents = False
End Sub

Sub highlight_outliers_4095()
    Dim raw As Worksheet
    Dim rw As Range
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    Set raw = Worksheets(1)
    For Each rw In raw.UsedRange.Rows
        If Cells(rw.Row, 3).value >= 4095 And IsNumeric(Cells(rw.Row, 3).value) Then
            rw.EntireRow.Interior.ColorIndex = c_saturated
        End If
    Next rw

    Application.ScreenUpdating = currentUpdating
    Application.DisplayAlerts = True
End Sub

Sub MergeCSVs(control As IRibbonControl)
    On Error GoTo SMACK_PAM
    Dim planes, radius As Integer
    Dim currentUpdating As Boolean
    Dim folderName As Variant
    Dim cell_to_paste_next_dataset As Range
    Dim active_workbook, dataset_workbook As Workbook
    Dim active_sheet As Worksheet
    planes = 0

```

```

radius = 0

'Get folder
Dim fd As FileDialog
Set fd = Application.FileDialog(msoFileDialogFolderPicker)
With fd
    If .Show = -1 Then
        folderName = .SelectedItems.Item(1)
    Else
        Exit Sub
    End If
End With
Set fd = Nothing

Call Setup_Workbook

'Lists all the files in the current directory
Set cell_to_paste_next_dataset = Cells(1, 1)
Set active_workbook = ActiveWorkbook
Set active_sheet = Sheets("Raw")

Dim fool As String
currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

Debug.Print (folderName & "*.csv")
fool = Dir(folderName & "\\*.csv")
Dim paste_row As Integer
paste_row = 1 ' so I don't skip the first row...
Do While fool <> vbNullString
    Debug.Print fool
    If active_workbook.name <> fool And fool <> "" Then
        Workbooks.Open Filename:=folderName & "\" & fool
        Set dataset_workbook = ActiveWorkbook
        ' valid same parameters before adding!
        If (planes <> 0) Then
            If planes <> Cells(1, 2).value Or radius <> Cells(1, 4).value Then
                MsgBox ("File " & fool & " has different processing parameters. Ignoring!")
                fool = Dir
                GoTo OOPS
            End If
        Else
            planes = Cells(1, 2).value
            radius = Cells(1, 4).value
        End If
    End If

```

```

Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
active_sheet.Activate
Cells(paste_row, 1).Select
ActiveSheet.Paste
dataset_workbook.Close
paste_row = ActiveCell.SpecialCells(xlLastCell).Row + 1
End If
OOPS:
fool = Dir
Loop
' bring in T test chart!
Set active_sheet = Sheets("ASTM")
Debug.Print MyDocsPath & "astm.xlsx"
Workbooks.Open Filename:=MyDocsPath & "astm.xlsx"
Set dataset_workbook = ActiveWorkbook
Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
active_sheet.Activate
Cells(1, 1).Select
ActiveSheet.Paste
dataset_workbook.Close
paste_row = ActiveCell.SpecialCells(xlLastCell).Row + 1
Sheets("Raw").Activate

Call highlight_outliers_4095
Debug.Print planes & " " & radius
Application.DisplayAlerts = True
Application.ScreenUpdating = currentUpdating
Call UnSelectActiveCell
Exit Sub
SMACK_PAM:
MsgBox "Put the astm.xlsx file in your My Documents folder!"
End Sub

Sub process_merged(control As IRibbonControl)
Dim currentUpdating As Boolean
Dim source, processing As Worksheet
Dim i As Integer

Set source = Worksheets(1)
Set processing = Worksheets(2)

currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

source.Activate

```

```

Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
processing.Activate
Cells(1, 1).Select
ActiveSheet.Paste

i = 3
' remove dupe captions
Do
    If Cells(i, 1).value Like "planes" Or Cells(i, 1).value Like "image name" Then
        processing.Rows(i).EntireRow.Delete
    Else
        i = i + 1
    End If
Loop Until (i > processing.UsedRange.Rows.count Or IsEmpty(Cells(i, 1).value))
i = 3
' remove pegged rows
Do
    If Cells(i, 3).value >= 4095 Then
        processing.Rows(i).EntireRow.Delete
    Else
        i = i + 1
    End If
Loop Until i > processing.UsedRange.Rows.count

' assign sort column
' hint_col = processing.UsedRange.Columns.count + 2
' Cells(3, hint_col).Select
' ActiveCell.Formula = "=GetElement(B3,1,""-")"
' ActiveCell.FormulaR1C1 = "=GetElement(RC[-13],3,""-")"
' ActiveCell.AutoFill Range(ActiveCell, Cells(processing.UsedRange.Rows.count,
ActiveCell.Column))

' sort ranges
Dim start_row, stop_row As Integer
i = 3
Do
    start_row = i
    stop_row = GetStopRow(start_row)
    i = stop_row + 1

    Debug.Print start_row & " " & stop_row
    With processing.Sort
        .SortFields.Clear
        .SortFields.Add Key:=Range(Cells(start_row, c_z), Cells(stop_row, c_z)), _
SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
    End With

```

```

        .SetRange Range(Cells(start_row, 1), Cells(stop_row, c_meanbkg))
        .Header = xlNo
        .Orientation = xlTopToBottom
        .SortMethod = xlPinYin
        .Apply
    End With
Loop Until i > processing.UsedRange.Rows.count

'processing.Columns(hint_col).EntireColumn.Delete
processing.Activate
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True

Call Stat_Columns(3, processing.UsedRange.Rows.count)
Call UnSelectActiveCell
End Sub

Sub Label_Columns()
    Cells(2, c_intensityerror).value = "intensity error"
    Cells(2, c_offset).value = "offset"
    Cells(2, c_offsetstdev).value = "offset stdev"
    Cells(2, c_zmicrons).value = "z (microns)"
    Cells(2, c_zerror).value = "z error"
    Cells(2, c_count).value = "count"
    Cells(2, c_rollingz).value = "Rolling Z"
    Cells(2, c_rollingzstdev).value = "Rolling Z Stdev"
    Cells(2, c_ttest).value = "T Test"
    Cells(2, c_smoothedz).value = "Smoothed Z"
    Cells(2, c_smoothedcount).value = "Smoothed Count"
    Cells(1, c_ttest).value = "Fudge"
    Cells(1, c_smoothedz).Select
    If (IsEmpty(ActiveCell.value)) Then ActiveCell.value = 5

    Cells(2, c_graph_zmicrons).Select
    ActiveCell.value = "z (microns)"
    Cells(2, c_graph_meanbkg).Select
    ActiveCell.value = "mean-background"
    Cells(2, c_graph_rollingz).Select
    ActiveCell.value = "Rolling Z"

    Cells(1, c_avgz).value = "# beads"
    Cells(1, c_avgmeanbkg).Select
    If (IsEmpty(ActiveCell.value)) Then ActiveCell.value = 20
    Cells(2, c_avgz).value = "Average Z"
    Cells(2, c_avgmeanbkg).value = "Average mean-background"
    Cells(1, c_stdevz).value = "Graph from Z"

```



```

Cells(2, c_stdevz).value = "Stdev Z"
Cells(1, c_stdevmeanbkg).Select
If (IsEmpty(ActiveCell.value)) Then ActiveCell.value = 0.4
Cells(2, c_stdevmeanbkg).value = "Stdev mean-background"
Cells(2, c_minz).value = "Min Z"
Cells(2, c_maxz).value = "Max Z"
End Sub

Sub Stat_Columns(ByVal first As Integer, ByVal last As Integer)
    Dim processed As Worksheet
    Dim currentUpdating As Boolean
    Dim start_row, stop_row, i As Integer
    Dim arr As Range

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    Application.EnableEvents = False

    Set processed = Worksheets(2)
    processed.Activate
    'Debug.Print processed.UsedRange.Columns.count & "," &
processed.UsedRange.Rows.count
    'free_col = processed.UsedRange.Columns.count + 1
    Call Label_Columns
    'Cells(2, c_intensityerror).value = "intensity error"
    Cells(3, c_intensityerror).Select
    ActiveCell.Formula = "=sqrt(J3^2+L3^2)"
    ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

    'free_col = processed.UsedRange.Columns.count + 1
    'Cells(2, c_offset).Select
    'ActiveCell.value = "offset"
    'Cells(2, c_offsetstdev).Select
    'ActiveCell.value = "offset stdev"
    i = first
    Do
        start_row = i
        stop_row = GetStopRow(start_row)
        i = stop_row + 1

        Cells(start_row, c_offset).Select
        ActiveCell.Formula = "=GetOffset(" & Range(Cells(start_row, c_z),
Cells(stop_row, c_z)).Address & ")"
        ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))
    
```

```

Cells(start_row, c_offsetstdev).Select
ActiveCell.Formula = "=GetOffsetStdev( " & Range(Cells(start_row, c_z),
Cells(stop_row, c_z)).Address & _
", " & Cells(start_row, c_offset).Address(False, True) & ")"
ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))

```

Loop Until i > last

```

'Cells(2, c_zmicrons).value = "z (microns)"
Cells(3, c_zmicrons).Select
ActiveCell.Formula = "=0.1 * (h3-o3)"
ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

```

```

'Cells(2, c_zerror).value = "z error"
Cells(3, c_zerror).Select
ActiveCell.Formula = "=sqrt(0.1^2*(1^2 + (P3)^2 + 1^2) + (H3-O3)^2 * 0.001^2)"
ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

```

```

Set arr = Range(Cells(3, c_zmicrons), Cells(processed.UsedRange.Rows.count,
c_zmicrons))
'Cells(2, c_count).value = "count"
'Cells(3, c_count).Select
'ActiveCell.Formula = "=GetBinCount(" + arr.Address + "," + Cells(3,
c_zmicrons).Address(False, True) + "-" + _
'Cells(3, c_zerror).Address(False, True) + "," + Cells(3, c_zmicrons).Address(False,
True) + "+" + Cells(3, c_zerror).Address(False, True) + ")"
'ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

```

```

'Cells(2, c_rollingz).value = "Rolling Z"
'Cells(3, c_rollingz).Select
'ActiveCell.Formula = "=GetRollingZ(" + arr.Address + "," + Cells(3,
c_zmicrons).Address(False, True) + "-" + _
'Cells(3, c_zerror).Address(False, True) + "," + Cells(3, c_zmicrons).Address(False,
True) + "+" + Cells(3, c_zerror).Address(False, True) + ")"
'ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

```

```

'Cells(2, c_rollingzstdev).value = "Rolling Z Stdev"
'Cells(3, c_rollingzstdev).Select
'ActiveCell.Formula = "=GetRollingZstdev(" + arr.Address + "," + Cells(3,
c_zmicrons).Address(False, True) + "," + Cells(3, c_zmicrons).Address(False, True) + "-
" + _

```

```

'Cells(3, c_zerror).Address(False, True) + "," + Cells(3, c_zmicrons).Address(False,
True) + "+" + Cells(3, c_zerror).Address(False, True) + ")"
'ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

```

```

'Cells(2, c_ttest).value = "T Test"
'Cells(2, c_smoothedz).value = "Smoothed Z"
'Cells(2, c_smoothedcount).value = "Smoothed Count"
'Cells(1, c_ttest).value = "Fudge"
'Cells(1, c_smoothedz).value = 5

```

```

'Cells(2, c_graph_zmicrons).Select
'ActiveCell.value = "z (microns)"
'Cells(2, c_graph_meanbkg).Select
'ActiveCell.value = "mean-background"
'Cells(2, c_graph_rollingz).Select
'ActiveCell.value = "Rolling Z"

```

```

'Cells(1, c_avgz).value = "# beads"
'Cells(1, c_avgmeanbkg).Select
'If (IsEmpty(ActiveCell.value)) Then ActiveCell.value = 10
'Cells(2, c_avgz).value = "Average Z"
'Cells(2, c_avgmeanbkg).value = "Average mean-background"
'Cells(1, c_stdevz).value = "Graph from Z"
'Cells(2, c_stdevz).value = "Stdev Z"
'Cells(1, c_stdevmeanbkg).Select
'If (IsEmpty(ActiveCell.value)) Then ActiveCell.value = 0
'Cells(2, c_stdevmeanbkg).value = "Stdev mean-background"
'Cells(2, c_minz).value = "Min Z"
'Cells(2, c_maxz).value = "Max Z"

```

```

' explicitly update t test the first time
Call t_test

```

```

Application.EnableEvents = True
Application.DisplayAlerts = True
Application.ScreenUpdating = currentUpdating
End Sub

```

```

Function GetElement(text As Variant, n As Integer, _
    delimiter As String) As String
    GetElement = Val(Split(text, delimiter)(n - 1))
End Function

```

```

Function GetOffset(arr As Range)
    Dim i, count As Long

```

```

Dim total As Double
Dim rw As Range
Dim foo() As Integer
Dim currentUpdating As Boolean
currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

ReDim foo(arr.count)
' pull array
i = 1
For Each rw In arr
    foo(i) = rw.Cells(1, 1).value
    'Debug.Print "foo(i) " & foo(i)
    i = i + 1
Next rw
' sort array
Dim done As Boolean
Dim swap As Integer
Do
    done = True
    For i = 1 To arr.count - 1
        If foo(i) > foo(i + 1) Then
            swap = foo(i)
            foo(i) = foo(i + 1)
            foo(i + 1) = swap
            done = False
        End If
    Next i
Loop Until done = True
' average of top 6 slices
total = 0
count = 0
'Debug.Print "start " & foo(1)
For i = 1 To arr.count
    If foo(1) + 6 > foo(i) Then
        'Debug.Print foo(i)
        total = total + foo(i)
        count = count + 1
    End If
Next i
'Debug.Print "foo " & total & " " & count
GetOffset = total / count
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

```

```

Function GetOffsetStdev(arr As Range, mean As Double)
    Dim i, count As Long
    Dim total As Double
    Dim rw As Range
    Dim foo() As Integer
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    ReDim foo(arr.count)
    ' pull array
    i = 1
    For Each rw In arr
        foo(i) = rw.Cells(1, 1).value
        i = i + 1
    Next rw
    ' sort array
    Dim done As Boolean
    Dim swap As Integer
    Do
        done = True
        For i = 1 To arr.count - 1
            If foo(i) > foo(i + 1) Then
                swap = foo(i)
                foo(i) = foo(i + 1)
                foo(i + 1) = swap
                done = False
            End If
        Next i
    Loop Until done = True
    ' average of top 6 slices
    total = 0
    count = 0
    'Debug.Print "start " & foo(1)
    For i = 1 To arr.count
        If foo(1) + 6 > foo(i) Then
            'Debug.Print foo(i)
            total = total + ((mean - foo(i)) ^ 2)
            count = count + 1
        End If
    Next i
    If count < 2 Then
        GetOffsetStdev = "undefined"
    End If
End Function

```

```

    Exit Function
End If
'Debug.Print "foo " & total & " " & count
GetOffsetStdev = Sqr(total / count)
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

```

```

Function GetZStdev(arr As Range, low As Double, high As Double)

```

```

    Dim i, count As Integer
    Dim total As Double
    Dim rw As Range
    Dim foo() As Double
    Dim currentUpdating As Boolean

```

```

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

```

```

    ReDim foo(arr.count)

```

```

    ' pull array

```

```

    i = 1

```

```

    For Each rw In arr

```

```

        foo(i) = rw.Cells(1, 1).value

```

```

        i = i + 1

```

```

    Next rw

```

```

    ' average of slices in range

```

```

    total = 0

```

```

    count = 0

```

```

    Dim mean As Double

```

```

    For i = 1 To arr.count

```

```

        If foo(i) >= low And foo(i) <= high Then

```

```

            'Debug.Print foo(i)

```

```

            total = total + foo(i)

```

```

            count = count + 1

```

```

        End If

```

```

    Next i

```

```

    If count < 2 Then

```

```

        GetZStdev = "undefined"

```

```

        Exit Function

```

```

    End If

```

```

    mean = total / count

```

```

    total = 0

```

```

    count = 0

```

```

    For i = 1 To arr.count

```

```

    If foo(i) >= low And foo(i) < high Then
        'Debug.Print foo(i)
        total = total + ((foo(i) - mean) ^ 2)
        count = count + 1
    End If
Next i
'Debug.Print "foo " & total & " " & count
GetZStdev = Sqr(total / (count - 1))
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

Function GetZError(arr As Range, low As Double, high As Double)
    Dim count As Integer
    Dim total As Double
    Dim rw As Range

    Dim foo() As Double
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    ReDim foo(arr.count)
    total = 0
    count = 0
    ' pull array
    For Each rw In arr
        If rw.Cells(1, 1).value >= low And rw.Cells(1, 1).value < high Then
            If total < rw.Cells(1, 2).value Then
                total = rw.Cells(1, 2).value
                count = count + 1
            End If
        End If
    Next rw

    If count < 2 Then
        GetZError = "undefined"
    Else
        GetZError = total
    End If
    Application.ScreenUpdating = currentUpdating
    Application.DisplayAlerts = True
End Function

```

```

Function GetIntensity(arr As Range, low As Double, high As Double)
    Dim count, i As Integer
    Dim total As Double
    Dim rw As Range
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    ' pull array
    total = 0
    count = 0
    ' average of slices in range
    Debug.Print Cells(3, c_zmicrons)
    For i = arr.Row To arr.Row + arr.Rows.count - 1
        If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
            total = total + Cells(i, c_mean).value - Cells(i, c_background).value
            count = count + 1
        End If
    Next i
    If count < 1 Then
        GetIntensity = "undefined"
    Else
        GetIntensity = total / count
    End If
    Application.ScreenUpdating = currentUpdating
    Application.DisplayAlerts = True
End Function

```

```

Function GetIntensityStdev(arr As Range, low As Double, high As Double)
    Dim count As Integer
    Dim total, mean As Double
    Dim rw As Range
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    ' pull array
    total = 0
    count = 0
    ' mean of slices in range
    Dim i As Integer
    For i = arr.Row To arr.Row + arr.Rows.count - 1
        If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
            total = total + Cells(i, c_mean).value - Cells(i, c_background).value

```



```

        count = count + 1
    End If
Next i
If count < 2 Then
    GetIntensityStdev = "undefined"
    Exit Function
End If
mean = total / count
'stdev
total = 0
For i = arr.Row To arr.Row + arr.Rows.count - 1
    If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
        total = total + ((Cells(i, c_mean).value - Cells(i, c_background).value) - mean) ^ 2
    End If
Next i

GetIntensityStdev = Sqr(total / (count - 1))
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

Function GetIntensityError(arr As Range, low As Double, high As Double)
    Dim count As Integer
    Dim total As Double
    Dim rw As Range
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    ' pull array
    total = 0
    count = 0
    ' mean of slices in range
    Dim i As Integer
    For i = arr.Row To arr.Row + arr.Rows.count - 1
        If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
            total = total + Cells(i, c_intensityerror).value ^ 2
            count = count + 1
        End If
    Next i
    If count < 2 Then
        GetIntensityError = "undefined"
    Else
        GetIntensityError = Sqr(total) / count
    End If
End Function

```

```

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Function

```

```

Function GetCount(arr As Range, low As Double, high As Double)
    Dim foo() As Double
    Dim i As Integer
    Dim rw As Range

    ReDim foo(arr.count)
    ' pull array
    i = 1
    For Each rw In arr
        foo(i) = rw.Cells(1, 1).value
        i = i + 1
    Next rw
    GetCount = 0
    For i = 1 To arr.count
        If foo(i) >= low And foo(i) < high Then
            GetCount = GetCount + 1
        End If
    Next i
End Function

```

```

Function GetZAvg(arr As Range, low As Double, high As Double)
    Dim foo() As Double
    Dim count As Integer
    Dim total As Double
    Dim rw As Range

    Debug.Print "range " & arr.Address

    ReDim foo(arr.count)
    ' pull array
    For Each rw In arr
        If rw.Cells(1, 1).value >= low And rw.Cells(1, 1).value < high Then
            total = total + rw.Cells(1, 1)
            count = count + 1
        End If
    Next rw
    If count < 1 Then
        GetZAvg = "undefined"
    Else
        GetZAvg = total / count
    End If
End Function

```

```

Function GetBinCount(arr As Range, low As Double, high As Double)
    Dim rw As Range
    Dim count As Integer
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    count = 0
    ' count points
    For Each rw In arr
        If rw.Cells(1, 1).value >= low And rw.Cells(1, 1).value < high Then
            count = count + 1
        End If
    Next rw
    GetBinCount = count
    Application.ScreenUpdating = currentUpdating
    Application.DisplayAlerts = True
End Function

```

```

Sub BetterRollingZ(arr As Range, ByVal rw As Long)
    Dim i As Integer
    Dim count As Integer
    Dim bins() As Double
    Dim low, high, fudge, tmp As Double
    Dim total, rollingZ, rollingZStdev, smoothedz, t As Double
    ReDim bins(arr.Rows.count)
    If Cells(rw, c_zmicrons).Interior.ColorIndex > 0 Then
        Exit Sub
    End If
    fudge = Cells(1, c_smoothedz)
    low = Cells(rw, c_zmicrons).value - Cells(rw, c_zerror).value
    high = Cells(rw, c_zmicrons).value + Cells(rw, c_zerror).value
    rollingZ = 0
    rollingZStdev = 0
    count = 0
    t = 0
    ' count points
    For i = arr.Row To arr.Row + arr.Rows.count - 1
        tmp = Cells(i, c_zmicrons).value
        If tmp >= low And tmp < high Then
            count = count + 1
            bins(count) = Cells(i, c_meanbkg).value
        End If
    Next i

```

```

Next i

' average points
If count > 0 Then
    total = 0
    For i = 1 To count
        total = total + bins(i)
    Next i
    rollingZ = total / count
End If
' stdev
If count > 1 Then
    total = 0
    For i = 1 To count
        total = total + (bins(i) - rollingZ) ^ 2
    Next i
    rollingZStdev = Sqr(total / (count - 1))
    If rollingZStdev <> 0 Then
        ' t test
        t = Abs(Cells(rw, c_meanbkg).value - rollingZ) / rollingZStdev
        If count < 3 Then
            Cells(rw, c_ttest).Interior.ColorIndex = c_dontgraph
        ElseIf count > 147 And t >= Sheets("ASTM").Cells(Application.Min(count, 147)
- 1, 3).value Then
            Cells(rw, c_ttest).Interior.ColorIndex = c_pamdecide
        ElseIf t >= Sheets("ASTM").Cells(Application.Min(count, 147) - 1, 3).value Then
            Cells(rw, c_ttest).Interior.ColorIndex = c_badpoint
        Else
            Cells(rw, c_ttest).Interior.ColorIndex = 0
        End If
    Else
        Cells(rw, c_ttest).Interior.ColorIndex = c_badpoint
    End If
End If
Cells(rw, c_count).value = count
Cells(rw, c_rollingz).value = rollingZ
Cells(rw, c_rollingzstdev).value = rollingZStdev
Cells(rw, c_ttest).value = t
If count < 2 Then
    Cells(rw, c_ttest).Interior.ColorIndex = c_dontgraph
End If
count = 0
low = Cells(rw, c_zmicrons).value - (fudge + Cells(rw, c_zerror).value)
high = Cells(rw, c_zmicrons).value + (fudge + Cells(rw, c_zerror).value)
' count points
For i = arr.Row To arr.Row + arr.Rows.count - 1

```

```

    tmp = Cells(i, c_zmicrons).value
    If tmp >= low And tmp < high Then
        count = count + 1
        bins(count) = Cells(i, c_meanbkg).value
    End If
Next i
' average points
If count > 0 Then
    total = 0
    For i = 1 To count
        total = total + bins(i)
    Next i
    smoothedz = total / count
End If
Cells(rw, c_smoothedz).value = smoothedz
Cells(rw, c_smoothedcount).value = count
End Sub

Sub BinZ(arr As Range)
    Dim binsize, i, j, count As Integer
    Dim avgz, avgmbkg, maxz, minz, stdevz, stdevmbkg, totalz, totalmbkg As Double
    Dim kill As Range

    count = 3
    binsize = Cells(1, c_avgmeanbkg).value
    ' idiot check
    If binsize < 1 Or IsEmpty(Cells(1, c_avgmeanbkg).value) Then
        MsgBox "Error: Number of beads must be greater than 0"
        Exit Sub
    End If

    ' kill it with fire!
    Set kill = Range(Cells(3, c_avgz), Cells(65536, c_maxz))
    kill.ClearContents

    For i = arr.Row To arr.Row + arr.Rows.count - 1 Step binsize
        ' determine we have enough points
        For j = 0 To binsize - 1
            If IsEmpty(Cells(i + j, c_graph_zmicrons)) Then
                Exit Sub
            End If
        Next j
        ' find averages
        avgz = 0
        avgmbkg = 0
        totalz = 0

```

```

totalmbkg = 0
maxz = -999999
minz = 999999
For j = 0 To binsize - 1
    totalz = totalz + Cells(i + j, c_graph_zmicrons).value
    totalmbkg = totalmbkg + Cells(i + j, c_graph_meanbkg).value
    If Cells(i + j, c_graph_zmicrons).value > maxz Then
        maxz = Cells(i + j, c_graph_zmicrons).value
    End If
    If Cells(i + j, c_graph_zmicrons).value < minz Then
        minz = Cells(i + j, c_graph_zmicrons).value
    End If
Next j
avgz = totalz / binsize
avgmbkg = totalmbkg / binsize
stdevz = 0
stdevmbkg = 0
totalz = 0
totalmbkg = 0
If binsize > 1 Then
    For j = 0 To binsize - 1
        totalz = totalz + (Cells(i + j, c_graph_zmicrons).value - avgz) ^ 2
        totalmbkg = totalmbkg + (Cells(i + j, c_graph_meanbkg).value - avgmbkg) ^ 2
    Next j
    stdevz = Sqr(totalz / (binsize - 1))
    stdevmbkg = Sqr(totalmbkg / (binsize - 1))
End If
'report
Cells(count, c_avgz).value = avgz
Cells(count, c_avgmeanbkg).value = avgmbkg
Cells(count, c_stdevz).value = stdevz
Cells(count, c_stdevmeanbkg).value = stdevmbkg
Cells(count, c_minz).value = minz
Cells(count, c_maxz).value = maxz
count = count + 1
Next i
End Sub

Sub prune_t_outliers(control As IRibbonControl)
    Dim i, j As Long
    Dim value As Double
    Dim foo As Double
    Dim ulimit As Double
    Dim arr As Range
    Dim currentUpdating As Boolean

```

```

currentUpdating = Application.ScreenUpdating
Application.EnableEvents = False
Application.ScreenUpdating = False
Application.DisplayAlerts = False
For i = 3 To ActiveSheet.UsedRange.Rows.count
    If Cells(i, c_ttest).Interior.ColorIndex = c_badpoint Then
        Set arr = Range(Cells(i, c_name), Cells(i, 26))
        ' flag row in raw sheet
        Dim name, roi As String
        name = Cells(i, c_name).value
        roi = Cells(i, c_roi).value
        For j = 3 To Sheets("Raw").UsedRange.Rows.count
            ' If Sheets("Raw").Cells(j, c_name).value = name And Sheets("Raw").Cells(j,
c_roi).value = roi Then
                Range(Sheets("Raw").Cells(j, 1), Sheets("Raw").Cells(j,
26)).Interior.ColorIndex = 6
                GoTo KEEP_SEARCHING
            ' End If
        Next j
    'KEEP_SEARCHING:
        Range(Cells(i, 1), Cells(i, 2)).Rows(1).EntireRow.Delete
        ' don't decrement row if we fail to delete, otherwise infinite loop
        If highlight_and_delete_row(arr, c_badpoint) Then
            i = i - 1
        End If
    End If
Next i

' explicitly update t test the first time
Call t_test

Application.EnableEvents = True
Application.DisplayAlerts = True
Application.ScreenUpdating = currentUpdating
End Sub

Sub test()
    Dim foo As Integer
    foo = Application.Min(4, 5)
    Debug.Print foo
End Sub

Sub t_test()
    Dim arr As Range
    Dim i As Integer

```

```

Set arr = Range(Cells(3, c_zmicrons),
Cells(Sheets("Processed").UsedRange.Rows.count, c_zmicrons))

' flag any fails before going on
Dim cl As Range
For Each cl In Range(Cells(3, c_name), Cells(arr.Row + arr.Rows.count - 1,
c_ttest)).Cells
    If CStr(cl.value) = "undefined" Then
        cl.EntireRow.Interior.ColorIndex = c_badpoint
    End If
Next cl

For i = 3 To arr.Row + arr.Rows.count - 1
    Call BetterRollingZ(arr, i)
Next i
End Sub

Sub t_test_button(control As IRibbonControl)
    Call t_test
End Sub

Sub relabel(control As IRibbonControl)
    Call Label_Columns
End Sub

```

### 3. *Resolution\_Tools*

Option Explicit

```

Const c_name As Integer = 1
Const c_roi As Integer = 2
Const c_peakx As Integer = 3
Const c_peaky As Integer = 4
Const c_peakz As Integer = 5
Const c_medz As Integer = 6
Const c_medmax As Integer = 7
Const c_fwhm As Integer = 8
Const c_dlh As Integer = 9
Const c_left As Integer = 10
Const c_right As Integer = 11
Const c_medfwhm As Integer = 12
Const c_meddlh As Integer = 13
Const c_medleft As Integer = 14
Const c_medright As Integer = 15
Const c_status As Integer = 16

```



Const c\_madmax As Integer = 17  
Const c\_madmaxmed As Integer = 18  
Const c\_madl1 As Integer = 19  
Const c\_madl1med As Integer = 20  
Const c\_madl2 As Integer = 21  
Const c\_madl2med As Integer = 22  
Const c\_madr1 As Integer = 23  
Const c\_madr1med As Integer = 24  
Const c\_madr2 As Integer = 25  
Const c\_madr2med As Integer = 26  
Const c\_offset As Integer = 27  
Const c\_offsetstdev As Integer = 28  
Const c\_zmicrons As Integer = 29  
Const c\_zerror As Integer = 30

Const c\_resstatus As Integer = 11  
Const c\_resa As Integer = 12  
Const c\_resaerr As Integer = 13  
Const c\_resb As Integer = 14  
Const c\_resberr As Integer = 15  
Const c\_resx0 As Integer = 16  
Const c\_resx0err As Integer = 17  
Const c\_resy0 As Integer = 18  
Const c\_resy0err As Integer = 19  
Const c\_resrsquare As Integer = 20  
Const c\_resoffset As Integer = 22  
Const c\_resoffsetstdev As Integer = 23  
Const c\_reszmicrons As Integer = 24  
Const c\_reszerror As Integer = 25  
Const c\_resfwhm As Integer = 26  
Const c\_resfwhmerror As Integer = 27  
Const c\_resrollingfwhm As Integer = 28  
Const c\_resrollingstdev As Integer = 29  
Const c\_rescount As Integer = 30  
Const c\_resttest As Integer = 31  
Const c\_ressmoothedfwhm As Integer = 32  
Const c\_ressmoothedcount As Integer = 33

Const c\_graph\_z As Integer = 35  
Const c\_graph\_fwhm As Integer = 36  
Const c\_graph\_smoothedfwhm As Integer = 37

Const c\_resavgz As Integer = 39  
Const c\_resavgfwhm As Integer = 40  
Const c\_resstdevz As Integer = 41  
Const c\_resstdevfwhm As Integer = 42

```
Const c_resminz As Integer = 43
```

```
Const c_resmaxz As Integer = 44
```

```
Const FORMAT_MESSAGE_FROM_SYSTEM = &H1000
```

```
Private Declare Function FormatMessage Lib "kernel32" Alias _  
    "FormatMessageA" (ByVal dwFlags As Long, lpSource As Long, _  
    ByVal dwMessageId As Long, ByVal dwLanguageId As Long, _  
    ByVal lpBuffer As String, ByVal nSize As Long, Arguments As Any) _  
    As Long
```

```
Private Function MessageText(lCode As Long) As String
```

```
    Dim sRtrnCode As String
```

```
    Dim lRet As Long
```

```
    sRtrnCode = Space$(256)
```

```
    lRet = FormatMessage(FORMAT_MESSAGE_FROM_SYSTEM, 0&, lCode, 0&, _  
        sRtrnCode, 256&, 0&)
```

```
    If lRet > 0 Then
```

```
        MessageText = Left(sRtrnCode, lRet)
```

```
    Else
```

```
        MessageText = "Error not found."
```

```
    End If
```

```
End Function
```

```
Sub fruitcake_median(control As IRibbonControl)
```

```
    Dim free_col, i, j, k As Integer
```

```
    Dim processed As Worksheet
```

```
    Set processed = Sheets("Processed")
```

```
    Dim currentUpdating As Boolean
```

```
    currentUpdating = Application.ScreenUpdating
```

```
    Application.ScreenUpdating = False
```

```
    Application.DisplayAlerts = False
```

```
    free_col = processed.UsedRange.Columns.count + 2
```

```
    Cells(1, free_col).Select
```

```
    ActiveCell.value = "binning"
```

```
    Cells(2, free_col).Select
```

```
    ActiveCell.value = "z (microns)"
```

```
    Cells(2, free_col + 1).Select
```

```
    ActiveCell.value = "z avg"
```

```
    Cells(2, free_col + 2).Select
```

```

ActiveCell.value = "z stdev"
Cells(2, free_col + 3).Select
ActiveCell.value = "z error"
Cells(2, free_col + 4).Select
ActiveCell.value = "z error total"
Cells(2, free_col + 5).Select
ActiveCell.value = "FWHM"
Cells(2, free_col + 6).Select
ActiveCell.value = "FWHM stdev"
Cells(2, free_col + 7).Select
ActiveCell.value = "count"

Dim start_row, stop_row, last_row As Integer
Dim low, high As Double
Dim arr As Range
start_row = 3
stop_row = processed.UsedRange.Rows.count
k = start_row
For j = 0 To 150 Step 5
    Cells(k, free_col).value = j

    If j = 0 Then
        low = -100
    Else
        low = j - 2.5
    End If
    If j = 150 Then
        high = 1000
    Else
        high = j + 2.5
    End If

    Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zmicrons))
    Cells(k, free_col + 1).Select
    ActiveCell.Formula = "=GetZAvg(" & arr.Address & "," & low & "," & high & ")"
    Cells(k, free_col + 2).Select
    ActiveCell.Formula = "=GetZStdev(" & arr.Address & "," & low & "," & high & ")"
    Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zerror))
    Cells(k, free_col + 3).Select
    ActiveCell.Formula = "=GetZError(" & arr.Address & "," & low & "," & high & ")"
    Cells(k, free_col + 4).Select
    ActiveCell.Formula = "=iferror(sqrt(" & Cells(k, free_col + 2).Address & "^2 + " &
Cells(k, free_col + 3).Address & "^2)," & Chr(34) & "undefined" & Chr(34) & ")"
    Cells(k, free_col + 5).Select

```

```

        Set arr = ActiveSheet.Range(Cells(start_row, c_medfwhm), Cells(stop_row,
c_zmicrons))
        ActiveCell.Formula = "=GetFWHM(" & arr.Address & "," & low & "," & high &
")"
        Cells(k, free_col + 6).Select
        ActiveCell.Formula = "=GetFWHMStdev(" & arr.Address & "," & low & "," &
high & ")"
        Cells(k, free_col + 7).Select
        Set arr = ActiveSheet.Range(Cells(start_row, c_zmicrons), Cells(stop_row,
c_zmicrons))
        ActiveCell.Formula = "=GetCount(" & arr.Address & "," & low & "," & high & ")"
        k = k + 1
    Next j

    Application.ScreenUpdating = False
    Application.DisplayAlerts = currentUpdating

```

End Sub

Function GetFWHM(arr As Range, low As Double, high As Double)

Dim count As Integer

Dim total As Double

Dim rw As Range

' pull array

total = 0

count = 0

' average of slices in range

Dim i As Integer

Debug.Print Cells(3, c\_zmicrons)

For i = arr.Row To arr.Row + arr.Rows.count - 1

    If Cells(i, c\_zmicrons).value >= low And Cells(i, c\_zmicrons).value < high Then

        total = total + Cells(i, c\_medfwhm).value

        count = count + 1

    End If

Next i

If count < 1 Then

    GetFWHM = "undefined"

Else

    GetFWHM = total / count

End If

End Function

Function GetFWHMStdev(arr As Range, low As Double, high As Double)

Dim count As Integer

Dim total, mean As Double

```

Dim rw As Range

' pull array
total = 0
count = 0
' mean of slices in range
Dim i As Integer
For i = arr.Row To arr.Row + arr.Rows.count - 1
    If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
        total = total + Cells(i, c_medfwhm).value
        count = count + 1
    End If
Next i
If count < 2 Then
    GetFWHMStdev = "undefined"
    Exit Function
End If
mean = total / count
'stdev
total = 0
For i = arr.Row To arr.Row + arr.Rows.count - 1
    If Cells(i, c_zmicrons).value >= low And Cells(i, c_zmicrons).value < high Then
        total = total + ((Cells(i, c_medfwhm).value) - mean) ^ 2
    End If
Next i

    GetFWHMStdev = Sqr(total / (count - 1))
End Function

Sub highlight_outliers_median()
    Dim raw As Worksheet
    Dim rw As Range
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    Set raw = Sheets("Raw")
    For Each rw In raw.UsedRange.Rows
        If Cells(rw.Row, c_status).value <> 0 And IsNumeric(Cells(rw.Row,
c_status).value) Then
            rw.EntireRow.Interior.ColorIndex = 3
        End If
    Next rw

```

```

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Sub

```

```

Sub Label_Columns_Res()
'caption result rows
Cells(2, c_resa).value = "a"
Cells(2, c_resaerr).value = "a err"
Cells(2, c_resb).value = "b"
Cells(2, c_resberr).value = "b err"
Cells(2, c_resx0).value = "x0"
Cells(2, c_resx0err).value = "x0 err"
Cells(2, c_resy0).value = "y0"
Cells(2, c_resy0err).value = "y0 err"
Cells(2, c_resrsquare).value = "rsquare"
Cells(2, c_resoffset).value = "offset"
Cells(2, c_resoffsetstdev).value = "offset stdev"
Cells(2, c_reszmicrons).value = "z"
Cells(2, c_reszerror).value = "z error"
Cells(2, c_resfwhm).value = "FWHM"
Cells(2, c_resfwhmerror).value = "FWHM error"

Cells(2, c_resrollingfwhm).value = "Rolling FWHM"
Cells(2, c_resrollingstdev).value = "Rolling FWHM stdev"
Cells(2, c_rescount).value = "Count"
Cells(2, c_restttest).value = "T"
Cells(1, c_restttest).value = "Fudge"
If (IsEmpty(Cells(1, c_ressmoothedfwhm).value)) Then Cells(1,
c_ressmoothedfwhm).value = 5
Cells(2, c_ressmoothedfwhm).value = "Smoothed FWHM"
Cells(2, c_ressmoothedcount).value = "Smoothed Count"
Cells(2, c_graph_z).value = "Z"
Cells(2, c_graph_fwhm).value = "FWHM"
Cells(2, c_graph_smoothedfwhm).value = "Rolling FWHM"
Cells(1, c_resavgz).value = "Bin size"
Cells(2, c_resavgz).value = "Average Z"
If (IsEmpty(Cells(1, c_resavgfwhm).value)) Then Cells(1, c_resavgfwhm).value = 10
Cells(2, c_resavgfwhm).value = "Average FWHM"
Cells(1, c_resstdevz).value = "Graph from Z"
Cells(2, c_resstdevz).value = "Stdev Z"
If (IsEmpty(Cells(1, c_resstdevfwhm).value)) Then Cells(1, c_resstdevfwhm).value =
0.4
Cells(2, c_resstdevfwhm).value = "Stdev FWHM"
Cells(2, c_resminz).value = "Min Z"
Cells(2, c_resmaxz).value = "Max Z"

```

End Sub

```
Sub MergeCSVs_median(control As IRibbonControl)
    Dim planes, disprange, intradius, medradius, flattop As Integer
    Dim threed As String
    Dim currentUpdating As Boolean
    Dim folderName As Variant
    Dim cell_to_paste_next_dataset As Range
    Dim active_workbook, dataset_workbook As Workbook
    Dim active_sheet As Worksheet
    planes = 0
    disprange = 0
    intradius = 0
    medradius = 0
    flattop = 0
    threed = 0

    'Get folder
    Dim fd As FileDialog
    Set fd = Application.FileDialog(msoFileDialogFolderPicker)
    With fd
        If .Show = -1 Then
            folderName = .SelectedItems.Item(1)
        Else
            Exit Sub
        End If
    End With
    Set fd = Nothing

    Call Setup_Workbook

    'Lists all the files in the current directory
    Set cell_to_paste_next_dataset = Cells(1, 1)
    Set active_workbook = ActiveWorkbook
    Set active_sheet = Sheets("Raw")

    Dim fool As String
    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    Debug.Print (folderName & "/*.csv")
    fool = Dir(folderName & "\\*.csv")
    Dim paste_row As Integer
    paste_row = 1 ' so I don't skip the first row...
```

```

Do While fool <> vbNullString
  Debug.Print fool
  If active_workbook.name <> fool And fool <> "" Then
    Workbooks.Open Filename:=folderName & "\" & fool
    Set dataset_workbook = ActiveWorkbook
    ' valid same parameters before adding!
    If (planes <> 0) Then
      If planes <> Cells(1, 2).value Or _
        disprange <> Cells(1, 4).value Or _
        intradius <> Cells(1, 6).value Or _
        medradius <> Cells(1, 8).value Or _
        flattop <> Cells(1, 10).value Or _
        threed <> Cells(1, 12).value Then
        MsgBox ("File " & fool & " has different processing parameters. Ignoring!")
        fool = Dir
        GoTo OOPS
      End If
    Else
      planes = Cells(1, 2).value
      disprange = Cells(1, 4).value
      intradius = Cells(1, 6).value
      medradius = Cells(1, 8).value
      flattop = Cells(1, 10).value
      threed = Cells(1, 12).value
    End If
    Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
    active_sheet.Activate
    Cells(paste_row, 1).Select
    ActiveSheet.Paste
    dataset_workbook.Close
    paste_row = ActiveCell.SpecialCells(xlLastCell).Row + 1
  End If
OOPS:
  fool = Dir
Loop

' bring in T test chart!
Set active_sheet = Sheets("ASTM")
Debug.Print MyDocsPath & "astm.xlsx"
Workbooks.Open Filename:=MyDocsPath & "astm.xlsx"
Set dataset_workbook = ActiveWorkbook
Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
active_sheet.Activate
Cells(1, 1).Select
ActiveSheet.Paste
dataset_workbook.Close

```



```

paste_row = ActiveCell.SpecialCells(xlLastCell).Row + 1
Sheets("Raw").Activate

'Call highlight_outliers_median
Application.DisplayAlerts = False
Application.ScreenUpdating = currentUpdating
End Sub

Sub prune_median(control As IRibbonControl)
    Dim currentUpdating As Boolean
    Dim source, processing As Worksheet
    Dim i As Integer

    Set source = Sheets("Raw")
    Set processing = Sheets("Processed")

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    source.Activate
    Range(ActiveCell.SpecialCells(xlLastCell), Cells(1)).Copy
    processing.Activate
    Cells(1, 1).Select
    ActiveSheet.Paste

    i = 3
    'remove dupe captions
    Do
        If Cells(i, c_name).value Like "planes" Or Cells(i, c_name).value Like "image
name" Then
            processing.Rows(i).EntireRow.Delete
        Else
            i = i + 1
        End If
    Loop Until i > processing.UsedRange.Rows.count
    i = 3
    'remove non 0 status
    Do
        If Cells(i, c_status).value <> 0 Then
            processing.Rows(i).EntireRow.Delete
        Else
            i = i + 1
        End If
    Loop Until i > processing.UsedRange.Rows.count

```

```

    ' sort ranges
Dim start_row, stop_row As Integer
i = 3
Do
    start_row = i
    stop_row = GetStopRow(start_row)
    i = stop_row + 1

    Debug.Print start_row & " " & stop_row
    With processing.Sort
        .SortFields.Clear
        .SortFields.Add Key:=Range(Cells(start_row, c_medz), Cells(stop_row, c_medz)), _
            SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
        .SetRange Range(Cells(start_row, 1), Cells(stop_row, c_madr2med))
        .Header = xlNo
        .Orientation = xlTopToBottom
        .SortMethod = xlPinYin
        .Apply
    End With
Loop Until i > processing.UsedRange.Rows.count

processing.Activate
Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True

Call stat_columns_median
End Sub

Sub sigmafit(control As IRibbonControl)
    ' copy everything not flagged as bad to sheet 2
    Dim currentUpdating As Boolean
    Dim binning, source, processing As Worksheet
    Dim i As Integer
    Dim sel, arr As Range

    Set source = Sheets("Raw")
    Set processing = Sheets("Processed")
    Set binning = Sheets("Binning")

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False

    source.Activate
    Set sel = Range(ActiveCell.SpecialCells(xlLastCell), Cells(1))
    sel.Copy

```

```

processing.Activate
Range(Cells(1, 1), Cells(sel.Columns.count, sel.Rows.count)).Select
'transpose
Selection.PasteSpecial Paste:=xlPasteAll, Operation:=xlNone, SkipBlanks:= _
    False, Transpose:=True

i = 3
'remove dupe captions
Do
    If Cells(1, i).value Like "planes" Or Cells(1, i).value Like "image name" Then
        processing.Columns(i).EntireColumn.Delete
    Else
        i = i + 1
    End If
    'Debug.Print (i)
Loop Until (i > processing.UsedRange.Columns.count Or IsEmpty(Cells(1, i).value))

'prune beads w/ a bad status
'do nothing for now
i = 3
Do
    If Cells(c_resstatus, i).value = 1 Then
        processing.Columns(i).EntireColumn.Interior.ColorIndex = c_pamdecide
    End If
    i = i + 1
Loop Until (i > processing.UsedRange.Columns.count Or IsEmpty(Cells(1, i).value))

' find range
Dim lastcell As Integer
lastcell = c_resstatus + 1
Do Until IsEmpty(Cells(lastcell, 2).value)
    lastcell = lastcell + 1
Loop

i = 3

'caption result rows
Cells(lastcell + 1, 2).value = "a"
Cells(lastcell + 2, 2).value = "a err"
Cells(lastcell + 3, 2).value = "b"
Cells(lastcell + 4, 2).value = "b err"
Cells(lastcell + 5, 2).value = "x0"
Cells(lastcell + 6, 2).value = "x0 err"
Cells(lastcell + 7, 2).value = "y0"
Cells(lastcell + 8, 2).value = "y0 err"
Cells(lastcell + 9, 2).value = "rsquare"

```

```

Cells(lastcell + 11, 2).value = "offset"
Cells(lastcell + 12, 2).value = "offset stdev"
Cells(lastcell + 13, 2).value = "z"
Cells(lastcell + 14, 2).value = "z error"
Cells(lastcell + 15, 2).value = "FWHM"
Cells(lastcell + 16, 2).value = "FWHM error"

```

```
'run through sigmaplot
```

```

Dim SigmaPlot As Object
Set SigmaPlot = CreateObject("SigmaPlot.Application")
SigmaPlot.Visible = False
Dim Notebook As Object

```

```
On Error GoTo ITBARFED
```

```
Do Until IsEmpty(Cells(c_resstatus + 1, i))
```

```
    If IsEmpty(Cells(lastcell + 2, i)) Then
```

```
        SigmaPlot.Notebooks.Add
```

```
        Set Notebook = SigmaPlot.ActiveDocument
```

```
        'copy row 12 to infinity over
```

```
        Set arr = Range(Cells(c_resstatus + 1, i), Cells(lastcell, i))
```

```
        arr.Select
```

```
        Selection.Copy
```

```
        Notebook.Activate
```

```
        SigmaPlot.ActiveDocument.CurrentDataItem.InsertionMode = True
```

```
        SigmaPlot.ActiveDocument.CurrentDataItem.Paste
```

```
        'run fit
```

```
        Call fitit(lastcell + 1, i, SigmaPlot)
```

```
        Call SigmaPlot.ActiveDocument.Close(False, "")
```

```
    End If
```

```
    i = i + 1
```

```
    Debug.Print "Bead " + Str(i)
```

```
    ' bail every 100
```

```
    If i Mod 100 = 0 Then
```

```
        Call SigmaPlot.Quit
```

```
        Set SigmaPlot = Nothing
```

```
        Set SigmaPlot = CreateObject("SigmaPlot.Application")
```

```
        SigmaPlot.Visible = False
```

```
    End If
```

```
Loop
```

```
'copy back
```

```
'Dim foo()
```

```
'ReDim foo(3)
```

```
'foo(0) = 2
```

```

'foo(1) = 0
'foo(2) = 2
'foo(3) = 3
'SigmaPlot.ActiveDocument.CurrentDataItem.SelectionExtent = foo
'SigmaPlot.ActiveDocument.CurrentItem.Copy
'processing.Cells(lastcell + 2, i).Select
'processing.Paste

'transpose back
processing.Activate
Set sel = Range(ActiveCell.SpecialCells(xlLastCell), Cells(1))
sel.Copy
binning.Activate
Range(Cells(1, 1), Cells(sel.Columns.count, sel.Rows.count)).Select
'transpose
Selection.PasteSpecial Paste:=xlPasteAll, Operation:=xlNone, SkipBlanks:= _
    False, Transpose:=True
Range(Cells(1, c_resstatus + 1), Cells(i, lastcell)).Columns.EntireColumn.Delete

' sort the sheet
Call sortit

' add fwhm formulas

' z microns
Cells(3, c_resstatus + 13).Select
ActiveCell.Formula = "=0.1 * (E3-V3)"
ActiveCell.Interior.ColorIndex = 0
ActiveCell.AutoFill Range(ActiveCell, Cells(binning.UsedRange.Rows.count,
ActiveCell.Column))
'z error
Cells(3, c_resstatus + 14).Select
ActiveCell.Formula = "=SQRT(0.1^2*(1^2 + (W3)^2 + 1^2) + (E3-V3)^2 * 0.001^2)"
ActiveCell.Interior.ColorIndex = 0
ActiveCell.AutoFill Range(ActiveCell, Cells(binning.UsedRange.Rows.count,
ActiveCell.Column))
' fwhm
Cells(3, c_resstatus + 15).Select
ActiveCell.Formula = "=N3*2*SQRT(2*LN(2))*0.1"
ActiveCell.Interior.ColorIndex = 0
ActiveCell.AutoFill Range(ActiveCell, Cells(binning.UsedRange.Rows.count,
ActiveCell.Column))
'fwhm error
Cells(3, c_resstatus + 16).Select
ActiveCell.Formula = "=SQRT((O3*2*SQRT(2*LN(2)))^2+0.001^2)"
ActiveCell.Interior.ColorIndex = 0

```

```
ActiveCell.AutoFill Range(ActiveCell, Cells(binning.UsedRange.Rows.count,
ActiveCell.Column))
```

```
Application.ScreenUpdating = currentUpdating
```

```
Application.DisplayAlerts = True
```

```
On Error GoTo -1
```

```
Exit Sub
```

```
ITBARFED:
```

```
Dim Msg As String
```

```
' If an error occurs, construct an error message.
```

```
On Error Resume Next
```

```
Msg = MessageText(Err.Number)
```

```
MsgBox "Automation Error " & vbCrLf & Err.Number & _  
" (" & Hex(Err.Number) & ")" & vbCrLf & Msg
```

```
' grab a new reference
```

```
Call SigmaPlot.Quit
```

```
'Set SigmaPlot = CreateObject("SigmaPlot.Application")
```

```
On Error GoTo -1
```

```
End Sub
```

```
Sub rollingfwhm(control As IRibbonControl)
```

```
' add the rolling columns to the table and flag the stdev col based on the ASTM table
```

```
Dim currentUpdating As Boolean
```

```
Dim lastcell, i As Integer
```

```
Dim binning As Worksheet
```

```
Set binning = Sheets("Binning")
```

```
currentUpdating = Application.ScreenUpdating
```

```
Application.ScreenUpdating = False
```

```
Application.DisplayAlerts = False
```

```
' find range
```

```
lastcell = c_resstatus + 1
```

```
Do Until IsEmpty(Cells(lastcell, 2).value)
```

```
lastcell = lastcell + 1
```

```
Loop
```

```
lastcell = lastcell - 1
```

```
binning.Activate
```

```
Call Label_Columns_Res
```

```
'Cells(2, c_resrollingfwhm).value = "Rolling FWHM"
```

```
'Cells(2, c_resrollingstdev).value = "Rolling FWHM stdev"
```

```
'Cells(2, c_rescount).value = "Count"
```

```

Cells(2, c_resttest).value = "T"
Cells(1, c_resttest).value = "Fudge"
If (IsEmpty(Cells(1, c_ressmoothedfwhm).value)) Then Cells(1,
c_ressmoothedfwhm).value = 5
Cells(2, c_ressmoothedfwhm).value = "Smoothed FWHM"
Cells(2, c_ressmoothedcount).value = "Smoothed Count"
Cells(2, c_graph_z).value = "Z"
Cells(2, c_graph_fwhm).value = "FWHM"
Cells(2, c_graph_smoothedfwhm).value = "Rolling FWHM"
Cells(1, c_resavgz).value = "Bin size"
Cells(2, c_resavgz).value = "Average Z"
If (IsEmpty(Cells(1, c_resavgfwhm).value)) Then Cells(1, c_resavgfwhm).value = 10
Cells(2, c_resavgfwhm).value = "Average FWHM"
Cells(2, c_resstdevz).value = "Stdev Z"
Cells(2, c_resstdevfwhm).value = "Stdev FWHM"
Cells(2, c_resminz).value = "Min Z"
Cells(2, c_resmaxz).value = "Max Z"

```

```

For i = 3 To lastcell
    Call BetterRollingFWHM(Range(Cells(3, c_reszmicrons), Cells(lastcell,
c_reszmicrons)), i)
Next i

```

```

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
End Sub

```

```

Sub BetterRollingFWHM(arr As Range, ByVal rw As Long)
    Dim i As Integer
    Dim count As Integer
    Dim bins() As Double
    Dim low, high, fudge, tmp As Double
    Dim total, rollingfwhm, rollingStdev, smoothedz, t As Double
    ReDim bins(arr.Rows.count)

```

```

' don't process stuff with not offset stdev
If Cells(rw, c_resoffsetstdev).value = "undefined" Then
    Exit Sub
End If

```

```

low = Cells(rw, c_reszmicrons).value - Cells(rw, c_reszerror).value
high = Cells(rw, c_reszmicrons).value + Cells(rw, c_reszerror).value
rollingfwhm = 0
rollingStdev = 0
count = 0

```

```

t = 0
' count points
For i = arr.Row To arr.Row + arr.Rows.count - 1
    tmp = Cells(i, c_reszmicrons).value
    If tmp >= low And tmp < high Then
        count = count + 1
        bins(count) = Cells(i, c_resfwhm).value
    End If
Next i

' average points
If count > 0 Then
    total = 0
    For i = 1 To count
        total = total + bins(i)
    Next i
    rollingfwhm = total / count
End If
' stdev
If count > 1 Then
    total = 0
    For i = 1 To count
        total = total + (bins(i) - rollingfwhm) ^ 2
    Next i
    rollingStdev = Sqr(total / (count - 1))
    If rollingStdev <> 0 Then
        ' t test
        t = Abs(Cells(rw, c_resfwhm).value - rollingfwhm) / rollingStdev
        If count < 3 Then
            Cells(rw, c_resttest).Interior.ColorIndex = c_dontgraph
        ElseIf count > 147 And t >= Sheets("ASTM").Cells(Application.Min(count, 147)
- 1, 3).value Then
            Cells(rw, c_resttest).Interior.ColorIndex = c_pamdecide
        ElseIf t >= Sheets("ASTM").Cells(Application.Min(count, 147) - 1, 3).value Then
            Cells(rw, c_resttest).Interior.ColorIndex = c_badpoint
        Else
            Cells(rw, c_resttest).Interior.ColorIndex = 0
        End If
    Else
        Cells(rw, c_resttest).Interior.ColorIndex = c_badpoint
    End If
End If
Cells(rw, c_rescount).value = count
Cells(rw, c_resrollingfwhm).value = rollingfwhm
Cells(rw, c_resrollingstdev).value = rollingStdev
Cells(rw, c_resttest).value = t

```



```

If count < 2 Then
    Cells(rw, c_resttest).Interior.ColorIndex = c_dontgraph
End If

fudge = Cells(1, c_ressmoothedfwhm)
count = 0
low = Cells(rw, c_reszmicrons).value - (fudge + Cells(rw, c_reszerror).value)
high = Cells(rw, c_reszmicrons).value + (fudge + Cells(rw, c_reszerror).value)
' count Points
For i = arr.Row To arr.Row + arr.Rows.count - 1
    tmp = Cells(i, c_reszmicrons).value
    If tmp >= low And tmp < high Then
        count = count + 1
        bins(count) = Cells(i, c_resfwhm).value
    End If
Next i
' Average Points
If count > 0 Then
    total = 0
    For i = 1 To count
        total = total + bins(i)
    Next i
    smoothedz = total / count
End If
Cells(rw, c_ressmoothedfwhm).value = smoothedz
Cells(rw, c_ressmoothedcount).value = count
End Sub

Sub sortit()
    Dim i, start_row, stop_row As Integer
    Dim binning As Worksheet

    Set binning = Sheets("Binning")

    ' sort ranges
    i = 3
    Do
        start_row = i
        stop_row = GetStopRow(start_row)
        i = stop_row + 1

        Debug.Print start_row & " " & stop_row
        With binning.Sort
            .SortFields.Clear
            .SortFields.Add Key:=Range(Cells(start_row, 5), Cells(stop_row, 5)), _

```

```

SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
.SetRange Range(Cells(start_row, 1), Cells(stop_row, 21))
.Header = xlNo
.Orientation = xlTopToBottom
.SortMethod = xlPinYin
.Apply
End With
Loop Until i > binning.UsedRange.Rows.count

i = 3
Do
    start_row = i
    stop_row = GetStopRow(start_row)
    i = stop_row + 1
    'offset
    Cells(start_row, c_resstatus + 11).Select
    ActiveCell.Formula = "=GetOffset(" & Range(Cells(start_row, 5), Cells(stop_row,
5)).Address & ")"
    ActiveCell.Interior.ColorIndex = 0
    ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))
    'offset stdev
    Cells(start_row, c_resstatus + 12).Select
    ActiveCell.Formula = "=GetOffsetStdev( " & Range(Cells(start_row, 5),
Cells(stop_row, 5)).Address & _
    ", " & Cells(start_row, c_resstatus + 11).Address(False, True) & ")"
    ActiveCell.Interior.ColorIndex = 0
    ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))

    Loop Until i > binning.UsedRange.Rows.count
End Sub

Sub fitit(rw As Integer, col As Integer, SigmaPlot As Object)
    Dim SigmaPlot As Object
    'Set SigmaPlot = CreateObject("SigmaPlot.Application.1")
    'SigmaPlot.ActiveDocument.CurrentDataItem.Open
    'SigmaPlot.ActiveDocument.NotebookItems.Add (SigmaPlot.CT_GRAPHICPAGE)
    Dim ColumnsPerPlot()
    ReDim ColumnsPerPlot(2)
    ColumnsPerPlot(0) = 0
    ColumnsPerPlot(1) = 0
    ColumnsPerPlot(2) = 31999999
    Dim PlotColumnCountArray()
    ReDim PlotColumnCountArray(0)
    PlotColumnCountArray(0) = 1

```

```

'Call SigmaPlot.ActiveDocument.CurrentPageItem.CreateWizardGraph("Scatter Plot",
"Simple Scatter", "Single Y", ColumnsPerPlot, PlotColumnCountArray, "Worksheet
Columns", "Standard Deviation", "Degrees", 0#, 360#, , "Standard Deviation", True)
'Call SigmaPlot.ActiveDocument.CurrentPageItem.Select(False, -334, -749, -334, -
749)
Dim CurItem As Object
Set CurItem = SigmaPlot.ActiveDocument.CurrentItem
Dim ActiveDoc As Object
Set ActiveDoc = SigmaPlot.ActiveDocument
Call SigmaPlot.Notebooks.Open("C:\Documents and Settings\payoung.ADS\My
Documents\SigmaPlot\SPW11\STANDARD.JFL", ".JFL")
Dim FitFile As Object
Set FitFile = SigmaPlot.Notebooks("C:\Documents and Settings\payoung.ADS\My
Documents\SigmaPlot\SPW11\STANDARD.JFL")
ActiveDoc.Activate
CurItem.IsCurrentItem = True
Dim FitObject As Object
Set FitObject = SigmaPlot.Notebooks("C:\Documents and Settings\payoung.ADS\My
Documents\SigmaPlot\SPW11\STANDARD.JFL").NotebookItems("Gaussian, 4
Parameter")
FitObject.Open
FitObject.DatasetType = 3
FitObject.Variable("x") = "data(1,size(col(1)))"
FitObject.Variable("y") = "col(1)"
FitObject.Run
SigmaPlot.ActiveDocument.NotebookItems("Data 1").Open
SigmaPlot.ActiveDocument.CurrentDataItem.Open
FitObject.OutputReport = False 'false later
FitObject.OutputEquation = False
FitObject.ResidualsColumn = -1
FitObject.PredictedColumn = -1
FitObject.ParametersColumn = -1
FitObject.OutputGraph = False
FitObject.OutputAddPlot = False 'false
FitObject.ConfidenceBands = False
FitObject.ExtendFitToAxes = False
FitObject.AddEquationToTitle = False
FitObject.AddPlotGraphIndex = 0
FitObject.XColumn = -1
FitObject.YColumn = -1
FitObject.ZColumn = -2

Dim Stats As Object
Set Stats = FitObject.FitResults

Cells(rw, col).value = Stats.ParameterRegressionCoefficient("a")

```

```

Cells(rw + 1, col).value = Stats.ParameterStandardError("a")
Cells(rw + 2, col).value = Stats.ParameterRegressionCoefficient("b")
Cells(rw + 3, col).value = Stats.ParameterStandardError("b")
Cells(rw + 4, col).value = Stats.ParameterRegressionCoefficient("x0")
Cells(rw + 5, col).value = Stats.ParameterStandardError("x0")
Cells(rw + 6, col).value = Stats.ParameterRegressionCoefficient("y0")
Cells(rw + 7, col).value = Stats.ParameterStandardError("y0")
Cells(rw + 8, col).value = Stats.RSquare

' Debug.Print "RegrCoeff (a): " + CStr(Stats.ParameterRegressionCoefficient("a")) +
vbCrLf + _
"RegrCoeff (b): " + CStr(Stats.ParameterRegressionCoefficient("b")) + vbCrLf + _
"RegrCoeff (x0): " + CStr(Stats.ParameterRegressionCoefficient("x0")) + vbCrLf + _
"RegrCoeff (y0): " + CStr(Stats.ParameterRegressionCoefficient("y0")) + vbCrLf + _
"rsquare: " + CStr(Stats.RSquare) + vbCrLf + _
"stderr (a): " + CStr(Stats.ParameterStandardError("a")) + vbCrLf + _
"stderr (b): " + CStr(Stats.ParameterStandardError("b")) + vbCrLf + _
"stderr (x0): " + CStr(Stats.ParameterStandardError("x0")) + vbCrLf + _
"stderr (y0): " + CStr(Stats.ParameterStandardError("y0")) + vbCrLf

FitObject.Finish
FitFile.Close (False)
Set FitObject = Nothing
Set FitFile = Nothing
Set Stats = Nothing

End Sub

Sub stat_columns_median()
Dim processed As Worksheet
Dim currentUpdating As Boolean
Dim free_col, start_row, stop_row, i As Integer

currentUpdating = Application.ScreenUpdating
Application.ScreenUpdating = False
Application.DisplayAlerts = False

Set processed = Sheets("Processed")
'Debug.Print processed.UsedRange.Columns.count & ", " &
processed.UsedRange.Rows.count

free_col = processed.UsedRange.Columns.count + 1
Cells(2, free_col).Select
ActiveCell.value = "offset"
Cells(2, free_col + 1).Select

```

```

ActiveCell.value = "offset stdev"
i = 3
Do
    start_row = i
    stop_row = GetStopRow(start_row)
    i = stop_row + 1

    Cells(start_row, free_col).Select
    ActiveCell.Formula = "=GetOffset(" & Range(Cells(start_row, c_medz),
Cells(stop_row, c_medz)).Address & ")"
    ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))
    Cells(start_row, free_col + 1).Select
    ActiveCell.Formula = "=GetOffsetStdev(" & Range(Cells(start_row, c_medz),
Cells(stop_row, c_medz)).Address & "," & _
Cells(start_row, c_offset).Address & ")"
    ActiveCell.AutoFill Range(ActiveCell, Cells(stop_row, ActiveCell.Column))

Loop Until (i > processed.UsedRange.Rows.count Or IsEmpty(Cells(i, 1).value))

free_col = processed.UsedRange.Columns.count + 1
Cells(2, free_col).Select
ActiveCell.value = "z (microns)"
Cells(3, free_col).Select
ActiveCell.Formula = "=0.1 * (" & Cells(3, c_medz).Address(False, True) & "-" &
Cells(3, c_offset).Address(False, True) & ")"
ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

free_col = processed.UsedRange.Columns.count + 1
Cells(2, free_col).Select
ActiveCell.value = "z error"
Cells(3, free_col).Select
ActiveCell.Formula = "=sqrt(0.1^2*(1^2 + (" & Cells(3, c_offsetstdev).Address(False,
True) & ")^2 + 1^2) + (" & _
Cells(3, c_medz).Address(False, True) & "-" & Cells(3, c_offset).Address(False, True)
& ")^2 * 0.005^2)"
ActiveCell.AutoFill Range(ActiveCell, Cells(processed.UsedRange.Rows.count,
ActiveCell.Column))

Application.DisplayAlerts = False
Application.ScreenUpdating = currentUpdating
End Sub

Sub BinResZ(arr As Range)
    Dim binsize, i, j, count As Integer
    Dim avgz, avgfwhm, maxz, minz, stdevz, stdevfwhm, totalz, totalfwhm As Double

```

Dim kill As Range

count = 3

binsize = Cells(1, c\_resavgfwhm).value

' idiot check

If binsize < 1 Or IsEmpty(Cells(1, c\_resavgfwhm).value) Then

    MsgBox "Error: Number of beads must be greater than 0"

    Exit Sub

End If

' kill it with fire!

Set kill = Range(Cells(3, c\_resavgz), Cells(65536, c\_resmaxz))

kill.ClearContents

For i = arr.Row To arr.Row + arr.Rows.count - 1 Step binsize

    ' determine we have enough points

    For j = 0 To binsize - 1

        If IsEmpty(Cells(i + j, c\_graph\_z)) Then

            Exit Sub

        End If

    Next j

    ' find averages

    avgz = 0

    avgfwhm = 0

    totalz = 0

    totalfwhm = 0

    maxz = -999999

    minz = 999999

    For j = 0 To binsize - 1

        totalz = totalz + Cells(i + j, c\_graph\_z).value

        totalfwhm = totalfwhm + Cells(i + j, c\_graph\_fwhm).value

        If Cells(i + j, c\_graph\_z).value > maxz Then

            maxz = Cells(i + j, c\_graph\_z).value

        End If

        If Cells(i + j, c\_graph\_z).value < minz Then

            minz = Cells(i + j, c\_graph\_z).value

        End If

    Next j

    avgz = totalz / binsize

    avgfwhm = totalfwhm / binsize

    stdevz = 0

    stdevfwhm = 0

    totalz = 0

    totalfwhm = 0

    If binsize > 1 Then

        For j = 0 To binsize - 1

```

        totalz = totalz + (Cells(i + j, c_graph_z).value - avgz) ^ 2
        totalfwhm = totalfwhm + (Cells(i + j, c_graph_fwhm).value - avgfwhm) ^ 2
    Next j
    stdevz = Sqr(totalz / (binsize - 1))
    stdevfwhm = Sqr(totalfwhm / (binsize - 1))
End If
'report
Cells(count, c_resavgz).value = avgz
Cells(count, c_resavgfwhm).value = avgfwhm
Cells(count, c_resstdevz).value = stdevz
Cells(count, c_resstdevfwhm).value = stdevfwhm
Cells(count, c_resminz).value = minz
Cells(count, c_resmaxz).value = maxz
count = count + 1
Next i
End Sub

```

```

Sub graphres(control As IRibbonControl)
    Dim arr As Range
    Dim dst, xaxis, fwhm As Range
    Dim current, i, start_row, stop_row As Long
    Dim zlimit As Double
    Dim currentUpdating As Boolean

    currentUpdating = Application.ScreenUpdating
    Application.ScreenUpdating = False
    Application.DisplayAlerts = False
    'Application.EnableEvents = False

    Dim binning As Worksheet

    Set binning = Sheets("Binning")
    binning.Activate

    'copy
    current = 3
    stop_row = ActiveSheet.UsedRange.Rows.count
    For i = 3 To stop_row
        If (Cells(i, c_resttest).Interior.ColorIndex < 1 Or Cells(i,
c_resttest).Interior.ColorIndex = c_dontgraph) Then
            Cells(current, c_graph_z).value = Cells(i, c_reszmicrons).value
            Cells(current, c_graph_fwhm).value = Cells(i, c_resfwhm).value
            Cells(current, c_graph_smoothedfwhm).value = Cells(i,
c_ressmoothedfwhm).value
            current = current + 1
        End If
    Next i
End Sub

```

```

Next i
Set xaxis = Range(Cells(3, c_graph_z), Cells(stop_row, c_graph_z))
Set fwhm = Range(Cells(3, c_graph_fwhm), Cells(stop_row, c_graph_fwhm))
Set dst = Range(Cells(3, c_graph_smoothedfwhm), Cells(stop_row,
c_graph_smoothedfwhm))
Set arr = Range(Cells(3, c_graph_smoothedfwhm), Cells(stop_row,
c_graph_smoothedfwhm))

stop_row = current

'sort
With ActiveSheet.Sort
.SortFields.Clear
.SortFields.Add Key:=Range(Cells(3, c_graph_z), Cells(stop_row, c_graph_z)), _
SortOn:=xlSortOnValues, Order:=xlAscending, DataOption:=xlSortTextAsNumbers
.SetRange Range(Cells(3, c_graph_z), Cells(stop_row, c_graph_smoothedfwhm))
.Header = xlNo
.Orientation = xlTopToBottom
.SortMethod = xlPinYin
.Apply
End With

' find start_row based on Z criteria!
start_row = 3
' idiot check
If Not IsNumeric(Cells(1, c_resstdevfwhm).value) Or IsEmpty(Cells(1,
c_resstdevfwhm).value) Then
MsgBox "Error: Graph from Z must be a number!"
Exit Sub
End If
zlimit = Cells(1, c_resstdevfwhm).value
For start_row = 3 To stop_row
If Cells(start_row, c_graph_z).value >= zlimit Then
Exit For
End If
Next start_row

'generate extra averaged stuff
Debug.Print "Start row " & start_row
Set arr = Range(Cells(start_row, c_graph_smoothedfwhm), Cells(stop_row,
c_graph_smoothedfwhm))
Call BinResZ(arr)

'graph

Dim CHObj As MyChartObject

```



```

Set CHObj = New MyChartObject
Set CHColl = New Collection

Range(Cells(start_row, c_graph_z), Cells(stop_row,
c_graph_smoothedfwhm)).Activate
ActiveSheet.Shapes.AddChart(Excel.XlChartType.xlXYScatter).Select
Set CHObj.CO = ActiveChart
Debug.Print ActiveChart.name
CHColl.Add Item:=CHObj, Key:=ActiveChart.name

Set xaxis = Range(Cells(start_row, c_graph_z), Cells(stop_row, c_graph_z))
Set fwhm = Range(Cells(start_row, c_graph_fwhm), Cells(stop_row, c_graph_fwhm))
Set dst = Range(Cells(start_row, c_graph_smoothedfwhm), Cells(stop_row,
c_graph_smoothedfwhm))

'ActiveChart.SeriesCollection.NewSeries
ActiveChart.SeriesCollection(1).name = ""FWHM""
ActiveChart.SeriesCollection(1).XValues = xaxis
ActiveChart.SeriesCollection(1).Values = fwhm
'ActiveChart.SeriesCollection.NewSeries
ActiveChart.SeriesCollection(2).name = ""smoothed Z""
ActiveChart.SeriesCollection(2).XValues = xaxis
ActiveChart.SeriesCollection(2).Values = dst

ActiveChart.SeriesCollection(1).Select
With Selection
    .MarkerStyle = xlMarkerStyleDiamond
    .MarkerSize = 2
End With
ActiveChart.SeriesCollection(2).Select
With Selection
    .MarkerStyle = 1
    .MarkerSize = 2
End With
ActiveChart.Axes(xlCategory).MinimumScale = 0
Dim offset As Integer
offset = ActiveChart.Parent.Top + ActiveChart.Parent.Height + 50

' chart 2.0
Set CHObj = New MyChartObject
Set CHColl = New Collection

Range(Cells(3, c_graph_z), Cells(stop_row, c_graph_smoothedfwhm)).Activate
ActiveSheet.Shapes.AddChart(Excel.XlChartType.xlXYScatter).Select
Set CHObj.CO = ActiveChart

```

```

Debug.Print ActiveChart.name
CHColl.Add Item:=CHObj, Key:=ActiveChart.name

ActiveChart.SeriesCollection(1).name = """"FWHM""""
ActiveChart.SeriesCollection(1).XValues = xaxis
ActiveChart.SeriesCollection(1).Values = fwhm

Set xaxis = Range(Cells(3, c_resavgz), Cells(Range(Cells(65536,
c_resavgz).Address).End(xlUp).Row, c_resavgz))
Set dst = Range(Cells(3, c_resavgfwhm), Cells(Range(Cells(65536,
c_resavgfwhm).Address).End(xlUp).Row, c_resavgfwhm))

ActiveChart.SeriesCollection(2).name = """"averaged Z""""
ActiveChart.SeriesCollection(2).XValues = xaxis
ActiveChart.SeriesCollection(2).Values = dst

ActiveChart.SeriesCollection(1).Select
With Selection
    .MarkerStyle = xlMarkerStyleDiamond
    .MarkerSize = 2
End With
ActiveChart.SeriesCollection(2).Select
With Selection
    .MarkerStyle = 1
    .MarkerSize = 2
End With
ActiveChart.Axes(xlCategory).MinimumScale = 0
ActiveChart.Parent.Top = offset

Application.ScreenUpdating = currentUpdating
Application.DisplayAlerts = True
Application.EnableEvents = False
End Sub

Sub relabelres(control As IRibbonControl)
    Call Label_Columns_Res
End Sub

```

## VIII. REFERENCES

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## CURRICULUM VITAE

Pamela Anne Young

### **Education:**

Indiana University, Indianapolis, Indiana  
Ph.D. Biomolecular Imaging and Biophysics 2010  
Dissertation: *The Effects of Refractive Index Mismatch on Multiphoton Fluorescence Excitation Microscopy of Biological Tissue*  
Committee Chair and Advisor: Kenneth W. Dunn

Indiana University, Bloomington, Indiana  
Bachelors of Science: Physics - Graduation with Departmental Honors 2003  
Bachelors of Science: Mathematics - Minor in Astronomy/Astrophysics 2003  
*General Honors Notation*

### **Research Experience:**

**Ph.D.**

**2004-2010**

**Indiana University  
Indianapolis, IN**

- Established a protocol to evaluate the quality of a microscope system with respect to the point spread function, resolution, and fluorescence signal with imaging depth of the microscope.
- Established a protocol for live animal imaging of the rat kidney using multiphoton microscopy, requiring absolutely no movement by the animal to acquire quantitative point spread function data.
- Established a protocol for aligning the two-photon excitation path added to an Olympus Fluoview 1000 microscope housed by the Indiana Center for Biological Microscopy. This protocol included the installation of a collimator/beam expander to fill the back aperture of the microscope objective.
- Small animal surgery skills include anesthesia, physiological monitoring, cannulation of carotid artery, femoral vein, and tail vein, exposure of kidney through left lateral flank incision, euthanasia by overdose, exsanguinations, and bilateral pneumothorax.
- Digital image analysis experience includes MetaMorph, ImageJ, and Voxx software.
- Additional experience includes colocalization techniques, fluorescence recovery after photobleaching (FRAP), fluorescence resonance energy transfer (FRET), fluorescence life time imaging, fluorescence loss in photobleaching (FLIP), and measuring flow rates using fluorescence microscopy.

**Related Experience:**

**Animal Technician**

**Indiana University School of Medicine**

**2008**

**Indianapolis, IN**

- Zebrafish husbandry.
  - Responsible for several large aquarium units housing several hundred zebrafish.
  - Monitor zebrafish health within the Institutional Animal Care and Use Committee (IUCAC) guidelines.

**Scientist /Quality Control**

**Polymer Technology Systems, Inc.**

**2003-2004**

**Indianapolis, IN**

- Assembled experimental strips, performed blood testing on strips, recorded and wrote up results.
- Tested meters, checked incoming and outgoing shipments, and checked returned goods.

**Laboratory Assistant**

**Indiana University Cyclotron Facility**

**2002-2003**

**Bloomington, IN**

- Calibration team for the STAR Endcap Electromagnetic Calorimeter project.
  - This project brought together groups from around the country to design and build an electromagnetic calorimeter for the Solenoidal Tracker (STAR) detector on Brookhaven National Laboratory's Relativistic Heavy Ion Collider (RHIC).
- Assembled splitter boxes, fiber optic cables, and detector boxes for calibration system.
- Attached fiber optics to connectors, sanded and polished connectors, scribed fiber optics, attached fiber optics to fiber routing layers.
- Labeled PMT boxes and fibers.
- Contributed to installing the detector at BNL.

**Undergraduate Assistant**

**WonderLab Museum of Science, Health & Technology**

**2002-2003**

**Bloomington, IN**

- Designed and fabricated the lobby exhibit "Cosmic Dance," 5 floor panels that light up when a cosmic ray passes through, for WonderLab Museum
  - The detector consists of 2 scintillation panels held in parallel under a glass floor panel, each with a fiber optic routed within the panel then out to a photomultiplier tube.
  - The electronics were designed to turn on light bulbs under the glass floor panel whenever a signal was detected simultaneously in the top and bottom scintillator panels.
- Wrote a detailed account of the design of this system and turned in for my senior thesis earning honors in physics.

**Undergraduate Intern**

**Indiana University Mathematics Department**

**2001-2003**

**Bloomington, IN**

- Taught students in one-on-one and group environments.
- Provided general assistance to professor.

### **Grants and Awards:**

NIH George M. O'Brien Award (P30 DK 079312-01)	2005-2010
Microscopy Society of America Presidential Award	2009
Indiana Microscopy Society Student Travel Award	2009
SPIE Education Scholarship in Optical Science and Engineering	2008
Educational Enhancement Grant	2008
Indiana University-Purdue University Indianapolis	
1 <sup>st</sup> Place Student Presenter	2007
at Joint Local Affiliate Societies	
of the Microscopy Society of America Meeting	

### **Publications:**

Young, P. A., S. G. Clendenon, J. M. Byars, R. S. Decca, K. W. Dunn. *The Effects of Spherical Aberration on Multiphoton Fluorescence Excitation Microscopy*. Journal of Microscopy, 2010 (submitted).

Young, P. A., S. G. Clendenon, J. M. Byars, K. W. Dunn. *The Effects of Refractive Index Heterogeneity within Kidney Tissue on Multiphoton Fluorescence Excitation Microscopy*. Journal of Microscopy, 2010 (submitted).

Young, P.A., S.G. Clendenon, K.W. Dunn. *Practical Limitations in Intravital Multiphoton Microscopy of the Kidney*, in Proceedings of Microscopy and Microanalysis 2009, Richmond, VA, USA, July 26-30, 2009.

Muriello\*, P.A., S. G. Clendenon, K.W. Dunn. *The Effects of Refractive Index Mismatch on Signal and Resolution in Multiphoton Microscopy*, in Proceedings of Microscopy and Microanalysis 2008, Albuquerque, NM, USA, August 3-7, 2008.

Muriello\*, P.A., K.W. Dunn. *Improving Signal Levels in Intravital Multiphoton Microscopy using an Objective Correction Collar*. Optics Communications, Volume 281, Issue 7, 1 April 2008, Pages 1806-1812.

Dunn, K.W. and P.A. Young, *Principles of multiphoton microscopy*. Nephron Exp Nephrol, 2006. 103(2): p. e33-40.

Miller, Michael A., Pamela A. Young, S.K. Hekmatyar, Navin Bansal, Gary D. Hutchins. *Registration of High Resolution Small Animal PET, CT and MR Images*. Poster Presentation, 2005.

\*married name

**Professional Development:**

Microscopy Society of America	2006-present
Optical Society of America	2005-present
SPIE (Society of Photo-optical Instrumentation Engineers)	2007-present
Indiana Microscopy Society	2004-2010
• Student Representative to Executive Council	2006-2010
Graduate Student Organization	2007-2009
Indiana University Purdue University-Indianapolis	
Graduate Student Organization-Indiana University School of Medicine	
• President	2007-2009
• Biophysics Representative	2004-2010
Underrepresented Professional and Graduate Student Organization	2006-2010
Campus Center Advisory Board	2008-2009
Indiana University Physics and Astronomy Society	2000-2003
Sigma Pi Sigma	2003-present
Society of Physics Students	2000-2003
Indiana University Math Club	2000-2003